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Automatic epileptic seizure prediction based on convolutional neural network and EEG signal

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Abstract: Epilepsy is a neurological disorder that affects approximately 1% of the world's population. To diagnose and estimate the occurrence of epilepsy, neurologists analyze recorded brain activity. However, this process is not only time-consuming and tedious but also susceptible to occasional human error. Therefore, researchers have aimed to develop an automated method for diagnosing and **estimating** the occurrence of epilepsy in recent decades. In this study, we propose two new methods based on brain signals and a convolutional neural network (CNN). Our approach utilizes a sequential three-layer structure in the CNN. We conducted numerous experiments, and the proposed methods achieved an accuracy of 95% without feedback and 97% with feedback for estimating epilepsy. Our proposed methods outperform previous methods and have the potential to be employed as a physician's assistant in the field of operation.

Keywords: Epilepsy; Electroencephalogram; Convolutional neural networks; Brain signal integral; Brain signal derivative

1. Introduction

Epileptic seizures are a significant problem, affecting approximately 70 million individuals worldwide [1]. Currently, the disease is controlled and treated with medications in mild cases, and with surgery in acute ones. However, no definitive therapy is available yet [2, 3]. Patients with epilepsy cope with harmful risks in daily life (e.g., driving, sleeping, and doing daily activities) [4, 5-6]. Predicting epilepsy can prodigiously aid individuals with epilepsy [7]. Using Electroencephalography (EEG) to study brain signals is simpler and cheaper than the other methods [8, 9-10]. The traditional method of studying brain signals is complex, time-consuming, and error-prone [11]. Despite the introduction of novel techniques for diagnosing epileptic seizures, their clinical use has not yet been reported [12]. The epileptic patients' brain signals are divided into ictal and inter-ictal [13]. Besides, in the classifiers' section, classifier types such as Support Vector Machine (SVM), Sparse Representation classification (SRC), the K-Nearest Neighbor (KNN), and the Multilayer Perceptron (MLP) are employed [14,15]. In older techniques, statistical properties were used as attributes, including mean, standard deviation, median, irregularity, elongation, skewness, and signal energy [16, 17-18]. Another technique proposes creating 3D images of brain signals and applying them to a CNN to diagnose and estimate epileptic seizures [19]. In recent studies, using a CNN has been widespread in diagnosing and estimating epileptic seizures. To increase the accuracy of this method, functions were used before the CNN. Such functions have significantly increased these methods' accuracy from 58% to about 93%. The so-called principle functions embrace the use of Principal Component Analysis (PCA) and Independent Component Analysis (ICA) [20]. Another utilized function before the CNN is the Fast Fourier transform function [21]. An additional

central technique was the time-frequency domain conversion [22, 23]. The Reconstructed Phase Space (RPS) technique is the other critical utilized function before the CNN [24]. The Pearson correlation coefficient and maximum information coefficient were the other functions used to increase the method's accuracy in such studies [25]. Zuyi Yu et al. used a Local Mean Analysis (LMD) before CNN to extract the feature [26]. Jana. R et al. generated sub-signals with a sampling time of 1 second to test and train the CNN [27]. S. Muhammad Usman et al. used the time-frequency domain conversion as a primary feature to increase the accuracy of the algorithm [28]. In the study of Abdulnasir Yildiza et al., the domain-time conversion of brain signals along with class activation mapping of brain signals was used [29]. Zuochen Wei et al. reported the initial feature by using the maximum and minimum points of brain signals called MIDS prior to the CNN [30]. S. Raghu et al. used frequency spectrum as a primary feature before CNN [31]. S. R. Ashokkumar et al. exploited two different primary functions, including time-frequency conversion and entropy as two primary features before the CNN with the intention of diagnosing epileptic seizures [32]. J. Lian et al. used the relationship between different channels signals as a primary feature [33]. In the reviewed sources, applying a function prior to the CNN augmented the accuracy by approximately 58% and the accuracy with the numerical value of 93% has been reported. Since accessing the accuracy of more than 93% was a demanding challenge to overcome in the above-mentioned studies, a newly proposed method is presented. In the present paper, by using brain signals, a combined function incorporating integral signal, derivative signal, and the main signal itself before the CNN were utilized with the intention of automatic detection and estimation of epileptic seizures and enhancing the accuracy of the method. In the current investigation, the output of the hybrid function included an integral signal with KI coefficient and derivative signal with KD coefficient, as well as the signal itself with KP coefficient. However, these coefficients were selected as variables to achieve maximum accuracy. Thenceforth, after selecting the so-called coefficients and magnifying the differences in the three states of brain signals using the stated hybrid function, a CNN was employed to create the final feature and decision.

2. Materials and Methods

In the present section, the exploited database in the current study will be examined and the mathematical background related to the convolutional neural networks will be presented.

2.1. *DATA*

In the present inquiry, Brain signals were used from the Massachusetts Institute of Technology database (MIT, USA), which includes data of the 16 participants with 23 channels, with a sampling frequency of 256 Hz. From the so-called 16 participants, 11 were female and 5 male. Epileptic seizures occurred for several minutes during the recording of brain signals in 16 participants. The age range of females was between 1.5-19 years and for the males was 3-22 years. For each of the selected data, the onset and ending time of the epileptic seizure has been determined, which is different for each participant in the test. The brain signals with a sampling time of 1 second of the subjects were divided into 3 classes, including ictal, pre-ictal, and inter-ictal. Besides, the number of samples to be tested were equally selected for all three modes (i.e., ictal, Pre-ictal, and Inter-ictal).

2.2. *Convolutional neural network*

The CNN was introduced in 1998 by Fukushima [34]. It was not widely used in the early periods due to hardware and computational limitations for network training.
 Sermanet et al used the CNN in 2013 for large-scale imaging and film detection [35]. In recent years, convolutional neural networks were extensively used in studies of brain signals, including the prediction of epileptic seizures [36]. The CNN is designed and configured in accordance with the input information of the neural network in various respects, incorporating one-dimensional, two-dimensional, and in some cases three-dimensional. In this configuration, the input data is applied to the neural network as an n × m image. The above neural network consists of three main layers embracing the

convolutional layer, Max Pooling Layer, and fully connected layer. The structure of each of these layers will be described in the following sections.

2.2.1. Convolution Layer

In the convolutional layer, the input images to the neural network were swept with a kernel. The dimensions of the kernels vary according to the design and were selected as 3 × 3 and sometimes 5 × 5. In the above layer, images were created from the input image according to the number of selected filters as a feature. In most neural network architectures, 32 filters were selected. But in this study, to reduce the computational load, after a trial and error, 8 filters were selected. In summary, the function of the conventional layer can be expressed by Equation 1, in which z_n^{in} is the input matrix and z_j^{out} is the output matrix of the conventional layer. Where x_{nj} and b_j are the convolution filter between the n-th offset matrix of the neurons corresponding to the j-th output map. In this regard, f is a nonlinear activation function. The popular activation function are sigmoid, tanh and rectified linear unit (ReLU), etc. in the present work, ReLU is selected for activation function and equation 2 shows the ReLU function.

$$z_j^{out} = f\left\{\sum_n z_n^{in} \otimes x_{nj} + b_j\right\} \tag{1}$$

$$f(x) = \begin{cases} x & if \ x \succ 0 \\ 0 & other \end{cases} \tag{2}$$

2.2.2. Max Pooling Layer

In the Max Pooling layer, the image dimensions were reduced. In this layer, the produced images were reduced in the convolutional layer of the sampling. In other words, the dimensions of the images were halved in this layer. The equation 3 is shown rule of the max-pooling layer.

$$z^{out} = subsampling(z^{in}) \tag{3}$$

2.2.3. Fully-connected Layer

In the fully connected layer, the properties of the input images were displayed in pixels. Following several convolutional and Max Pooling operations, in the fully-connected layer, the properties appeared as pixels, which were represented as a vector. In the fully connected layer, the created vector was used for the final decision.

2.3. Proposed method

This section describes our proposed method for predicting and diagnosing epileptic seizures, which consists of two separate approaches. The first method, called the Basic suggestion method, is illustrated in Figure 1. To detect and predict epileptic seizures in this method, we utilized a proposed function and a CNN. First, the brain signals were segmented into one-second intervals, and then passed through the proposed function, which is explained in more detail below. The output of the proposed function was then converted into 2D images in the 'convert to image' section, and these images were subsequently fed into the CNN to extract features and make the final decision. To enhance the accuracy and reliability of our approach, we also developed an alternative method called the feedback proposed method, which is depicted in Figure 2. In our proposed method, we utilized feedback from the algorithm's accuracy results to optimize the proposed function by adjusting the values of the proportional coefficients KP, derivative coefficient KD, and integral coefficient Ki. During the pre-ictal state and particularly near the onset of the main epilepsy (ictal state), the frequency of sub-bands of brain signals changes compared to the inter-ictal state. Therefore, it is essential to detect these changes. To accomplish this, we employed a second-order system whose parameters,

including KP, KD, and Ki, are automatically adjusted based on the resulting accuracy. The changes to the coefficients continue until the maximum accuracy is attained, at which point the values of KP, KD, and Ki become stable. The output of this system differs for ictal, pre-ictal, and inter-ictal states. Consequently, the resulting images from the output of the system also vary depending on the pre-ictal or inter-ictal state.
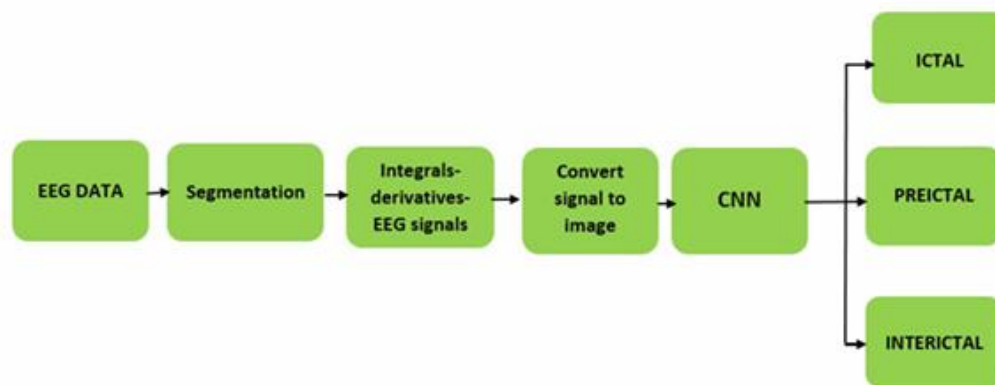

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Figure 1. Block diagram of the Basic Suggestion Method.
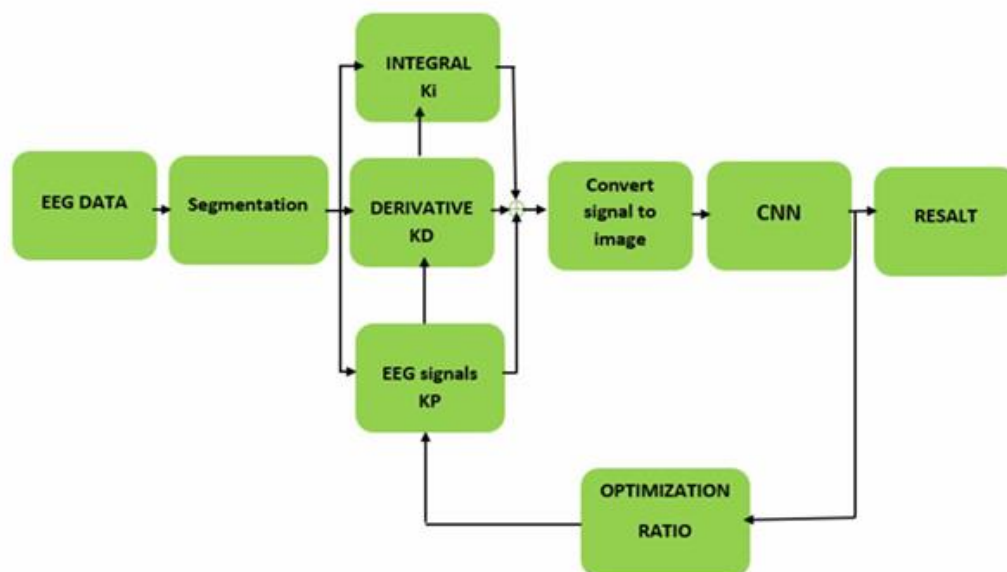

Figure 2. Block diagram of the proposed feedback method.

2.3.1. Data preprocessing

In this section, we describe the preprocessing steps and the performance of the proposed function to prepare the brain signals for the CNN application. Firstly, we extracted brain signals with a duration of 1 second for three modes: Ictal, Pre-ictal, and Inter-ictal, from the Massachusetts Institute of Technology (MIT, USA) database, as shown in Figures 3, 4, and 5. Then, we converted these signals into 2D images using the 'imagesc (A)' command available in MATLAB software, which displays the 256×23 matrix as an 876×586 image. **It should be noted that for each of the mentioned modes, 200 image samples were created for testing.** In order to apply these images to the neural network, we resized them to 64×64 dimensions, as shown in Figure 6. To create the initial feature of the segmented

brain signals, we passed these signals through the proposed function, as shown in Figure 7. The function consisted of the sum of signal integrals, signal derivatives, and the signal itself, with coefficients Ki, KD, and KP. We used the proposed function to extract the features from the brain signals before applying them to the CNN.

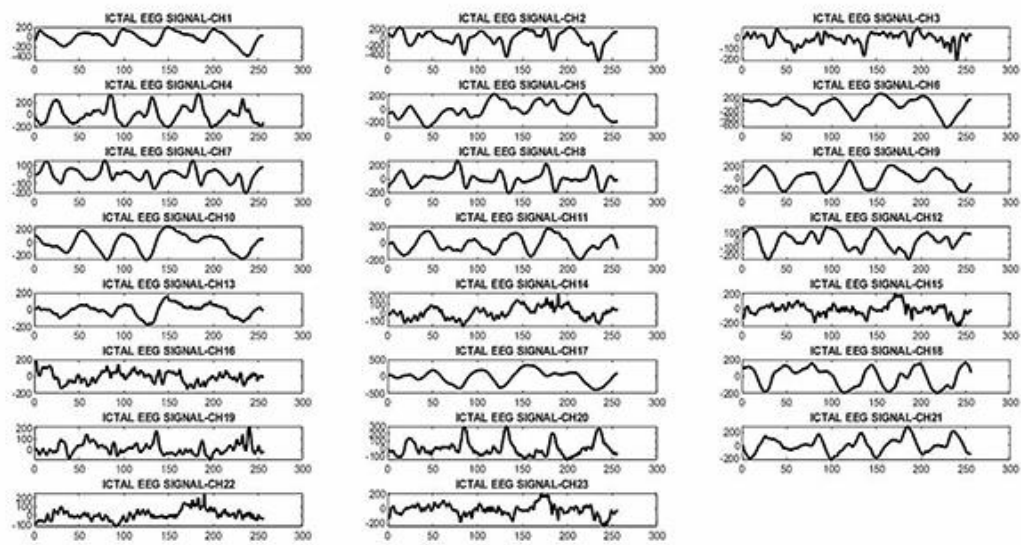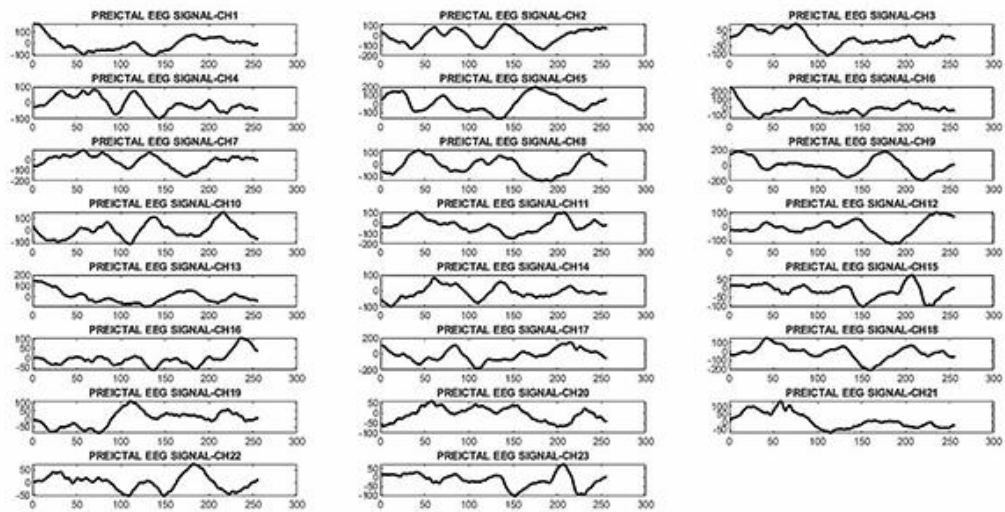**Figure 3.** 23 channel signal in ictal mode.
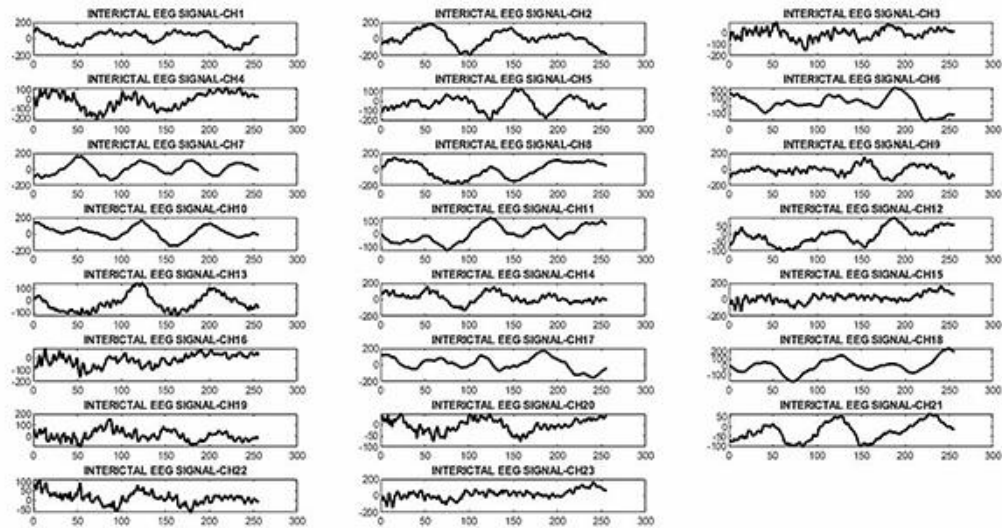

Figure 4. 23 channel signal in pre-ictal mode.

Figure 5. 23 channel signal in inter-ictal mode.
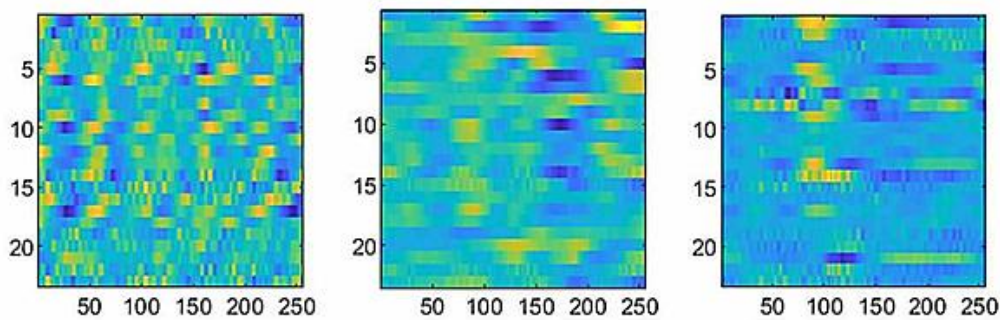
Figure 6. Images generated from ictal, pre-ictal, and inter-ictal brain signals.
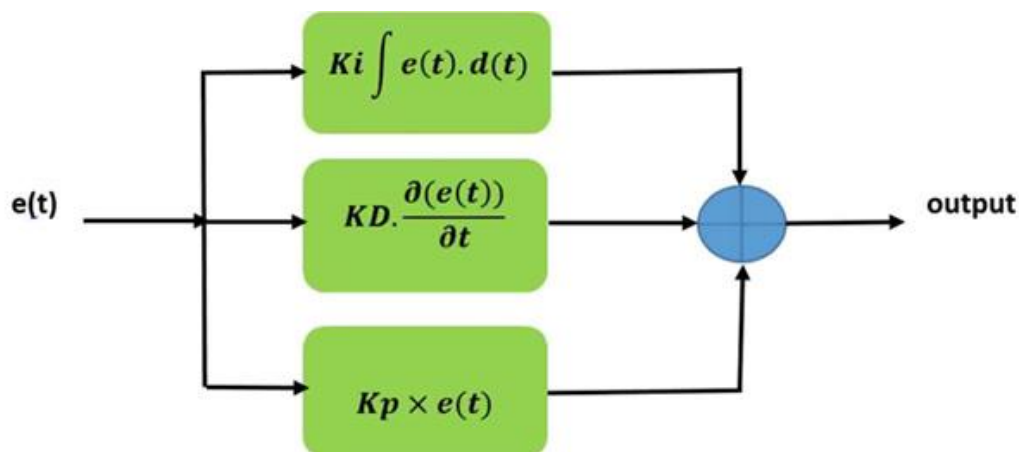
Figure **7.** Block diagram of the proposed function.

2.3.2. Proposed neural network architecture

In the present study, the CNN was used with the structure shown in Figure 8 to extract the features from the images produced by the proposed function and the final decision. The presented structure was obtained through trial and error, and the precise characteristics are shown in Table 1 for each of the convolutional neural networks used in the test. This structure is divided into three

parts, each with a convolutional layer and a max pooling layer. In the last part of the architecture, a full connection layer was utilized for the final decision. Moreover, a 3 × 3 mask was used for the convolution of the input images in each of the convolutional layers, and the results of the convolutional classes were then passed through a ReLU function, which benefited from the Arctanh function. At the output of the first part, from the input image with dimensions of 64 × 64, 8 images were produced with dimensions of 64 × 64. Down-sampling operations were performed on the aforementioned images in the following max pooling layer, yielding images with 32 × 32 dimensions. At the output of the second part, from the input image with dimensions of 32 × 32 resulting from the first layer, 16 images with dimensions of 32 × 32 were generated in the convolutional layer. Subsequently, in the max pooling layer, down-sampling operations were performed on the above-stated images, and images with 16 × 16 dimensions were created. In the output of the third part, from the input images with dimensions of 16 × 16 produced in the second layer, 32 images with dimensions of 8 × 8 were produced. The dimensions of the input and output images of each of the above classes are shown in Table 2. In the deep neural network, the results obtained from the third layer included 2048 pixels. However, for the final decision, only 1024 significant pixels have been selected from the total number of pixels.
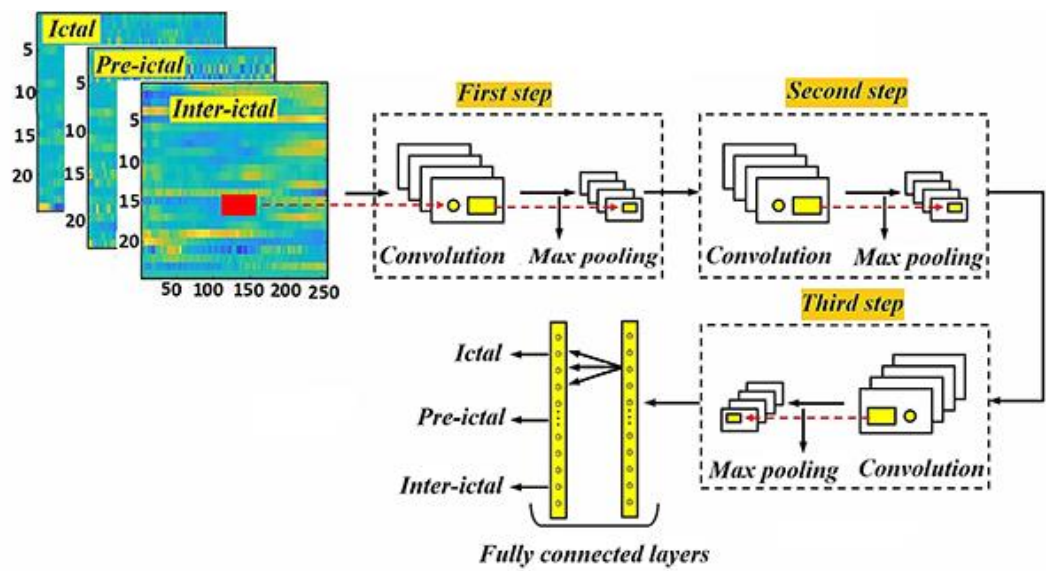
Figure 8. Convolutional neural network configuration.

Table 1. Characteristics of each convolutional neural network used in the test.

Parameter	Search Space	Optimal Value
Optimizer	RMSProp, Adam, Sgd, Adamax, Steplr, Cycliclr	Sgd
Cost function	MSE, Cross-entropy	Cross-entropy
Dropout rate	0,0.2,0.3,0.4,0.5	0.2
Batch Size	4,8,10,16,32,64,100	4
Learning rate	0.01,0.001,0.0001	0.0001
Momentum and Gamma Parameters	0.6,0.7,0.8,0.9	0.9
Decay Rate of the Weights	$2e^{-4}, 3e^{-4}, 4e^{-4}, 5e^{-4}, 6e^{-4}$	$5e^{-4}$
Activation function after the BN Layer	Leaky-Relu , Sigmoid , Relu , Linear	Relu
Activation function in the first FC Layer	Leaky-Relu , Sigmoid , Relu , Linear	Relu
Activation function in the Last Layer	Softmax, Sigmoid	Softmax

Table 2. Dimensions of input and output images for each convolutional neural network used in the study.

Convolutional network architecture	Filter dimensions	Input image dimensions	Dimensions of the output image of the convolutional floor	Dimensions of Max Pauling floor output image	Number and dimensions of the output image
First part	3×3	64×64	64×64	32×32	8@(32×32)
second part	3×3	32×32	32×32	16×16	16@(16×16)
third part	3×3	16×16	8×8	8×8	32@(8×8)

2.3.3. Data collection training and evaluation

In this part, initially, the data for each of the individuals were divided into 3 modes: ictal, pre-ictal, and inter-ictal, with a 1-second sampling interval. Afterward, the data of the individuals were separately tested with the proposed methods. Next, from the data of 16 individuals, the data of 10 participants were selected whose epileptic seizures were longer than those of other individuals. Subsequently, the data of the 10 participants were combined in two ways: an identical merge and a non-identical merge. In the identical merge mode, 60 samples were selected equally from 10 participants for each of the ictal, pre-ictal, and inter-ictal modes. Finally, 600 sample images were collected for each of the 3 modes. In total, 1800 sample images were selected for each of the three modes mentioned. Figure 9 describes how the test ratio is selected based on the above-stated training. Data were randomly selected from each individual in the non-uniform merging mode, with a different number of samples for each of the three modes mentioned. The test-to-train ratio was selected at 20% to 80%, respectively, for each of the identical and non-identical merges and independent reviews of the data of each participant in the current analysis.
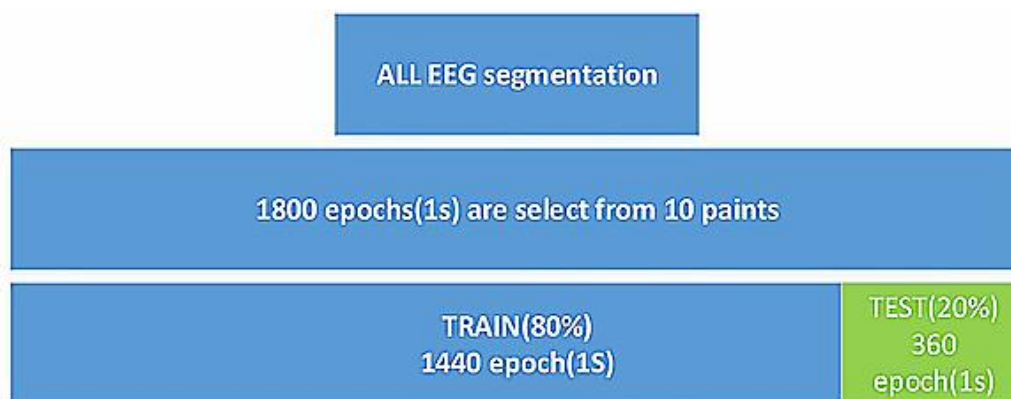

Figure 9. Illustrates the process of testing and training the convolutional neural network.

3. Results

In order to improve the accuracy of the method, the images were used as input to the CNN in this study. At the output of the proposed function, 2D images were generated as illustrated in Figure 10.
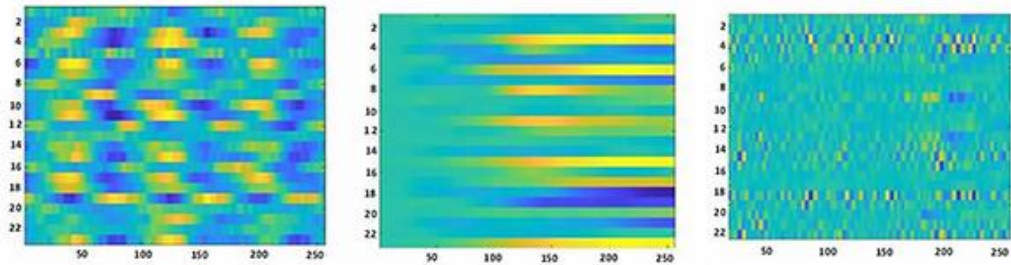

Figure 10. Image generated by applying a hybrid function to ICTAL-INTERICTAL-PRE-ICTAL brain signals

In order to prove the suggested features for the proposed method and the identical and non-identical merge methods, various tests were performed on the data obtained from patients, the results of which are presented separately to confirm the accuracy of the proposed method compared to other techniques. **The tests conducted were generally of three classes and included ictal, pre-ictal, and inter-ictal.** The results obtained from the tests of 16 patients were almost the same and therefore, in the following the results obtained from patients' number 08-21 are presented. In the present study, in order to demonstrate the effects of KP, Ki, and KD coefficients, various experiments were performed on the collected data from the CHB-MIT database, the results of which are shown in Table 3.

Table 3. Test results of conventional method and the effects of KP, Ki, and KD coefficients on data obtained from the CHB-MIT database.

Patient ID	conventional method			basic method KP=0.5,KI=0.5,KD=5			basic method KP=0,KI=0,KD=5			basic method KP=KD=0,KI=10		
	acc	sen	spe	acc	sen	spe	acc	sen	spe	acc	acc	acc
1	0.611	0.781	0.720	0.8650	0.7738	0.8539	0.5833	0.9184	0.2333	0.6465	0.8387	0.5581
2	0.682	0.697	0.690	0.8565	0.7674	0.8621	0.6204	0.8889	0.3929	0.6162	0.7143	0.5641
3	0.656	0.660	0.658	0.7037	0.6239	0.7596	0.5463	0.8333	0.1724	0.6667	0.6458	0.7500
4	0.642	0.687	0.666	0.8608	0.8608	0.8132	0.5048	0.5345	0.4750	0.4921	0.4412	0.5625
5	0.600	0.645	0.623	0.8481	0.7778	0.8352	0.5714	0.6364	0.6389	0.5556	0.4999	0.7619
6	0.595	0.632	0.615	0.8312	0.7529	0.8242	0.5048	0.5345	0.4750	0.5873	0.4865	0.8542
7	0.620	0.666	0.643	0.8186	0.7294	0.7912	0.5349	0.7143	0.4717	0.5476	0.4881	0.8810
8	0.684	0.707	0.696	0.7829	0.7447	0.8077	0.5581	0.7547	0.4902	0.6984	0.5857	0.8667
9	0.642	0.625	0.633	0.8519	0.7660	0.9189	0.4806	0.7143	0.3922	0.6190	0.5181	0.8571
10	0.652	0.641	0.646	0.6952	0.5435	0.7500	0.5079	0.6418	0.5000	0.5079	0.6667	0.5714

11	0.657	0.649	0.653	0.8083	0.7334	0.8333	0.6566	0.7500	0.6154	0.6977	0.6744	0.6780
12	0.663	0.660	0.661	0.7847	0.7170	0.7963	0.7172	0.7381	0.6944	0.6883	0.5957	0.6939
13	0.645	0.628	0.636	0.8186	0.7619	0.7826	0.6162	0.7143	0.5641	0.7172	0.7381	0.6944
14	0.653	0.643	0.648	0.7132	0.8000	0.6905	0.7048	0.6739	0.7941	0.6667	0.6458	0.7500
15	0.636	0.615	0.625	0.7265	0.6465	0.7907	0.6970	0.7200	0.6452	0.7048	0.6739	0.7941
16	0.632	0.609	0.620	0.7847	0.7170	0.7963	0.4952	0.5818	0.5750	0.6286	0.5273	0.7317

The table also shows the results of conventional method tests, which could be useful for comparing with the results of the basic method. In order to determine the influence of each of the mentioned coefficients, various experiments were conducted on one of the samples. In all stages of these experiments, one of the coefficients of the variable was selected and the other coefficients were kept constant. The results of these experiments are shown in Tables 4 and 5.

Table 4. Test results of the effect of the KD coefficient on the information downloaded from the CHB-MIT database of patient No. 08.

patient No. 08	basic method KP=0.5,KI=0.2			basic method KP=0.3,KI=0.3			basic method KP=0.3,KI=0.5			basic method KP=0.3,KI=0.6		
	%acc	%sen	%spe	%acc	%sen	%spe	%acc	%sen	%spe	%acc	%sen	%spe
KD=0.1	0.8608	0.8235	0.8161	0.8734	0.7907	0.8824	0.8734	0.8118	0.8588	0.8945	0.8608	0.8506
KD=0.2	0.8608	0.7952	0.8333	0.9072	0.8391	0.9136	0.8228	0.7556	0.8111	0.9156	0.8750	0.8851
KD=0.3	0.8734	0.8000	0.8636	0.8861	0.8295	0.8941	0.8861	0.8391	0.8706	0.8523	0.7727	0.8636
KD=0.4	0.8439	0.7294	0.8539	0.8861	0.8276	0.8824	0.8887	0.8395	0.8750	0.9072	0.8537	0.8953
KD=0.5	0.9072	0.8571	0.8929	0.9072	0.8675	0.8824	0.8903	0.8452	0.8706	0.8861	0.8395	0.8506
KD=0.6	0.8903	0.8140	0.8996	0.8439	0.7447	0.8721	0.8439	0.7391	0.8721	0.8819	0.8421	0.8352
KD=0.7	0.8481	0.7831	0.8222	0.8734	0.8049	0.8539	0.8891	0.7791	0.9176	0.8692	0.8353	0.8576
KD=0.8	0.8987	0.8022	0.9286	0.8861	0.8395	0.8506	0.8945	0.8214	0.8941	0.8945	0.8434	0.8736
KD=0.9	0.8776	0.8415	0.8409	0.8734	0.7955	0.8824	0.8819	0.8375	0.8409	0.8987	0.8391	0.8902
KD=1.00	0.8945	0.8642	0.8506	0.8819	0.8313	0.8506	0.8776	0.8313	0.8636	0.8819	0.8333	0.8953

Table 5. Test results of the effect of the Ki coefficient on the information downloaded from the CHB-MIT database of patient No. 08.

patient No. 08	basic method KP=0.4,KD=0.9			basic method KP=0.5,KD=0.9			basic method KP=0.6,KD=0.9			basic method KP=0.7,KD=0.9		
	%acc	%sen	%spe	%acc	%sen	%spe	%acc	%sen	%spe	%acc	%sen	%spe
Ki=0.1	0.8565	0.8721	0.8172	0.8608	0.8608	0.8132	0.8608	0.7955	0.8571	0.8987	0.8919	0.8352
Ki=0.2	0.8776	0.8642	0.8391	0.9114	0.8690	0.9059	0.8565	0.7792	0.8211	0.8734	0.8424	0.8523
Ki=0.3	0.8565	0.8101	0.8111	0.8603	0.8118	0.8363	0.8692	0.8272	0.8352	0.9030	0.8452	0.9048
Ki=0.4	0.8903	0.8500	0.8636	0.8481	0.7778	0.8352	0.8143	0.7284	0.7872	0.8650	0.8272	0.8409
Ki=0.5	0.8312	0.7529	0.8242	0.8565	0.8023	0.8427	0.8776	0.8125	0.8556	0.8650	0.7976	0.8506
Ki=0.6	0.8397	0.8705	0.8043	0.8565	0.8272	0.8111	0.8776	0.7976	0.8636	0.8903	0.8519	0.8523
Ki=0.7	0.8397	0.7412	0.8352	0.8776	0.8333	0.8444	0.8776	0.8072	0.8652	0.8650	0.8140	0.8588
Ki=0.8	0.8945	0.8353	0.9059	0.8692	0.8493	0.8105	0.8819	0.8500	0.8523	0.8945	0.8659	0.8605
Ki=0.9	0.8565	0.8068	0.8488	0.8481	0.7412	0.8539	0.8734	0.8171	0.8427	0.8987	0.8235	0.8953
Ki=1.00	0.8186	0.7294	0.7912	0.8945	0.8395	0.8652	0.8608	0.7619	0.8556	0.8945	0.8642	0.8506

Furthermore, in order to compare the results of the patient's classified information, **including inter-ictal, ictal, and pre-ictal,** the proposed feedback method (Figure 2) was applied, and 97% accuracy was obtained, which indicates an increase of 4% compared to the results of previous studies. Moreover, according to the results of the experiments, the effect of the KD coefficient can be observed on the downloaded information from the CHB-MIT database, and the best case in Table 4 is related to the coefficients KI = 0.6, KP = 0.3, and KD = 0.2. By examining the test results, the effect of the Ki coefficient can be realized on the downloaded information from the CHB-MIT database, the best case of which is shown in Table 5 and is related to the coefficients KP = 0.5, KI = 0.2, and KD = 0.9. The mentioned steps were performed using the feedback method and 97% accuracy was obtained. In the next step, the signals of 10 participants were merged into two identical and non-identical partnerships. Table 6 shows the results of the identical and non-identical participatory integration tests for the base method.

Table 6. Results of identical and non-identical integration tests on the base method.

	KP, Ki and KD coefficients	Results of identical integration tests			Results of non-identical integration tests		
		%acc	%sen	%spe	%acc	%sen	%spe
1	basic method KP=0.3,Ki=0.1,KD=0.8	0.6694	0.7329	0.6620	0.5048	0.5345	0.4750
2	basic method KP=0.3,Ki=0.8,KD=0.5	0.6148	0.7288	0.6000	0.5048	0.5345	0.4750
3	basic method KP=0.3,Ki=0.8,KD=0.2	0.6889	0.6942	0.7500	0.5048	0.5345	0.4750
4	basic method KP=0.3,Ki=0.4,KD=1	0.7037	0.6239	0.7596	0.5714	0.6364	0.6389
5	basic method KP=0.2,Ki=0.8,KD=0.2	0.6704	0.6466	0.7027	0.4762	0.4800	0.5217
6	basic method KP=0.3,Ki=0.8,KD=0.5	0.7000	0.6917	0.7624	0.5048	0.5345	0.4750
7	basic method KP=0.2,Ki=0.7,KD=2	0.7037	0.6581	0.7670	0.5714	0.6364	0.6389
8	basic method KP=0.7,Ki=0.2,KD=2	0.6926	0.6789	0.7156	0.8945	0.8642	0.9059
9	basic method KP=Ki=0.1,KD=5	0.7000	0.6695	0.7596	0.5079	0.6418	0.5000
10	basic method KP=Ki=0.1,KD=2	0.9114	0.8690	0.8506	0.5079	0.6418	0.5000

It can be observed in Table 6 that the maximum percentage of identical and non-identical participatory integration for the base method is related to the states KI = KP = 0.1, KD = 2. The mentioned steps were performed using the feedback method. Following the implementation of the feedback method for identical and non-identical participatory integration modes, all different values for KP, Ki, and KD coefficients were automatically tested, and finally, the feedback algorithm determined the maximum accuracy. It is noteworthy that in this evaluation, the maximum accuracy was 95% for the integration of identical participation and 93% for the integration of non-identical participation. The proposed base method is shown in Figure 1. According to this figure, it is evident that the existence of the new function leads to a significant improvement in the accuracy of the method. The feedback proposed method, which is in fact a combination of the feedback and the basic suggestion method, was presented in Figure 2 in order to enhance the performance of the basic structure. The advantages of this method incorporate higher reliability and enhanced accuracy than the conventional method and the proposed basic method. It should be noted that the primary function has not been used in conventional methods and therefore exhibits low accuracy and sensitivity. In order to analyze the data in each of the proposed methods and the conventional method, several testing and training techniques were applied. One of these techniques is the conventional method in which the testing and training of the CNN are considered separately for each participant. The second technique

of testing that is applied to the proposed method and the conventional method is the participatory approach of uniform integration of the data of the test subjects. Both the proposed method and the conventional method utilized the same data for the training and testing of neural networks. However, in the participatory method(uniform and non-uniform integration), image data was divided into three classes, including epilepsy, pre-epilepsy, and normal state, and were utilized non-uniformly in the testing and training of convolutional neural network. The main feature of these techniques of identical and non-identical integration is that they make it conceivable for epilepsy diagnosis and prediction methods to be universally available for patients with epileptic seizures. In other words, it prevents the diagnostic device from being proprietary to a particular patient, which diminishes the additional costs associated with designing and manufacturing proprietary equipment. Indubitably, it should be noted that the power of generalization in the non-identical participation method was much greater than the identical integration method in a way that the data of individuals outside the sampling can also be evaluated. Using the results obtained from the application of the developed integration approach on the proposed methods and conventional method, it is observed that the accuracy of the feedback and basic methods was much higher than the conventional method and can be employed in various applications such as clinical therapies and medical diagnostic equipment. Table 7 illustrates a comparison between the results of the proposed method and the conventional method. According to this table, it is observed that under comparable conditions and by using the same participation method, the accuracy of the feedback, basic, and conventional methods is equal to 95%, 91%, and 50%, respectively. It should be noted that conventional methods are those in which no function or filter is used to extract the signal feature and the signal is directly applied to the neural network. However, these results are slightly lower than the ones obtained with a similar method through the application of the non-identical integration method. The accuracy of the feedback, basic, and conventional methods are 93%, 89%, and 47%, respectively. Table 8 exhibits a detailed comparison between the proposed methods and the previous studies. According to the results of Table 8, it is observed that the proposed methods, under the same conditions, including the use of the same database, demonstrated a significant advantage in the values of accuracy, sensitivity, and specificity. The only limitations of the proposed method were the time required for the implementation of the proposed feedback method, which took around 14 hours for training and initial testing, of which 11.2 hours were training time and 2.8 hours were testing time.

Table 7. Comparison between the results of the proposed methods and the conventional method.

case	method	Accuracy% non-uniform integration method	Accuracy% uniform integration method
1	conventional method	47%	50%
2	basic method	89%	91%
3	feedback method	93%	95%

Table 8. Comparison between the results of the proposed method and other methods.

Case	Authors	Dataset	Accuracy%	Sensitivity%	Specificity%
1	Xiaoyan Wei et al, 2018.[19]	Department of Neurology-Xinjiang Medical University	90	88.9	93.78
2	M. Hosseini et al , 2017.[20]	the Center for Epilepsy	93	94	94
3	Mengni Zhou1 et al, 2018.[21]	The CHB-MIT	91.1	83.6	85.1
4	Zhang, S. et al , 2020.[25]	The CHB-MIT	89.98	92.9	87.04
5	Zuyi Yu · Weiwei Nie, 2018.[26]	the Center for Epilepsy at Freiburg University Hospital in Germany	-	87.7	-
6	Jana R., 2020.[27]	The CHB-MIT	94.33	96	94.39
7	S. Muhammad Usman, 2020.[28]	The CHB-MIT	-	92.7	90.8
8	Zuochen Wei, 2019.[30]	The CHB-MIT	81.49	70.68	92.30
9	S. Raghu, 2020.[31]	The Temple University Hospital (TUH)	88.3	88.4	84.1
10	proposed method	The CHB-MIT	97.1	97.5	96.3

4. Discussion

In the present paper, a basic method and a feedback method were proposed for predicting, detecting, and analyzing brain signals in epileptic seizures. In addition to these two methods, two novel testing and training methods were introduced in order to achieve a method of prediction and diagnosis of generalized epileptic seizures called the identical integration participatory method and the non-identical integration participatory method. According to the execution time of the program and the accuracy of the previous experiments, 600 image samples were selected to perform the identical and non-identical integration tests. It should be noted that initially, the different data integration methods have been investigated using the conventional and the base methods. By examining the results, it is clear that the proposed method was able to enhance the response accuracy of the method by intensifying the accuracy by 50%. After reviewing the results of the conventional method, two proposed methods of merging equal and unequal participation were applied to the proposed methods: the basic method, and the feedback method. Examining the results obtained from the experiments, it was shown that compared to the conventional method, both proposed basic and feedback methods led to enhanced results. Furthermore, using the obtained results, it was found that by applying the identical and non-identical participatory methods, the accuracy degree of the conventional method was equal to 50% and 47%, respectively. However, under similar conditions, applying the basic and feedback methods achieved better results. Hence, the accuracy of the basic method was equal to 91% for the identical participation method and 89% for the non-identical participation method. It should be noted that the accuracy of the proposed feedback method by applying the identical method of integration was equal to 95% and for the method of non-identical participation was equal to 93%. These results indicated that the proposed basic method along with the feedback method demonstrated the ability to enhance accuracy. Therefore, they can be used to reduce the error in the epileptic seizure in a short period, as well as the side costs of manufacturing medical equipment. It should also be noted that the main feature of applying the proposed participatory methods was to make it possible to build equipment for predicting and diagnosing epilepsy as a unit for all patients so that the constructed device could be initially trained with the initial data recorded in the computer and subsequently be utilized by the public without any necessity for re-training.

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