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Article

The Effect of Ageing on Phase Transformations and Nanoindentation Behaviour in Ni-Rich NiTi Alloys.

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Abstract: In the article, the results of research on a NiTi alloy with a high nickel content (51.7 at.%), produced using the additive technology SLM method and subjected to isothermal aging after solution annealing, are presented. The study involved the determination of the sequence of phase transformations occurring using differential scanning calorimetry (DSC), and the determination of the temperature range of these transformations. In parallel, the phase composition was determined using the XRD method; hardness and the Young's modulus were also determined. The analysis of the DSC results obtained indicates the following characteristic features of the NiTi alloy, which change with ageing time: (1) during cooling (from +150°C to -50°C), the type of transformation changes from a one-step transformation after solution annealing to a two-step transformation after the ageing process over 1, 20 and 100 hours at 500°C; (2) during heating (from -50°C to +150°C) for all the samples, regardless of the ageing time, only a one-step transformation from martensite M(B19') to austenite A(B2) is observed; (3) the temperature at which the transformation starts increases with the ageing time, (4) the width of the total temperature range of the transformation M(B19') → A(B2) during heating changes from large ($\Delta T=49.7^\circ\text{C}$), after solution annealing, to narrow ($\Delta T=19.3^\circ\text{C}$ and $\Delta T=17.9^\circ\text{C}$ after 20 h and 100 h of ageing) and, most importantly, (5) a comparison with literature data shows that, irrespective of the composition of the NiTi alloy and the manufacturing technology of the alloy samples (regardless of the fact whether this was traditional or additive technology), a sufficiently long ageing process period leads to the occurrence of the *martensite* → *austenite* transformation in the same temperature range.

Keywords: NiTi; phase transformation; additive manufacturing; SLM; solution annealing; aging

1. Introduction

Additive technologies are increasingly used in the manufacture of a wide variety of parts, from aerospace applications to biomedical engineering. They are used to produce complex, non-standard elements that would be labour-intensive to produce using traditional methods. In the area of biomedical engineering, it is anticipated that additive manufacturing (AM) will have a revolutionary impact on the manufacture of implants and tissue engineering structures, resulting in a personalised approach to regenerative medicine that is tailored to the individual patient. [1–6]. In the aeronautical and aerospace sectors, they are used to manufacture lightweight and high-strength components that meet stringent safety standards [8,9]. Additive technologies are evolving and they create opportunities for applications in new areas. Their flexibility, fast operation and ability to create non-standard components make them highly effective technologies. One example is the increasing use of

additive technologies to produce components in NiTi alloy (nickel-titanium alloys—Nitinol), characterised by unique thermo-mechanical properties. 3D printing of NiTi alloy components opens the way to more advanced applications in various industries and biomedical engineering [10–14]. However, there are also technical challenges associated with 3D printing of NiTi alloys, such as control of the microstructure and mechanical properties, which require further research and technological development.

One of the phenomena that occur during the additive manufacturing of Nitinol products using the SLM method is the loss of nickel in the matrix [15–20] due to its evaporation. The loss is dependent on the process parameters and results in a temperature shift of the martensite \rightarrow austenite transformation towards higher temperatures, compared to transformations in the output powder. Hence, it is of key importance to establish the relationship between the SLM process parameters and the amount of evaporated nickel. Independently, the loss of nickel can be controlled in the matrix, and thus influence the temperature changes of phase transformations, by applying an appropriate post-process heat treatment. The treatment results in a separation of nickel-enriched secondary phases, such as Ni_4Ti_3 , for example, resulting in a reduction in the nickel content of the matrix [20–27]. Even a small fluctuation of 0.1 at.% in the composition of the alloy can significantly change the onset and end temperatures of phase transformations, which in turn determines the potential for the use of Nitinol in various smart structures in a wide range of industries and in biomedicine [28,29]. In other words, by controlling the composition of the alloy and its microstructure, it is possible to influence its functional temperatures, ones which determine the shape memory effect and the superelasticity of the alloy.

Nevertheless, the relationship between the nickel and titanium content in the output powder, the 3D printing process parameters and post-process heat treatment parameters, and the temperature at which phase transformations occur, as well as their sequence of occurrence, combined with the achievement of optimal mechanical properties of these alloys for a given application, still require intensive research. This paper presents studies that contribute to this important research area, carried out on NiTi alloy samples that are rich in Ni (51.7 at.% Ni), produced by means of additive technology using the SLM method. In particular, the relationship between the post-process heat treatment time and the martensite/austenite phase transformation temperature was investigated. The accompanying changes in hardness and the Young's modulus were also investigated.

2. Materials and Methods

2.1. Material

Ni-Ti powder with the following composition: Ni (51.7 at.%) and Ti (48.3 at.%) was supplied by BIMO TECH Sp. z o.o. The purpose of selecting the chemical composition of the powder, characterised by an excess of nickel, was to study the effect of the separation of secondary phases, as a result of heat treatment after the SLM process, on the change in phase transformation temperatures and on the change in hardness and the Young's modulus.

Independently, the elemental composition of the alloy was determined using the EDX method, i.e., energy dispersive X-ray spectrometry (EDX), carried out using a JEOL SEM LV 5500 scanning electron microscope and, in parallel, through a phase composition analysis using the XRD method. In addition, the temperature ranges of the phase transformations were determined by differential scanning calorimetry (DSC), covering the onset and end temperatures of the austenitic transformation: $[A_s, A_f]$, the onset and end temperatures of the intermediate transformation, i.e., the R phase: $[R_s, R_f]$, and the onset and end temperatures of the martensitic transformation: $[M_s, M_f]$.

2.2. SLM Process

The samples were produced using an ORLAS CREATOR® machine (O. R. Lasertechnologie GmbH, Dieburg, Germany) for selective laser melting (SLM). In the SLM method, the coating arm spreads a layer of powder on the working platform. The laser beam scans the surface of the layer according to a computer model. An appropriate selection of the process parameters allows a specific

volume of the powder to be completely melted. The cycle is repeated until a complete component is obtained. In the SLM process, the printing environment is an important factor. To prevent oxidation of the material melted, the working chamber must be filled with a protective gas [30,31]. In this case, argon was used. Residual oxygen levels in the working chamber ranged from 0.05% to 0.1%. The post-production sample preparation included mechanical removal of supports and ultrasonic cleaning in distilled water.

2.3. Methods of Sample Characterisation

2.3.1. Density

The density of the samples was measured using the Archimedes method and the relative density was calculated from the formula: $q_r = q_e / q_t$, where q_r is relative density, q_e is experimental density and q_t is theoretical density of 6.50 g/cm³.

2.3.2. Differential Scanning Calorimetry, DSC

The DSC thermal method was used to determine phase transformation temperatures. The tests were carried out using a Netzsch DSC Polyma 214 device in argon atmosphere. The thermal cycling range tested was from -50°C to +150°C, and from +150°C to -50°C, maintaining a heating/cooling rate of 10°C/min.

2.3.3. Phase Analysis

The phase composition of the NiTi samples was determined by X-ray diffraction (XRD) in the Bragg-Brentano geometry, using an Empyrean diffractometer (Malvern Panalytical, UK) with a Cu-K α radiation source ($\lambda = 1.5406 \text{ \AA}$). The HighScore Plus software was used to analyse the diffractograms obtained, linked to the ICDD PDF 4+ 2023 diffraction image database.

2.3.4. Sample Morphology

The morphology of the samples after the process was observed using a ThermoFisherDualBeam SCIOS II scanning electron microscope with an ETD secondary electron detector and a TEM to THEMIS microscope with a Field Emission Gun (FEG) electron source. The observations were carried out in a scanning-transmission mode (STEM) and TEM.

2.3.5. Hardness and Young's Modulus

The indentation measurements were carried out using a G200 nanoindenter from KLA-Tencor Corporation, fitted with a Berkovich diamond indenter. Load and indentation depth curves were obtained in a linear load growth mode. The loading and unloading times of the indenter during the measurement were 90 s. The tip radius of the Berkovich indenter was 0.2 μm . Calibration was carried out on fused silica. The hardness and Young's modulus values were determined from indentation curves using the Oliver-Pharr model.

3. Results

3.1. Powder Characteristics

3.1.1. Morphology

The surface morphology of the powders is shown in Figure 1. As can be seen, the powders are characterised by almost spherical shapes with diameters in the range of 20-60 μm .

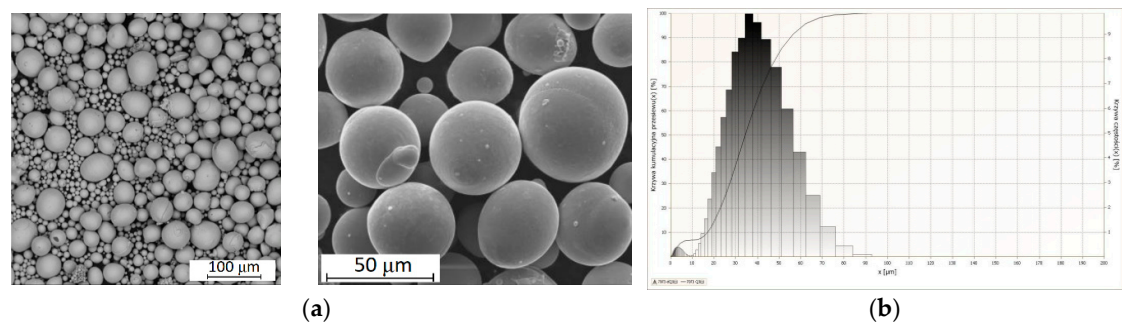


Figure 1. Powder morphologies and distribution: (a) powder morphology; (b) powder distribution.

3.1.2. Elemental Composition

The elemental composition determined using the EDX method (Figure 2) is consistent with the powder supplier’s certification.

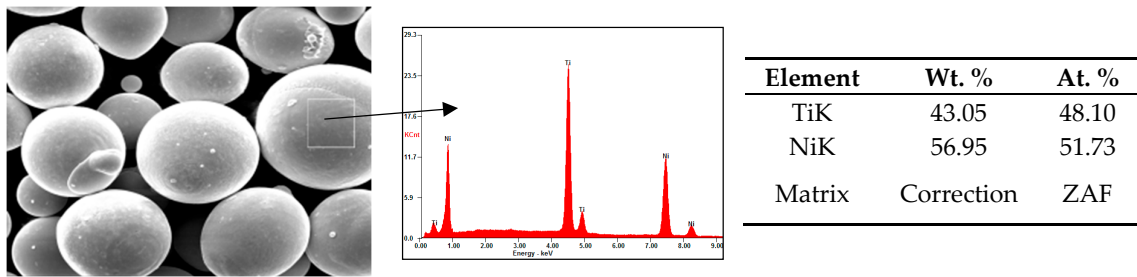


Figure 2. Elemental composition of powder determined using EDX method.

In addition, the investigations of the phase composition using the XRD method (Section 3.1.3) and the phase transformation temperatures determined (Section 3.1.2) using differential scanning calorimetry qualitatively confirm the elemental composition of the powder. According to the literature [32], the powder with the elemental composition specified by the supplier, examined at room temperature using XRD, should possess an austenitic structure. Indeed, the analysis of the XRD diffractogram shown in Figure 3 confirms this phase structure of the powder. Also, the austenite/martensite and martensite/austenite phase transformations take place at temperatures below 0°C (Figure 4), which is a characteristic property of the alloy with the elemental composition specified by the supplier.

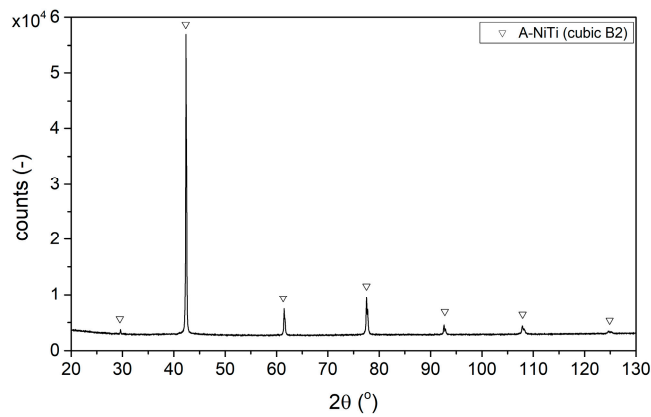


Figure 3. X-ray diffraction pattern observed in raw powder (A-austenite).

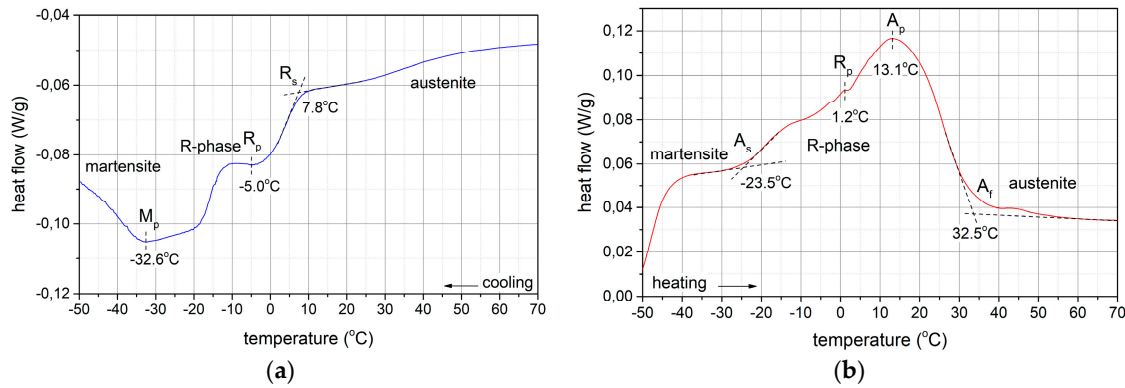


Figure 4. DSC (Differential Scanning Calorimetry) curves of raw powder.

3.1.3. Phase Structure

The phase composition studies of the NiTi powder were carried out using X-ray diffraction method in the Bragg-Brentano geometry using a Cu-K α radiation source ($\lambda = 1,5406 \text{ \AA}$). The sample rotation with a period of 8 s was used to obtain a random grain distribution during the measurement. From the analysis of the diffractogram shown in Figure 3, it is evident that the powder has a crystalline structure and that all the diffraction peaks recorded are characteristic of the presence of a single phase, i.e., an intermetallic NiTi phase with a spatially centred cubic lattice (B2), i.e., austenite (γ -NiTi).

3.1.4. Phase Transformations

The waveforms recorded (Figure 4) of heat flux changes using the differential scanning calorimetry (DSC) method are characterised by two exothermic peaks during the sample cooling from +150°C as well as two endothermic peaks during the sample heating from -150°C. During cooling, the first exothermic peak corresponds to the transformation of austenite A (B2) to the R phase, while the second exothermic peak observed at lower temperature is related to the transformation of the R phase to martensite M (B19'). Thus, the powder investigated shows a two-step transformation during cooling, according to the sequence: A(B2) \rightarrow R \rightarrow M(B19'). During the heating process, a two-step transformation: M(B19') \rightarrow R \rightarrow A(B2) was also observed, manifested by endothermic peaks. The crystal lattice of the R phase is a distortion of the austenite lattice, taking the form of a primitive hexagonal lattice (a rhombohedral structure). What acts as a catalyst for the B2 \rightarrow R phase transformation is the presence of intermetallic secondary phases, such as Ni₄Ti₃. [33–39]

In particular, the characteristic temperatures (Figure 5) at which the peaks representing a given transformation reach their maximum value are as follows:

- $TR_{\max} = -5^{\circ}\text{C}$, A \rightarrow R transformation during cooling
- $TM_{\max} = -32,6^{\circ}\text{C}$, R \rightarrow M transformation during cooling
- $TR_{\max} = 1,2^{\circ}\text{C}$, M \rightarrow R transformation during heating
- $TA_{\max} = 13,10^{\circ}\text{C}$, R \rightarrow A transformation during heating

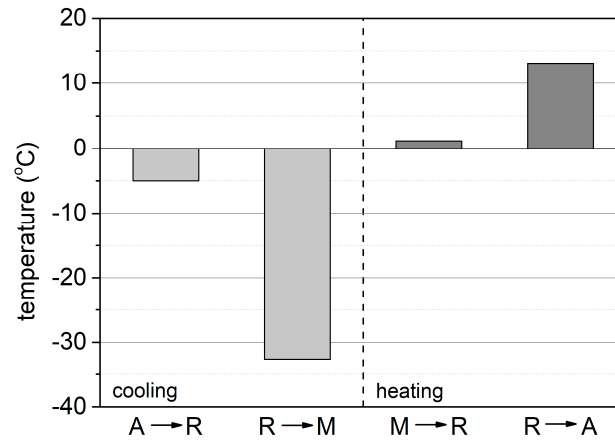


Figure 5. Characteristic temperatures at which the peaks representing a given transformation reach their maximum values.

3.2. Input-Output Correlation

3.2.1. Input Parameters

The samples were fabricated by SLM using a process with the following parameters: laser power $P = 186$ W, scanning speed $V = 1100$ mm/s, line hatch spacing $h = 0.08$ mm, single layer thickness $T = 0.03$ mm. Based on the values of the input parameters used, the VED power density per unit volume of 70.45 J/mm³ was calculated.

$$VED = \frac{P}{v \cdot h \cdot t}$$

The VED parameter defines how much energy is released from a unit volume of the material during the SLM process. It can also be defined as a quantitative expression of thermal energy available for the of the material from the powder state to the dense state [26]. Samples of NiTi alloy after the process were subjected to solution annealing in a tubular furnace at a temperature of 1223 K for 0.5 hours in an Ar atmosphere, and then water-quenched.

3.2.2. Sample Characteristics

3.2.2.1. Density

The density of samples is one of the elementary parameters characterising samples after the additive manufacturing process, which is mainly determined by the presence of pores. The main cause of their formation in samples during the SLM process is gas entrapment. Density values can also be affected by cracks caused by high residual stresses. In the research presented in [40], it was established that what is a prerequisite for preventing pore formation is the use of relatively high laser power and appropriate values for the other SLM 3D printing parameters, ones that provide a relatively high VED to melt the powder in one layer and re-melt the previous layer to ensure epitaxial solidification.

In the study presented here, the density value obtained of the samples (ρ) determined according to the Archimedes' law and the relative density value ρ_r , i.e., related to the theoretical density value ($\rho_t = 6.50$ g/cm³) are respectively: $\rho = 6.432$ g/cm³ and $\rho_r = 99.0\%$. This demonstrates that the selection of the process parameters, from the perspective of the density of the samples produced, was optimal.

3.2.2.2. XRD Phase Analysis

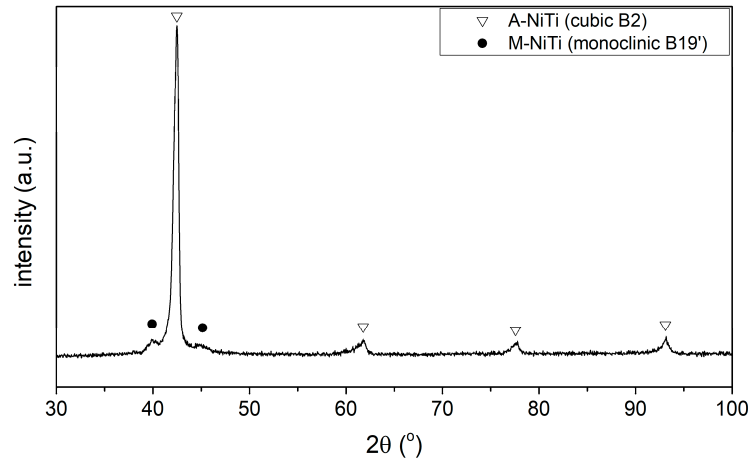


Figure 6. X-ray diffraction pattern of sample.

Figure 6 shows an X-ray diffractogram of the sample after the SLM process and after solution annealing at 950°C for 0.5 hour. According to the diffractogram presented, the sample at room temperature is characterised by an austenitic-martensitic phase structure. The lines with the highest intensity come from the austenite NiTi phase, which proves its highest volume fraction. The appearance of low-intensity diffraction lines originating from the martensitic phase is an evidence of a shift in the onset of the martensitic transformation towards higher temperatures in relation to the NiTi powder which the samples were made from, indicating a decrement of nickel during the incremental manufacturing process.

3.2.2.3. Microstructure

The microstructural structure of the samples obtained was revealed by scanning electron microscopy in the backscattered electrons mode and by transmission microscopy (Figure 7).

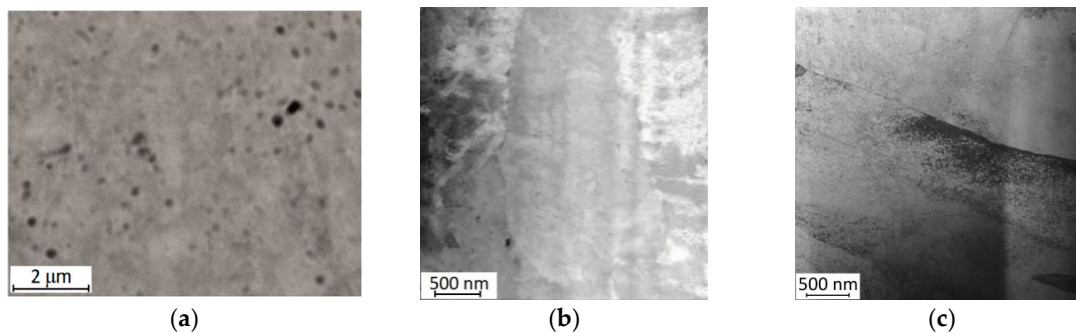


Figure 7. (a) SEM images of cross-sections of sample in backscattered electrons mode and (b and c) STEM images.

In the SEM image presented (7a), a relatively small number of pores can be observed, both spherical and irregularly shaped ones, whose dimensions do not exceed several dozen of nanometres. These observations correspond with the relative density ($\rho_r=99\%$) determined, indicating that the pores occupy a small fraction of the sample's volume. The STEM microphotographs seen in Figures 7b and 7c show grains with elongated shapes, characteristic of the SLM method. This is a result of the crystallisation conditions and the cooling rate during the process.

3.2.2.4. Phase Transformations

The peaks recorded by differential scanning calorimetry, both exothermic ones during cooling and endothermic ones during heating, indicate a single-step phase transformation.

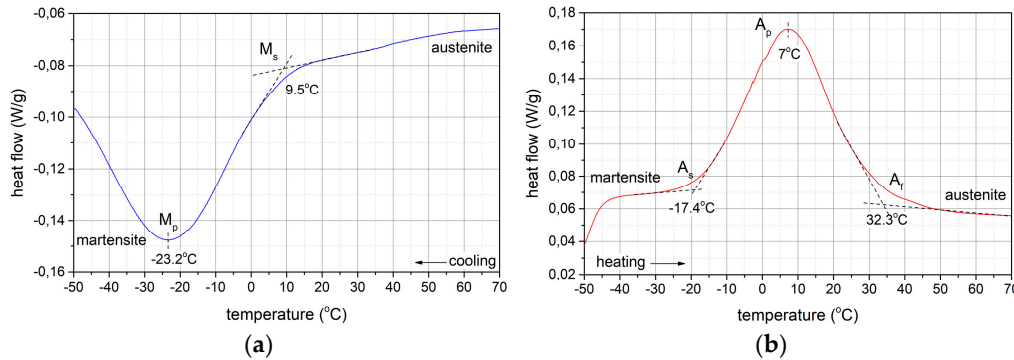


Figure 8. DSC (Differential Scanning Calorimetry) curves of the sample.

During cooling (Figure 8a), the exothermic peak corresponds to the transformation from the austenite A(B2) to the martensite M (B19') phase, while during heating (Figure 8b), the endothermic peak represents the reverse M \rightarrow A transformation.

The characteristic temperatures at which the peaks caused by a given transformation reach their maximum values are as follows:

- $TM_{max} = -23.3^{\circ}C$: A \rightarrow M transformation during cooling,
- $TA_{max} = 7^{\circ}C$: M \rightarrow A transformation during heating.

Compared to the phase transformations identified by DSC in the powder, the A(B2) \rightarrow R and M(B19') \rightarrow R transformations disappear in the samples after the SLM process and dissolution annealing. This is due to the homogenisation of the phase composition of the samples, i.e., the dissolution of the secondary phases present in the powder, which conduce to the formation of the R phase.

3.3. Isothermal Ageing

3.3.1. Phase Composition Analysis

After the SLM process and dissolution annealing at $950^{\circ}C$ for $t=0.5h$, the samples were subjected to isothermal annealing (ageing) at $500^{\circ}C$ for 1, 20 and 100 h. The aim of these heat treatments was to produce Ni_4Ti_3 precipitates in the NiTi alloy with increased nickel content (51.7 at.%) and to study their effects on the sequence of phase transformations, on the characteristic transformation temperatures and on the change in hardness and the Young's modulus. An interpretation of the phase and microstructural changes in the samples after a specific ageing time was carried out using complementary methods, i.e., differential scanning calorimetry (DSC) and X-ray diffraction (XRD).

In the additive manufacturing of NiTi alloy samples, differential scanning calorimetry (DSC) is the main method for monitoring phase transformation temperatures. First and foremost, it enables the determination of the temperature at which the austenitic (B2) phase transforms into the martensitic (B19') phase and vice versa, which allows the determination of the temperature range at which the shape memory effect is activated. This makes it possible to identify the area of potential applications of the unique functional characteristics of the NiTi alloy.

X-ray diffraction provides complementary information about the phase composition of samples. Among other things, this method makes it possible to identify secondary phases separated as a result of ageing at elevated temperatures.

Figure 9 shows thermograms of the samples after specific ageing times, recorded using differential scanning calorimetry (DSC).

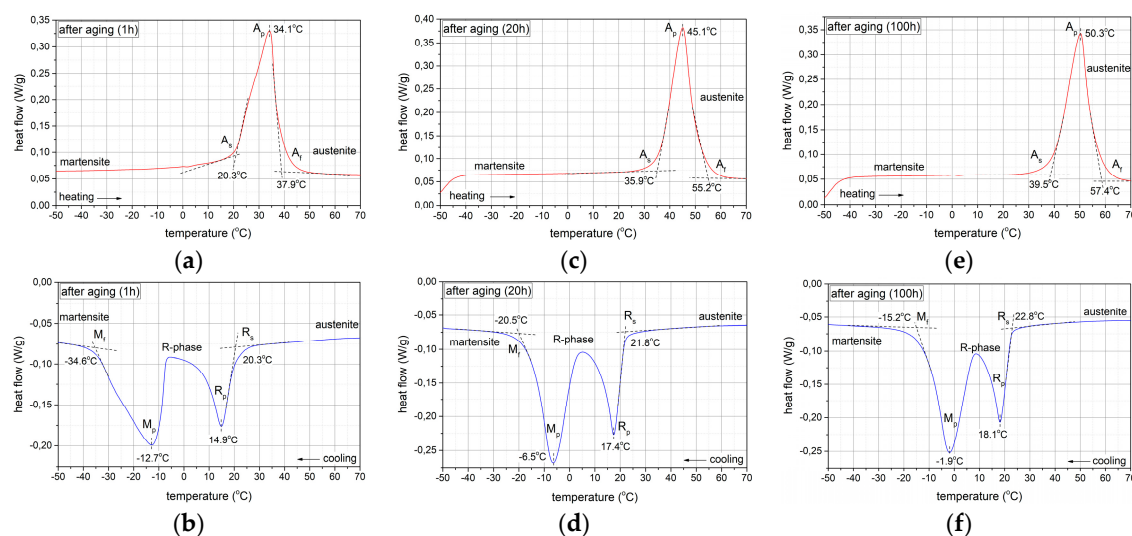


Figure 9. DSC (Differential Scanning Calorimetry) curves of samples after (a,b) 1 h, (c,d) 20 h, (e,f) 100 h ageing.

After all of the ageing times, i.e., 1, 20 and 100 h, the phase transformations during cooling follow the sequence: $A(B2) \rightarrow R \rightarrow M(B19')$, thus a two-step transformation occurs. In contrast, during heating, the formation of the R-phase is not visible in the thermograms (DSC), indicating that the martensitic phase transforms directly into the austenitic phase $M(B19') \rightarrow A(B2)$. In order to gain additional knowledge of the phase transformation sequence, the samples were tested at room temperature by XRD after the ageing process (20 h, 500°C) (Figure 10). One sample was tested immediately after the ageing process (Figure 10a), while the other sample was cooled to -20°C after ageing and then heated to room temperature (Figure 10b).

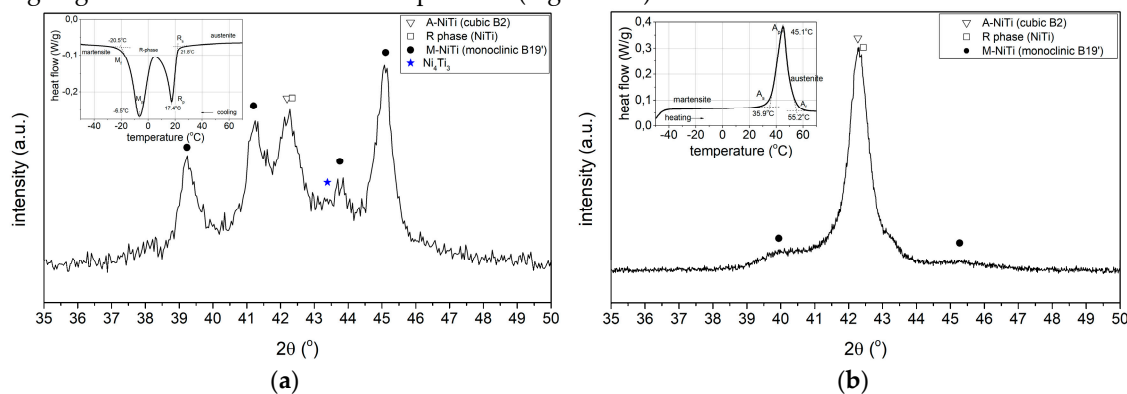


Figure 10. X-ray diffraction pattern of sample (a) directly after 20 h ageing, (b) after aging for 20 h and then cooled to -20°C and in next step heated to room temperature.

In the case of a sample being immediately after ageing, the X-ray diffraction pattern (Figure 10a) shows diffraction peaks from the martensitic, austenitic and rhombohedral phases R. Typical martensite plates for the alloy under study (Figure 11.) were observed by transmission electron microscopy (TEM). These results confirm the analysis carried out with DSC demonstrating that a two-stage phase transformation occurs during cooling (Figure 9d).

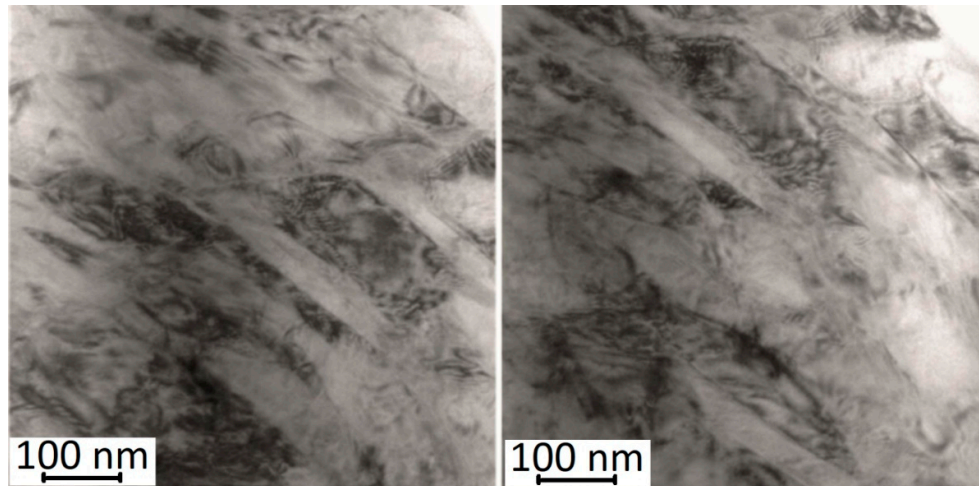
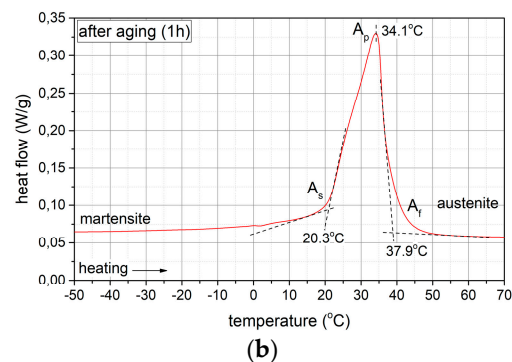
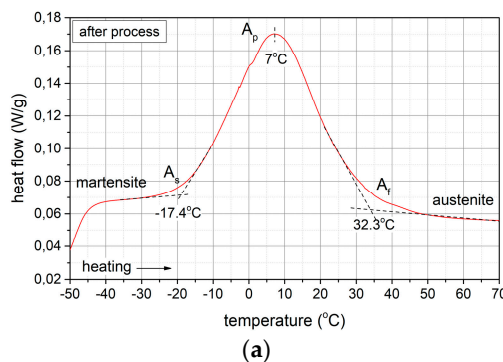


Figure 11. Martensite plates in NiTi alloy samples after ageing for 20h at 500°C.

In contrast, lines from the austenitic phase with high intensity and much smaller lines from the martensitic phase were recorded in the sample after ageing and cooling to a negative temperature (-20°C) and then heating to room temperature (Figure 10b). These results also correspond with the DSC thermogram (Figure 9c) and indicate that during heating from a negative temperature, a one-step transformation from martensite to austenite occurs in the sample.

Comparing the thermograms (DSC) shown in Figure 12, it can be seen that for the sample being immediately after the SLM process, the characteristic peak associated with the formation of the austenitic phase in the sequence: $\text{M}(\text{B19}') \rightarrow \text{A}(\text{B2})$ is much broader, i.e., the total temperature range of the $\text{M} \rightarrow \text{A}$ transformation is much greater compared to aged samples. In addition, the onset (A_s) and end (A_f) temperatures of this transformation as well as the temperature at which the peak maximum (A_p) occurs shift towards higher temperatures by several dozen of degrees after ageing. This evolution of the phase transformation characteristics as a result of an increase in the ageing process time is related to changes occurring within the structure of the material. Above all, the Ni_4Ti_3 phases released during ageing, initially coherent with the matrix with increasing ageing time, become heterogeneous with the matrix [42]. Figure 12 shows a microscopic image (STEM) illustrating the presence of Ni_4Ti_3 phases after 100 h of ageing. The precipitations possess lenticular and disc-like shapes, and they reach dimensions of approximately 200 nm.



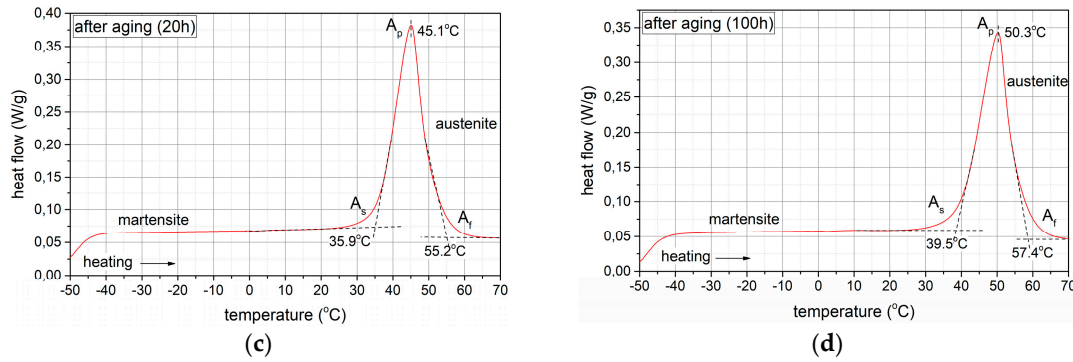


Figure 12. DSC thermograms during heating of NiTi samples (a) shortly after SLM process and after ageing at 500°C: (b) for 1 h, (c) for 20 h (d) for 100 h.

Secondary phases act as a catalyst for the formation of the pre-martensitic R-phase [33–35], while the shift in characteristic phase transformation temperatures towards higher temperatures is due to an increase in the number of secondary phases separated, of the Ni_4Ti_3 type binding more nickel than titanium and thus lowering the content of this element in the matrix [41,42].

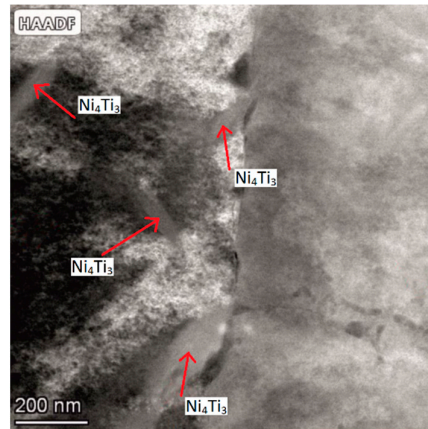


Figure 13. TEM micrographs of microstructure after aging process at $T=500^\circ\text{C}$, $t=100$ h.

In summary, the analysis of the DSC thermograms presented in the study, confirmed by XRD tests, indicates the following characteristic features of the Ni-rich NiTi alloy that change with the ageing time: (1) during cooling, the type of the transformation changes from a one-step transformation after solution annealing to a two-step transformation after the ageing process over 1, 20 and 100 h; (2) when heating the samples from low temperatures for all of the ageing times, only a one-step transformation from $M(B19')$ to $A(B2)$ is observed in the DSC thermograms; (3) the temperature at which the transformation starts increases with the ageing time; (4) the width of the total temperature range of the $M \rightarrow A$ transformation during heating changes from large ($\Delta T=49.7^\circ\text{C}$, after solution annealing) to narrow ($\Delta T=19.3^\circ\text{C}$, after 20 h of ageing).

The results presented, for shorter ageing times, differ from those presented in the key publication [42] on phase transformations in aged NiTi alloy samples. In the study described involving samples made using the traditional method with Ni content of 50.8 at.%, which had previously been aged for 1 and 10 h, only a sequence of two-step phase transformations, i.e., $M(19') \rightarrow R \rightarrow A(B2)$ was observed during their heating using the DSC method. In contrast, a very good convergence of results was obtained after 100 h of ageing. In the studies compared, only a one-step transformation $M(B19') \rightarrow A(B2)$ was observed in the DSC thermograms during heating. Moreover, the peak maximum representing this transformation was practically recorded at the same temperature, i.e., $T_{A_{\max}} = 50^\circ\text{C}$. It follows that, irrespective of the composition of the NiTi alloy and the manufacturing technology of this alloy samples, a sufficiently long ageing process time (in the

cases analysed, at 500°C for 100 h) leads to the occurrence of the martensite → austenite transformation in the same temperature range.

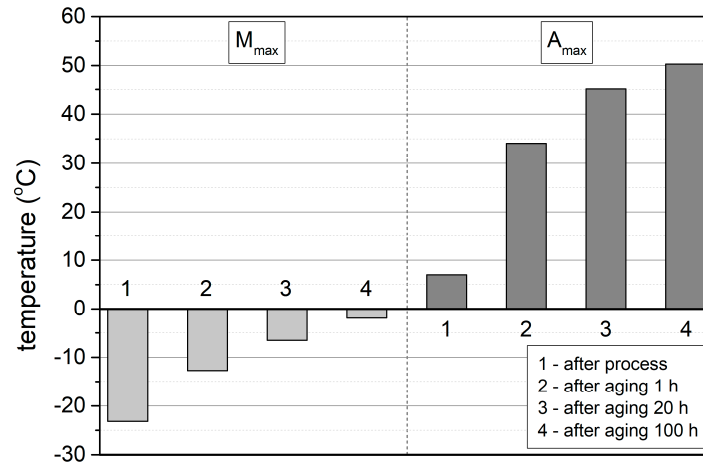


Figure 14. Temperatures at which peak maxima occur from B2→B19' (M_{max}) and B19'→B2 (A_{max}) transformations immediately following the SLM process and solution annealing (950°C, t=0.5 h) and after 1, 20 and 100 h of ageing, recorded in DSC thermograms.

3.3.2. Hardness and Young's Modulus

The highest hardness value of the samples was measured after dissolution annealing, i.e., annealed at 950°C for 0.5 hours and cooled in water (Figure 15). Subsequently, it was observed that the hardness decreases during the ageing process. The greatest decrease occurs after one hour of ageing, from the value of 310 HV to 240 HV and, after 20 hours, the hardness reaches the value of 200 HV, after which it does not change any further with increasing ageing time. The Young's modulus remains practically unchanged during ageing, ranging from 52 to 54 MPa.

The results of the hardness changes correspond to the evolution of phase transformations in the alloys, as illustrated in Figure 14, where the hardness changes are compared with the temperature at which the maximum peaks of the M(B19') → A(B2) transformation occur (T_{Amax}). As can be seen, the greatest changes both in hardness and temperature occur after one hour of ageing. This is due to the fact that the NiTi alloy samples, after the dissolution annealing process, constitute a supersaturated Ni solution in the NiTi matrix, which has the highest hardness, and the ageing process generates the release of Ni₄Ti₃ secondary phase particles, which are initially coherent with the matrix. With ageing, their dimensions increase and they become heterogeneous with the matrix. These processes cause a further decrease in the hardness and depletion of the matrix in Ni, resulting in a shift of the M → A transformation towards higher temperatures.

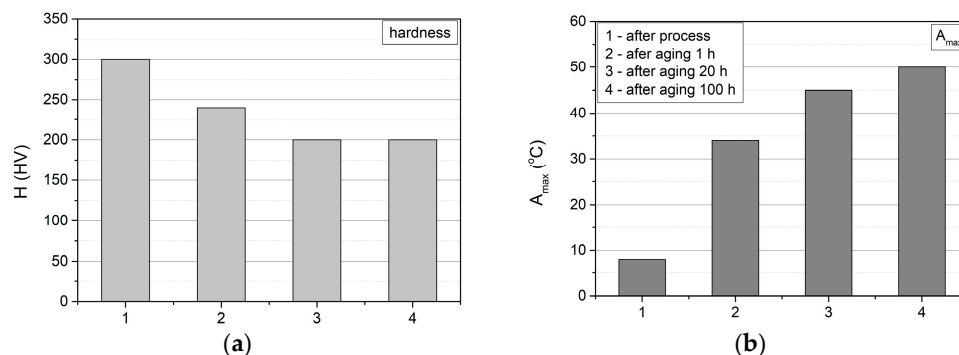


Figure 15. (a) Hardness of NiTi tubes and (b) the temperatures at which peak maximum (DSC) representing M(B19) → A(B2) transformation occurs.

5. Conclusions

Phase transformation temperatures, especially those at which A(B2) transforms into M(B19') directly or via the R-phase during cooling and reverse transformation temperatures during heating when M(B19') transforms into A(B2), are of crucial importance mainly from the technological perspective, as they determine at what temperature the shape memory effect is activated. To date, significant advances have been made in the knowledge of the properties of shape memory NiTi alloys, which enabled the development of diverse and interesting applications [43,44]. In the research on NiTi alloys, a lot of attention has been paid to multistage martensitic transformations. Among others, in the studies [17,18,42], it was pointed out that the microstructure of NiTi alloys and, in particular, dislocation substructures and Ni₄Ti₃ precipitation, are among those factors that influence the thermodynamic and kinetic conditions of martensitic transformation processes. Studies by Bataillard et al. [41,45] on multistage martensitic transformations, using transmission electron microscopy (TEM), led to the proposal of a mechanism for these transformations, which relates to the presence of stresses around coherent Ni₄Ti₃ precipitation. Results from high-resolution TEM confirm that the presence of these stresses promotes the formation of martensite [46–48]. The study by Khalil-Allafi et al. [42] explained the formation of two-step transformation sequences as a result of changes in Ni concentrations, due to Ni₄Ti₃ phase precipitation and differences in nucleation barriers between the R and B19' phases.

The research described in this paper also focused on the role of secondary phase precipitation in NiTi alloys with high Ni content (Ni=51.7 at.%) on phase transformation temperatures and the change in hardness and in the Young's modulus. Phase transformation temperatures were determined by differential scanning calorimetry DSC and, independently, by XRD. The test samples were fabricated using additive technology and the SLM method. After the SLM process, the samples were dissolution annealing at 950°C for 15 minutes and cooled in water. They were then subjected to annealing (ageing) at 500°C for 1, 20 and 100 hours. Simultaneously with the determination of the phase transformation temperatures, hardness and the Young's modulus were measured. Observations of the microstructures were also carried out using TEM. The following conclusions were drawn based on the results obtained:

- During cooling, the type of transformation changes from one-step after solution annealing to two-step after ageing for 1, 20 and 100 hours.
- During heating of the samples from low temperatures, for all the ageing times, only a one-step transformation from M(B19') to A(B2) is observed in the DSC thermograms.
- The transformation temperature M(B19') → A(B2) increases with the ageing time.
- The width of the total transformation temperature range M(B19') → A(B2) during heating varies from large ($\Delta T=49.70^\circ\text{C}$) after solution annealing to narrow ($\Delta T=19.30^\circ\text{C}$) after 20 hours of ageing.
- The change in the hardness values as a result of the ageing process corresponds to the change in temperature, at which the maximum peak reflecting the M(B19') → A(B2), transformation is observed, i.e., the changes in hardness minimise after 20 hours of ageing.
- Comparison with literature data proves that, irrespective of the NiTi alloy composition and sample manufacturing technology, a sufficiently long ageing process time (in the cases analysed, at 500°C) leads to the occurrence of the martensite → austenite transformation in the same temperature range.

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References

1. Aimar, A.; Palermo, A.; Innocenti, B. The role of 3D printing in medical applications: a state of the art. *J. Healthc. Eng.* **2019**, *2019*, 5340616. <https://doi.org/10.1155/2019/5340616>
2. Velasco-Hogan, A.; Xu, J.; Meyers, M.A. Additive manufacturing as a method to design and optimize bioinspired structures. *Adv. Mater.* **2018**, *30*(52), 1800940. <https://doi.org/10.1002/adma.201800940>
3. Sabahi, N.; Chen, W.; Wang, C.H.; Kruzic, J.J.; Li, X. A review on additive manufacturing of shape-memory materials for biomedical applications. *JOM* **2020**, *72*, 1229-1253. <https://doi.org/10.1007/s11837-020-04013-x>
4. Yan, Q.; Dong, H.; Su, J.; Han, J.; Song, B.; Wei, Q.; Shi, Y. A review of 3D printing technology for medical applications. *Engineering* **2018**, *4*(5), 729-742. <https://doi.org/10.1016/j.eng.2018.07.021>
5. Ye, J.; Wilson, D.A.; Tu, Y.; Peng, F. 3D-Printed Micromotors for Biomedical Applications. *Adv. Mater. Technol.* **2020**, *5*(11), 2000435. <https://doi.org/10.1002/admt.202000435>
6. Ahangar, P.; Cooke, M.E.; Weber, M.H.; Rosenzweig, D.H. Current biomedical applications of 3D printing and additive manufacturing. *Appl. Sci.* **2019**, *9*(8), 1713. <https://doi.org/10.3390/app9081713>
7. Yuan, L.; Ding, S.; Wen, C. Additive manufacturing technology for porous metal implant applications and triple minimal surface structures: A review. *Bioact. Mater.* **2018**, *4*, 56-70. <https://doi.org/10.1016/j.bioactmat.2018.12.003>
8. Sacco, E.; Moon, S.K. Additive manufacturing for space: status and promises. *Int. J. Adv. Man. Technol.* **2019**, *105*, 4123-4146. <https://doi.org/10.1007/s00170-019-03786-z>
9. Ishfaq, K.; Asad, M.; Mahmood, M.A.; Abdullah, M.; Pruncu, C. Opportunities and challenges in additive manufacturing used in space sector: a comprehensive review. *Rapid Prototyping J.* **2022**, *28*(10), 2027-2042. <https://doi.org/10.1108/RPJ-05-2022-0166>
10. Lu, H.Z.; Ma, H.W.; Luo, X.; Wang, Y.; Wang, J.; Lupoi, R.; Yin, S.; Yang, C. Microstructure, shape memory properties, and in vitro biocompatibility of porous NiTi scaffolds fabricated via selective laser melting. *J. Mater. Res. Technol.* **2021**, *15*, 6797-6812. <https://doi.org/10.1016/j.jmrt.2021.11.112>
11. Zhang, Y.; Attarilar, S.; Wang, L.; Lu, W.; Yang, J.; Fu, Y. A review on design and mechanical properties of additively manufactured NiTi implants for orthopedic applications. *Int. J. Bioprinting* **2021**, *7*(2), 340. <https://doi.org/10.18063/ijb.v7i2.340>
12. Chmielewska, A.; Dobkowska, A.; Kijeńska-Gawrońska, E.; Jakubczak, M.; Krawczyńska, A.; Choińska, E.; Jastrzębska, A.; Dean, D.; Wysocki, B.; Świążkowski, W. Biological and corrosion evaluation of in situ alloyed NiTi fabricated through laser powder bed fusion (LPBF). *Int. J. Mol. Sci.* **2021**, *22*(24), 13209. <https://doi.org/10.3390/ijms222413209>
13. Xu, Z.; Guo, Y.; Liu, Y.; Jia, B.; Sha, P.; Li, L.; Yu, Z.; Zhang, Z.; Ren, L. An extremely efficiency method to achieve stable superhydrophobicity on the surface of additive manufactured NiTi Alloys: "Ultrasonic Fluorination". *Appl. Surf. Sci.* **2023**, *612*, 155947. <https://doi.org/10.1016/j.apsusc.2022.155947>
14. Habijan, T.; Haberland, C.; Meier, H.; Frenzel, J.; Wittsiepe, J.; Wuwer, C.; Greulich, C.; Schildhauer, T.A.; Köller, M. The biocompatibility of dense and porous nickel–titanium produced by selective laser melting. *Mater. Sci. Eng. C* **2013**, *33*(1), 419-426. <https://doi.org/10.1016/j.msec.2012.09.008>
15. Chekotu, J.C.; Goodall, R.; Kinahan, D.; Brabazon, D. Control of Ni-Ti phase structure, solid-state transition temperatures and enthalpies via control of L-PBF process parameters. *Mater. Design* **2022**, *218*, 110715. <https://doi.org/10.1016/j.matdes.2022.110715>
16. Ye, D.; Li, S.F.; Misra, R.D.K.; Zheng, R.; Yang, Y.F. Ni-loss compensation and thermomechanical property recovery of 3D printed NiTi alloys by pre-coating Ni on NiTi powder. *Addit. Manuf.* **2021**, *47*, 102344. <https://doi.org/10.1016/j.addma.2021.102344>
17. Saedi, S.; Turabi, A.S.; Andani, M.T.; Haberland, C.; Elahinia, M.; Karaca, H. Thermomechanical characterization of Ni-rich NiTi fabricated by selective laser melting. *Smart Mater. Struct.* **2016**, *25*(3), 035005. <https://doi.org/10.1088/0964-1726/25/3/035005>
18. Saedi, S.; Turabi, A.S.; Andani, M.T.; Haberland, C.; Karaca, H.; Elahinia, M. The influence of heat treatment on the thermomechanical response of Ni-rich NiTi alloys manufactured by selective laser melting. *J. Alloy. Compd.* **2016**, *677*, 204-210. <https://doi.org/10.1016/j.jallcom.2016.03.161>
19. Feng, B.; Wang, C.; Zhang, Q.; Ren, Y.; Cui, L.; Yang, Q.; Hao, S. Effect of laser hatch spacing on the pore defects, phase transition and properties of selective laser melting fabricated NiTi shape memory alloys. *Mater. Sci. Eng. A* **2022**, *840*, 142965. <https://doi.org/10.1016/j.msea.2022.142965>
20. Khoo, Z.X.; Liu, Y.; An, J.; Chua, C.K.; Shen, Y.F.; Kuo, C.N. A review of selective laser melted NiTi shape memory alloy. *Materials* **2018**, *11*(4), 519. <https://doi.org/10.3390/ma11040519>
21. Allafi, J.K.; Ren, X.; Eggeler, G. The mechanism of multistage martensitic transitions in aged Ni-rich NiTi shape memory alloys. *Acta Mater.* **2002**, *50*(4), 793-803. [https://doi.org/10.1016/S1359-6454\(01\)00385-8](https://doi.org/10.1016/S1359-6454(01)00385-8)
22. Zhou, N.; Shen, C.; Wagner, M.X.; Eggeler, G.; Mills, M.J.; Wang, Y. Effect of Ni₄Ti₃ precipitation on martensitic transition in Ti–Ni. *Acta Mater.* **2010**, *58*(20), 6685-6694. <https://doi.org/10.1016/j.actamat.2010.08.033>

23. Yao, X.; Amin-Ahmadi, B.; Li, Y.; Cao, S.; Ma, X.; Zhang, X.P.; Schryvers, D. Optimization of Automated Crystal Orientation Mapping in a TEM for Ni₄Ti₃ Precipitation in All-Round SMA. *ShapeMem. Superelast.* **2016**, *2*, 286-297. <https://doi.org/10.1007/s40830-016-0082-z>
24. Ma, C.; Gu, D.; Dai, D.; Xia, M.; Chen, H. Selective growth of Ni₄Ti₃ precipitate variants induced by complicated cyclic stress during laser additive manufacturing of NiTi-based composites. *Mater. Charact.* **2018**, *143*, 191-196. <https://doi.org/10.1016/j.matchar.2018.04.004>
25. Novák, P.; Pokorný, P.; Vojtěch, V.; Knaislová, A.; Školáková, A.; Čapek, J.; Kopeček, J. Formation of Ni-Ti intermetallics during reactive sintering at 500–650°C. *Mater. Chem. Phys.* **2015**, *155*, 113-121. <https://doi.org/10.1016/j.matchemphys.2015.02.007>
26. Ma, J.; Franco, B.; Tapia, G.; Karayagiz, K.; Johnson, L.; Liu, J.; Arroyave, R.; Karaman, I.; Elwany, A. Spatial control of functional response in 4D-printed active metallic structures. *Sci. Rep.* **2017**, *7*(1), 46707. <https://doi.org/10.1038/srep46707>
27. Elahinia, M.; Moghaddam, N.S.; Amerinatanzi, A.; Saedi, S.; Toker, G.P.; Karaca, H.; Bigelow, G.S.; Benafan, O. Additive manufacturing of NiTiHf high temperature shape memory alloy. *Scripta Materialia* **2018**, *145*, 90-94. <https://doi.org/10.1016/j.scriptamat.2017.10.016>
28. Bormann, T.; de Wild, M.; Beckmann, F.; Müller, B. Assessing the morphology of selective laser melted NiTi-scaffolds for a three-dimensional quantification of the one-way shape memory effect. *Proc. SPIE* **2013**, *8689*, 281-288. <https://doi.org/10.1117/12.2012245>
29. Bormann, T.; Schumacher, R.; Müller, B.; Mertmann, M.; De Wild, M. Tailoring selective laser melting process parameters for NiTi implants. *J. Mater. Eng. Perform.* **2012**, *21*, 2519-2524. <https://doi.org/10.1007/s11665-012-0318-9>
30. Bose, S.; Ke, D.; Sahasrabudhe, H.; Bandyopadhyay, A. Additive manufacturing of biomaterials. *Prog. Mater. Sci.* **2018**, *93*, 45-111. <https://doi.org/10.1016/j.pmatsci.2017.08.003>
31. DebRoy, T.; Wei, H.L.; Zuback, J.S.; Mukherjee, T.; Elmer, J.W.; Milewski, J.O.; Beese A.M.; Wilson-Heid A.; De A.; Zhang, W. Additive manufacturing of metallic components—process, structure and properties. *Prog. Mater. Sci.* **2018**, *92*, 112-224. <https://doi.org/10.1016/j.pmatsci.2017.10.001>
32. Horvay, K.M.; Schade, C.T. Development of nitinol alloys for additive manufacturing. *Mater. Sci. Technol.* **2018**, *2018*, 63-70.
33. Uchil, J.; Kumara, K.G.; Mahesh, K.K. Effect of thermal cycling on R-phase stability in a NiTi shape memory alloy. *Mater. Sci. Eng. A* **2002**, *332*(1-2), 25-28. [https://doi.org/10.1016/S0921-5093\(01\)01711-7](https://doi.org/10.1016/S0921-5093(01)01711-7)
34. Khalil-Allafi, J.; Schmahl, W.W.; Toebbens, D.M. Space group and crystal structure of the R-phase in binary NiTi shape memory alloys. *Acta Mater.* **2006**, *54*(12), 3171-3175. <https://doi.org/10.1016/j.actamat.2006.02.040>
35. Wang, X.; Kustov, S.; Verlinden, B.; Van Humbeeck, J. Fundamental development on utilizing the R-phase transition in NiTi shape memory alloys. *Shape Mem. Superelast.* **2015**, *1*, 231-239. <https://doi.org/10.1007/s40830-015-0007-2>
36. Honarvar, M.; Konh, B.; Podder, T.K.; Dicker, A.P.; Yu, Y.; Hutapea, P. X-ray diffraction investigations of shape memory NiTi wire. *J. Mater. Eng. Perform.* **2015**, *24*, 3038-3048. <https://doi.org/10.1007/s11665-015-1574-2>
37. Feng, B.; Kong, X.; Hao, S.; Liu, Y.; Yang, Y.; Yang, H.; Cui, L. In-situ synchrotron high energy X-ray diffraction study of micro-mechanical behaviour of R phase reorientation in nanocrystalline NiTi alloy. *Acta Mater.* **2020**, *194*, 565-576. <https://doi.org/10.1016/j.actamat.2020.05.004>
38. Duerig, T.W.; Bhattacharya, K. The influence of the R-phase on the superelastic behavior of NiTi. *ShapeMem. Superelast.* **2015**, *1*, 153-161. <https://doi.org/10.1007/s40830-015-0013-4>
39. Šittner, P.; Landa, M.; Lukáš, P.; Novák, V. R-phase transition phenomena in thermomechanically loaded NiTi polycrystals. *Mech.Mater.* **2006**, *38*(5-6), 475-492. <https://doi.org/10.1016/j.mechmat.2005.05.025>
40. Chekotu, J.C.; Groarke, R.; O'Toole, K.; Brabazon, D.; Advances in selective laser melting of nitinol shape memory alloy part production, *Materials* **2019**, *12*(5), 809. <https://doi.org/10.3390/ma12050809>
41. Michutta, J.; Somsen, C.; Yawny, A.; Dlouhy, A.; Eggeler, G. Elementary martensitic transition processes in Ni-rich NiTi single crystals with Ni₄Ti₃ precipitates. *Acta Mater.* **2006**, *54*(13), 3525-3542. <https://doi.org/10.1016/j.actamat.2006.03.036>
42. Khalil-Allafi, J.; Dlouhy, A.; Eggeler, G. Ni₄Ti₃-precipitation during aging of NiTi shape memory alloys and its influence on martensitic phase transitions. *Acta Mater.* **2002**, *50*(17), 4255-4274. [https://doi.org/10.1016/S1359-6454\(02\)00257-4](https://doi.org/10.1016/S1359-6454(02)00257-4)
43. Barras, C.D.J.; Myers, K.A. Nitinol—its use in vascular surgery and other applications. *EJVES* **2000**, *19*(6), 564-569. <https://doi.org/10.1053/ejvs.2000.1111>
44. Laurentis, K.J.D.; Mavroidis, C. Mechanical design of a shape memory alloy actuated prosthetic hand. *Technol. Health Care* **2002**, *10*(2), 91-106. <https://doi.org/10.3233/THC-2002-10202>
45. Bataillard, L.; Bidaux, J.E.; Gotthardt, R. Interaction between microstructure and multiple-step transition in binary NiTi alloys using in-situ transmission electron microscopy observations. *Philos. Mag. A* **1998**, *78*(2), 327-344. <https://doi.org/10.1080/01418619808241907>

46. Waitz, T.; Kazykhanov, V.; Karnthaler, H.P. Martensitic phase transitions in nanocrystalline NiTi studied by TEM. *Acta Materialia* **2004**, *52*(1), 137-147. <https://doi.org/10.1016/j.actamat.2003.08.036>
47. Gall, K.; Juntunen, K.; Maier, H.J.; Sehitoglu, H.; Chumlyakov, Y.I. Instrumented micro-indentation of NiTi shape-memory alloys. *Acta Materialia* **2001**, *49*(16), 3205-3217. [https://doi.org/10.1016/S1359-6454\(01\)00223-3](https://doi.org/10.1016/S1359-6454(01)00223-3)
48. Waitz, T.; Karnthaler, H.P. Martensitic transition of NiTi nanocrystals embedded in an amorphous matrix. *Acta Materialia* **2004**, *52*(19), 5461-5469. <https://doi.org/10.1016/j.actamat.2004.08.003>

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