

Essay

Not peer-reviewed version

Mid-Infrared 2.79 μm Band Er, Cr: YSGG Laser Transmission Anti-Bending Low-Loss Anti-Resonant Hollow-Core Fiber

[Lei Huang](#) , Peng Wang , Ze Yin Wang , Qing Ting Cheng , [Li Wang](#) , [Haihe Jiang](#) *

Posted Date: 26 March 2024

doi: 10.20944/preprints202403.1526.v1

Keywords: laser delivery; Cr, Er: YSGG; anti-resonant hollow-core fiber; bending loss



Preprints.org is a free multidiscipline platform providing preprint service that is dedicated to making early versions of research outputs permanently available and citable. Preprints posted at Preprints.org appear in Web of Science, Crossref, Google Scholar, Scilit, Europe PMC.

Copyright: This is an open access article distributed under the Creative Commons Attribution License which permits unrestricted use, distribution, and reproduction in any medium, provided the original work is properly cited.

Article

Mid-Infrared 2.79 μm Band Er, Cr: YSGG Laser Transmission Anti-Bending Low-Loss Anti-Resonant Hollow-Core Fiber

Lei Huang ^{1,2}, Peng Wang ¹, Yinze Wang ^{1,2}, Tingqing Cheng ², Li Wang ³ and Haihe Jiang ^{1,2,*}

¹ Anhui Province Key Laboratory of Medical Physics and Technology, Institute of Health and Medical Technology, Hefei Institutes of Physical Science, Chinese Academy of Sciences, Hefei Anhui 230031, China

² University of Science and Technology of China, Hefei Anhui 230026, China

³ Anhui Institute of Optics and Fine Mechanics, Hefei Institutes of Physical Science, Chinese Academy of Sciences, Hefei Anhui 230031, China

* Correspondence: hjjiang@hfcas.ac.cn

Abstract: A large core size and bending resistance are very important properties of mid-infrared energy transfer fibers, but large core sizes usually lead to a deterioration of bending properties. A negative-curvature nested node-free anti-resonant hollow-core fiber (AR-HCF) based on quartz is proposed. It was made by adding a nested layer to a previous AR-HCF design to provide an additional anti-resonance region while keeping the gap between adjacent tubes strictly correlated to the core diameter to produce a node-free structure. These features improve the fiber's bending resistance while achieving a larger core diameter. The simulation results show that the radial air-glass anti-resonant layer is increased by the introduction of the nested anti-resonant tube, and the weak interference overlap between the fiber core and the cladding mode is reduced, so the fiber core's limiting loss and the sensitivity to bending are effectively reduced. When the capillary wall thickness t of the fiber is 0.71 μm , the core diameter D is 70 μm , the ratio of the inner diameter of the cladding capillary to the core diameter d/D is 0.62, and the diameter of the nested tube is $d_0=29$ μm , the fiber has a lower limiting loss at the wavelength of 2.79 μm , and the limiting loss is 3.28×10^{-4} dB/m. At the same time, the optimized structure also has good bending resistance. When the bending radius is 30 mm, the bending loss is only 4.72×10^{-2} dB/m. To our knowledge, this is the first research to achieve an anti-bending low-loss micro-structure hollow fiber with a bending radius of less than 30 mm in the 2.79 μm band. An anti-bending low-loss anti-resonant hollow-core fiber with this structure constitutes a reliable choice for the light guiding system of a 2.79 μm band erbium laser therapy instrument.

Keywords: laser delivery; Cr, Er: YSGG; anti-resonant hollow-core fiber; bending loss

1. Introduction

Mid-infrared 2.79 μm band laser is located in the strong absorption peak region of water molecules and hydroxyapatite, and it has important application value and potential in biomedicine, remote sensing, military equipment, and other fields due to its special wavelength [1]. In the field of biomedicine, carriers for flexible laser transmission (i.e., transmission along paths of arbitrary shape) are the focus of research on 2.79 μm medical laser devices. The traditional 2.79 μm Er, Cr: YSGG medical solid-state laser uses a light guide arm composed of multi-reflection lenses to transmit the laser beam. The transmission loss is large because of the lenses at the multiple joints of the laser beam path. Moreover, the rigid structure makes it difficult to realize flexible operation of the optical carrier in any direction under small bending radii as encountered in the mouth and nasal cavity. Therefore, the light guide arm has severe limitations as a carrier for transmitting 2.79 μm band laser. The use of fiber to transmit 2.79 μm band laser not only ensures flexible transmission but also avoids the

interference of the external environment, thereby improving the transmission efficiency, and the better bending characteristics of the fiber can also provide safer protection for medical services.

Examples of solid-core fibers that can transmit mid-infrared 2.79 μm band laser include SiO_2 fibers, ZBLAN fibers [2], and Al_2O_3 fibers [3,4]. However, previously used fibers have significant faults for this purpose. Quartz fiber has a large transmission loss, and fluoride fiber has poor bending performance. Also, sapphire fiber is expensive and short production lengths of it cannot achieve single-mode transmission. Solid-core fiber has limitations in mid-infrared 2.79 μm band laser transmission. However, Pryamikov et al. [5] adopted anti-resonant hollow-core fiber to achieve low-loss flexible transmission of laser with a wavelength longer than 3.5 μm , so the intrinsic problem of solid-core fiber transmission in the mid-infrared band was successfully solved, this kind of fiber has become a research hotspot in the application of mid-infrared laser transmission. This anti-resonant hollow-core fiber is composed of a single-layer quartz tube, which is a structure that is simple and easy to pull. Mainly due to the anti-resonance guide light and inhibition of the coupling effect, this fiber can achieve small loss and large width [6] at the same time because the glass material occupies just a small proportion of the fiber, and the laser propagates in an air core similar to a free space environment. This fiber has the characteristics of high damage threshold and extremely low transmission loss [7–11].

Because the bending loss is a vital consideration for hollow core fibers in practical applications, this aspect is particularly worth studying. Research progress on bending loss in the near-infrared band has been relatively successful. In 2022, Zhao et al. [12] designed a nested hollow-core fiber with a bending loss of 0.001 dB/m at a minimum bending radius of 50 mm and a wavelength of 1.55 μm . In the same year, Liu et al. [13] designed an AR-HCF with a glass sheet nested structure and calculated that its bending loss of LP_{01} - LP_{31} mode is less than 3.0×10^{-4} dB/m in the wavelength range of 1.4–1.61 μm when the bending radius is 60 mm. However, the research progress on bending loss in the mid-infrared band has been relatively slow, mainly because the wavelength is longer and it is more sensitive to the loss caused by bending deformation. In 2012, Urich et al. [14] used a triangular cladding AR-HCF to transmit a 2.94 μm high-energy microsecond pulse laser and measured a bending loss of $0.183 \text{ dB/m} \pm 0.05 \text{ dB/m}$ at a minimum bending radius of 250 mm. In 2012, Fei Yu et al. [15] from the University of Bath in the United Kingdom designed an ice-cream AR-HCF, which achieved a transmission loss of 0.034 dB/m at a wavelength of 3.05 μm , and its light intensity transmitted at a bending radius of 200 mm is less than half that at a bending radius of 600 mm. In 2014, Knight et al. [16] of the University of Bath in the United Kingdom adopted an AR-HCF composed of 10 capillaries at a wavelength of 3.1 μm to achieve 0.1 dB/m transmission loss, with a minimum bending radius of 80 mm and a bending transmission loss of 0.3 dB/m. The above research on the transmission of infrared laser by hollow fiber with different single cladding structures achieves low transmission loss, but unfortunately, the single cladding structure deviates from the desired matching of the core diameter and the cladding capillary gap when the bending deformation is severe, resulting in a large minimum bending radius and high bending loss.

In recent years, the anti-bending properties of nested anti-resonant hollow-core fibers have attracted much attention. In 2019, Mariusz Klimczak et al. [17] of the University of Warsaw reported a nested anti-resonant hollow-core fiber with a core diameter of 62 μm that can achieve mid-infrared band transmission, with a bending loss of 0.5 dB/m at a wavelength of 4 μm and a bending radius of 40 mm. When the bending radius is 15 mm, the bending loss is 5 dB/m, showing that this nested anti-resonant hollow-core fiber has good bending resistance in the mid-infrared band. AR-HCF is the ideal fiber for laser transmission in the 2.79 μm band. However, a medical laser transmission system usually requires a larger core diameter in order to transmit more laser energy, and a large core size will lead to a deterioration of bending performance. Therefore, a large core size to obtain a large mode field area and strong bending resistance with low bending loss are very important performance indicators of mid-infrared fiber. To some extent, a fiber's ability to mechanically and optically bend to a relatively small radius determines whether it can enter commercial and practical applications.

In this paper, a negative curvature nested anti-resonance hollow-core fiber based on quartz is designed, which provides additional anti-resonance region by adding a nesting layer, keeps the gap

between adjacent tubes and the core diameter consistent, and makes each capillary have no nodes; this combination improves the fiber's bending resistance. Moreover, it has the characteristics of a large core diameter, simple structure, high flexibility, and simple manufacturing process. Finite element and control variable methods are used to study the transmission performance of the structures with different parameters. The structural parameters affecting the bending loss are optimized, which significantly improves the transmission characteristics of the optimized anti-resonant hollow-core fiber. The introduction of the nested anti-resonant tube increases the radial air-glass anti-resonant layer, and the embedded tube can reduce the weak interference overlap between the fiber core and the cladding mode, effectively reducing the limiting loss and bending loss of the fiber core. The simulation proves that it is feasible to transmit mid-infrared medical 2.79 μm band laser, so this new fiber is expected to replace the traditional guide arm system currently used in 2.79 μm medical lasers.

2. AR-HCF Is Designed to Transmit 2.79 μm Band Laser

Figure 1 shows the radial section structure of the new fiber. AR-HCF is composed of six tubes surrounded by capillary walls with thickness t . The core is the largest tangent circle with diameter D , the inner diameter of each capillary is d , and the gap between capillaries is g . The white part is air, and the brown part is quartz, the base material. The six non-contacting capillaries form a cladding structure. The non-contacting geometry can eliminate Fano resonance [18], so each tube is regarded as an isolated tube and is tangent to the outer layer, which mainly plays a role of protection and support.

The fiber characteristics are calculated using numerical methods, namely finite element mode solvers (Comsol Multiphysics), along with optimized mesh sizes and perfectly matched layers (PML). In the numerical simulation, the outermost layer of the outer envelope is set as the perfect matching layer, which is the critical edge that only absorbs and does not reflect. The intersection of the capillary and the outer layer is optimized (Figure 1(a)), which can greatly improve the accuracy of the calculation. The perfectly matched layer grid is a map with a maximum cell size of $\lambda/6$, and the rest of the grid is divided into a free triangle grid (Figure 1(b)). The maximum cell size distribution in the air and quartz regions is $\lambda/5$ and $\lambda/4$. The refractive index of air is 1, and the refractive index of quartz is related to the wavelength (λ). According to the Sellmeier [19] equation, the refractive index at 2.79 μm is 1.424. Figure. 2 shows the mode field distribution of LP_{01} (Figure 2(a)) and LP_{11} (Figure 2(b)) of the anti-resonant hollow-core fiber at a wavelength of 2.79 μm . It can be seen that the electric field is confined well within the air fiber core.

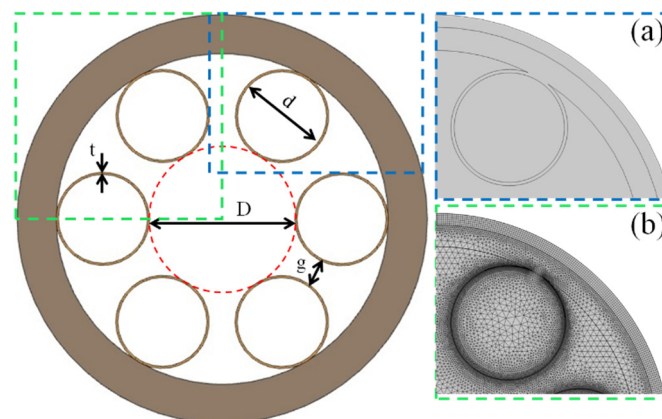


Figure 1. Cross-sectional structure diagram of anti-resonant hollow-core fiber. (a) Post-processing structure diagram at the intersection of the capillary and the outer layer. (b) Grid division diagram of a fiber structure quarter.

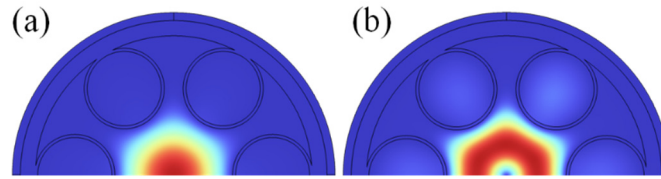


Figure 2. Mode field distribution of anti-resonant hollow-core fiber at wavelength 2.79 μm .

3. Parameter Optimization

3.1. Effect of Capillary Wall Thickness on AR-HCF Transmission Characteristics

For anti-resonant hollow-core fibers, the capillary wall thickness is an important parameter that directly affects the transmission characteristics of the fiber. When the fiber material and its refractive index are determined, the capillary wall thickness directly determines the resonance and anti-resonance wavelength. When the capillary wall thickness t satisfies equation (1), then the wavelength of 2.79 μm is in the anti-resonance wavelength region, and the light in the fiber that does not resonate with the cladding formed by the capillary wall is reflected back into the core and transmitted in the core with low loss. When t satisfies equation (2), the 2.79 μm wavelength is in a resonant state, and the light in the air fiber core will not be restricted, and at the same time, it will leak into the capillary cladding, resulting in a sharp increase in fiber loss and even damage to the cladding structure [20].

$$t_1 = \frac{(m-0.5)\lambda}{2\sqrt{n_1^2 - n_0^2}} \quad (1)$$

$$t_2 = \frac{m\lambda}{2\sqrt{n_1^2 - n_0^2}} \quad (2)$$

Here, λ is the wavelength, m is an integer, n_0 is the air with a refractive index of 1, n_1 is the quartz refractive index (1.424 at the wavelength of 2.79 μm), t_1 is the thickness of the capillary wall at the time of anti-resonance, and t_2 is the thickness of the capillary wall at the time of resonance.

The initial condition was set as follows: the core diameter D was 30 times the wavelength 83.7 μm , and the ratio d/D of the capillary inner diameter to the core diameter was kept unchanged at 0.68. The parametric scanning interval of t was 0.3 μm -2.0 μm . Figure 3(a) shows the anti-resonance curve of constraint loss with cladding capillary wall thickness when the anti-resonance wavelength is 2.79 μm , showing a periodicity of anti-resonance and resonance alternating action. The capillary wall thickness does not need to be completely consistent with the wall thickness calculated by equation (1), and an anti-resonance effect can also be generated near it. In the resonant region (1.33 $\mu\text{m} < t < 1.58 \mu\text{m}$), the core mode is partially coupled with the cladding mode, which leads to a large confinement loss of several hundred dB/m. As can be seen from the illustration, a large number of electric fields are distributed in the capillary cladding. In the anti-resonance region ($t > 1.58 \mu\text{m}$, $t < 1.33 \mu\text{m}$), the core mode is well-confined in the fiber core, and the constraint loss is low. Figure 3(b) shows the variation curve of the effective refractive index of the core with the capillary wall thickness. In the resonant region of 1.33 $\mu\text{m} < t < 1.58 \mu\text{m}$, the effective refractive index is not continuous, and the resonance between the light and the quartz cladding is the largest, which explains the root cause of the high loss in Figure 3(a). The coupling of the core mode and the cladding mode causes the discontinuity of the effective refractive index of the fundamental mode.

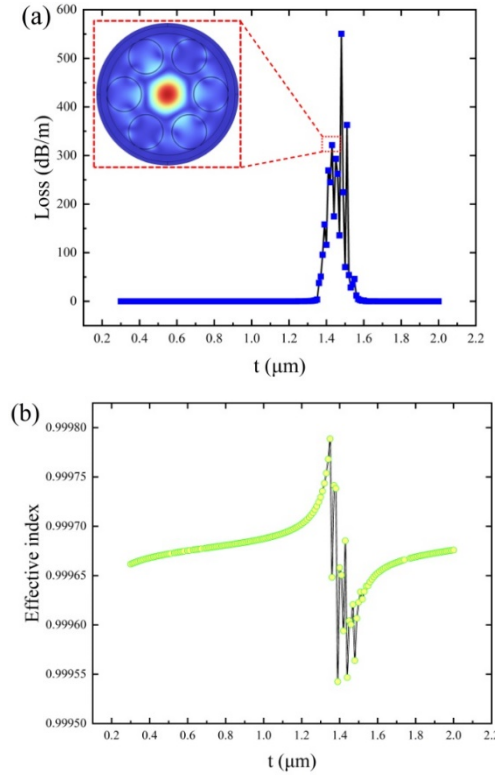


Figure 3. (a) Transmission loss and (b) effective refractive index changes with capillary wall thickness t .

To find the optimal capillary wall thickness, the anti-resonance region ($0.3 \mu\text{m} < t < 1.2 \mu\text{m}$) was scanned with a step length of 0.001, as shown in Figure 4(a). At $t=0.723 \mu\text{m}$, the basic mode loss of LP_{01} reaches its minimum at 8×10^{-3} dB/m. For anti-resonant hollow-core fibers, the single-mode characteristics are usually described by the high-order mode extinction ratio (HOMER), which is calculated by comparing the minimum LP_{11} mode loss with the core LP_{01} mode loss [21]:

$$\text{HOMER} = \frac{\text{loss}_{\text{LP}_{11}}}{\text{loss}_{\text{LP}_{01}}} \quad (3)$$

When the HOMER value is greater than 100, the fiber can be considered to maintain single-mode transmission. At $t=0.723 \mu\text{m}$, the high-order mode extinction ratio reaches 414. Figure 4(b) shows the mode field distribution of LP_{01} and LP_{11} in the fiber core at $t=0.723 \mu\text{m}$. It can be seen that the mode of LP_{01} is well-confined in the air fiber core, and no electric field distribution occurs in the capillary wall cladding. The LP_{11} mode is distributed in the air core and cladding tube, resulting in increased loss, which is advantageous for single-mode transmission fibers.

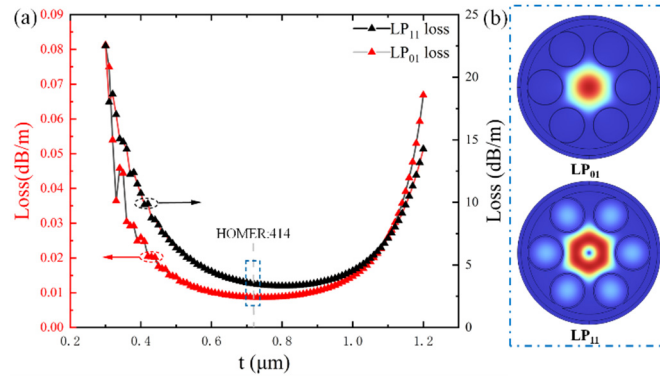


Figure 4. (a) The change of limiting loss in the range of t values $0.3 \mu\text{m}$ - $1.2 \mu\text{m}$, and (b) the mode field distribution of core fundamental mode and high-order mode when $t=0.723 \mu\text{m}$.

When the anti-resonant hollow-core fiber is used as the light guide system of a 2.79 μm laser medical instrument, bending is inevitable in clinical application, and bending will introduce bending loss. When the fiber is bent, the refractive index of the cladding layer and the core change, which changes the phase of the core mode and cladding mode. When the phase between the core mode and cladding mode meets certain matching conditions, the core mode leaks into the cladding, resulting in bending loss. With the reduction of the bending radius, the bending loss gradually becomes the dominant optical fiber transmission loss, and even affects the transmission mode of the optical fiber to appear some disturbance modes, which lose their constraints in the core, resulting in the bending loss. Therefore, to preserve the fiber's ability to maintain high-efficiency and low-loss single-mode transmission under different bending radii, we studied the losses corresponding to different capillary wall thicknesses and bending radii to find the most suitable capillary wall thicknesses, as shown in Figure 5. In this numerical calculation, the core effective refractive index (n_{eq1}) and cladding refractive index (n_{eq1_silica}) of the bent fiber can be changed on the basis of the straight fiber:

$$n_{eq1} = n_l \cdot \exp(x / R_b) \quad (4)$$

$$n_{eq1_silica} = n_{silica} \cdot \exp(x / R_b) \quad (5)$$

Here, R_b is the bending radius, n_l is the core refractive index of the straight fiber, n_{silica} is the cladding refractive index of the straight fiber, and x is the transverse distance from the center of the curved fiber.

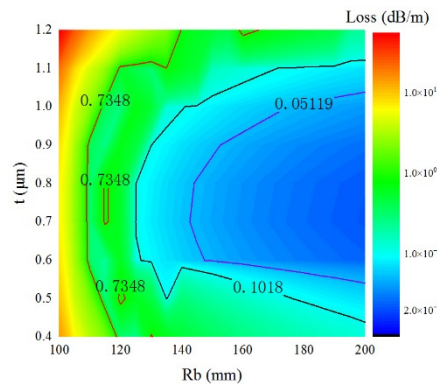


Figure 5. Surface diagram of bending loss table for adjusting different capillary wall thicknesses.

The combined parameterization scans the loss of the anti-resonance region of the capillary wall thickness ($0.4 \mu\text{m} < t < 1.2 \mu\text{m}$) within the bending radius of 100-200 mm. Figure 5 shows that when $t=1.2 \mu\text{m}$, the bending loss is sensitive to the bending radius, and when the bending radius is 100 mm, the bending loss reaches 53.4 dB/m, although the bending loss can also reach 1 dB/m under larger bending radius. When $t=0.71 \mu\text{m}$, the bending loss is not sensitive to the bending radius. When the bending radius is 115 mm, the bending loss is 0.7348 dB/m, and when the bending radius is 150 mm, the bending loss is only 0.05119 dB/m. To achieve AR-HCF with practical resistance to loss due to bending, $t=0.71 \mu\text{m}$ was selected as the result of optimization.

3.2. Influence of Capillary Inner Diameter on AR-HCF Transmission Characteristics

The change of capillary inner diameter directly affects the change of core diameter and the loss of core basic mode and high-order mode, so optimizing capillary inner diameter is also very important. On the basis of the parameter optimization in Section 3.1, the core diameter $D=83.7 \mu\text{m}$ and capillary wall thickness $t=0.71 \mu\text{m}$ remained unchanged, and d/D was varied within a scanning range of 0.4-0.9. The results are shown in Figure 6. Changing the inner diameter of the cladding capillary also changes the capillary gap g , and this inter-tube gap is also an important part of the cladding effect, so its influence on the optical properties should also be quantified. The relationship of each geometry can be expressed as:

$$g = (D+d)\sin(\pi/N) - d \quad (6)$$

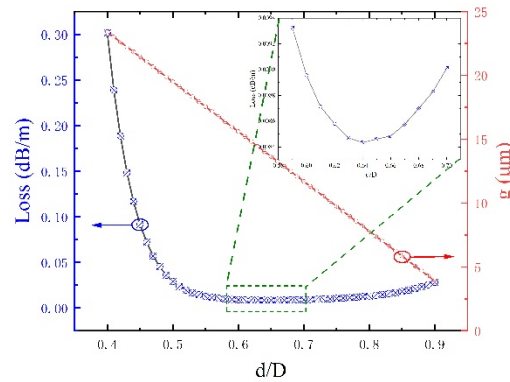


Figure 6. Variation curve of transmission loss of anti-resonant hollow-core fiber with d/D .

Figure 6 shows that with the increase of the inner diameter of the capillary cladding, the capillary gap decreases linearly, and the loss decreases. When $d/D=0.64$ and the inner diameter of the cladding tube $d=53.6 \mu\text{m}$, the loss reaches the minimum value of $8.4 \times 10^{-3} \text{ dB/m}$. When $d/D < 0.64$, the loss increases significantly with a decreasing d because a decrease of d corresponds to an increase of tube spacing, which will cause light leakage [22–25]; see Figure 8(b). Another reason we consider is that with the decrease of d , the total perimeter of the capillary cladding decreases, and the spatial overlap increases between the modes of the air layer and the modes of the glass layer; that is, the coupling strength increases, which leads to the loss of the modes of the air layer. When $d/D > 0.64$, the loss increases rather than decreases. The main reason is that when d increases past a certain threshold, the surface tension between the cladding capillaries leads to the formation of local nodes between the capillaries, which greatly increases the fiber's transmission loss. The transmission loss is consistent with the change of the imaginary part of the effective refractive index (Figure 7).

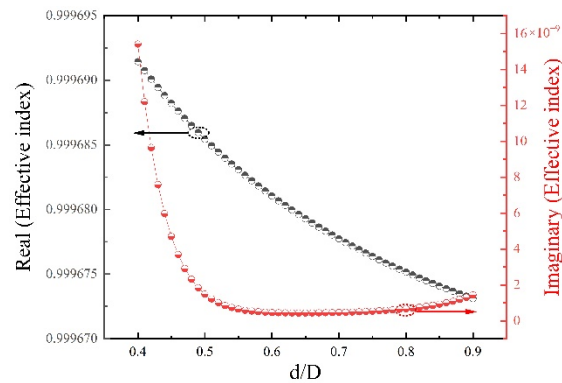


Figure 7. The relationship between the imaginary and real parts of the effective refractive index with d/D .

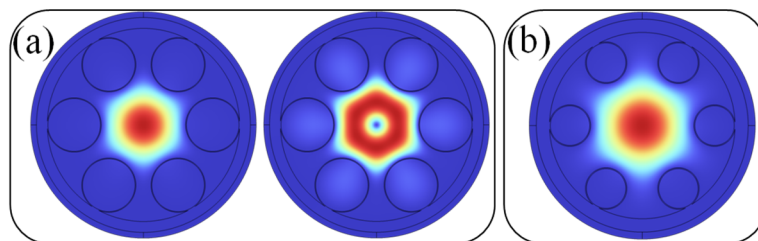


Figure 8. (a) $d/D=0.64$ core pattern field distribution, (b) $d/D=0.4$ core pattern distribution.

We use the same combination of parameters to scan for the effect of the d/D ratio on bending losses. For this testing, we use a d/D value with small loss (0.6-0.8) and a bending radius of 100-200 mm, which is a very limiting bending radius for most anti-resonant air-core fibers. As can be seen from Figure 9, when $d/D < 0.62$, the fiber is not sensitive to the bending radius, even when it is 100 mm; as can be seen from the red contour line in the figure, the bending loss is only 0.7418 dB/m. The choice of $d/D = 0.62$ ensures low loss and low sensitivity to bending radius.

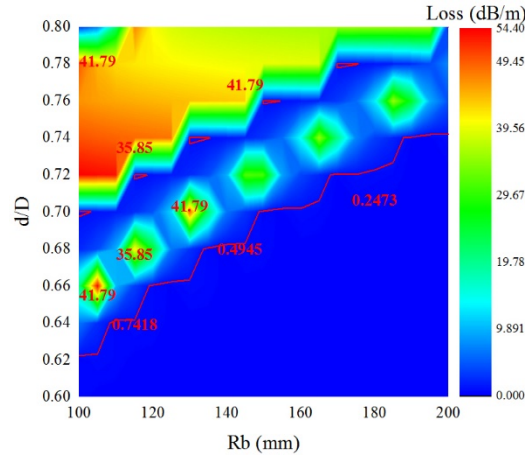


Figure 9. Effect of d/D ratio on fiber loss at different bending radii.

3.3. Influence of Fiber Core Diameter on AR-HCF Transmission Characteristics

The core diameter directly affects AR-HCF loss. The optimal core diameter can be obtained by numerical calculation based on the relationship between fiber loss and core diameter. After fixing $d/D = 0.62$ and $t = 0.71 \mu\text{m}$, the relationship between loss and core diameter can be obtained by parametric scanning of D , as shown in Figure 10. It can be seen from the figure that the fiber loss decreases with the increase of the core diameter. When $D = 120 \mu\text{m}$, the loss is the lowest, reaching $3.0 \times 10^{-3} \text{ dB/m}$, and the high-order mode extinction ratio reaches 935. Without considering the bending loss, $D = 120 \mu\text{m}$ is the best choice. Figure 11 shows the relationship between the real and imaginary parts of the effective refractive index of the fiber core and the diameter of the fiber core. The real part increases with increasing diameter. The main reason is that the larger the diameter of the core, the farther the center of the fiber transmission is from the cladding tube wall, so the less the coupling effect between the fiber core transmission mode and the cladding tube mode, and the closer the real part of the effective refractive index of the fiber core fundamental mode becomes to the air refractive index.

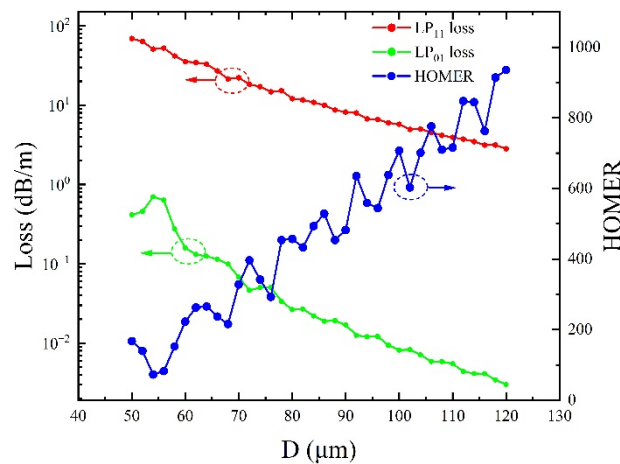


Figure 10. Relationship between core base mode and high-order mode loss, high-order mode extinction ratio, and core diameter.

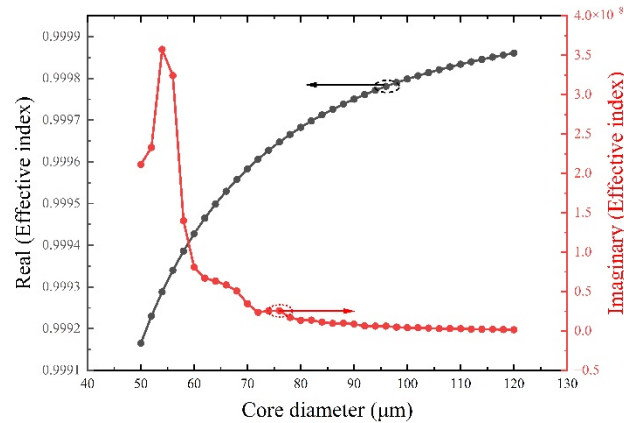


Figure 11. Relationship between the real and imaginary parts of the core effective refractive index and the core diameter.

To obtain the anti-bending characteristics of the new AR-HCF, we varied the loss of D in the lower loss range of 70-90 μm corresponding to different bending radii (100-200 mm) to find out the optimal D value; Figure 12 shows the results. When the bending radius $R=100$ mm, the bending loss of $D=70$ μm is the lowest, which can be seen from the contour line to 0.3089 dB/m. When $D>80$ μm , the bending loss is greater than 37 dB/m, which shows the AR-HCF's great sensitivity to the bending radius. Figure 13 shows the distribution diagram of the core fundamental mode field corresponding to different D values when the bending radius $R=100$ mm. It can be seen from the diagram that when $D=70$ μm , the fundamental mode is confined well in the air core, and only a small part of the electric field leaks into the cladding tube, which corresponds to the low loss in Figure 12. When $D=74$ μm , a large part of the electric field leaks into the cladding tube, and the loss reaches 37.07 dB/m. When $D=86$ μm , there is strong coupling between the cladding tube and the air fiber core mode, and only a small part of the field exists in the air core. In this situation, most of the field is coupled to the cladding tube, resulting in a huge increase in the loss value of 47.63 dB/m. The core electric field distribution diagram (Figure 13) corresponds to the loss diagram (Figure 12). Based on these results, $D=70$ μm is chosen as the best air core diameter of these anti-bending low-loss anti-resonant hollow-core fibers.

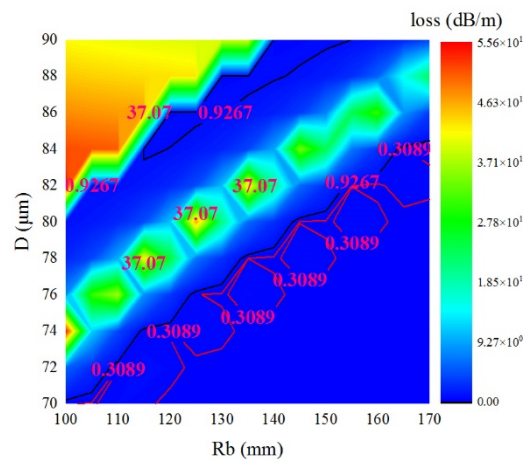


Figure 12. Fiber bending loss at different core diameters D and bending radii.

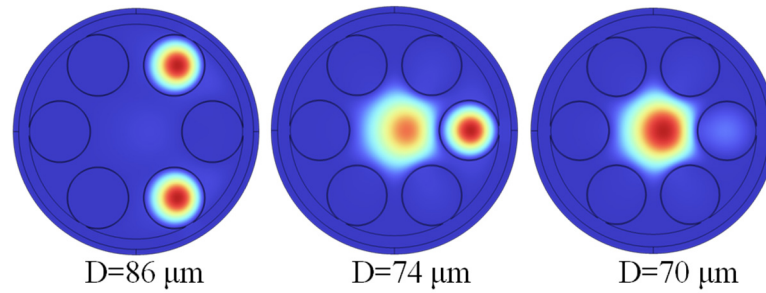


Figure 13. When the bending radius is 100 mm, the electric field distribution of $D=86\ \mu\text{m}$, $74\ \mu\text{m}$, and $70\ \mu\text{m}$ core fundamental mode.

4. Results and Discussion

4.1. Influence of Inner Diameter of Casing on Bending Loss

Section 3 analyzed how different capillary wall thicknesses, ratios of cladding wall thickness to core, and core diameters affect the transmission characteristics. The analysis revealed that the transmission loss is 0.02 dB/m when $t=0.71\ \mu\text{m}$, $d/D=0.62$, $D=70\ \mu\text{m}$, and the bending loss is 0.31 dB/m when the bending radius $R=100\ \text{mm}$. To further reduce the loss of fiber and the sensitivity to the bending radius, we introduce a nested anti-resonant tube based on the above structural parameters, in order to increase the radial air-glass anti-resonant layer and reduce the limiting loss of the fiber core, denoting the wall thickness of the embedded capillary as d_0 . The structure is shown in Figure 14.

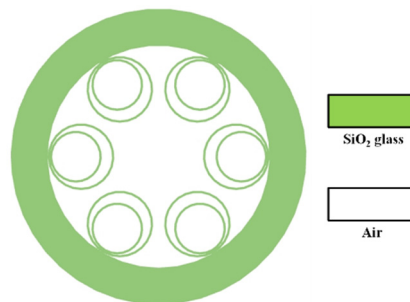


Figure 14. Structure diagram of nested anti-resonant hollow-core fiber.

Keeping the wall thickness of the embedded tube the same as the wall thickness of the outer capillary tube, the influence of different d_0 on the loss in a smaller bending radius (10-100 mm) was studied; the results are shown in Figure 15. When the bending radius $R=30\ \text{mm}$ and $d_0=29\ \mu\text{m}$, the bending loss of the AR-HCF with nested structure is $4.72 \times 10^{-2}\ \text{dB/m}$. When $R=50\ \text{mm}$, the bending loss is $5.86 \times 10^{-3}\ \text{dB/m}$, and when $R=100\ \text{mm}$, the bending loss is only $9.93 \times 10^{-4}\ \text{dB/m}$. Compared with the single-layer structure, these results are three orders of magnitude lower (i.e., better) with a smaller bending radius and a larger bending degree. The fiber of this nested structure begins to be sensitive to the bending radius only when the bending radius is less than 30 mm. The righthand figure in Figure 15 shows the x and y polarization distribution of the core fundamental mode at bending radius $R=30\ \text{mm}$ and $d_0=29\ \mu\text{m}$. It can be seen that the fundamental mode is well-confined within the core. When a bending radius is fixed and the d_0 value is small, the casing gradually moves away from the core, which cannot play a good role in confining the light of the core, resulting in increased loss. When d_0 is large, the diameter of the casing is closer and closer to the cladding capillary, which will cause the proximity area of the two glass rings to gradually become larger, thus forming a thick glass ring similar to the air defect, which will increase the fiber loss. Therefore, it is necessary to select the appropriate d_0 value to reduce the limiting loss and increase the bending resistance. In this paper, $d_0=29\ \mu\text{m}$ is selected according to the calculation results.

For comparison with single-layer structures, the bending losses of $d_0=29\ \mu\text{m}$ and $R=100\ \text{mm}$ were calculated, as shown in Figure 16. In the illustration, we can see that the fundamental modes in both directions are well-confined within the core, and there are no leaked patterns in the cladding. In contrast, in the single-cladding structure (Figure 13 ($D=70\ \mu\text{m}$)), we can see that some patterns leak into the cladding. The results show that adding a nesting layer can effectively inhibit the coupling between cladding mode and fiber core mode to significantly reduce the bending loss. The curve of the virtual part of the effective refractive index changing with the bending radius in Figure 16(b) fundamentally explains that the nested structure (black curve) is not sensitive to the bending radius. The virtual part of the effective refractive index of the nested structure is always smaller than that of the single cladding structure, and the virtual part of the effective refractive index can intuitively show the loss of the fiber. The bending loss of the single cladding structure is obviously greater than that of the nested structure.

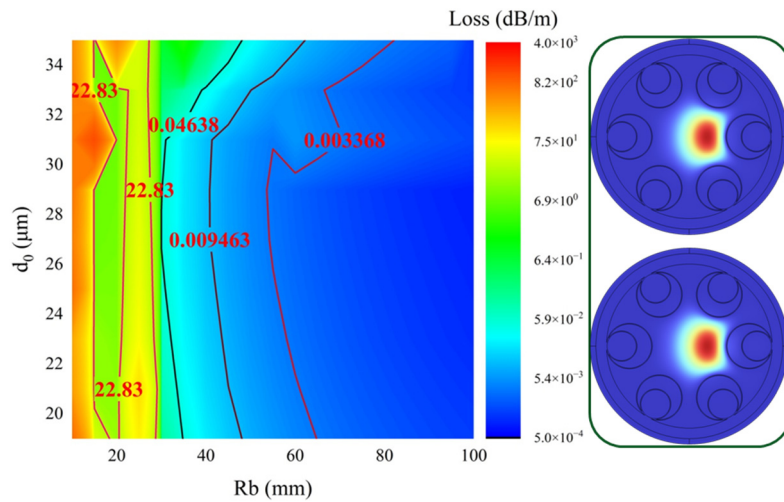


Figure 15. Fiber loss under different insert diameters and bending radii, and the distribution diagram of the core's fundamental mode field at $R=30\ \text{mm}$ and $d_0=29\ \mu\text{m}$.

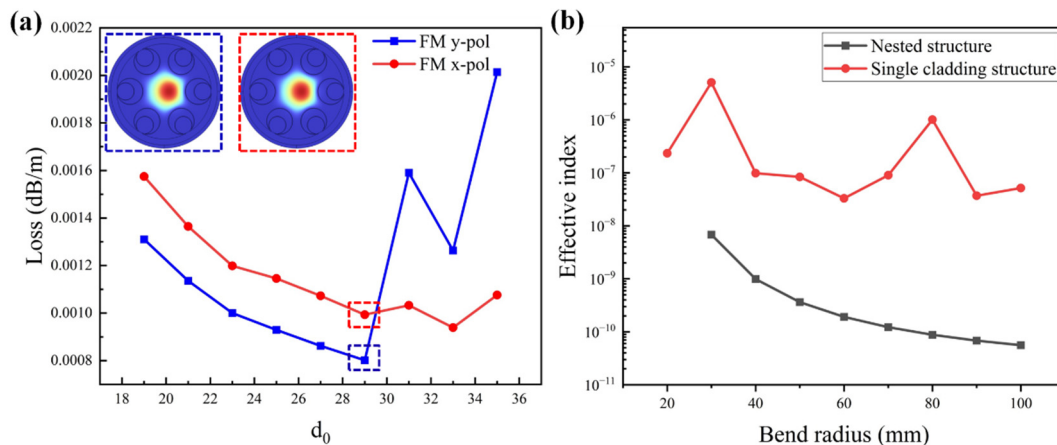


Figure 16. (a) The limiting loss value changes with d_0 when $R=100\ \text{mm}$. The illustration is the x and y polarization fundamental mode field distribution of the fiber core when $d_0=29\ \mu\text{m}$. (b) The variation curve of the imaginary part of the effective refractive index of the core of the nested structure and the single cladding structure with the bending radius.

4.2. Influence of Capillary Gap on Bending Loss

The core diameter is $70\ \mu\text{m}$, the capillary wall thickness is $0.71\ \mu\text{m}$, the inner diameter of the embedded tube is $29\ \mu\text{m}$, and the wavelength used in the simulation is $2.79\ \mu\text{m}$. We now discuss the influence of the capillary gap on the bending loss of the nested fiber. At the bottom of Figure 16 is a

larger view of some areas of the structure under consideration (the parts within the rectangles of different colors). It is worth noting that for all the simulated structures, in order to improve the accuracy of the simulation, a small penetration of $0.1 \mu\text{m}$ was added to all the cladding tubes, as illustrated by the enlarged diagram at the bottom of Figure 17(b).

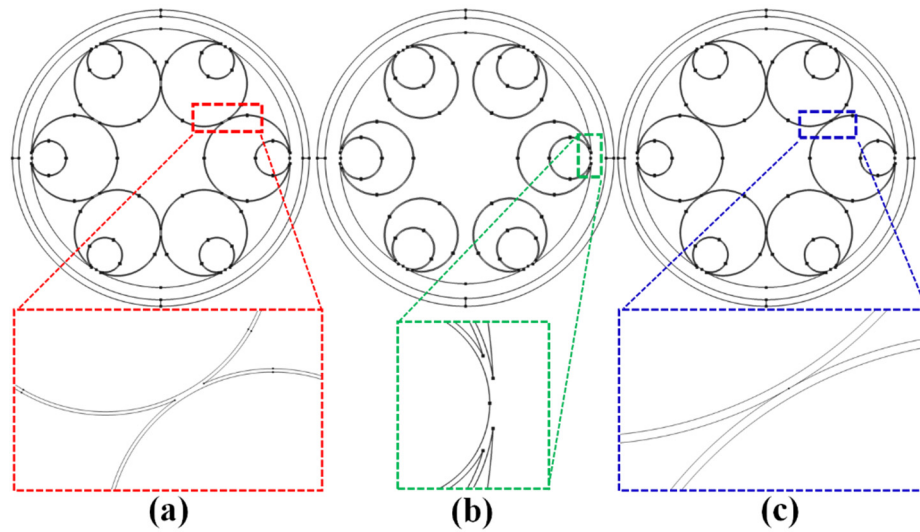


Figure 17. (a) Structure diagram of capillary gap less than 0, (b) structure diagram of capillary gap greater than 0, (c) structure diagram of capillary gap equal to 0.

We change the size of the gap by adjusting the ratio between the inner diameter of the outer layer tube and the diameter of the fiber core. For the convenience of expression, we define this ratio as τ , and the capillary gap is inversely proportional to τ . The calculation results are shown in Figure 17. In the structure of $\tau = 1$ (green line in Figure 18, structure in Figure 17(c)), the capillary gap is 0, and each capillary is tangent. In this configuration, the bending loss is large due to the strong influence of the coupling between the core base mode and cladding mode, and the limiting loss increases due to the generation of nodes. It can also be noted that the bending loss decreases when the cladding tube spacing increases (τ decreases). For more suitable tube spacing, the anti-resonant capillary drives the electric field away from its surrounding area, which causes a small percentage of the power to leak through the capillary, so the loss is minimal. However, when the bending radius is greater than 40 mm, $\tau=0.72$ corresponds to the smallest loss value. The main reason is that with the increase in pipe clearance, the leakage loss also increases. We conclude from this that since the amount of leakage increases as τ decreases, a correct balance is needed to design fibers with low bending losses.

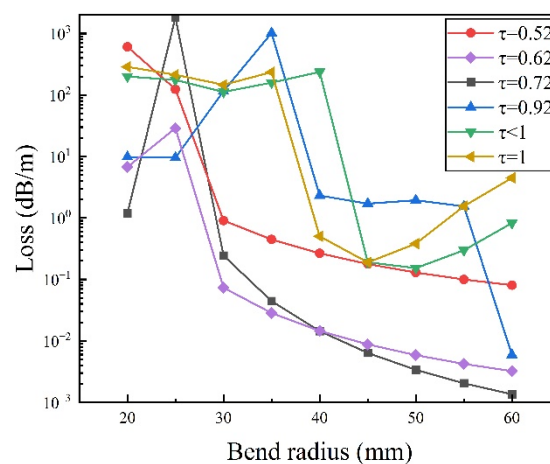


Figure 18. Bending loss corresponding to different capillary gaps.

5. Conclusions

In this paper, a negative curvature nested anti-bending low-loss anti-resonant hollow-fiber based on quartz material is proposed. The simulation results show that the radial air-glass anti-resonant layer is increased by the introduction of the nested anti-resonant tube, the weak interference overlap between the fiber core and cladding mode is reduced effectively, and the limiting loss of the fiber core is reduced effectively. The anti-resonant hollow-fiber fiber with this structure has a low limiting loss of 3.28×10^{-4} dB/m at the 2.79 μm band, has good bending resistance, and can maintain a fundamental mode loss of less than 4.72×10^{-2} dB/m at a bending radius as low as 30 mm. This bending resistance is far beyond the minimum bending radius of traditional solid-core fiber, allowing the new fiber to meet clinical requirements. We believe that the negative curvature nested structure scheme and the designed anti-resonant hollow-core fiber with large core diameter open up new possibilities for the application research of mid-infrared laser light conduction systems and the light transmission of 2.79 μm solid-state medical laser.

Author Contributions: Conceptualization, L.H. and H.J.; methodology, L.H.; software, L.H. and P.W.; validation, Y.W.; formal analysis, T.C. and L.H.; investigation, L.H.; resources, L.H. and L.W.; data curation, L.H.; writing—original draft preparation, L.H.; writing—review and editing, L.H.; L.W.; and H.J.; visualization, L.H.; supervision, H.J.; project administration, T.C.; funding acquisition, T.C.; and H.J.; All authors have read and agreed to the published version of the manuscript.

Funding: This work was funded by: Wanjia Center industrialization project (WJ21CYHXM06); National Key Research and Development Program of China(2018YFB0407204).

Institutional Review Board Statement: Not applicable.

Informed Consent Statement: Not applicable.

Data Availability Statement: Data underlying the results presented in this paper are not publicly available at this time but may be obtained from the authors upon reasonable request.

Conflicts of Interest: The authors declare no conflicts of interest.

References

1. Zheng, d., X.; Ling, L., J.; Ting, Q., C.; Hai, h., J. 100 Hz repetition-rate 2.794 μm Cr,Er:YSGG passively Q-switched laser with Fe2+:ZnSe saturable absorber. *Infrared Physics and Technology* **2022**, 122, 104087.
2. Guo, B.; Xiao, Q. L.; Wang, S. H. 2D layered materials: synthesis, nonlinear optical properties, and device applications. *Laser and Photonics Reviews* **2019**, 13, 1800327.
3. N. J. Scott; R. A. Barton; A. L. Casperson, A.; T., K.; Levin, D. Tran; N. M. Fried. Mid-IR germanium oxide fibers for contact erbium laser tissue ablation in endoscopic surgery. *IEEE J. Sel. Top. Quantum Electron.* **2007**, 13, 1709-1714.
4. N. M. Fried; Y. B. Yang; C. A. Chaney; D. Fried. Transmission of Q-switched Er :YSGG ($\lambda=2.79 \mu\text{m}$) and Er: YAG ($\lambda=2.94 \mu\text{m}$) laser radiation through germanium oxide and sapphire optical fibers at high pulse energies. *Lasers Med. Sci.* **2004**, 19, 155-160.
5. Andrey, D. P.; Alexander S. B.; Alexey, F. K.; Victor, G. P.; Sergei L. S.; E. M. D. Demonstration of a waveguide regime for a silica hollow - core micro-structured optical fiber with a negative curvature of the core boundary in the spectral region $> 3.5 \mu\text{m}$. *Opt. Express* **2011**, 19, 1441-1448.
6. Md. Selim, Habib; Ole, Bang; and Morten, Bache. Low-loss single-mode hollow-core fiber with anisotropic anti-resonant elements. *Opt. Express* **2016**, 24, 8429-8436.
7. J. B.; S. E. B.; Thomas, S.; Anders B. Analysis of air-guiding photonic bandgap fibers. *Opt. Lett.* **2000**, 25, 96-98.
8. G. J. Pearce; J. M. Pottage; D. M. Bird; P. J. Roberts; J. C. Knight; and P. St.J. Russell. Hollow-core PCF for guidance in the mid to far infra-red. *Opt. Express* **2005**, 13, 6937-6946.
9. Jonathan, Hu; Curtis, R. M. Leakage loss and bandgap analysis in air-core photonic band gap fiber for nonsilica glasses. *Opt. Express* **2007**, 15, 339-349.
10. Shuai, G.; Xin, W.; Hao, Q. J.; Zhen, X.; Shu, Q. L. Single-mode bend-resistant hollow-core fiber with multi-size anti-resonant elements. *Infrared Physics and Technology* **2022**, 123, 104159.

11. Liang, L.; Guan, J.; Zhu, X.; Wang, Y.; Wu, D.; Yu, F.; Han, Y. Delivery of Nearly Diffraction-Limited Picosecond Laser Pulses in the Air-Filled Anti-Resonant Hollow-Core Fiber at 1 μm Wavelength. *Photonics* **2023**, *10*, 416.
12. Xing, t. Z.; Xuan, R. W.; Xiaobo, L.; Jie L.; Lei Z.; Peng L.; Jing l. X.; Wen b. M.; Shu t. W. 5-tube hollow-core anti-resonant fiber with ultralow loss and single mode. *Optics Communications* **2021**, 501,127347.
13. Hua, B. L.; Yu, W.; Yan, Z.; Zu, G. G.; Zhang, W. Y.; Qiang L.; Si L., Jie S.; Don G. H.; Daru C. Low bending loss few-mode hollow-core anti-resonant fiber with glass-sheet conjoined nested tubes. *Opt. Express* **2022**, *30*, 21833-21842.
14. A. Urich; R. R. J. Maier; Fei, Y.; J. C. Knight; D. P. Hand; J. D. Shephard. Flexible delivery of Er: YAG radiation at 2.94 μm with negative curvature silica glass fibers: a new solution for minimally invasive surgical procedures. *Biomed. Opt. Express* **2013**, *4*, 193-205.
15. Fei, Y.; William J. Wadsworth; Jonathan C. Knight. Low loss silica hollow core fibers for 3-4 μm spectral region. *Opt. Express* **2012**, *20*, 11153-11158.
16. Walter, Belardi; Jonathan, C. Knight. Hollow anti resonant fibers with low bending loss. *Opt. Express* **2014**, *22*, 10091-10096.
17. Mariusz, K.; Dominik, D.; Amar, Nath, G.; Grzegorz, S.; Dariusz, P.; Guillaume, H.; Thibaut, S.; and R. B. Nested capillary anti-resonant silica fiber with mid-infrared transmission and low bending sensitivity at 4000 nm. *Opt. Lett.* **2019**, *44*, 4395-4398.
18. L. Vincetti and V. Setti. Extra loss due to Fano resonances in inhibited coupling fibers based on a lattice of tubes. *Opt. Express* **2012**, *20*, 14350-14361.
19. Santos, D. F.; G. A.; Baptista, J. M. SPR. Microstructured D-Type Optical Fiber Sensor Configuration for Refractive Index Measurement. *Sensors Journal IEEE* , **2015**, *15*, 5472-5477.
20. N. M. L.; A. K. A.; C. Headley; B. J. E. Anti-resonant reflecting photonic crystal optical waveguides. *Opt. Lett.* **2002**, *27*, 1592-1594.
21. Shi, B. Y.; Shu, Q. L.; Wan, Z.; Zheng, G. L. Single-polarization single-mode double-ring hollow-core anti-resonant fiber. *Opt. Express* **2018**, *26*, 31160-31171.
22. Da, K. W.; Fei, Y.; Mei, S. L. Understanding the material loss of anti-resonant hollow-core fibers. *Opt. Express* **2020**, *28*, 11840-11851.
23. C. F.; B. F.; Roberts, P. J.; Generation; Photonic. Guidance of Multi-Octave Optical-Frequency Combs. *Science*, **2007**, 318:1118-1121.
24. Francesco, Poletti. Nested anti-resonant nodeless hollow core fiber. *Opt. Express* **2014**, *22*, 23807-23828.
25. M. S. Habib; O. Bang; M. Bache. Low-Loss Hollow-Core Anti-Resonant Fibers With Semi-Circular Nested Tubes. *IEEE Journal of Selected Topics in Quantum Electronics* **2016**, *22*, 156-161.

Disclaimer/Publisher's Note: The statements, opinions and data contained in all publications are solely those of the individual author(s) and contributor(s) and not of MDPI and/or the editor(s). MDPI and/or the editor(s) disclaim responsibility for any injury to people or property resulting from any ideas, methods, instructions or products referred to in the content.