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Keywords: traumatic brain injury (TBI); PEG-bis-AA/HA-DXM hydrogel; dexamethasone; secondary injury; cognitive function recovery



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## Article

# Point of Injury Treatment with Hydrogel Containing Dexamethasone Improves Cognitive Function and Reduces Secondary injury Response After TBI

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## Abstract

Functional recovery after traumatic brain injury (TBI) is hindered by progressive neurodegeneration resulting from neuroinflammation and other secondary injury. Dexamethasone (DX), a synthetic glucocorticoid, has been shown to reduce inflammation, but its systemic administration can cause a myriad of other medical issues. We aim to provide a local, sustained treatment of DX for TBI. We demonstrated that PEG-bis-AA/HA-DXM hydrogels composed of polyethyleneglycol-bis-(acryloyloxy acetate) (PEG-bis-AA) and dexamethasone-conjugated hyaluronic acid (HA-DXM) reduced secondary injury and motor functional recovery at 7 days post injury (DPI) in a rat moderate controlled cortical impact (CCI) TBI model. In this study, we evaluated the effect of PEG-bis-AA/HA-DXM hydrogel on cognitive function and secondary injury at 14 DPI. Immediately after injury, hydrogel was placed on a injured brain and cognitive function was evaluated by Morris Water Maze test and secondary injury was evaluated by histological analysis. The hydrogel treatment groups demonstrated a decreased time to find hidden platform (target), distance to swim to target, and percent time to swim in border compared to TBI untreated rats on both training period and the probe test. We also observed reduced lesion volume and inflammatory response and apoptosis in hydrogel treatment groups compared to the untreated TBI group.

**Keywords:** Traumatic brain injury (TBI); PEG-bis-AA/HA-DXM hydrogel; Dexamethasone; Secondary injury; Cognitive function recovery

## 1. Introduction

Traumatic brain injury (TBI) is a two faceted injury. After the initial trauma on the brain, the secondary injury is elicited by a severe inflammatory response and breakdown of the blood brain barrier (BBB) that leads to continued damage to the tissue. The progression of the secondary injury manifest as altered motor, sensory or cognitive skills or psychological changes [1–3]. One clinical study reported 30% of patients who receive a moderate to severe injury became worse in the following 5 consecutive years post injury [4]. Lifelong cost associated with TBI total approximately \$76.5 billion in direct and indirect expenses [5]. Moderate to severe TBIs result in hospitalization where patients are monitored for intracranial pressure, blood flow, and excitotoxicity. Surgical interventions include removing blood clots, decompressive craniectomy, implantation of monitoring device and/or implantation of ventriculoperitoneal shunts to relieve pressure. Currently there is no established drug therapy targeting the underlying progressive pathophysiology damage in TBI, but

symptoms are managed through use of steroids, anti-anxiety, anticoagulants, anticonvulsants, antidepressants, diuretics, muscle relaxants or stimulants [6,7]. Current preclinical research is focused on diminishing the inflammatory reaction initiated by the secondary injury.

Preclinical therapies for TBI focus to reducing the deleterious effects of the inflammatory reaction in the microenvironment [7]. The secondary injury is characterized by the breakdown of the BBB, infiltration and activation of monocytes/macrophages, inflammation, axonal injury, apoptosis, and activation of glial cells [8,9]. After injury the BBB increases permeability and facilitates infiltration of pro-inflammatory phenotypic monocytes/macrophages [9,10]. Astrocytes, a type of glial cell, rapidly activate by upregulating the expression of glial fibrillar acidic protein (GFAP), an intermediate filament protein, and form a barrier that limits neurotrauma by preserving neuronal synapses, reduce the spread of inflammatory cytokines, reduce excitotoxicity and supports the recovery of the extracellular matrix [10–16]. Activation of astrocytes leaded to the formation of glial scar which causes detrimental effects such as reduced neuronal plasticity, inhibition of axonal extension, decreased ability for regeneration with the release of inhibitory growth molecules such as chondroitin and keratan sulfate proteoglycans, and the promotion of cytotoxic edema [10–12,17–20]. By 10-14 days-post-injury (DPI) there is a decrease in the number of infiltration of macrophages and number of activated astrocytes at the site of injury, but the detrimental results from the glial scar can be observed [8,21–23]. It is notable that multiple studies have shown that blocking macrophage entry and eliminating astrocyte activity completely after injury did not improve neurological outcomes [8,16,24]. This leads to the potential for anti-inflammatory therapeutics in the acute phase to limit activation of glial cells and modulate the molecular components of injury induced inflammation [24,25]. Assessment of remaining tissue during this resolution phase can indicate the ramifications of acute neuroinflammation and effectiveness of treatments [26].

Dexamethasone, a synthetic glucocorticoid steroid, has previously been investigated to limit the neuroinflammatory reaction from TBI [27,28]. Several studies indicate the potential to decrease pro-inflammatory cytokine expression, reduce neuronal damage, and decrease activation of astroglia [29,30]. Unfortunately, systemic administration of high doses required for therapeutic effect negatively impact multiple organs and organ systems [31]. Furthermore, when used to treat TBI patients clinically, there was an observed significant increase in risk of infection, chance of disability and mortality rate [32–34].

To overcome the severe side effects associated with high dose systemic administration of DX, we developed a polyethylene glycol-bis-acryloyloxy acetate (PEG-bis-AA) hydrogel for local and sustained delivery of dexamethasone (DX) and reported that PEG-bis-AA/HA-DXM hydrogel treated animals exhibited significantly improved motor function by rotarod test and cognitive function by Morris water maze test compared to untreated TBI animals and reduced inflammatory response, apoptosis, and lesion volume compared to untreated TBI animals at 14 DPI in a rat mild controlled cortical impact (CCI) TBI model [36, 39]. We also reported that PEG-bis-AA/HA-DXM hydrogel treatment can improve motor function and inhibits secondary injury in a rat moderate CCI TBI model (35). It was observed that hydrogel treatment attenuated lesion volume, GFAP expression, apoptosis, and macrophages infiltration and increased neuronal survival and M2 macrophages in a rat moderate CCI TBI model at 7 DPI (Acute injury phase). These results suggest that local and sustained release of DX hydrogels can improve recovery in moderate TBI, likely through a reduction in secondary injury. In this study, we evaluated PEG-bis-AA/HA-DXM hydrogel treatment on cognitive function recovery by Morris Water Maze (MWM) test and secondary injury by histological analysis at 14 DPI (Chronic injury phase) in a rat moderate CCI TBI model.

## 2. Materials and Methods

### 2.1. PEG-Bis-AA/HA-DXM Hydrogel Preparation

PEG-bis-AA/HA-DXM hydrogels were prepared as previously described [35,36, 39]. Briefly, PEG-bis-AA and HA-DXM were dissolved in Dulbecco's phosphate buffer saline (PBS) without  $\text{Ca}^{++}$

and Mg<sup>+</sup> and to a final concentration of 6% (w/v) and 0.72% w/v, respectively. Irgacure 2959 (I-2959, 10% (w/v) dissolved in ethanol) was added for a final concentration of 0.1% w/v. Hydrogel discs were photopolymerized between two coverslips separated by 0.5 mm spacers using low intensity UV light (365 nm, 10 mW/cm<sup>2</sup>, Black-Ray B100-AP, Upland, CA, USA) for 5 minutes per side (16 µL of PEG-bis-AA/HA-DXM macromer solution/ gel). PEG-bis-AA/HA-DXM hydrogels were 5 mm diameter, 0.5 mm thick and contain 3 µg of DX/hydrogel. Hydrogels were stored in PBS at 4°C overnight before tested for therapeutic efficacy in moderate TBI model.

## 2.2. Animal Care and Surgical Procedure

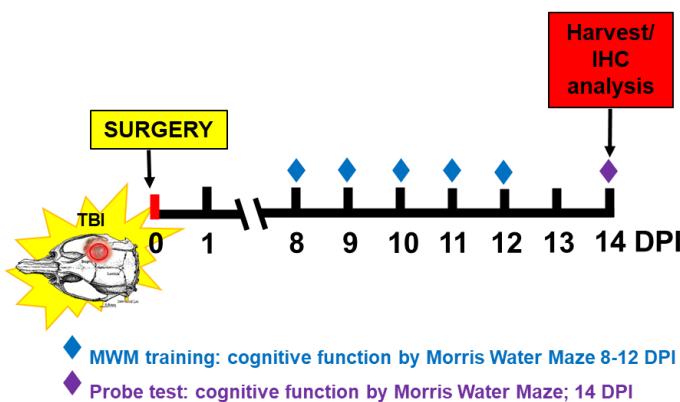
Twenty Male Sprague Dawley rats (8-9 weeks, Charles River, Wilmington, MA) between 290-350 g were randomly assigned to one of three groups: 1) Normal group: no surgery, 2) Untreated TBI group, and 3) PEG-bis-AA/HA-DXM gel treated group (3 µg of DX/hydrogel). Rats were housed in 12-hour light/dark cycle in Godley-Snell Research Center (GSRC) at Clemson University (animal use protocol 2020-047). All animal care, maintenance and experimental procedures were approved by the Institutional Animal Care and Use Committee (IACUC) of Clemson University.

Generation of the moderate CCI injury models in rats was performed as described in our previous publication [35]. Briefly, rats were anesthetized using an intraperitoneal (IP) injection of ketamine (80 mg/kg) and xylazine (10 mg/kg). The head was secured in a stereotaxic frame (David Kopf Instruments, Tujunga, CA) and the surgical area was scrubbed with alcohol and betadine. Under aseptic conditions, a midline incision was performed and the skull was cleared of connective tissue. A 6 mm craniectomy was performed using a trephine burr, over the right hemisphere (midpoint 3.0 mm lateral, 1.0 mm caudal to bregma) without disruption of the dura. A moderate CCI injury was generated using a TBI impactor (Precision Systems and Instrumentation) armed with a 5 mm blunt end tip at the set velocity of 4 m/sec, a depth of 2.5 mm below the surface of the parietal cortex, dwell time of 250 msec [35]. A polypropylene ring (approximately 7 mm in diameter, 3.5 mm in height) was secured using acrylic resin (Ortho-Jet BCA, Lang Dental Manufacturing Company, Inc) to frame the craniectomy site and maintain gel positioning. Hydrogels were placed on the top of injured cortex. The incision site was sutured using 4-0 vicryl suture and the rats were recovered.

## 2.3. Cognitive Function by Morris Water Maze (MWM) Test

MWM test was performed from 8 DPI after the incision had healed. MWM test was comprised of 4 trials per day over a 5-day training period with a final “probe test” at 14 DPI (Scheme 1).

A circular pool (183 cm diameter) filled with water was maintained at 25°C and located in a dimly lit room. Non-toxic black paint, Prang (Dixon Ticonderoga company, FL, USA) was added to the water to make it dark and opaque. To evaluate spatial learning and memory function, visual cues are placed around the pool within the line of sight of the rats. A circular platform (15 cm diameter) was placed in a fixed location in the pool (south-west quadrant, SW) and submerged 2 cm below the water surface. Training began at 8 DPI and were continued for 5 consecutive days (4 acquisition trials/day). For each trial, the rat was released from a randomized starting point (north-west (NW), north (N), north-east (NE), east (E), south-east (SE)) facing the side of the pool. Rats were allowed to find the hidden platform within 60 seconds. If the rat found the platform, the rat would remain on the platform for 10 sec before being placed in its home cage. If the rat failed to find the platform within 60 sec, the rat was guided to the platform and allowed 10 sec to remain on the platform. During the trials, the swim paths were recorded using a video tracking system (SMART, Panlab, Harvard Apparatus) and the searching time to find the platform was recorded. For the probe test, the target platform was removed from the tank and the time required for rats to find platform and stay on the platform 1 second was recorded as a latency time. Video recording and analysis was performed using the PanLab SMART 3.0 software. [37,38].



**Scheme 1.** Experimental design of cognitive function and histological outcomes.

#### 2.4. Tissue Harvest and Histology Preparation

Brain tissue was harvested at 14 DPI after MWM test. Before sacrifice, rats were deeply sedated with an IP injection of EUTHASOL® (150mg/Kg pentobarbital sodium, Virbac, Westlake, TX). A midline thoracotomy was performed, and the rats were transcardially perfused with ice cold 0.9% saline to remove blood followed by cold 4% paraformaldehyde solution (PFA). Brain was isolated and post-fixed in PFA for 24 hours at 4°C. The isolated brains were rinsed using PBS before saturating in increasing concentration of sucrose (10, 20, and 30 % in PBS). Saturated brains were stored in 4°C until ready for sectioning. Cryosectioning was performed on a Leica CM cryostat (CM1950, Leica Biosystems, Buffalo Grove, IL). Brains were removed from 30% sucrose and rinsed in PBS before embedded in TrekTissue OCT compound (Fisher HealthCare, REF 4585, Huston, TX). Tissue was flash frozen in Freeze-It (Fisher Scientific, Kalamazoo, MI) and allowed to be at -20°C for two hour before sectioning. Coronal sections were made at 30  $\mu$ m thickness and stored in cryoprotectant (30% sucrose, 1% polyvinylpyrrolidone, and 30% ethylene glycol in 1X PBS) at -20 °C until ready for histological analysis.

#### 2.5. Histological Analysis

##### 2.5.1. Lesion Volume Analysis

Lesion volume was determined using Nissl staining of sequential sections at 0.36 mm intervals within the lesion. Brain sections were washed in three changes of 0.1 M PBS, mounted on charged slides, and left to air dry overnight. The next day sections washed in two changes of DI H<sub>2</sub>O before stained in 1% cresyl violet for 5 minutes. The stained sections were then dehydrated in increased concentrations of alcohol (50, 70, 90 100%) before the tissue was optically cleared in xylene, coverslipped with dibutylphthalate polystyrene xylene (DPX) mounting media (Electron Microscopy Science, Hatfield, PA) and allowed to cure at room temperature. Brightfield images were taken using the 10X objective on a Keyence All-in-One fluorescence microscope (Keyence BZ-X810, Osaka, Japan). Using ImageJ open source software the area of lesion per section was measured and the total volume of the brain lesion was determined using Cavalieri's equation of approximation [39].

##### 2.5.2. Inflammatory Response and Astrogliosis by Immunohistochemistry

To evaluate the effect of PEG-bis-AA/HA-DXM hydrogel on macrophage infiltration, astrogliosis, and neuron cell survival at 14 DPI, IHC staining was performed as previously described in our previous publication [35]. Briefly, sections were identified at the epicenter and +/-0.72 mm, +/-2.44 mm, +/-2.26 mm and +/-2.98 mm to the epicenter (total 9 sections/rat; Normal n= 5; TBI (untreated) n = 9; TBI + PEG-bis-AA/HA-DXM n = 8). Free floating sections were washed in three changes of 0.1M PBS before blocking in 0.1% Tween 20 (BP337-500, Fisher Chemical, Waltham, MA), 1% BSA (Rockland antibodies & assays, Limerick, PA), and 4 % normal goat serum (ab7481, Abcam,

Cambridge, MA) for 1 hour at room temperature. The sections were permeabilized in PBST (PBS + 0.1% Tween 20) before overnight incubation at 4°C in primary antibody solution (PBST with 1% BSA) rocking. Primary antibodies included Anti-GFAP antibody targeting glial fibrillary acidic protein in astrocytes (ab7260, Abcam, Cambridge, MA), Anti-NeuN antibody, clone A60 targeting neuronal cells (MAB 377, Millipore Sigma, Temecula, CA), Anti-Macrophage/monocyte antibody, clone ED1 (MAB1435, Millipore Sigma, Temecula, CA); and ARG1/Arginase 1 Antibody (E-2) (SC-271430, Santa Cruz Biotechnology, Santa Cruz, CA). Double staining was performed with GFAP (1:500 dilution) / NeuN (1:200 dilution) and ED1 (1:200 dilution, monocyte/macrophage marker) / Arg1 (1:250 dilution, M2 phenotype marker). The following day, sections washed in PBST before incubated for 2 hours at room temperature in secondary antibody solution (PBST supplemented with 1 % BSA). Secondary antibodies were AF488 conjugated goat anti-rabbit (1:250, A-11008, ThermoFisher Scientific, Rockford, IL) and Cy3 conjugated goat anti-mouse (1:200, 115-165-003, Jackson Immuno Research, West Grove, PA). After incubation, the sections were washed with 2 changes of PBST, a final wash with 0.1 M PBS, before coverslipped with VECTASHIELD Vibrance antifade mounting media with DAPI (H-1800, ThermoFisher Scientific, Eugene, OR). Images were taken of the perilesional cortex (using 10X objective) using Keyence BX-810 All- in -One fluorescence microscope. Analysis was performed using ImageJ. ED1<sup>+</sup> and Arg1<sup>+</sup> cells were identified with the DAPI overlay and normalized to area (mm<sup>2</sup>). NeuN positive cells were identified using a DAPI overlay and reported as a percentage of DAPI. GFAP expression was analyzed as fluorescent intensity and normalized to the corresponding location on an uninjured brain.

### 2.5.3. Apoptosis by TUNEL Assay

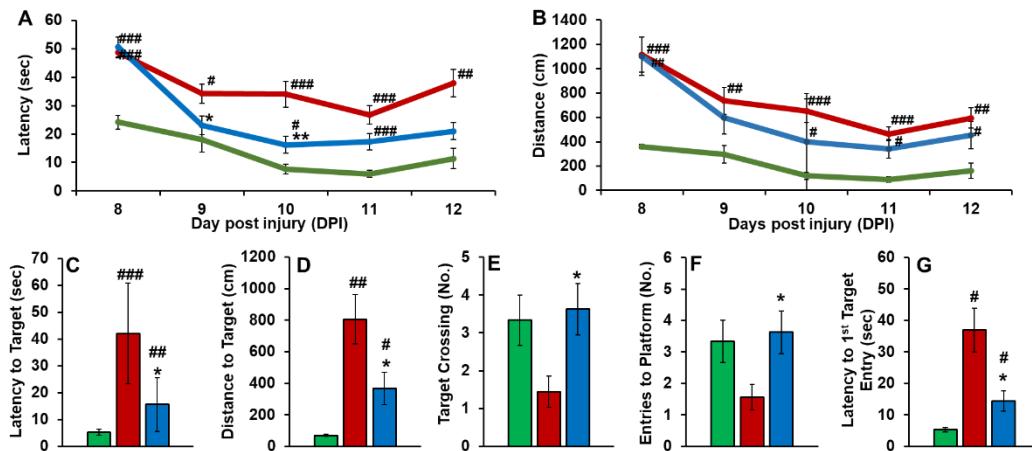
Apoptotic cells were detected using a ApopTag ® Plus Fluorescein In Situ Apoptosis detection kit (S7111, Millipore) for terminal deoxynucleotidyl transferase dUTP nick-end (TUNEL) labeling at 14 DPI (Scheme 1). Sections were again identified at the epicenter, +/-0.72 mm, +/-2.44 mm, +/-2.26 mm and +/-2.98 mm to the epicenter (total 9 sections/rat) and mounted to silane coated slides (63411-01, Electron Microscopy Science, Hatfield, PA). Sections were washed in 3 changes of 0.1 M PBS. Staining for cell death was carried out according to the manufacturer's specifications using material provided in their kit.

Briefly, sections were post-fixed for 5 minutes in pre-cooled (-20°C) ethanol: acetic acid solution (2:1 solution), before washed with PBST 3 changes for 5 minutes each. Sections were treated with the equilibration buffer and incubated with TdT enzyme diluted in primary antibody dilutant (PBST with 1% BSA) solution (7:3 dilution) at 37°C for 1 hour. Following incubation, the sections were submerged in stop/wash buffer for 10 minutes and washed with PBS. The fluorescein-labeled anti-digoxigenin conjugate was applied and allowed to incubate for 30 minutes at room temperature protected from light. The slides were washed in PBS before coverslipped with VECTASHIELD Vibrance antifade mounting media with DAPI (H-1800, ThermoFisher Scientific, Eugene, OR). The perilesional cortex was imaged using a Keyence BX-810 fluorescence microscope with the 10X objective. TUNEL<sup>+</sup> identified using the DAPI overlay and results are presented as percent TUNEL<sup>+</sup> cells.

## 3. Results

### 3.1. PEG-Bis-AA/HA-DXM Improves Cognitive Function

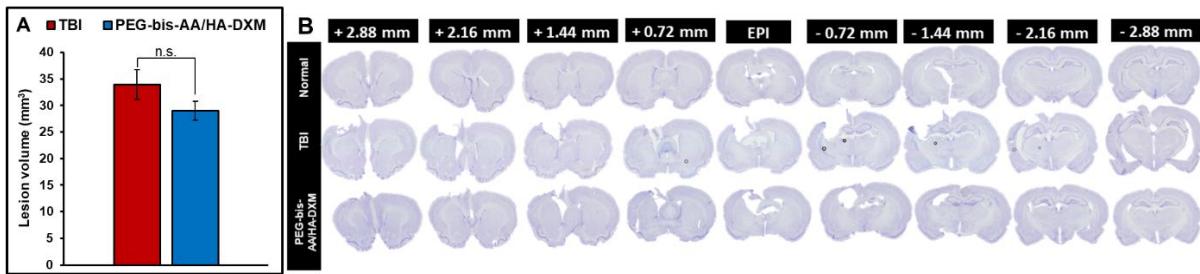
The effect of PEG-bis-AA/HA-DXM on cognitive function recovery was evaluated by MWM test. During the training days, PEG-bis-AA/HA-DXM treated rats showed decreased time to find the hidden target (Figure 1A) and decreased distance to find hidden target (Figure 1B) compared to that in untreated TBI group. For the probe test on 14 DPI, PEG-bis-AA/HA-DXM treated rats showed significantly shorter latency to target (Figure 1C), decreased distance to find the hidden target (Figure 1D), increased number of target crossings (Figure 1E), increased number of entry to the platform zone (Figure 1F), and decreased latency to 1st entry of target zone (Figure 1G) compared to those in untreated TBI rats, respectively.



**Figure 1.** Effect of PEG-bis-AA/HA-DXM on cognitive function by MWM test. During training period (A-B): A) Latency to target; B) Distance to target; For Probe test (C-G): C) Latency to target, D) Distance to target, E) number of Target crossing, F) Number of entry, G) Latency to 1<sup>st</sup> entry. Data presented mean +/- SEM. Normal group (n=3), TBI untreated group (n=9), and PEG-bis-AA/HA-DXM gel treated group (n=8); \*p < 0.05 ; \*\*p < 0.01; \*\*\*p < 0.001 compared to Normal, \* p < 0.05 ; \*\* p < 0.01; \*\*\* p < 0.001 compared to TBI.

### 3.2. PEG-bis-AA/HA-DXM reduces lesion volume

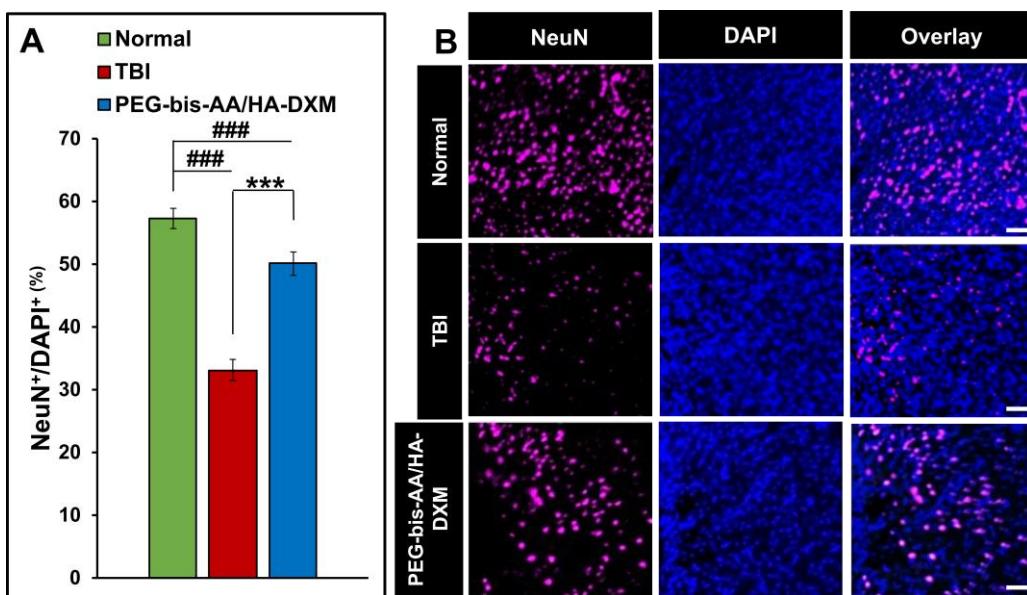
The effect of PEG-bis-AA/HA-DXM hydrogel treatment on lesion volume was determined using cavalier's formula of approximation based on area of lesion on serial sections. PEG-bis-AA/HA-DXM hydrogel treatment groups showed slightly decreased lesion volume compared to that in TBI untreated group even though it was not significantly different (Figure 2).



**Figure 2.** Effect of PEG-bis-AA/HA-DXM on lesion Volume by Nissl stain. A) Average lesion volume calculated by Cavalieri's approximation (n=19 Sections/ rat). Data presented mean +/- SEM TBI untreated group (n=9), and PEG-bis-AA/HA-DXM hydrogel treated group (n=8). B) Representative images of Nissl stained sections in various groups.

### 3.3. PEG-bis-AA/HA-DXM Improves Neuronal Cell Survival

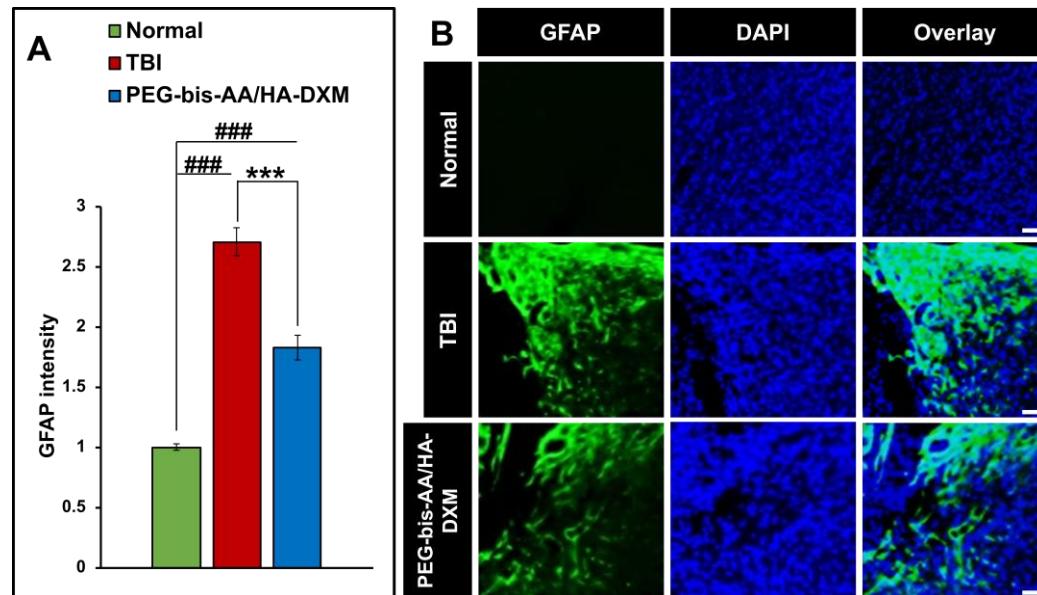
The effect of PEG-bis-AA/HA-DXM on neuronal cell survival was evaluated by IHC using antibody against NeuN. The percentage of NeuN<sup>+</sup> cells in PEG-bis-AA/HA-DXM treated groups was significantly increased compared to that in untreated TBI group (p <0.001) (Figure 4A). Figure 4B shows the representative images of NeuN<sup>+</sup> cells in various groups.



**Figure 3.** Effect of PEG-bis-AA/HA-DXM hydrogel on neuronal survival by NeuN staining. A) % NeuN<sup>+</sup> cells normalized number of total cells (DAPI<sup>+</sup>). Data presented mean +/- SEM TBI untreated group (n=9), and PEG-bis-AA/HA-DXM gel treated group (n=8); # p < 0.001 compared to Normal; \*\*\* p < 0.001 compared to TBI. B) Representative images of NeuN<sup>+</sup> cells in various groups. Scale bar = 500  $\mu$ m.

### 3.4. PEG-bis-AA/HA-DXM Reduces Astrogliosis

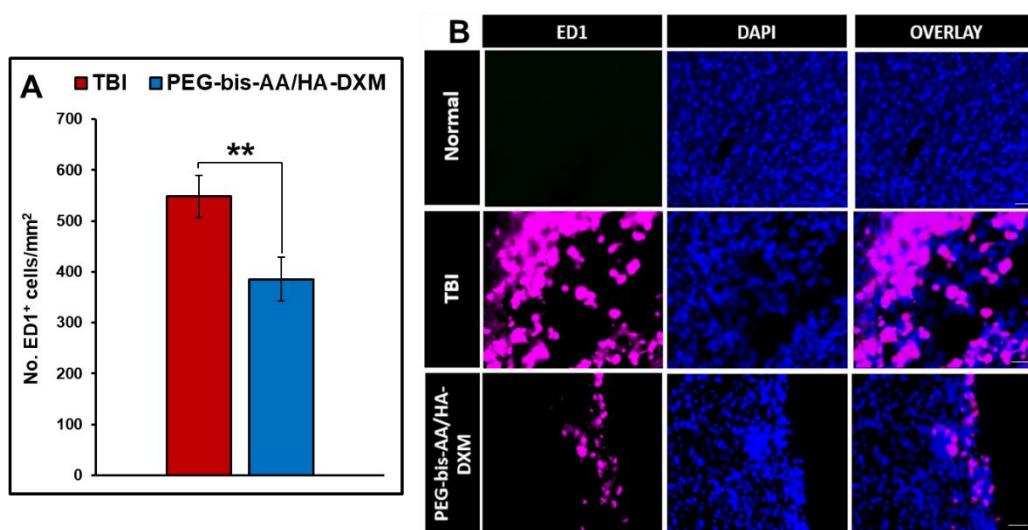
The effect of PEG-bis-AA/HA-DXM hydrogel treatment on astrogliosis was evaluated by intensity of GFAP<sup>+</sup> cells on the stained sections. We observed that PEG-bis-AA/HA-DXM hydrogel treated group showed significantly lower intensity of GFAP<sup>+</sup> cells compared to that in the untreated TBI group (Figure 4).



**Figure 4.** Effect of PEG-bis-AA/HA-DXM hydrogel on astrogliosis. A) GFAP intensity normalized to area (mm<sup>2</sup>). Data presented mean +/- SEM. TBI untreated group (n=9), and PEG-bis-AA/HA-DXM gel treated group (n=8); ###p < 0.001 compared to normal; \*\*\*p < 0.001 compared to TBI. B) Representative images of GFAP<sup>+</sup> cells in various groups. Scale bar = 500  $\mu$ m.

### 3.5. Effect of PEG-bis-AA/HA-DXM on Inflammatory Responses

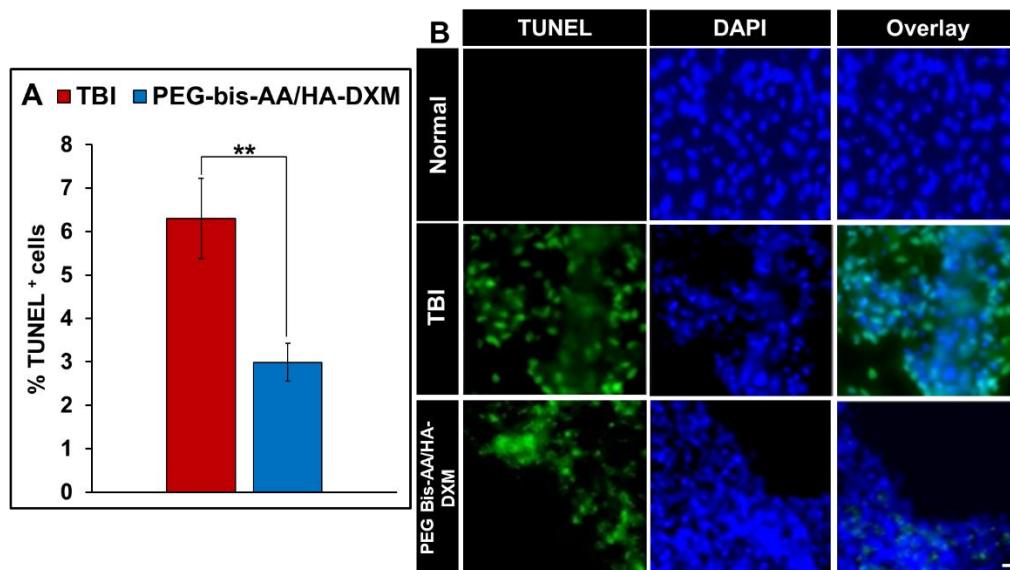
The effect of PEG-bis-AA/HA-DXM on inflammatory response was evaluated by IHC using antibody against ED1. The number of ED1+ cells in PEG-bis-AA/HA-DXM hydrogel treated groups showed significantly decreased compared to that in untreated TBI group ( $p < 0.01$ ) (Figure 5A). Figure 5B shows representative images of ED1+ cells in various groups.



**Figure 5.** Effect of PEG-bis-AA/HA-DXM on inflammatory responses. A) Number of ED1+ cells normalized to area ( $\text{mm}^2$ ) and B) representative images of ED1+ cells in various groups. Scale bar = 500  $\mu\text{m}$ . Data presented mean +/- SEM. TBI untreated group ( $n=9$ ), and PEG-bis-AA/HA-DXM gel treated group ( $n=8$ ); \*\* $p < 0.01$  compared to TBI.

### 3.6. Effect of PEG-bis-AA/HA-DXM on Apoptosis

The effect of PEG-bis-AA/HA-DXM on apoptosis was evaluated by TUNEL staining. The percentages of TUNEL + cells in PEG-bis-AA/HA-DXM hydrogel treatment group was significantly decreased compared to that in untreated TBI group ( $P < 0.01$ ) (Figure 6A). Figure 6B shows representative images of TUNEL+ cells in various groups.



**Figure 6.** Effect of PEG-bis-AA/HA-DXM on apoptosis. A) % TUNEL<sup>+</sup> cells. Data presented mean +/- SEM TBI untreated group (n=9), and PEG-bis-AA/HA-DXM gel treated group (n=8); \*\* p < 0.01 compared to TBI. B) Representative image of TUNEL<sup>+</sup> cells (Green) in various groups. Scale bar = 500  $\mu$ m.

#### 4. Discussion

TBI worsens progressively over the time in addition to mechanical primary injury due to secondary injury including edema, inflammation, astrogliosis, oxidative stress, and excitotoxicity. One of major neuronal cell death after TBI is neuroinflammation and many preclinical research focuses on minimizing the damage from the inflammatory reaction [7,40]. Glucocorticoid including dexamethasone are potent anti-inflammatory drugs and dexamethasone have showed promising results in decreasing proinflammatory cytokine expression, reducing histological markers for neurotrauma and strengthening the BBB through interaction with tight junction proteins, adherens junction and tissue inhibitors of metalloproteinases in preclinical studies [29,30,41–45]. Conversely, the high systemic doses of dexamethasone showed a high mortality rate and severe deleterious side effects which has effectively decreased enthusiasm in steroid treatment for TBI in clinical studies [32]. In addition, other studies using higher dose of DX administered resulted in aggravation of cognitive function impairment by MWM compared to TBI (untreated) [56,57] intraperitoneally Zhang et al., treated CCI TBI rats with high dose DX for 7 consecutive days (10 mg/kg for the first three days, 5 mg/kg on day 4, 2 mg/kg on day 5–6 and 1 mg/kg on day 7) and reported that aggravated the neurological and spatial learning impairment induced by TBI [56]. Chen et al., reported that TBI rats received high dose of DX (0.5–10 mg/kg) showed increase neuronal apoptosis in hippocampus and aggravate retrograde memory deficits induced by TBI [57].

In our previous published works, we demonstrated that local and sustained delivery of low dose DX (3  $\mu$ g /rat) by PEG-bis-AA/HA-DXM hydrogel can improve motor and cognitive function and reduce secondary injury in a rat mild CCI TBI model [36, 39]. We also demonstrated that local and sustained delivery of DX by PEG-bis-AA/HA-DXM hydrogel can improve motor function and reduce secondary injury at 7 DPI (acute phase injury) in a rat moderate CCI TBI model (ref). In this study, we evaluated the therapeutic efficacy of PEG-bis-AA/HA-DXM hydrogel on cognitive function and secondary injury at 14 DPI (Chronic injury phase) in a rat moderate CCI TBI model. We observed a decrease in latency to target and distance to target in PEG-bis-AA/HA-DXM hydrogel treatment over the training days when compared to TBI untreated. Increased visuospatial pattern recognition decreases latency to target and distance to target indicating a potential increase in recovery in the treatment group [37]. On 9, 10, and 11 DPI of training the group treated with PEG-bis-AA/HA-DXM indicated a faster latency to find hidden platform compared to the TBI untreated group (Figure 1A). This observation was also seen on 12 DPI (final day of training) when comparing distance traveled between PEG-bis-AA/HA-DXM hydrogel treated and untreated rats. During the probe test, hydrogel treatment group had a significantly decreased latency to target and distance to target, and an increase in number of target crossing (Figure 1C-D). These results are similar to those using this hydrogel treatment in a mild CCI model [39] and indicated local low dose DX treatment by hydrogel as an effective therapeutic strategy for the TBI repair.

After cognitive function testing at 14 DPI, we investigated the effect of PEG-bis-AA/HA-DXM on secondary injury by histological analysis. We first observed that lesion volume was decreased in hydrogel treated group compared to that in untreated TBI group even though it was not significantly different (Figure 2). In our previous study, we observed a significant decrease in the lesion volume at 7DPI in moderate CCI TBI model [35]. In our other previous study in a rat mild injury model, we observed that significant decrease in lesion volume at 7 DPI, while a non-significant decrease at 14 DPI [36,39]. This indicated the hydrogel treatment may show higher impact in acute phase more than chronic phase.

For the neuronal survival, we observed that hydrogel treated groups showed a significantly higher percentage of NeuN<sup>+</sup> cells compared to that in untreated TBI group (Figure 3). This suggests a neuroprotective characteristic of PEG-bis-AA/HA-DXM hydrogel and this result is consistent with

our previous study in a mild CCI TBI model for neuroprotective effect of PEG-bis-AA/HA-DXM hydrogel [39].

Increased astrocytes activation after injury can lead to glial scar formation that reduce neuronal plasticity and function [22,58]. Although there are benefits of gliosis in the acute phase, reducing the global astrocytic activity in acute phases may increase regenerative properties of the tissue long term [14–16,59]. In moderate TBI, astrocyte activity begins to resolve at 14 DPI time point [22]. The PEG-bis-AA/HA-DXM hydrogel treated group showed a significantly reduced fluorescent intensity by GFAP+ cells compared to that in untreated TBI group (Figure 4). This result was consistent with the results we observed at 7 DPI in the moderate injury model [35]. We think that reduction in astrocyte activity in the early days could lead to greater synaptic plasticity in the area that could indicate further recovery or ability to recover functional activity in the tissue.

We also observed the number of ED1<sup>+</sup> cells in the PEG-bis-AA/HA-DXM hydrogel treatment group was significantly lower compared to that in untreated TBI group (Figure 5). This result is also consistent with our previous study in a mild CCI injury model in which there is a significant decrease in ED1<sup>+</sup> cells at 14 DPI [39]. We believe that local sustained delivery of low dose dexamethasone by hydrogel can reduce the number of infiltration of macrophages in the lesion site and can be potential therapy for TBI [10,12,64].

Apoptosis is one of key features of secondary injury and continues due to prolonged neuroinflammation [61–63]. We evaluated the effect of PEG-bis-AA/HA-DXM hydrogel treatment on apoptosis. We observed that significant decrease in TUNEL<sup>+</sup> cells in PEG-bis-AA/HA-DXM treatment group compared to that in the untreated TBI group (Figure 6). Additionally, this significant decrease was also observed in our previous published studies in which there is a significant decrease in TUNEL<sup>+</sup> cells at 7 DPI time point [35] in the moderate injury model as well as at 7 and 14 DPI in the mild injury model [36,39]. This suggests our PEG-bis-AA/HA-DXM hydrogel treatment has a strong neuroprotective efficacy against the apoptotic pathway after TBI.

In summary, we observed many benefits of PEG-bis-AA/HA-DXM hydrogel treatment on increasing neuronal survival, decreasing neuroinflammation, and improving cognitive function recovery in a rat moderate injury model. We also have observed improved motor functional recovery and reduced secondary injury at 7 DPI in a rat moderate injury model [35]. The key findings of this study and our previous published studies are summarized in Table I. Overall, the results perpetuated the continued interest in the clinical potential of PEG-bis-AA/HA-DXM hydrogel for TBI.

**Table 1.** Key findings from PEG-bis-AA/HA-DXM hydrogel treatment on functional recovery and secondary injury observed in a rat mild and moderate CCI TBI model.

Assessment	MILD TBI		Moderate TBI	
	7DPI	14 DPI	7DPI	14 DPI
Lesion volume	↓	↓	↓	↓
Macrophage / Microglia	↓	↓	↓	↓
Reactive gliosis (GFAP)	↓	N/A	↓	↓
Apoptosis	↓	↓	↓	↓
Inflammatory gene expression	↓	↓	N/A	N/A
Neuronal cell survival	↑	↓	↑	↑
Motor function	↑	N/A	↑	N/A
Cognitive Function	N/A	↑	N/A	↑

**Note:** Histological, molecular and functional outcomes from PEG-bis-AA/HA-DXM hydrogel treatment relative to untreated TBI group at 7 DPI [36] and 14 DPI [39] in a rat mild TBI model and 7 DPI [35] and 14 DPI in a rat moderate TBI model. Changes in each outcome assessment within each individual study are indicated as statistical significance (thick arrows), qualitative or not statistically significant (Thin arrows or n.s.), and or not assessed (N/A).

## 5. Conclusions

We observed an increase in cognitive function recovery as determined by MWM test. Through histological analysis, we observed a significant decrease in macrophage infiltration, astrogliosis, apoptosis, and an increase in neuronal survival. These results support previous observations obtained in a rat mild CCI injury model and at 7 DPI in a rat moderate CCI TBI model. These findings support the continued development of PEG-bis-AA/HA-DXM hydrogel as a local sustained treatment of low dose dexamethasone after TBI.

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## Abbreviations

The following abbreviations are used in this manuscript:

TBI	Traumatic Brain Injury
DX	Dexamethasone
PEG-bis-AA	Polyethylene glycol-bis-(acryloyloxy acetate)
HA-DXM	Dexamethasone-conjugated hyaluronic acid
CCI	Controlled cortical impact
BBB	Blood brain barrier
GFAP	Glial fibrillar acidic protein
NeuN	Neuronal nuclei
DPI	Days-post-injury
MWM	Morris water maze
IHC	Immunohistochemistry
PBS	Phosphate buffer saline
ECM	Extracellular matrix
IACUC	Institutional Animal Care and Use Committee
IP	Intraperitoneal
PFA	Paraformaldehyde
DI H <sub>2</sub> O	Deionized H <sub>2</sub> O
DPX	Dibutylphthalate polystyrene xylene
BSA	Bovine serum albumin
TUNEL	Terminal deoxynucleotidyl transferase dUTP nick-end

DAPI 4',6-diamidino-2-phenylindole

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