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Role of Diffusion-weighted MRI in Differentiation between Benign and Malignant Anterior Mediastinal Masses

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Abstract: To describe the characteristics of anterior mediastinal masses on conventional magnetic resonance imaging (MRI) and to assess the role of Apparent Diffusion Coefficient (ADC) value in distinguishing benign from malignant mediastinal lesions.

We conducted a retrospective cross-sectional study in 55 patients with anterior mediastinal mass who were performed MRI before treatment. Biopsy and histopathological assessment were done after that.

The study was composed of 55 patients, with 5 benign lesions and 50 malignant lesions. The ADC_{mean} , ADC_{median} , ADC_{10} , ADC_{90} in the histogram-based approach and hot-spot-ROI-based mean ADC for the malignant lesions was significantly lower than those found in benign lesions (P value <0.05). The hot-spot-ROI-based mean ADC had the highest value in differentiation between benign and malignant mediastinal lesions, between group A (benign lesions, thymoma A, AB, B1) and group B (thymoma B2, B3 and other malignant lesions). The cut off point (with sensitivity, specificity) of the ADC value differentiating malignant from benign mediastinal lesions; differentiating group A from group B were $1.17 \times 10^{-3} \text{mm}^2/\text{s}$ (80%, 80%); $0.99 \times 10^{-3} \text{mm}^2/\text{s}$ (78.4% and 88.9%) respectively.

Diffusion weighted MRI and measurement of ADC value in histogram-based approach and hot-spot-ROI-based mean ADC are very helpful in the differentiation between benign and malignant anterior mediastinal lesions.

Keywords: anterior mediastinal lesions; diffusion weighted imaging; diffusion magnetic resonance imaging; gadolinium; thymoma; lymphoma; thymus neoplasms; biopsy

1. Introduction

Mediastinal masses are relatively rare entities which present a diverse array of histopathology, ranging from benign lesions to malignancies. Normally, the anterior mediastinum contains the thymus, lymph nodes, fat tissue, nerves, blood vessels, and sometimes the thyroid gland descending from the neck. Masses in the anterior compartment of mediastinum are often originated from these structures [1].

Imaging plays a pivotal role in establishing the initial diagnosis and guiding the selection of supplementary tests needed to reach the final diagnosis. Because of superior soft tissue contrast, MRI is considered an ideal tool for evaluating mediastinal masses.

Preoperative assessment of the involvement of the lesion with the pericardium, heart, spinal cord, and blood vessels is a common indication. In addition, non-contrast MRI is an alternative to evaluate mediastinal masses in patients who have contraindications to intravenous contrast. Chemical shift imaging has been shown to be useful in differentiating normal thymus and thymic hyperplasia from thymic neoplasms and lymphoma. Diffusion MRI is a novel technique which is able to assess physiologic differences between tissues based on random motion of water protons [2]. On diffusion-weighted pulse sequences, the motion causes scattering of spins resulting in signal loss. This signal loss can be quantified by calculating the ADC, which reflects the specific diffusion capacity of biological tissue. The presence of diffusion obstacles such as cell membranes, tight junctions, macromolecules, cell organelles and the movement of water protons will lead to decreased ADC. It is hypothesized that hypercellular tumors have low ADC value; whereas tissues with lower cell density (necrotic tissue, non-neoplastic tissue, etc.) have higher ADC values. Therefore, ADC value can be used to distinguish necrotic tissue and benign lesions from malignancies. The cellular structure of a tumor is considered an indicator of its progression and response to treatment. In malignant lesions, the extracellular space is markedly narrowed due to increased cellularity, cell volume and impaired cell membranes. Rapidly growing tumors have increased quantity of organelles and cytoskeleton. The increase in cellular density and microstructures will in turn restrict the movement of water molecules [3,4].

Although there have been several studies on the role of MRI in evaluating anterior mediastinal lesions, its value is still controversial. Some researches show that diffusion-weighted imaging is valuable in differentiating between benign and malignant anterior mediastinal lesions. This study was carried out with the aims of characterising anterior mediastinal masses on conventional and diffusion MRI, and evaluate the role of diffusion MRI in differentiating benign and malignant anterior mediastinal tumors.

2. Materials and Methods

This is a retrospective cross-sectional study including 55 patients with anterior mediastinal tumors, who underwent preinterventional chest MRI at University Medical Center Ho Chi Minh City from September 2018 to June 2021. The tumors were then pathologically examined with samples taken from operation or biopsy. Tumors without solid components or recurrent cases were excluded from the sample. Most cases underwent MRI to detect thymic lesions in patients with myasthenia gravis, and to evaluate local invasion of the tumors to heart, pericardium, large blood vessels.

All studies were performed on a 3 T MR unit (Magnetom, Siemens, Germany) at University Medical Center Ho Chi Minh City. The MRI protocol for each patient included T2 HASTE, T2 HASTIRM, DWI, T1 VIBE DIXON before and after Gadolinium injection, with the following parameters. Axial T2 HASTE: TR = 1000 ms, TE = 92 ms, slice thickness: 6 mm, field of view: 260x360 and matrix: 240x320. Sagittal T2 HASTE: TR = 600 ms, TE = 27 ms, slice thickness: 8 mm, field of view: 350x350 and matrix: 256x320. Coronal T2 HASTE: TR = 600 ms, TE = 26 ms, slice thickness: 8 mm, field of view: 400x400 and matrix: 256x320. Axial T2 HASTIRM: TR = 1600 ms, TE = 86 ms, slice thickness: 6.5 mm, field of view: 300x380 and matrix: 260x320. Axial T1 opphase: TR = 4.2 ms, TE = 1.3 ms, slice thickness: 3 mm, field of view: 280x380 and matrix: 240x320. Axial T1 inphase: TR = 4.2 ms, TE = 2.6 ms, slice thickness: 3 mm, field of view: 280x380 and matrix: 240x320. Axial DWI: TR = 6500 ms, TE = 72 ms, slice thickness: 6 mm, field of view: 320x400 and matrix: 120x150. Diffusion-weighted images were obtained by using a echo-planar imaging sequence with b values of 0 and 2000 s/mm². ADC maps were constructed by the machine's software and displayed simultaneously after DWI images were acquired.

MRI results were examined on PACS system at University Medical Center Ho Chi Minh City. The characteristics investigated include: size, border, presence of necrotic or cystic component, presence of lesional fat. These characteristics are analysed based on T1W DIXON images before and after Gadolinium injection, T2 HASTE, T2 TIRM.

Quantification of ADC values of solid component was acquired with b values of 0 and 2000 s/mm². Chemical shift imaging has been proved to be highly valuable in determining the fat composition of a lesion or an organ [9]. In order to accurately quantify the presence of fat, we used the SII, which stands for Signal Intensity Index. Fat composition was determined by comparing the signal intensity of the lesion on in- and out-of-phase T1-weighted images. ROI (Region of Interest) was placed on the slice with the largest tumor area with ROI area occupying approximately three fourths of tumor. The SII was calculated by the formula:

$$SII = \frac{(tSI_{in} - tSI_{op})}{tSI_{in}} \times 100$$

Regions of interest were manually placed on the ADC map at 3 different sites of solid tissue which had the lowest signals (ROI area of 0.5 cm²). Areas of fat, hemorrhage, necrosis, and cystic components were excluded from the ROI. The average of three ADC values was then obtained. For whole-tumor histogram analysis of ADC maps, we used Firevoxel, which is a software developed by Center for Biomedical Imaging, Department of Radiology, New York University. ROI was manually drawn on each slice. Large areas of fat, necrosis, cysts, and hemorrhage were removed from the ROI area. Eventually, the software constructed the histogram analysis of ADC values, including ADC mean, ADC median, 10th and 90th percentile of ADC.

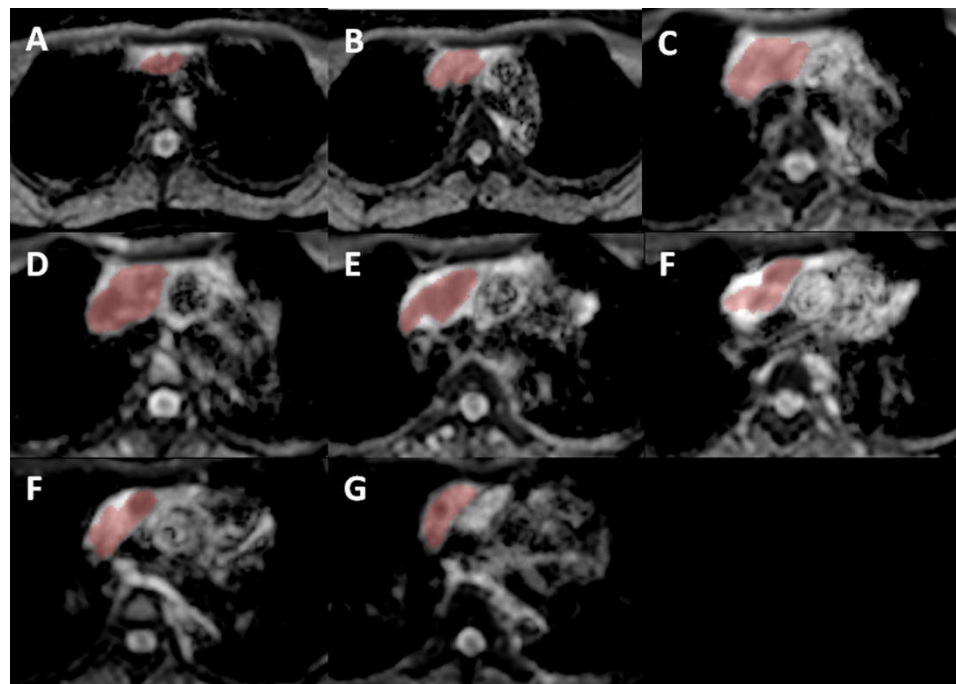


Figure 1. Whole-tumoral ROI was manually placed on the ADC map by using Firevoxel.

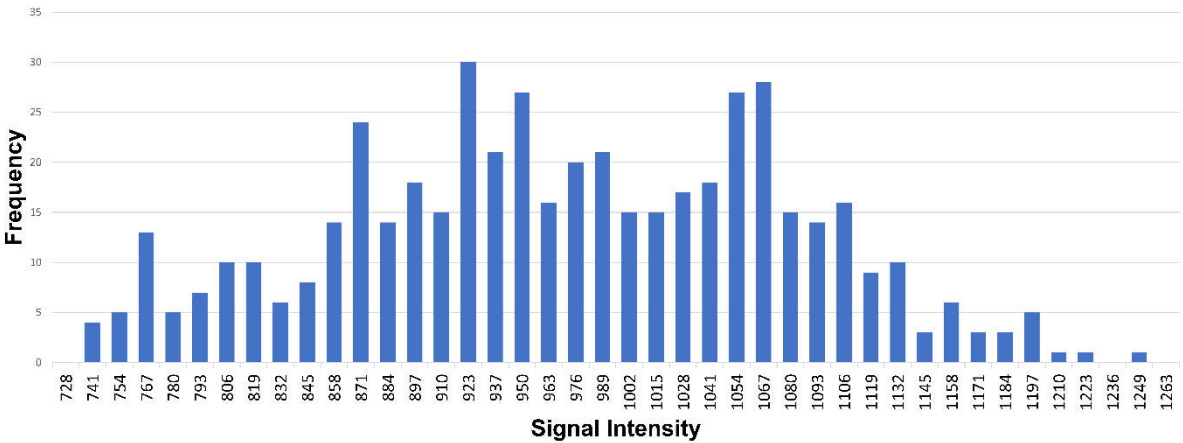


Figure 2. An example of whole-tumor histogram analysis of the ADC map.

A 35-year-old female patient with primary mediastinal large B-cell lymphoma.

Additionally, we divided the anterior mediastinal tumors into two groups in two different ways: group A (including benign tumors and type A, AB, B1 thymoma) and group B (including type B2, B3 thymoma and other malignancies); lymphoma and other malignancies. Datas are shown as frequency and percentage for qualitative variables; for normally distributed quantitative variables, datas are shown as mean values and standard deviation; for non-normally distributed quantitative variables, datas are shown as median and interquartile range. We used chi-squared and Fisher's tests to compare proportions. Mann–Whitney test was used to compare non-normally distributed means. Receiver operating characteristic curve was drawn to detect the cutoff ADC value with calculation of sensitivity, specificity, negative predictive value, positive predictive value. The data were analysed with STATA version 14.1 (STATA Corp., Texas, USA). P values of 0.05 or less indicated statistical significance.

3. Results

Our study included 55 patients (23 male, 32 female) with 5 benign lesions (9.1%) and 50 malignant lesions (90.9%). The pathological diagnostics of benign lesions were thymic hyperplasia, teratoma and Castleman disease. High risk thymoma had the highest rate in malignant group (32%). Pathological diagnostics are presented in Table 1.

Table 1. Pathological diagnostics.

Pathology	Quantity	Rate
<i>Benign tumor</i>	5	
Thymic hyperplasia	2	40%
Teratoma	2	40%
Castleman disease	1	20%
<i>Malignant tumor</i>	50	
Low risk thymoma	13	26%
High risk thymoma	16	32%
Thymic carcinoma	8	16%
Thymic NET	2	4%
Malignant germ cell tumor	4	8%
Lymphoma	7	14%

The mean age of benign group was 26.8 ± 10.5 (range 13-37). The mean age of malignant group was 49.5 ± 16.4 (range 15-82). Out of benign lesions, teratoma had the largest diameter of 114.5 mm, Castleman disease had the smallest diameter of 36 mm. Out of

malignant lesions, malignant germ cell tumor had the largest diameter of 124.8 mm, low risk thymoma had the smallest diameter of 54.2 mm. Thymic hyperplasia and Castleman disease had regular margins and no cystic component. Tumors derived from germ cell (teratoma, malignant germ cell tumor) all contained cystic component and had lobulated margin. Among thymic epithelial tumors (low risk thymoma, high risk thymoma and thymic carcinoma), rate of lesions containing fluid and having lobulated margin increased correspondingly to the degree of malignancy. Most of lymphoma did not contain fluid, and have quite equal rates between lobulated margin lesions and regular margin lesions. Thymic hyperplasia and teratoma had high SII, 60.5% and 41.7% respectively. Other tumors have low SII, range from -5.1 to 7.4. Table 2 summarizes the detailed relationship between MRI findings and pathological diagnostics.

Table 2. Relationship between MRI findings and pathological diagnostics.

Pathology	Diameter ¹ (mm)	Margin ²		Cystic ²		SII ¹
		Regular	Lobulated	No	Yes	
<i>Benign (N=5)</i>	<i>73.4 ± 39.3</i>					
Thymic hyperplasia	49.5 ± 7.8	2 (100)	0	2 (100)	0	60.5 ± 44.2
Teratoma	114.5 ± 20.5	0	2 (100)	0	2 (100)	41.7 ± 6.4
Castleman disease	39	1 (100)	0	1 (100)	0	-5.1
<i>Malignant (N=50)</i>	<i>71.9 ± 32.3</i>					
Low risk thymoma	54.2 ± 20.7	10 (76.9)	3 (23.1)	9 (69.2)	4 (30.8)	7.4 ± 17.8
High risk thymoma	63.4 ± 31.7	6 (37.5)	10 (62.5)	11 (68.7)	5 (31.3)	-0.8 ± 6.5
Thymic carcinoma	74.6 ± 19.2	1 (12.5)	7 (87.5)	4 (50)	4 (50)	2.6 ± 5.3
Thymic NET	88.5 ± 24.7	0	2 (100)	0	2 (100)	-4.3 ± 9.1
Malignant GCT	124.8 ± 35.1	0	4(100)	0	4 (100)	1.4 ± 3.9
Lymphoma	86.1 ± 30.7	3 (42.9)	4 (57.1)	6 (85.7)	1 (14.3)	0.5 ± 4.7

¹In diameter and SII, data are reported as mean ± standard deviation

²In margin and cystic, data are reported as quantity (percent)

SII: Signal intensity index NET: Neuroendocrine tumor GCT: germ cell tumor

The differences in hot-spot-ROI-based mean ADC between benign and malignant, group A and B, lymphoma and other malignant tumors were statistically significant. Group B exhibited significantly lower ADC10, ADCmedian, ADCmean, and ADC90 (p < 0.05) compared to group A. There were no significant differences in the ADC10, ADCmedian, ADCmean and ADC90 between benign and malignant tumors, lymphoma and other malignant tumors (p > 0.05).

Table 3 shows ADC values of different benign and malignant mediastinal lesions obtained by two approaches: hot-spot ROI and whole-lesion histogram.

Table 3. Hot-spot-ROI-based and Histogram-based ADC measurements.

Pathology	Mean ADC (x10 ⁻³ mm ² /s)	Histogram-based (x10 ⁻³ mm ² /s)			
		ADC _{mean}	ADC _{median}	ADC ₁₀	ADC ₉₀
<i>Benign (N=4)</i>					
Thymic hyperplasia	1.47 ± 0.34	1.33 ± 0.12	1.34 ± 0.16	1.08 ± 0.05	1.55 ± 0.17
Teratoma	1.46 ± 0.2	1.24 ± 0.01	1.23 ± 0.04	0.99 ± 0.16	1.52 ± 0.21
Castleman disease	0.8	0.84	0.82	0.7	1.05
<i>Malignant (N=43)</i>					
Low risk thymoma	1.19 ± 0.18	1.2 ± 0.2	1,2 ± 0.2	0.97 ± 0.2	1,45 ± 0,2
High risk thymoma	0.98 ± 0.36	1.05 ± 0.28	1.06 ± 0.29	0.81 ± 0.24	1.3 ± 0.31
Thymic carcinoma	0.9 ± 0.17	0.93 ± 0.15	0.93 ± 0.15	0.74 ± 0.14	1.12 ± 0.17
Thymic NET	0.6 ± 0.04	0.83 ± 0.04	0.82 ± 0.04	0.63 ± 0.03	1.03 ± 0.03
Malignant GCT	0.8 ± 0.16	1.1 ± 0.17	1.08 ± 0.16	0.82 ± 0.09	1.33 ± 0.19
Lymphoma	0.75 ± 0.12	0.95 ± 0.16	0.94 ± 0.17	0.76 ± 0.13	1.16 ± 0.2
Data are reported as mean ± standard deviation					
ADC: Apparent diffusion coefficient		NET: Neuroendocrine tumor		GCT: germ cell tumor	

ROC curves were drawn to determine the diagnostic value of hot-spot-ROI-based mean ADC and the histogram parameters for differentiating benign lesions and malignant lesions, group A and group B, lymphoma and other malignant tumors, with calculation of the cutoff value, sensitivity, specificity, and area under the ROC curve (AUC). Results are presented in table 4.

Table 4. Diagnostic Ability of Histogram-Based and Hot-Spot-ROI-Based ADC Measurements for differentiation between malignant and benign, A and B, Lymphoma and other malignant tumors.

<i>Benign and malignant</i>		AUC	Cut-off	Sensitivity	Specificity	Accuracy
Mean ADC		0.794	1.17	80	80	80
<i>Group A and B</i>		AUC	Cut-off	Sensitivity	Specificity	Accuracy
Mean ADC		0.843	0.99	78.4	88.9	81.8
Histogram-based approach	ADC _{mean}	0.755	1.04	64.9	83.3	70.9
	ADC _{median}	0.752	1.03	64.9	83.3	70.9
	ADC ₁₀	0.758	0.85	75.7	72.2	74.6
	ADC ₉₀	0.755	1.22	62.2	88.9	70.9
<i>Lymphoma and other malignant tumors</i>		AUC	Cut-off	Sensitivity	Specificity	Accuracy
Mean ADC		0.772	0.91	100	60.5	66
ADC: Apparent diffusion coefficient						

Mean ADC value based on hot-spot-ROI with the cutoff value of 1.17 had the highest sensitivity, specificity, accuracy in differentiating groups of tumors above. Out of ADC values obtained from whole-tumor histogram analysis, ADC10 was the most valuable in differential diagnostic, followed by ADCmean, ADC90 and ADCmedian. (Figure 3)

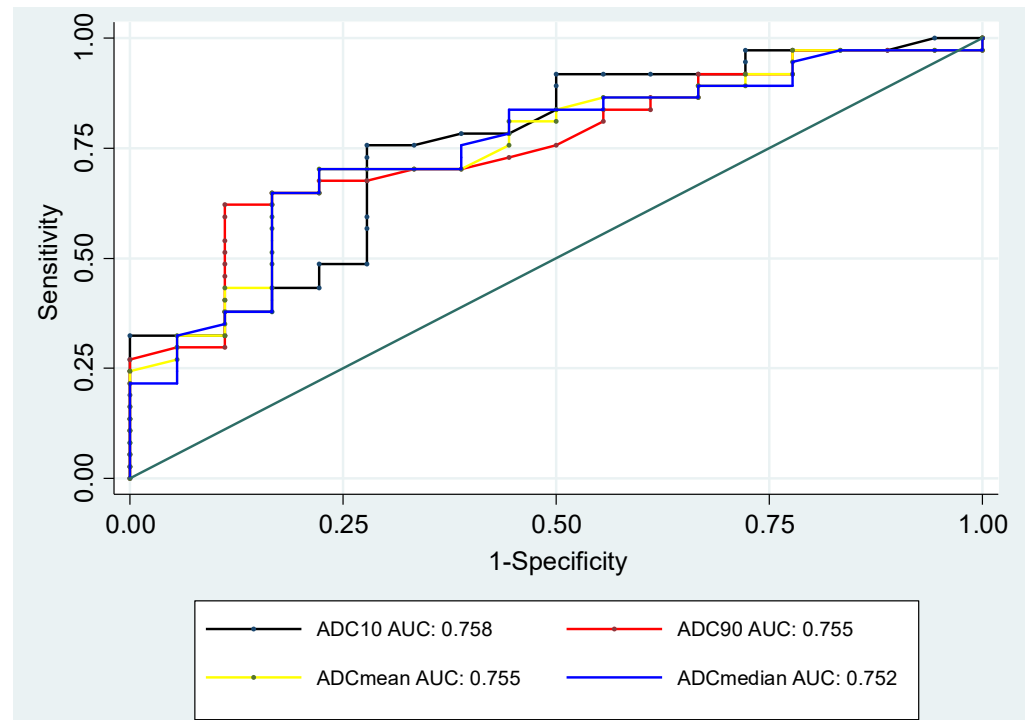


Figure 3. ROC curves of histogram-based ADC measurements for differentiating between A and B.

4. Discussion

The findings of the largest diameter, contour and cystic component of anterior mediastinal tumors in our study were quite similar to macroscopic appearance as well as radiographic features of these tumors described in textbooks [5-7].

Our study showed that average SII of thymic hyperplasia was 60.5%, and this result was close to the result of M. Priola et al, in which the average SII of thymic hyperplasia was 45.9% [8]. The mean SII value of teratoma was 41.7%, which was correlated well with the fat component in these lesions. Academically, macroscopic and microscopic appearance of Castleman disease and malignant tumors in anterior mediastinum show no fat component, and the low average SII of these lesions in our study demonstrated that fact as well. The low SII of malignant tumors in our study was also similar to the result of M. Priola et al [8]. M. Priola et al reported that SII was perfectly used to distinguish malignant tumors from thymic hyperplasia with the cut-off point of 8.92% (sensitivity and specificity 100%), and no overlap was found for SII between groups [8]. However, in our study, one case pathologically diagnosed as sclerosing thymoma, had a high SII value, which was overlapped with SII values in teratoma and thymic hyperplasia groups. It can be explained that when placing a ROI within the tumor to determine SII value, we accidentally chose the area having both tumoral tissue and normal thymic tissue, so that fat in normal thymic tissue raised the SII value. Similarly, there was a case report of a sclerosing thymoma by Li Xin et al, the surgical specimen of this case contained adipose tissue, imperfect degradation of thymus tissue and tumor components [9]. If the SII value of sclerosing thymoma was the outlier, there would be no overlapped values between teratoma, thymic hyperplasia group and other tumors group.

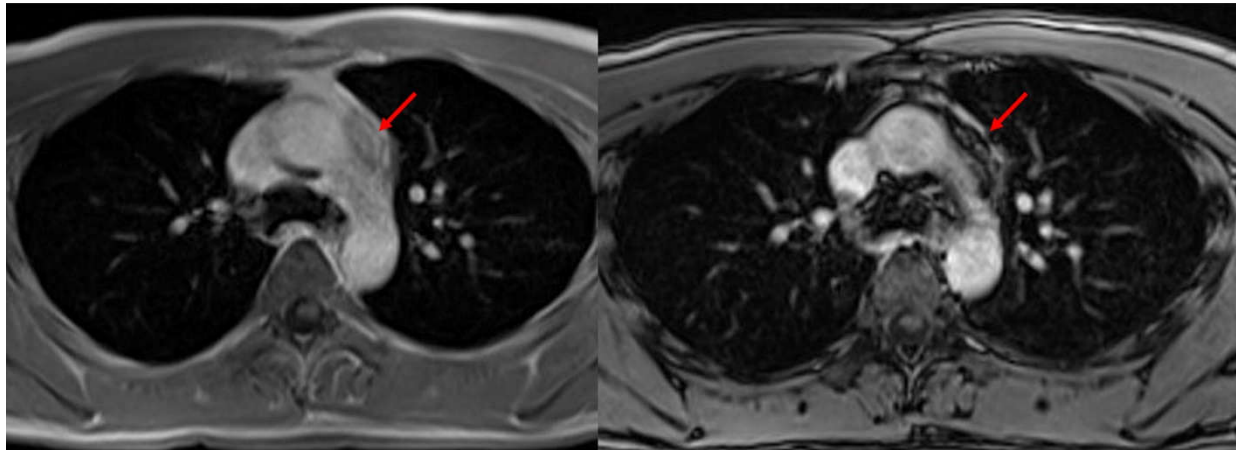


Figure 4. Sclerosing thymoma.

A 27-year-old male patient with an anterior mediastinal mass. Placing a ROI in A (inphase) and B (opphase) with the same position and area to identify SII. SII was calculated and the result was 64,6%. The pathological result was sclerosing thymoma.

When using the hot-spot approach, the mean ADC to distinguish malignant from benign tumors was $1.17 \times 10^{-3} \text{mm}^2/\text{s}$, with the area under curve ROC was 0.794, sensitivity and specificity were 80%. This result is concordant with that of Raafat et al who revealed that the cut-off ADC value for the differentiation between malignant and benign mediastinal lesions was $1.11 \times 10^{-3} \text{mm}^2/\text{s}$, with sensitivity of 90.9% and specificity of 100% [10]. However, our result is discordant with Usuda et al, who reported higher cut-off value of $2.21 \times 10^{-3} \text{mm}^2/\text{s}$ for the discrimination between malignant and benign mediastinal tumors [11]. The differences in sample size and ADC measurement method between our study and Usuda's may lead to the distinction of the two results. There were some cystic lesions in Usuda's study, whereas our study excluded the cystic lesions. In addition, when measuring the ADC values, Usuda et al placed a ROI around the margin of the tumor without excluding fatty, necrotic, cystic and hemorrhagic areas, leading to the higher ADC values.

When comparing the hot-spot-ROI-based mean ADC between group A and B, the results of our study demonstrated that the mean ADC value of group B was significantly lower than the mean ADC value of group A, with the cut-off point of $0.99 \times 10^{-3} \text{mm}^2/\text{s}$, sensitivity, specificity, accuracy were 78.4%, 88.9% and 81.8% respectively. In agreement with our study, Nars et al reported cut-off value of $1.15 \times 10^{-3} \text{mm}^2/\text{s}$, sensitivity was 95%, specificity was 93.8% and accuracy was 94.4% [2]. However, this was discordant with Razeq et al and Gumustas et al, they both reported higher cut off ADC value of $1.56 \times 10^{-3} \text{mm}^2/\text{s}$ and $1.39 \times 10^{-3} \text{mm}^2/\text{s}$ [12,13].

In agreement with Zhang et al, who reported that mean ADC of lymphoma was significantly lower than the mean ADC of thymic carcinoma, our study showed that the hot-spot-ROI-based mean ADC value of lymphoma was significantly lower than the mean ADC value of other malignant mediastinal tumors, with the cut-off point was $0.91 \times 10^{-3} \text{mm}^2/\text{s}$. However, Zhang et al reported the lower cut-off ADC value of $0.73 \times 10^{-3} \text{mm}^2/\text{s}$ [9]. This variation of cut-off ADC values is likely attributed to the discrepancy in the sample size. Our result was discordant with Razeq et al, Gumustas et al, Sabri et al, they were all reported that there was no significant difference in the mean ADC value between lymphoma and other malignant tumors [12-14].

When whole-lesion histograms were used to derive ADC parameters, our study showed that ADC₁₀, 90, mean, median in group B were significantly lower than those in group A. ADC₁₀ demonstrated a significantly better performance, when using ADC₁₀ = $0.85 \times 10^{-3} \text{mm}^2/\text{s}$ as the cut-off value, the optimal distinction could be obtained, with sensitivity was 75.7%, specificity was 72.2% and accuracy was 74.6%. This was quite similar to the result of Zhang et al, who reported that ADC₁₀ was superior to mean, median or 90th percentile ADC in differentiating tumors [9]. In agreement with our result, Kong et al

demonstrated that ADC10 showed best differentiating ability for discriminating low-risk thymoma from high-risk thymoma and thymic carcinoma [9]. Huang et al found that ADC10 was helpful in WHO grading of ependymoma [15]. Similarly, Donati et al showed that ADC10 correlated with Gleason score better than the other ADC did, suggesting that the 10th percentile ADC may be the best for distinguishing low- from intermediate- or high-grade prostate cancer [16]. Within a tumor with heterogeneous cellularity, focal areas with high cellularity were represented to a greater extent by the low percentile ADCs than mean or median ADCs. [17]. Therefore, it was easy to understand why ADC10 demonstrated a better differentiating performance.

Our study had some limitations. First, the sample size was small. Second, there was a wide spectrum of diseases and histopathological types in our study. Further studies focusing on specific tumor types with large sample size are recommended.

5. Conclusion

Chemical shift MRI is valuable for determining the fatty component of lesions and organs. We suggested that diffusion weighted MRI with ADC measurements may help in differentiating malignant tumors from benign tumors, lymphoma from other malignant tumors in anterior mediastinum and hot-spot-based-ROI mean ADC was the most useful value in distinguishing these groups of tumors.

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Informed Consent Statement: Informed consent was waived because of the retrospective nature of the study and the analysis used anonymous clinical data.

Data Availability Statement: Not applicable.

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