

Article

Biodegradable Polymer Nanosheets Incorporated with Zn-Containing Nanoparticles for Biomedical Applications

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Abstract: So far, poly(L-lactic acid), PLLA, nanosheets proved to be promising for wound healing. Such biodegradable materials are easy-to-prepare, bio-friendly, cost-effective, simple to apply and were shown to protect burn wounds and facilitate their healing. At the same time, certain metal ions are known to be essential for wound healing, which is why this study was motivated by the idea of incorporating PLLA nanosheets with Zn²⁺ ion containing nanoparticles. Upon being applied on wound, such polymer nanosheets should release Zn²⁺ ions, which is expected to improve wound healing. The work thus focused on preparing PLLA nanosheets embedded with several kinds of Zn-containing nanoparticles, their characterization and ion-release behavior. ZnCl₂ and ZnO nanoparticles were chosen because of their different solubility in water, with the intention to see the dynamics of their Zn²⁺ ion release in liquid medium with pH around 7.4. Interestingly, the prepared PLLA nanosheets demonstrated quit similar ion release rates, reaching the maximum concentration after about 10 h. This finding implies that such polymer materials can be promising as they are expected to release ions within several hours after their application on skin.

Keywords: biodegradable polymer nanosheets; wound healing; laser ablation in liquid; nanoparticles; ZnO; ZnCl₂

1. Introduction

The treatment of burn wound is known to be a long-lasting and complex process that requires new therapeutic options to improve and accelerate the healing progress [1-8]. An ideal wound dressing should accelerate one or several stages of the healing processes including the inflammatory, migratory, proliferative, and remodeling phases. A variety of wound dressings are available and still widely used to treat such wounds [1-4,7-10]. And even though the properties of ultimate wound dressings are well identified, major difficulties arise when it comes to combining them within the same material [1-4,7,9]. In other words, realizing an optimal combination of desired properties in one wrapping material is still challenging, and therefore new materials with improved properties are highly anticipated. In addition, even though it is well known that metal ions such as Zn, Mg, Fe and

Cu are necessary for efficient wound healing [11,12], their incorporation into dressings used for wound treatment was not attempted yet.

Recently, free-standing ultra-thin films (or so-called nanosheets, NSs) of biodegradable polymers (such as, e.g., poly(L-lactic acid), PLLA) have shown promise as efficient barrier covering wounds with any shape and protecting them for days without the need for daily changes [7-10,13]. The advantages of such NSs as wound wrapping material consist in: (i) relatively simple preparation procedure and easy thickness control; (ii) high surface adhesiveness and possibility to apply on surfaces with any shape; (iii) good air/gas exchange through such nano-scaled dressings and their biodegradability; (iv) excellent performance as barriers for infection and dirt, and so on [7-9,13]. Also, wound repair sites sealed by such NSs during surgery were reported to show neither scars nor tissue adhesion [5,7,8,10].

Several metal ions are known to be of high importance and stimulate skin repair and recovery. Among them, metal ions of Mg, Cu, Zn and Fe were reported to play the most significant role [11,12]: Mg functions as a co-factor for enzymes involved in protein and collagen formation; Cu is a required co-factor for cytochrome oxidase, for cytosolic antioxidant superoxide dismutase, and for the optimal cross-linking of collagen; Zn is a co-factor for both RNA and DNA polymerase and its deficiency slows down wound healing significantly; and finally Fe is required for the hydroxylation of proline and lysine, while its deficiency results in impaired collagen production [11,12]. Thus, loading NSs with nano-containers releasing the above metal ions is believed to stimulate faster skin regeneration/growth. This challenging task, upon successful realization, will certainly boost the use and market value of such NSs, also expanding significantly fields of their potential applications.

The laser ablation in liquid (LAL) is a quickly gaining in popularity and convenient laboratory technique to produce various nanostructures, including nanoparticles (NPs), nanocubes, hollow NPs, nanorods, nanoflakes and other structures of metals, metal oxides (see Fig.1), sulfides, carbides, etc. [14-31]. In this approach, laser beam is typically focused on a solid target, its pulses ablating the target and producing various nanostructures whose morphology, size and chemistry depend on the laser pulse parameters and liquid medium [14-16,18-21,25,29,30]. As a preparative method, LAL is attractive for several reasons: (i) it is an easy-to-use and green technique consuming minimum chemicals; (ii) a wide variety of nanostructures can be prepared, with control over their composition and morphology; (iii) the method operates at nominally room temperature while can often generate unique phases and morphologies. Importantly for the present study, LAL permits to prepare both Zn oxide and chloride NPs.

The overall goal of this work was to demonstrate that PLLA NSs can be embedded with NPs (as nanocontainers with Zn^{2+} ions) that can release metal ions when such NSs are placed on wet skin. Nanoparticles of ZnO and ZnCl_2 were chosen as model NPs as those containing Zn^{2+} ions and having different solubility in water. Prior to incorporating PLLA NSs with multiple metal ions, Zn-containing NSs were chosen as a proof-of-concept system. By means of spin-coating, we first prepared NSs incorporated by Zn-containing NPs (both LAL-generated NPs and commercially available ones with similar composition), after which we tested how the as-prepared NSs released Zn ions after immersion in water at 37 °C and pH 7.4, i.e. conditions close to those on human skin. Also, preliminary tests were carried out on LAL-prepared NPs to evaluate their ability to suppress *E. coli* bacteria. The obtained results will be of use for further development of PLLA nanosheets embedded with metal-ion releasing nanocontainers as a new-generation biomedical materials (dressing for wound healing).

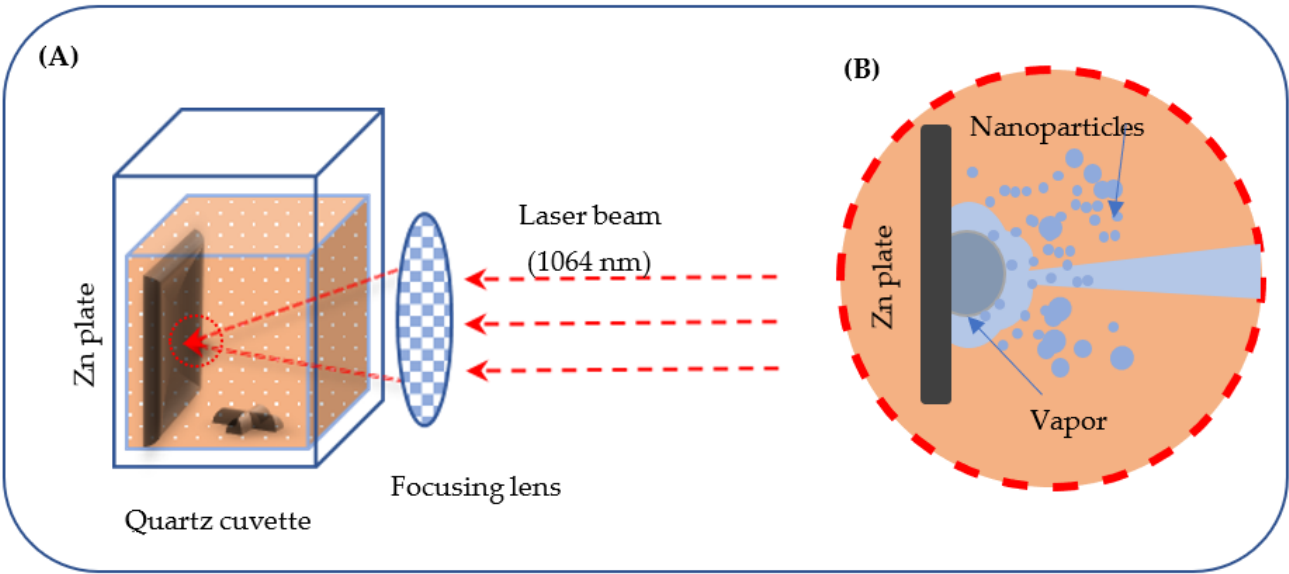


Figure 1. (A) Ablation of Zn plate immersed in chloroform with laser beam. (B) Nanoparticles forming in the ablation region and making a brown colloid.

2. Methods and Materials

2.1. Materials

Zinc metal plate (99.5% purity) was purchased from Nilaco Corp. Chloroform (99.0% purity), deionized water and ethanol (99.5%) were purchased from Wako Pure Chemical Industries (Japan). Phosphate-buffered saline solution (PBS) was purchased from Sigma-Aldrich, while polyvinyl alcohol, PVA was from Kanto Chemical Co. (Japan), and PLLA (Mw: 80–100 kDa) was supplied by Polysciences, Warrington, PA, USA). Zinc chloride salt was also purchased from Wako Pure Chemical Industries.

2.2. Nanoparticles

In this study, we prepared Zn-containing NPs by LAL of Zn in chloroform or water, aiming at obtaining ZnCl₂ and ZnO NPs, respectively. While laser ablation of metallic Zn in water is known to result in zinc oxide or/and hydroxide NPs [15,17,18,23,26,28,29,31], LAL processing of Zn plate in chloroform was not reported before. Chloroform was chosen as reaction medium for LAL for two reasons: (i) because ZnCl₂ based NPs were expected, and (ii) because chloroform was then used as solvent for spin-coating of PLLA NSs without the necessary to centrifuge produced NPs and redisperse them in chloroform.

Table 1. Laser parameters used in experiments.

	Ns-pulsed laser	Ms-pulsed laser
Laser output	40, 60, 80 mJ/pulse	2, 4, 6 kW
Pulse width	5-7 ns	2, 4, 6 ms
Frequency	10 Hz	10 Hz
Ablation time	15 min	15 min

A zinc metal plate with a thickness of 2.0 mm was cut into targets, 15 mm x 30 mm in size. The obtained plate was then immersed in ethanol and sonicated in an ultrasonic

bath for 5 min to remove grease and surface contaminations. After drying in air for several min, the plate was fixed inside a quartz cuvette containing 15 mL of chloroform. Two types of Nd: YAG lasers with the fundamental wavelength of 1064 nm and either milli-second- or nanosecond-long pulses were utilized for preparing nanomaterials. More details on setups and lasers used can be found elsewhere [17,18,30,31].

Chloroform used as liquid medium for LAL was stirred magnetically to disperse produced NPs throughout the ablation. As indicated in Table 1, experiments were conducted by using two lasers. The prepared colloids were then dropcast on Si wafers for X-ray photoelectron spectroscopy (XPS) analysis or on C-coated grids for transmission electron microscopy TEM.

2.3. Nanosheet preparation

At first, 0.6 mL of PVA solution used as sacrificial film was dropped onto a silicon substrate ($3 \times 3 \text{ cm}^2$), see Fig.2. The substrate was spin-coated at 4000 rpm for 20 s and then dried using a hot plate at 70°C for 90 s. In parallel, 20 mg of PLLA in crystal form was added to 2 mL of a proper dispersion of NSs. At this stage, either commercial NPs or those produced by LAL were mixed with chloroform in a proper ratio (typically, 1.0, 2.0 or 4.0 mg/mL). The mixture was shaken using vortex mixer vigorously until PLLA crystals dissolved completely.

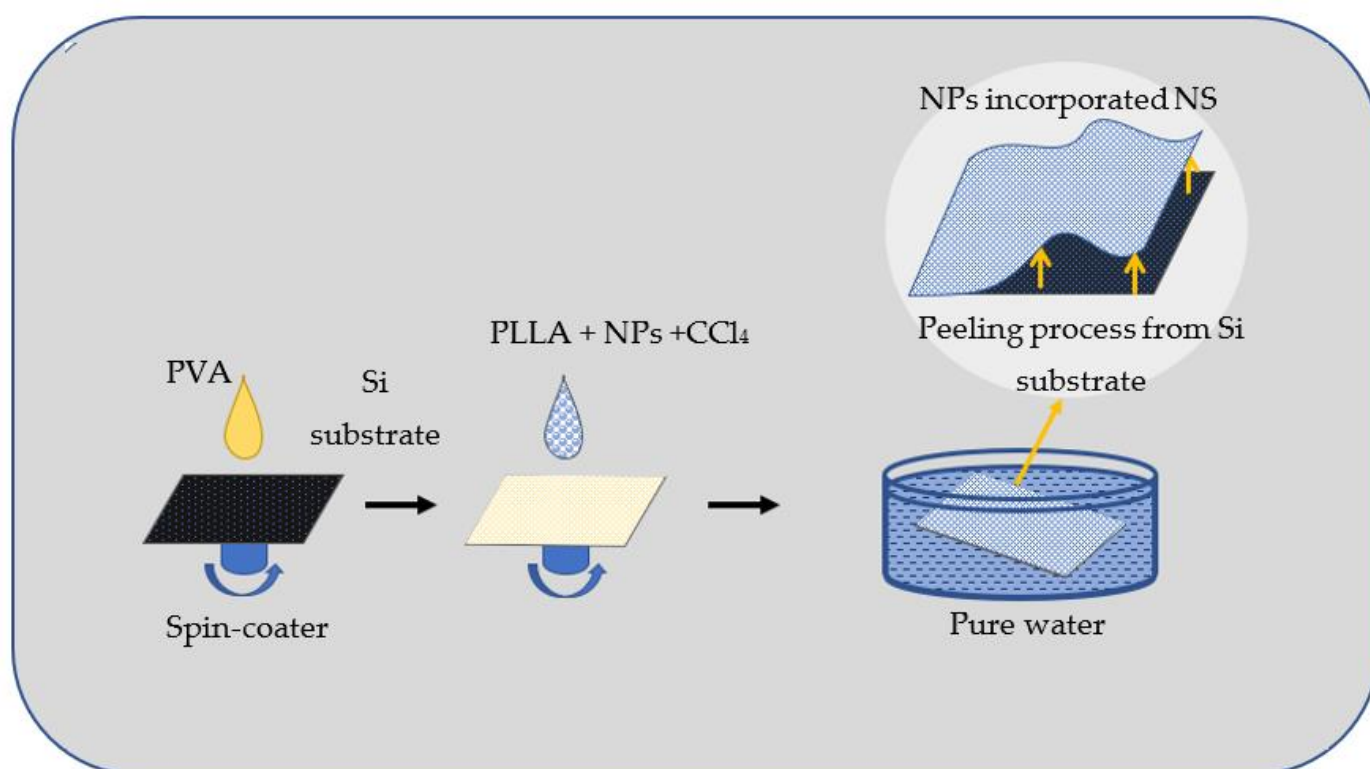


Figure 2. Preparation of nanoparticle-incorporated polymer nanosheets. PVA was used as sacrificial under-layer because of its solubility in water. When the formed PLLA/PVA structure is placed in water, the PLLA nanosheet begins to separate from Si substrate.

Then, 0.4 mL of the prepared mixture was spin-coated on the PVA-coated substrate. Again, the substrate was spun for 20 s and dried on a hot plate at 70°C for 90 s. By using a cutter, a light cut was made on the prepared sample to make a NS with the size of $3 \times 3 \text{ cm}^2$. The substrate was then immersed in pure water (Fig.2), where it was moved from

time to time using tweezers until the NS began to float. The NP-incorporated NSs were thus collected and transferred on polyester matts to preserve their shape.

2.4. Characterization

Morphology of obtained NPs and nanosheets were observed using scanning electron microscopy (SEM, S4800 from Hitachi, Tokyo, Japan) and transmission electron microscopy (HF-2200, Hitachi, Tokyo, Japan). Optical images of prepared NSs were observed by means of an SMZ 1500 (from Nikon, Japan) optical microscope. X-ray photoelectron spectroscopy (XPS) analysis was carried out on a PHI-1600 spectrometer (Physical Electronic Industries, Chanhassen, MN, USA), with all binding energies corrected for charge shifting by referencing to the adventitious carbon C1s line at 285 eV. Size of dispersed NPs was evaluated by means of dynamic light scattering (DLS) technique.

2.5. Ion release in buffered saline solution

The Zn^{2+} ion release from nanosheet samples was studied by means of inductively coupled plasma mass spectroscopy (ICP-MS). The samples were immersed in beakers with 40 mL of phosphate-buffered saline (PBS) solution (pH 7.4) at 37 °C. To determine the concentration of Zn^{2+} ions over time, aliquots of 1 mL were taken and analyzed after certain periods of time [32-34]. After each sampling, 1 mL of PBS solution was added to the sample. For each sample, experiments were carried out in triplicate, after which the obtained results were averaged.

To evaluate the antibacterial properties of incorporated nanoparticles, preliminary tests were conducted on LAL-generated NPs by pipetting them on a bacteria-coated medium and monitoring the growth of colony in the media by taking microscopic images using a laboratory microscope, as previously reported elsewhere [35].

3. Results and Discussion

3.1. Zn-containing nanoparticles

As a first step, we prepared various NPs via LAL, applying two different lasers (with millisecond- and nanosecond-long pulses) and using water or chloroform as liquid medium. Figure 3A presents a photograph of as-prepared colloid of Zn-based NPs produced via ablating Zn plate immersed in chloroform by means of ms-pulsed laser. Since chloroform was used as PLLA solvent during NS preparation, such homogeneous colloids with Zn-containing NPs were thus ready for further processing, i.e. for mixing with PLLA and spin-coating as NSs (see such a free-floating NS in Fig.3B).

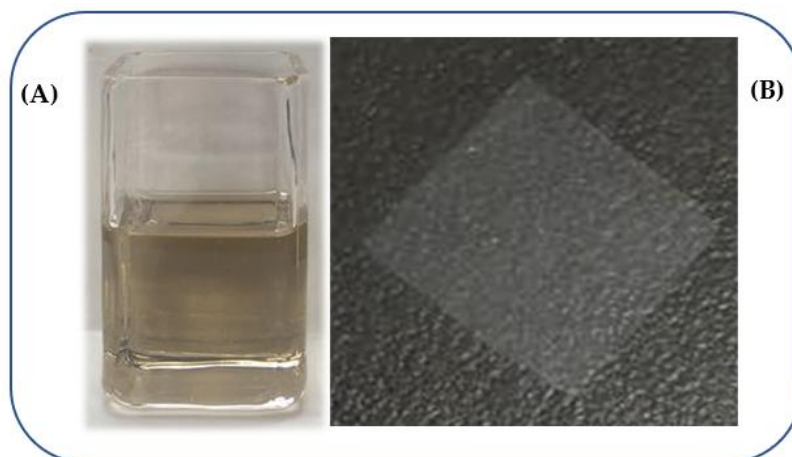


Figure 3. Cuvette with colloidal solution of Zn-Cl nanoparticles prepared via laser ablation in liquid (A) and free-standing PLLA nanosheet incorporated with such nanoparticles (B), floating on water.

The nanosheet is 3x3 cm² and about 50 nm thick, which provides superior flexibility and adhesion on any surface.

Figure 4 presents NPs prepared by ms-laser in chloroform (A,B) and by ns-laser in water (D). The particles in panels A and B look quite uniform, being around 30-70 nm in size and showing rather amorphous morphology (Fig.4B). Images of other NPs prepared by ms-laser in chloroform using different conditions are shown in *Supplementary Materials* Fig.S1, revealing quite similar morphology and sizes. As was revealed by XPS analysis (see Fig.5), NPs prepared by LAL of Zn in chloroform, along with dominating Zn-Cl species, also contained some fraction of surface Zn-OH, metallic Zn, and traces of C-Cl bonds [15,17,18,23,29,36]. Therefore, in contrast to NPs of commercial ZnCl₂ salt, for simplicity in this study we denoted such LAL-generated materials as Zn-Cl NPs.

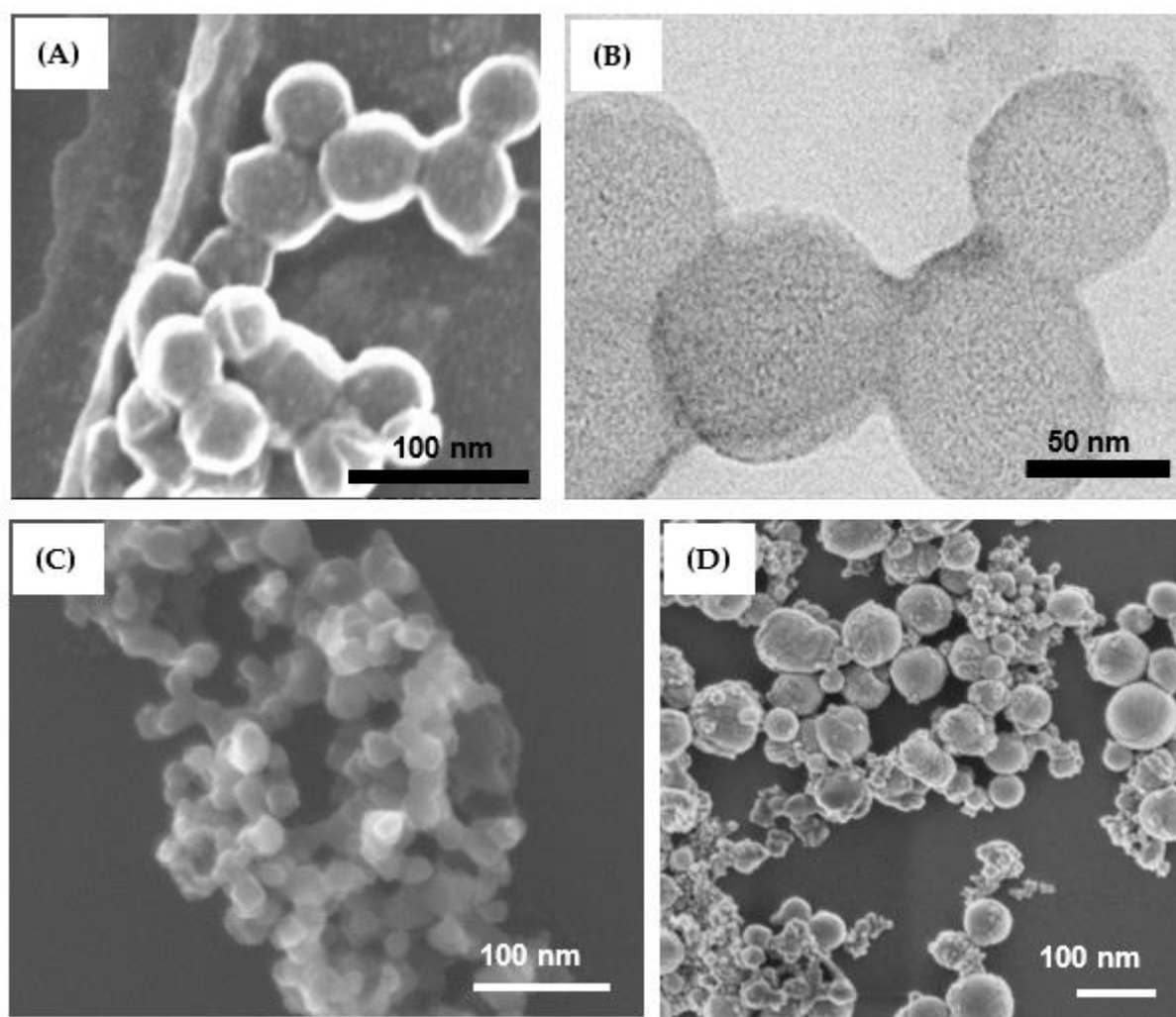


Figure 4. SEM (A) and TEM (B) images of Zn-Cl NPs prepared in chloroform by ms-laser. Pulse width, peak power and frequency used were 2 ms, 1 kW, and 10 Hz, respectively. SEM images of (C) commercial ZnO and (D) laser-produced ZnO NPs (ns-laser, water as medium).

Note that other Zn-Cl NPs produced by both ms-laser and ns-laser in chloroform also had similar species as their components, even though depending on conditions, such Zn-Cl NPs somewhat differed in chemical composition (see XPS spectra in *Supplementary Materials* Fig.S2). The composition of LAL-generated Zn-Cl NPs was also confirmed by FTIR spectroscopy which compared their spectra with commercial ZnCl₂ and ZnO products (see *Supplementary Materials* Fig.S3). Thus, we confirmed that ablation of Zn in chloroform

indeed led to NPs with ZnCl_2 as the main phase. Changing laser parameters (see Fig.S4), we could produce Zn-Cl NPs with slightly different sizes, generally within the range of ~30-150 nm. This is also confirmed by DLS results for two different Zn-Cl colloids presented in Fig.S5, where the average size of NPs produced by ms-laser is seen to be around 55-60 nm.

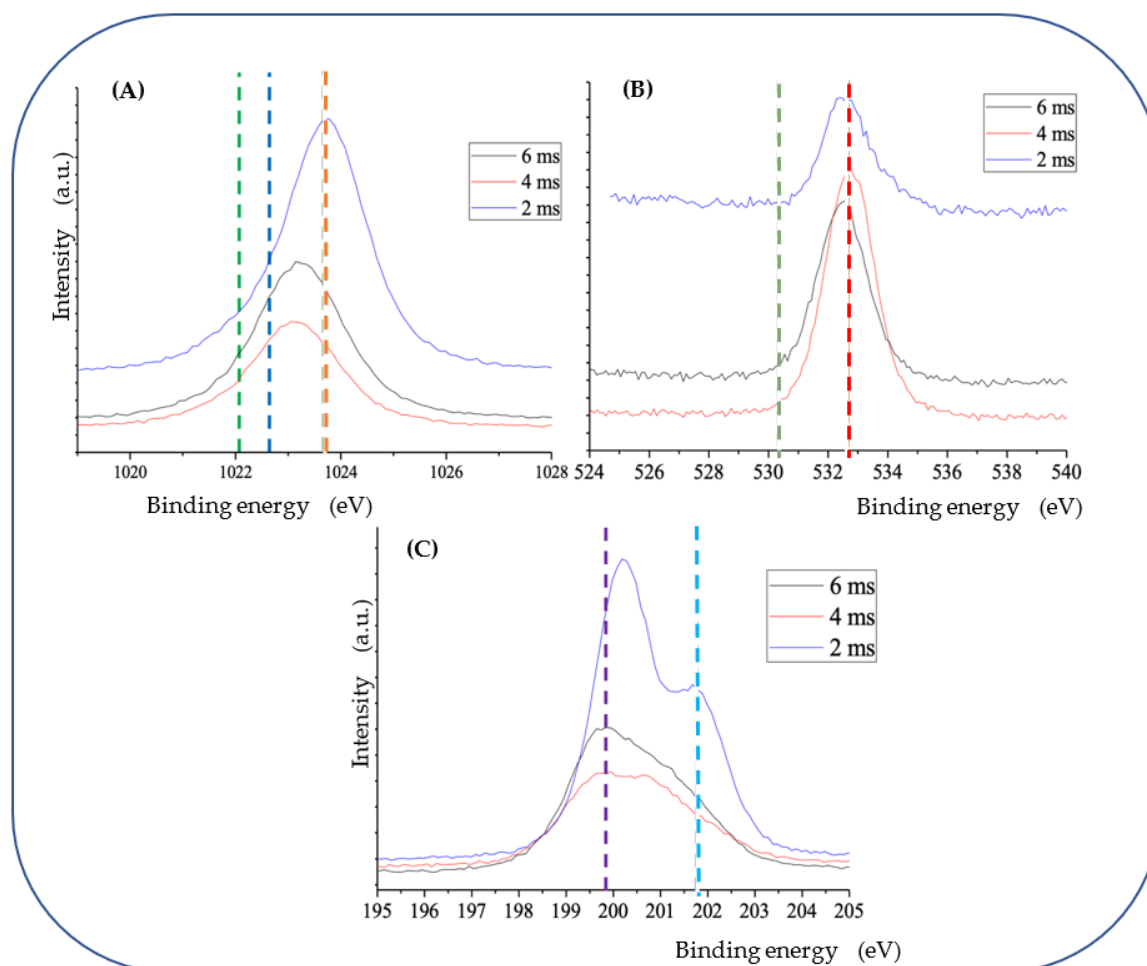


Figure 5. XPS spectra of Zn-Cl NPs produced with ms-laser in chloroform (pulse peak energy: 1 kW, varied pulse widths: 2, 4, 6 ms). (A) XPS Zn $2p_{3/2}$ spectra: metallic Zn (green dashed line); Zn-OH bonding (blue line); Zn-Cl bonding (orange line). (B) XPS O 1s spectra: O-C bonding (olive dashed line); OH species (red line). (C) XPS Cl 2p spectra: Zn-Cl bonding (purple dashed line); C-Cl bonding (light blue line).

Within the framework of the present study, no noticeable difference in Zn-ion release dynamics was observed between PLLA NSs incorporated with Zn-Cl NPs produced under different conditions (shown in Fig.4A,B and *Supplementary Materials* Fig.S1). Hence, here we only show representative SEM images (Fig.4A,B) and XPS spectra (Fig.5) of selected laser-produced Zn-Cl NPs, while more results are presented in Fig.S1 and Fig.S2.

For comparison, as source of Zn^{2+} ions, we also aimed at using commercially available ZnCl_2 NPs embedded into PLLA NSs. Since the salt was supplied in the form of relatively large particles (see *Supplementary Materials* Fig.S6 and Fig.S7), we attempted to reduce their size by irradiating their dispersion in chloroform. It is clearly seen in Fig.S6 and Fig.S7 that indeed irradiation of ZnCl_2 particles suspended in chloroform led to gradual reduction in their average size. For instance, according to DLS analysis, irradiation for 40 min is seen in Fig.S6 to permit to reduce ZnCl_2 NPs to average sizes around 120-140 nm. This size is already acceptable for embedding into NSs with average thickness ~100 nm.

In parallel, we also prepared ZnO NPs as their solubility in water is lower, and thus we expected slower Zn ion release from PLLA NSs incorporated with such particles. Commercial ZnO NPs with average size ~20-25 nm (Fig.4C) and those produced using ns-laser (Fig.4D) were thus used to incorporate to PLLA NSs and test their Zn ion release.

In addition, we also tested antibacterial properties of LAL-generated NPs, pipetting their dispersion on a bacteria-coated medium and monitoring the growth of colony in the media, following the methodology previously described elsewhere [35]. By taking optical microscopy images, we counted the number of colonies in presence and absence of laser-produced NPs, showing that the Zn-containing NPs we used inhibit the growth of *E. coli* to some extent (see *Supplementary Materials*, Fig.S10 and Fig.S11). The obtained preliminary results imply that there might be some antibacterial effect when such NPs are incorporated into PLLA NSs and the latter NSs are applied on skin or wound. This is in line with reports of others on antibacterial effect of various ZnO NPs previously published elsewhere [26,29,37,38]. According to the literature, Zn²⁺ ions released by Zn-containing NPs could be one of factors suppressing certain bacteria strains [26,29,37,38].

3.2. Zn-incorporated polymer nanosheets

As a second step, both the laser-produced and commercial ZnO NPs, as well as their counterparts based on ZnCl₂, were incorporated into PLLA nanosheets. This was achieved via spin-coating mixtures of PLLA polymer and colloidal NPs in chloroform as solvent. Figure 6 shows surface images of PLLA NSs incorporated with commercial ZnO NPs (A), LAL-prepared ZnO NPs (B), commercial ZnCl₂ NPs (C) and laser-prepared Zn-Cl NPs (D).

Since the thickness of spin-coated PLLA NSs was around 100 nm, various Zn-containing NPs from tens of nm to 100-120 nm are seen in Fig.6 to be well incorporated. Even though we did not aim at optimizing spin-coating process and reach extremely homogeneous NP distribution, the conditions used permitted to achieve quite uniform particle distribution over the entire NS surface. Expectedly, the smallest ZnO NPs are seen in Fig.6A to be distributed better and with minimum agglomerates over the sample surface, while both samples with ZnCl₂-based NPs are seen in panels C and D to demonstrate somewhat lower degree of uniformity over their surface, which is related to their larger NP size and wider size distribution.

We investigated the capacity of prepared PLLA NSs to incorporate ZnO NPs, which was done with commercial material. For this, NSs with 1, 2 and 4 mg/mL of ZnO powder (dispersed in PLLA solution in chloroform) were spin-coated. It was found that after more than 4 mg/mL of ZnO NPs, NSs prepared under the conditions used in this study were not mechanically strong and tended to disintegrate relatively easily. That is why, for ion release tests, NSs were prepared from ZnO dispersions in PLLA solution in chloroform with 1 and 2 mg/mL of ZnO.

For comparison, when preparing NSs incorporated with ZnCl₂ based NPs, we loaded them with 3.3 mg/mL of ZnCl₂ NPs, as this corresponds to the same amount of Zn ions as in 2 mg/mL of ZnO nanomaterial. However, it should be noted that during spin-coating the amount of incorporated nanomaterial depends on NP size, morphology and nature, given that the other parameters (such as PLLA concentration, chloroform as solvent and rotational speed) are fixed. Thus, embedding the same amount of Zn ions for different nanomaterials, even for ZnO NPs with different sizes, is quite difficult.

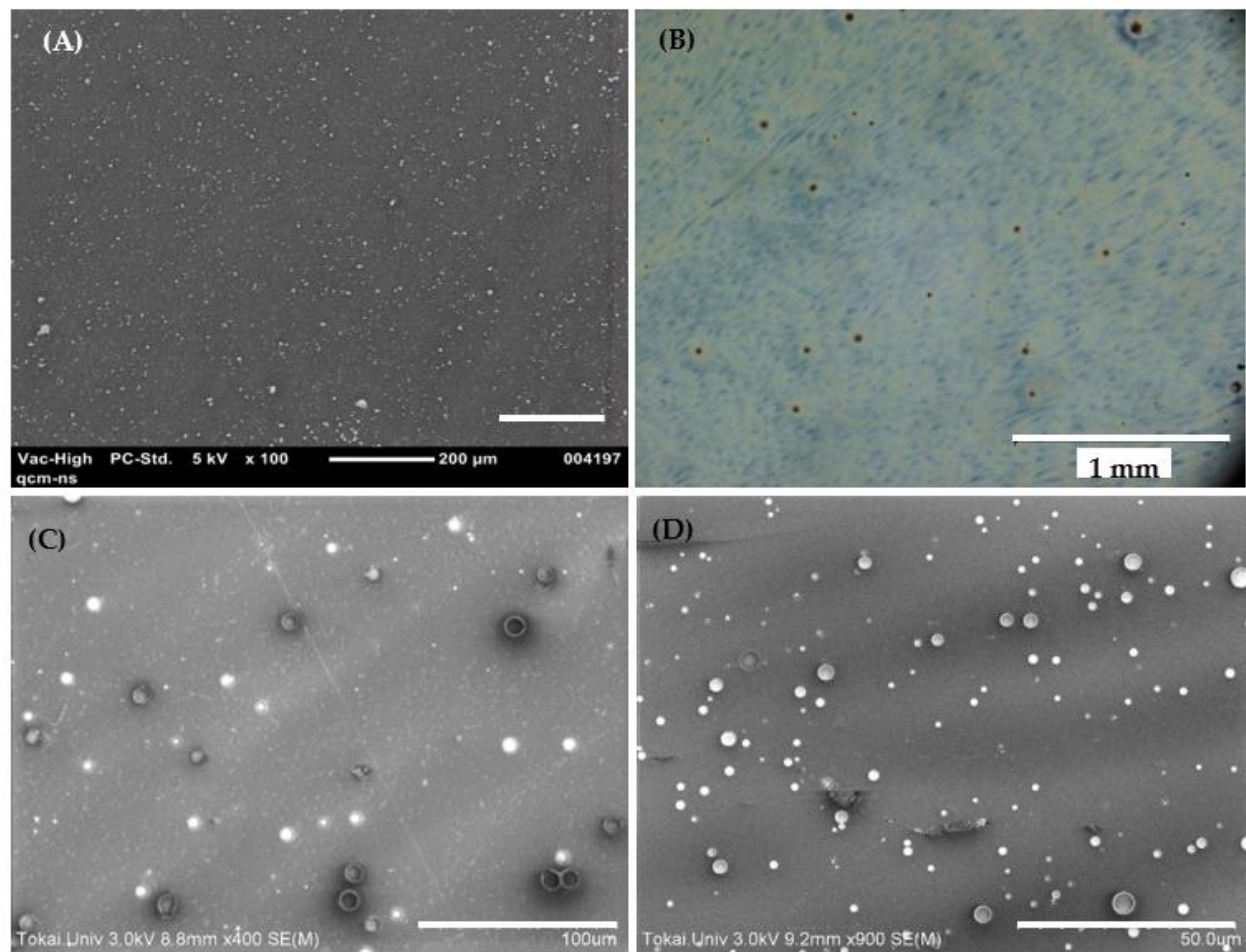


Figure 6. SEM images of PLLA NSs loaded with (A) commercial ZnO NPs, (C) Zn-Cl laser-generated NPs, and (D) commercial ZnCl₂ NPs. (B) Optical image of nanosheet loaded with laser-generated ZnO NPs (ns-laser, water medium). Scale bar indicates 200 μ m (A), 1 mm (B), 100 μ m (C), and 50 μ m (D).

3.3. Ion release from prepared polymer nanosheets

Figure 7 demonstrates how PLLA nanosheets embedded with different NPs released Zn²⁺ ions when immersed into physiological solution (pH 7.4). The solution simulated human body fluids and therefore was kept at 37 °C. Concentration of Zn ions released by 1 cm² of NSs incorporated with ZnO NPs and ZnCl₂ NPs is exhibited in panels (A) and (B), respectively. Except for one sample, which was incorporated with 1 mg/mL of commercial ZnO NPs (orange open circles, panel (A)), all the other NSs embedded with ZnO had either 2 mg/mL of ZnO (commercial NPs, orange solid circles) or 2 mg/mL of LAL-generated NPs (blue solid circles).

Comparison of the curves with orange and blue solid circles as markers (see Fig.7A) permits to conclude that both commercial and LAL-prepared ZnO NPs released Zn²⁺ ions in a similar way, with a similar slop and plateau reached after 12 to 20 h. Quite comparative level of maximum concentration was reached for NSs incorporated by ZnO with different sizes and size distribution. As mentioned above, the difference can be explained by a difference in the number and mass of ZnO particles spin-coated from different nano-materials. Importantly, however, when same ZnO NPs were spin-coated from their dispersions with different concentration (1 mg/mL and 2 mg/mL of ZnO NPs, see orange

empty and solid circles in Fig.7A), pretty good correlation was observed between the maximum concentrations achieved.

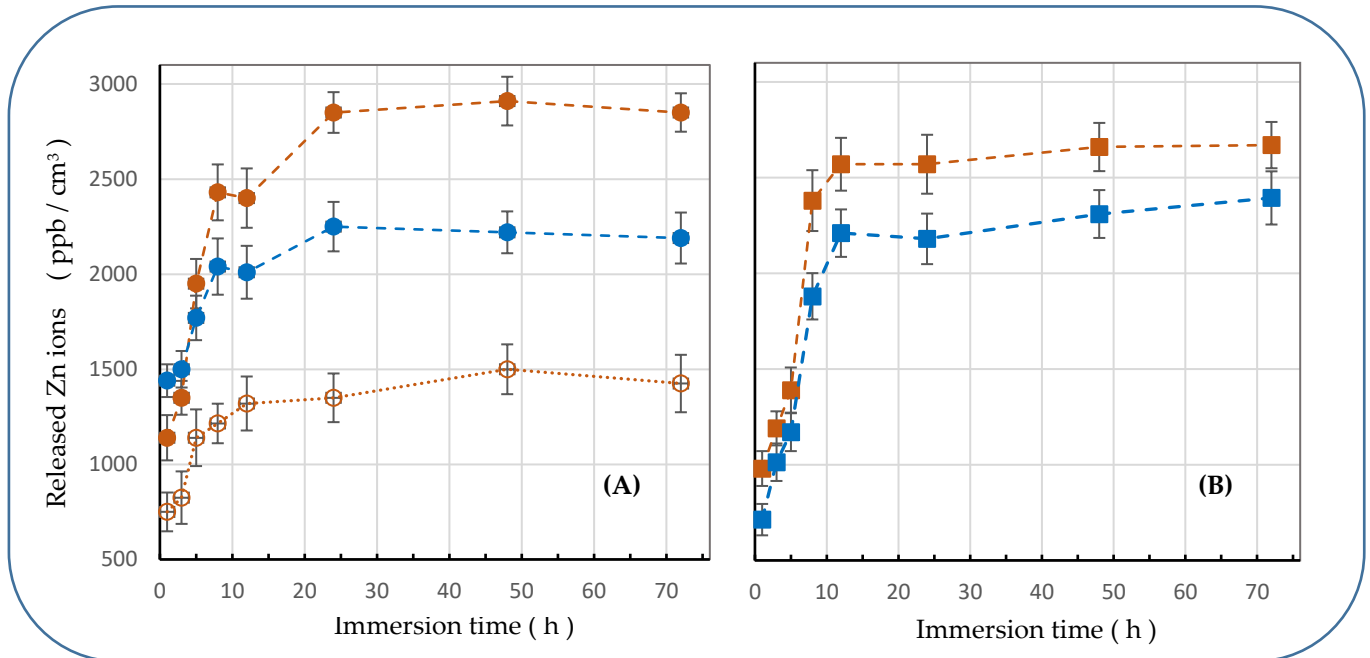


Figure 7. Concentration of Zn^{2+} ions released from PLLA NSs incorporated with ZnO NPs (A) and ZnCl_2 NPs (B) over time into liquid with pH 7.4 at 37 °C. (A): Commercial ZnO NPs (orange) were loaded to spin-coated liquid at 2 mg/mL (solid circles) and 1 mg/mL (open circles), blue circles indicate NSs incorporated with LAL-generated ZnO NPs. (B): Results for PLLA NSs incorporated with commercial ZnCl_2 (orange) and LAL-generated Zn-Cl NPs (blue) are presented (ms-pulsed laser was used). Dashed lines are only guide to the eye.

For PLLA NSs embedded with ZnCl_2 -based NPs (Fig.7B), again similar results were demonstrated by samples with LAL-generated and commercial NPs (curves with blue and orange markers). The most interesting observation is that in both panels (A) and (B), maximum Zn^{2+} concentration is basically achieved ~10-12h after immersion. This result is somewhat unexpected, taking into consideration the difference in water solubility between ZnO and ZnCl_2 . Probably, the similar dynamics of ion release observed in panels (A) and (B) (Fig.7) can be explained by: (i) relatively small sizes of ZnO NPs, which accelerated their dissolution in water, and (ii) permeability of PLLA NSs as a limiting stage for Zn^{2+} ion release.

Importantly, it is clearly seen in Fig.7 that all the NSs incorporated with Zn -containing NPs released Zn ions actively within ~10 h, after which quite steady concentrations were reached. In light of this, the obtained results look very promising as dressing materials applied onto skin wounds are typically kept there for ~1 day and are expected to provide drugs or ions incorporated into them (as acting species) within a few hours upon their placement.

It should be noted that so far, there is no information yet on the desired concentrations of Zn^{2+} expected on skin surface for efficient healing, and this is still a subject for future investigations. Therefore, here we only aimed at showing that concentration control of embedded Zn^{2+} ions is possible, and that embedded Zn-containing NPs can release ions within a short enough period of time. In parallel, the effect of developed Zn-incorpo-

rated NSs on healing of burn wounds on animals is also to be tested in the future. However, the fact that Zn ions get released from the developed polymer NSs as fast as within several hours shows promise. Obviously, wound dressings, when placed around wound area, should demonstrate their efficacy within several hours.

4. Conclusions

The study showed that biodegradable polymer nanosheets of poly(L-lactic acid), PLLA, incorporated by Zn-containing nanoparticles can be prepared in a simple way by means of spin-coating. For this, commercially available and prepared via laser ablation in liquid ZnO and ZnCl₂ nanoparticles were used. We show that PLLA nanosheets can be embedded by different Zn-containing nanoparticles, with different loading and with reasonably good (homogeneous) distribution of nanoparticles across entire nanosheet. After preparation, the nanosheets were immersed in a buffered liquid with pH 7.4 at 37 °C, where their Zn ion release was monitored over time. Interestingly, irrespective of the nature of Zn-containing nanoparticles, the dynamics of their Zn ion release was quite similar, with maximum concentration achieved before ~10h. This finding is very promising for further optimization and development of convenient wound patches based on such inexpensive biodegradable nanosheets, as release of incorporated metal ions within several hours after such patches are applied on skin is of high importance.

Author Contributions: Methodology, M.Q.H.I., S.A.K., and Y.O.; Conceptualization, S.A.K. and Y.O.; Investigation, M.Q.H.I., M.E.T., T.K., M.H., P.S., S.O.G.; Formal analysis, M.Q.H.I., P.S., M.E.T., S.O.G.; Supervision, M.H., T.K., P.S., S.I., and S.A.K.; Project administration, S.A.K. and S.I.; Data curation, P.S., S.I., Y.O., and S.A.K.; Writing- original draft, M.Q.H.I., M.E.T., and S.A.K.; Writing-review and editing, Y.O. and S.A.K.

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