

## Article

# Hybrid Vesicle Stability under Sterilisation and Preservation Processes Used in the Manufacture of Medicinal Formulations

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**Abstract:** Sterilisation and preservation of vesicle formulations are an important consideration for their viable manufacture for industry applications, particular those intended for medicinal use. Here we undertake an initial investigation of the stability of hybrid lipid – block copolymer vesicles to common sterilisation and preservation processes, with particular interest in how the block copolymer component might tune vesicle stability. We investigate two sizes of polybutadiene-*block*-poly(ethylene oxide) polymers (PBd<sub>12</sub>-PEO<sub>11</sub> and PBd<sub>22</sub>-PEO<sub>14</sub>) mixed with the phospholipid POPC considering the encapsulation stability of a fluorescent cargo and the colloidal stability of vesicle size distributions. We find that autoclaving and lyophilisation cause complete loss of encapsulation stability under the conditions studied here. Filtering through 200 nm pores appears to be viable for sterilisation for all vesicle compositions with comparatively low release of encapsulated cargo, even for vesicle size distributions which extend beyond the 200 nm filter pore size. Freeze-thaw of vesicles also shows promise for preservation of hybrid vesicles with high block copolymer content. We discuss the process stability of hybrid vesicles in terms of the complex mechanical interplay between bending resistance, stretching elasticity and lysis strain of these membranes and propose strategies for future work to further enhance the process stability of these vesicle formulations.

**Keywords:** liposomes; polymersomes; filtration; freeze-thaw; membrane mechanics; encapsulation stability

## 1. Introduction

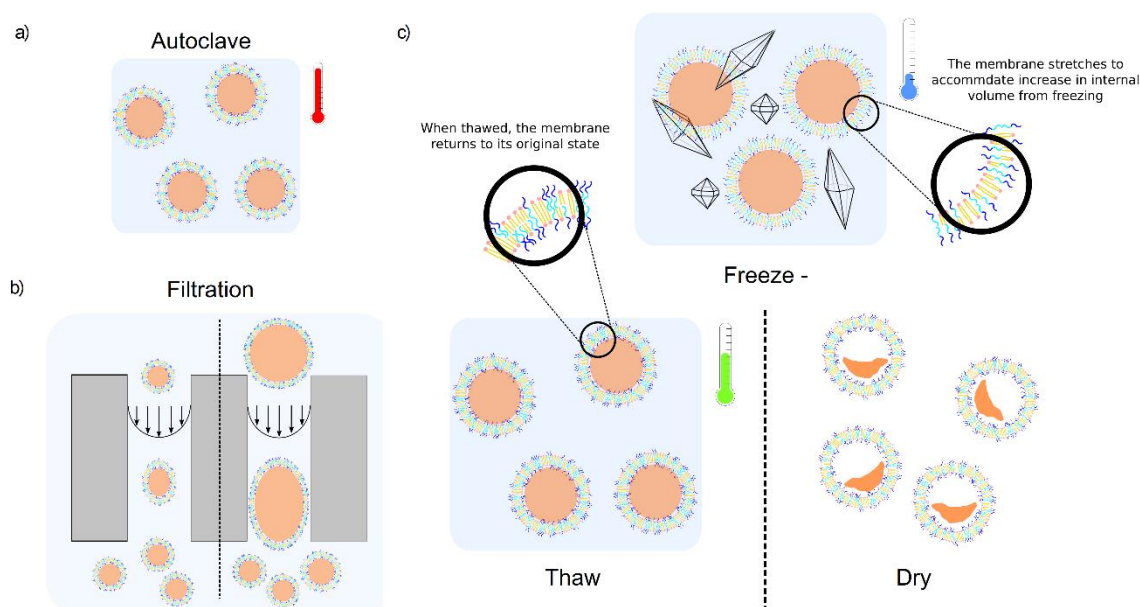
Hybrid vesicles aim to combine the properties of biomimetic liposomes and synthetic polymersomes into composite membrane-bound capsules with broader tuneability of material properties.[1-10] This expanded material parameter space is anticipated to be beneficial in the development of hollow vesicle structures for technological applications such as sensors, biotechnology, nanoreactors, synthetic biology and formulated products, including those intended for medicinal purposes.[11-21]

Individually, liposomes and polymersomes offer different advantages.[22] Liposomes, composed of natural lipids, form bilayer membranes that closely mimic the structural matrix of native biomembranes. This makes them highly biocompatible and provides a native-like environment if integral membrane proteins are desired to add functionality to the membrane.[23-27] However liposomes can have inherent instabilities. Their membranes are highly flexible under bending deformations, but weak under stretching deformations, with a lysis strain of less than 5% [28, 29]. The labile fluidity of the membrane can lead to transient membrane defects that frustrates long term encapsulation stability and lipid peroxidation can cause chemical instabilities in these structures.

Polymersomes, due to their synthetic nature, are often less biocompatible than their lipid counterparts but offer greater mechanical stability and a broader chemical parameter space.[30] Their membranes are often thicker than liposome membranes, which provides greater bending resistance and their enhanced elasticity under stretching makes them tough and durable.[22] The polymer chemistry can be designed to minimise chemical instability but also to incorporate novel functionality. In blending liposomes and polymersomes to create hybrid vesicles, the ambition is to combine advantageous properties of these materials while off-setting their weaknesses.[31]

For medicinal applications in particular, stringent regulatory requirements exist for the sterilisation and preservation during transportation and storage of these formulations.[32] Vesicles need to exhibit good stability under appropriate processing conditions that maintain the encapsulation of active compounds and the colloidal stability of vesicle structures.

Sterilisation is required to make the product safe for public use. It is the process by which all forms of life are destroyed, removed or permanently inactivated. Instead of an absolute measure of sterilisation, pharmaceutical industries use processes that reduces the probability of the survival of undesired organisms to a negligible level. Currently, pharmaceutical companies use thermal, filtration and irradiation techniques to sterilise their products [32, 33]. Thermal sterilisation (Fig. 1a), by using an autoclave, is the most common and the most reliable as it achieves destruction of microorganisms by irreversible denaturation of enzymes [32] and it allows the sterilisation of larger objects more easily than filtration [34].



**Figure 1. Schematic of sterilisation and preservation processes applied to vesicle formulations.** (a) Autoclaving; (b) filtration; (c) freeze-thaw and lyophilisation.

Filtration through a maximum of a 0.22  $\mu\text{m}$  membrane is usually used for sterilisation of thermally labile solutions while sterilisation of active ingredients or medical devices can be achieved by irradiation [33]. Filtration exerts fluid shear stresses on vesicles as they pass down channels in the filter membrane (Fig. 1b). While vesicles smaller than the filter pore size might fit within the channel without needing to deform, under flow, the Poiseuille velocity flow field in the channel indicates the fluid is moving much faster in the centre of the pore channel than at the edges. This will deform even small vesicles and, depending on the magnitude of these stresses, could induce transient pore formation in the membrane, compromising encapsulation stability, or even causing break-up of the vesicles. For larger vesicles, greater in size than the pore diameter, these vesicles must also deform at the entrance to the channel and will experience greater shear stresses that increases the probability that these vesicles might break-up into smaller structures.

Stability during storage and transportation of vesicle formulations can also be a challenge. This may be transport between primary and secondary manufacturing sites or between the manufacturer

and end-user. Once reaching the end-user, formulations may be stored for some time before their final use. Cold chain transportation is frequently used for medicinal products to maintain the stability and activity of their ingredients. Cryogenic conditions are frequently used for preservation during the transportation and storage of delicate biologics and labile formulations.

Liquid formulations are often frozen for preservation (Fig. 1c). However storing frozen samples for an extended period can cause ice crystal formation that could cause membrane damage for vesicles during freezing and thawing [35]. Besides potential damage from ice crystals, vesicles will become stressed by the expansion of water inside their lumen upon freezing. The volume of water expands by ~9% upon freezing, which will exert a ~6% areal strain on the confining membrane, which exceeds the lysis strain for lipid membranes. Indeed freeze-thaw cycles are used to intentionally rupture liposomes during the passive loading of compounds from the bulk medium. Formulations may experience several freeze-thaw processes during manufacture, transport and storage, whether deliberate or unintentional. Fluctuations in temperature during transport from improper storage and shipping can cause some samples to reach their destination past their shelf life. This makes some drug formulations ineffective or even harmful [36, 37].

Lyophilisation (freeze-drying) can also be used to maintain the stability of lipids during transportation and storage. During the freeze-drying process the product is frozen, thus immobilising the sample and allowing it to retain its original form, and then the water is removed by sublimation (Fig. 1c), preventing microbial growth [38]. For lipids, the absence of water would minimise the rate of hydrolysis during storage [39]. However lyophilisation of liposome formulations is challenging to maintain encapsulation and structural stability. Additives are required for liposome cryopreservation yet their efficacy can be variable and inconsistent.[40]

Here we investigate hybrid vesicles composed of a phospholipid 1-palmitoyl-2-oleoyl-sn-glycero-3-phosphocholine (POPC) and one of two amphiphilic polybutadiene-block-polyethylene oxide (PBd-*b*-PEO) diblock copolymers of different molecular weights under conditions designed to mimic industrial sterilisation and storage/transportation processes. We explore the full hybrid compositional space from pure lipid to pure polymer vesicles. Sterilisation is mimicked through autoclaving or multiple filtration passes through a filter with a 0.2  $\mu\text{m}$  pore size. The storage/transportation of samples is emulated through either lyophilisation and rehydration, or multiple freeze-thaw-vortex (FTV) cycles. This preliminary study of hybrid vesicle stability under these conditions is designed as a stringent test of their stability that will highlight advantages that can be gained through the composition of the hybrid formulation and to uncover aspects of these formulations that will require optimisation for future commercial translation. As such, we investigate the hybrid vesicle in a physiological saline buffer without additional additives for enhanced stability, such as potential cryo-preserved.

## 2. Materials and Methods

### 2.1. Materials

The di-block copolymers poly(1,2-butadiene)-*block*-(polyethylene oxide) (PBd-*b*-PEO) with total molecular weights of 1800  $\text{gmol}^{-1}$  and 1150  $\text{gmol}^{-1}$  were purchased from Polymer Source, Inc. (Montreal, Canada). PBd<sub>22</sub>-PEO<sub>14</sub> (PDI 1.01) has a hydrophobic PBd block of 1200  $\text{gmol}^{-1}$  (>85% 1,2 addition) and a hydrophilic PEO block of 600  $\text{gmol}^{-1}$  while PBd<sub>12</sub>-PEO<sub>11</sub> (PDI 1.09) has a hydrophobic PBd block of 650  $\text{gmol}^{-1}$  (85% 1,2 addition) and a hydrophilic PEO block of 500  $\text{gmol}^{-1}$ .

The lipid 1-palmitoyl-2-oleoyl-sn-glycero-3-phosphocholine (POPC) was purchased from Avanti Polar Lipids (Alabaster, AL, USA). 5(6)-Carboxyfluorescein (CF) and other reagents were purchased from Sigma Aldrich.

### 2.2. Vesicle Preparation

Large unilamellar vesicles (LUVs) were prepared by the thin film rehydration and extrusion method. To generate different hybrid vesicle compositions, relative volumes of POPC (32 mM) and PBd-PEO (6.57 mM) in chloroform were measured using a Hamilton syringe into a glass vial. The

solutions were dried in a vacuum desiccator to give a lipid/polymer film and then rehydrated with 1.0 mL of aqueous solution of 60 mM CF with 40 mM 4-(2-hydroxyethyl)-1-piperazineethanesulfonic acid (HEPES), 20 mM sodium chloride, adjusted the pH to 7.4 by dropwise addition of sodium hydroxide. The films were incubated at 50°C for 5 min and vortexed for 1 min. The suspensions were then frozen in liquid nitrogen, thawed in a 60°C water bath and vortexed for 10 s. This cycle was repeated 5 times. Suspensions were extruded 11 times through a 100 nm or 400 nm pore size polycarbonate membrane filters using a LiposoFast Basic Extruder. The nanovesicle samples were run on a Sephadex G50 column under gravity using 40 mM HEPES and 20 mM sodium chloride buffered to pH 7.4 as the mobile phase to remove unencapsulated CF dye. The resulting 3 mL fractions were characterised using dynamic light scattering (DLS) for particle size distribution to confirm the presence of vesicles. The hybrid vesicles are then further analysed for stability under sterilisation and preservation processes.

### 2.3. CF Release Assay

The 100 nm sized hybrid vesicle samples were split into 4 fractions of 500 µL (~2 mM). Fraction 1 was thermally sterilised using an autoclave at 121°C for 15 min. Fraction 2 was lyophilised using a VirTis Benchtop Pro Lyophiliser for 24 h after freezing the sample in nitrogen. Fraction 3 underwent 5 filtration cycles through a 13 mm PTFE 200 nm syringe filter device with polypropylene housing. Fraction 4 was frozen in liquid nitrogen, thawed in a water bath at 60°C and vortexed for 3 s. The samples undergo 4 of these freeze-thaw-vortex (FTV) cycles.

The 400 nm sized vesicles were filtered through a 13 mm PTFE 200 nm syringe filter device with a polypropylene housing 5 times.

CF is self-quenching at high concentrations (>40 mM) [41, 42], so the emission intensity at this concentration was often very low. The CF was encapsulated at 60 mM, so the control samples would have a low emission intensity. When the vesicles release the encapsulated CF, the CF was diluted by the external buffer and the fluorescence intensity increased.

To measure the CF release, 0.5 mL fractions were diluted to 2 mL (~18 µM) and the fluorescence emission at 519 nm of CF-encapsulated vesicles was measured with excitation set to 492 nm using a Horiba Scientific FluoroMax Plus. Measurements were made on initial vesicle fractions and between every processing cycle for each fraction. The initial vesicle preparations were ruptured with 50 µL of 10% (w/v) Triton X-100 (end concentration 0.91% (w/v)) to completely destabilise the vesicles and release the encapsulated CF before a final fluorescence emission at 519 nm was measured.

The CF % release was calculated by

$$\% CF release = \frac{I_i - I_0}{I_t - I_0} \times 100\%$$

Where  $I_0$  is the initial intensity of the sample,  $I_i$  is the intensity of the sample after each processing cycle (from autoclaving, lyophilisation, FTV or filtering), and  $I_t$  is the intensity after the initial sample is burst with Triton X-100.

### 2.4. Dynamic Light Scattering (DLS)

After separating hybrid vesicles with encapsulated CF from excess CF, the vesicles were characterised using a Malvern Zetasizer Nano ZSP with scattering angle 173° to determine their size. Each hybrid vesicle sample (0.5 mM) was measured at 25°C by the DLS and the results from 3 independent repeats were averaged. Size distributions were also measured after the processing steps described above to assess the colloidal stability of these vesicle formulations under these conditions.

### 2.5. Cryo-Electron Microscopy (cryo-EM)

Vesicles of 50 mol% PBd<sub>22</sub>-PEO<sub>14</sub> at 100 nm and 400 nm were imaged after initial preparation and after the final freeze-thaw-vortex and filtration cycles respectively. For 100 nm vesicles, 400 mesh 2/2 µm Cu Quantifoil grids were used, while for 400 nm vesicles 400 mesh Cu Lacey grids were used. All the carbon-coated grids were glow discharged for 33 s at 10 mA to render the surface hydrophilic.

Samples (3  $\mu$ L, ~2 mM) were placed directly onto the grid with a hold time of 40 s, using a FEI Vitrobot mkIV, using a blotting time of 6 s and a blot force of 6. The samples were kept in closed cryo-pucks under liquid nitrogen until required.

To image the grids, an FEI Titan KRIOS microscope with an accelerating voltage of 300 kV was used with a defocussing of 3  $\mu$ m at a magnification of  $\times 130000$  and  $\times 26000$ . The resolution for these images were 0.11 nm/pixel and 0.55 nm/pixel respectively.

Quantitative analysis of the images required taking diameter measurements and observations of all the vesicles in the grid holes of the carbon-coated copper grid using ImageJ. Histograms were made to document the size distribution observed in the grid holes, and notes were made on the ratio of multilamellar vesicles (MLVs) to unilamellar vesicles (ULVs).

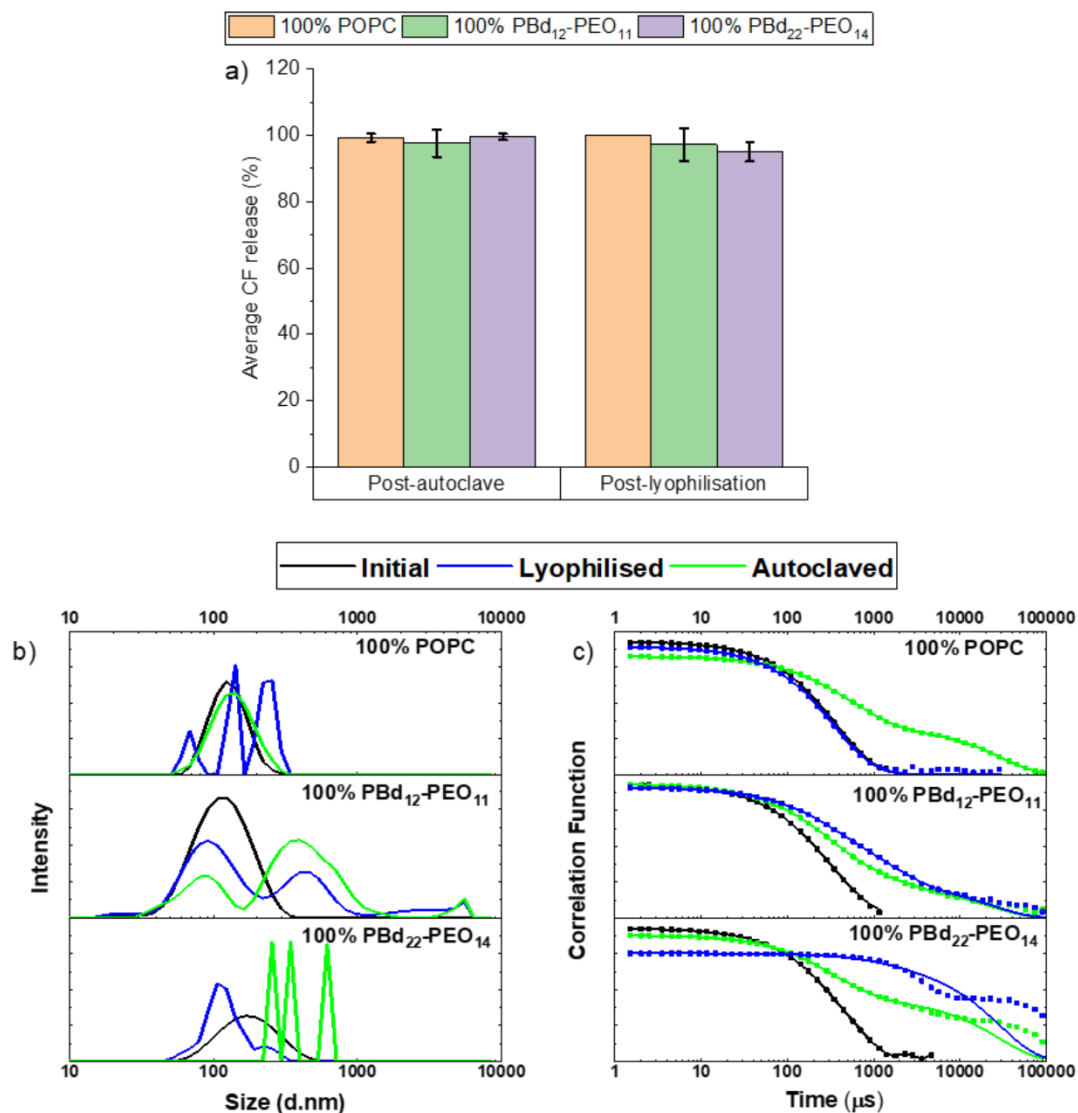
### 3. Results

We investigate the stability of hybrid vesicles under conditions designed to mimic industrial sterilisation and preservation processes. Our hybrid vesicles are composed of the lipid POPC blended with one of two PBd-*b*-PEO diblock copolymers of different length: PBd<sub>22</sub>-PEO<sub>14</sub> or PBd<sub>12</sub>-PEO<sub>11</sub>. We explore the full compositional parameter space from pure lipid to pure polymer vesicle compositions. Hybrid vesicles were formed by the thin film rehydration and extrusion method. The vesicles were loaded with the hydrophilic fluorophore CF as a model encapsulated compound. We study the encapsulation stability through release of CF from vesicles by fluorescence spectroscopy and the colloidal stability of the vesicle formulations from their hydrodynamic size distributions obtained by DLS.

#### 3.1. Autoclaving and Lyophilisation

Autoclaving and lyophilisation of hybrid vesicles would be the preferred choices for sterilisation and preservation, if these formulations can be made to be stable under these conditions. Unfortunately, both processes proved to be too destructive, causing vesicles to become unstable and release their entire contents. Only vesicles composed of the pure components were investigated: 100% POPC, 100% PBd<sub>22</sub>-PEO<sub>14</sub> and 100% PBd<sub>12</sub>-PEO<sub>11</sub>. As 100% CF release was observed in all cases (Fig. 2a), it was considered extremely unlikely that hybrid blends would perform any better.





**Figure 2. Release of encapsulated CF and size distributions from vesicles following autoclaving or lyophilisation.** (a) Vesicle compositions 100% POPC, 100% PBd<sub>12</sub>-PEO<sub>11</sub> and 100% PBd<sub>22</sub>-PEO<sub>14</sub> were investigated following autoclaving or lyophilisation. Each measurement was performed in triplicate and the errors data points represent mean  $\pm$  s.d. The DLS distributions of hydrodynamic diameters from (b) CONTIN fits size distributions and (c) the fitted autocorrelation functions. The size distributions shown represent the average distribution from three independent repeats.

The colloidal stability of the vesicles under these conditions was similarly poor. DLS size distributions were collected before and after autoclaving and lyophilisation (Fig. 2b). The fitting software returned errors for all post-process samples except for autoclaving of 100% liposomes. The poor fits to the auto-correlation function in these cases can be seen in Fig. 2c. We interpret this as aggregation and/or structural instabilities of the vesicles during autoclaving or lyophilisation.

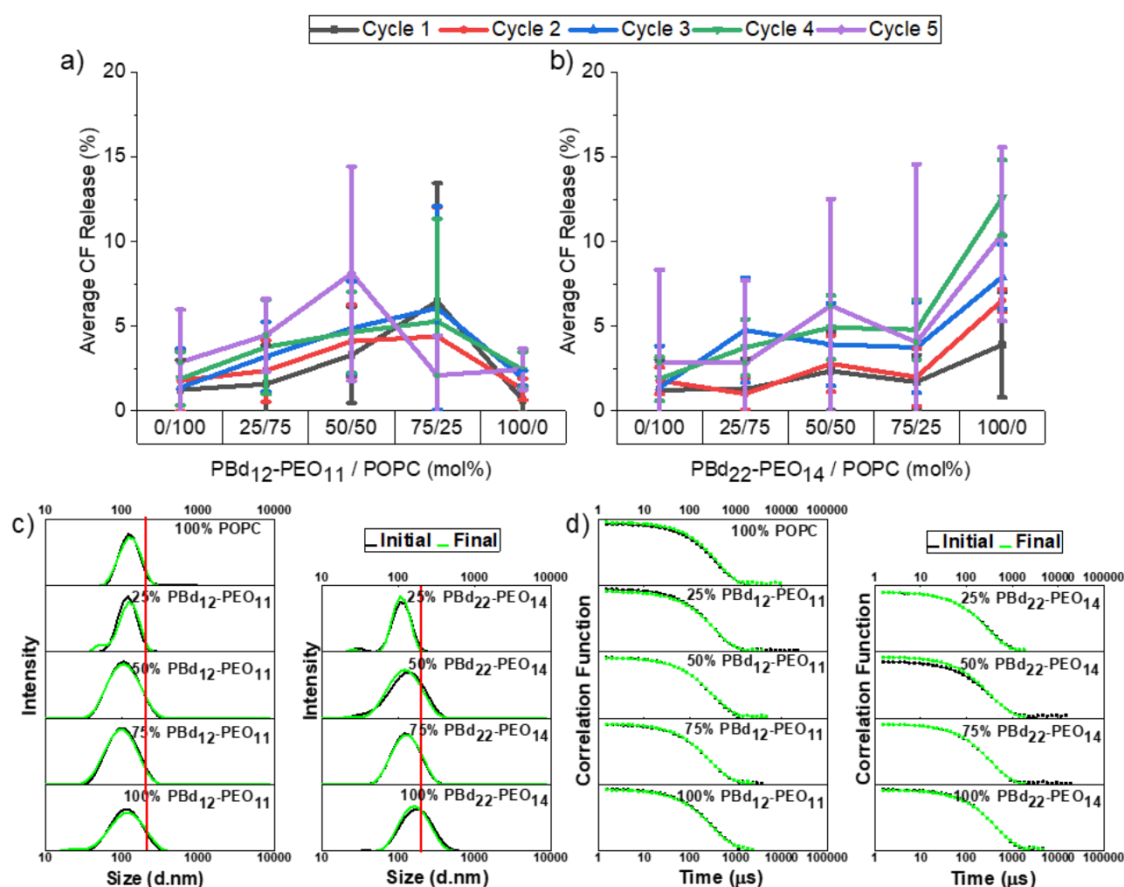
Since these vesicles are unstable under autoclaving and lyophilisation, we further investigate other potential methods of sterilisation and preservation. However, we do not conclude that these techniques are fundamentally hopeless for use with hybrid vesicles: further development of the vesicle formulations would be required, for example additional additives to the solution environment that help protect the integrity of the vesicles undergoing these processes.

### 3.2. Filtration

Sterilisation can be achieved by filtrations through a membrane with a maximum pore size of 0.22  $\mu\text{m}$ . Here, we use a 0.2  $\mu\text{m}$  pore size membrane to filter hybrid vesicles for between one and five cycles. Initially we investigated hybrid vesicles between 0 mol% to 100 mol% block copolymer content in 25 mol% increments for both PBd-*b*-PEO polymers. These vesicles were formed by extrusion through a 100 nm pore size membrane and encapsulated the CF dye.

All vesicle compositions only exhibited minimal contents release across five filtration cycles, with the average contents release reaching at most 10%. Fig. 3a shows filtration-induced contents release from hybrid vesicles containing the shorter PBd<sub>12</sub>-PEO<sub>11</sub> block copolymer. The unitary POPC and PBd<sub>12</sub>-PEO<sub>11</sub> vesicles exhibit very low (<5%) contents release across five filtration cycles and no vesicle composition exceeds 10% average release. Analysis of variance shows that there is no statistically significant ( $p < 0.05$ ) difference between the different vesicle compositions studied.

Perhaps surprisingly, the largest contents release occurred in vesicles composed of the larger PBd<sub>22</sub>-PEO<sub>14</sub> block copolymer (Fig. 3b), where a priori expectations might be that these would be the most mechanically stable vesicles. The only statistically significant difference in contents release is for pure PBd<sub>22</sub>-PEO<sub>14</sub> polymersomes, which is significant when compared to all other membrane compositions, where the extent of release marginally exceeds 10% for the 4<sup>th</sup> and 5<sup>th</sup> filtration cycle. However, this contents release is still relatively low even after several filtration cycles.

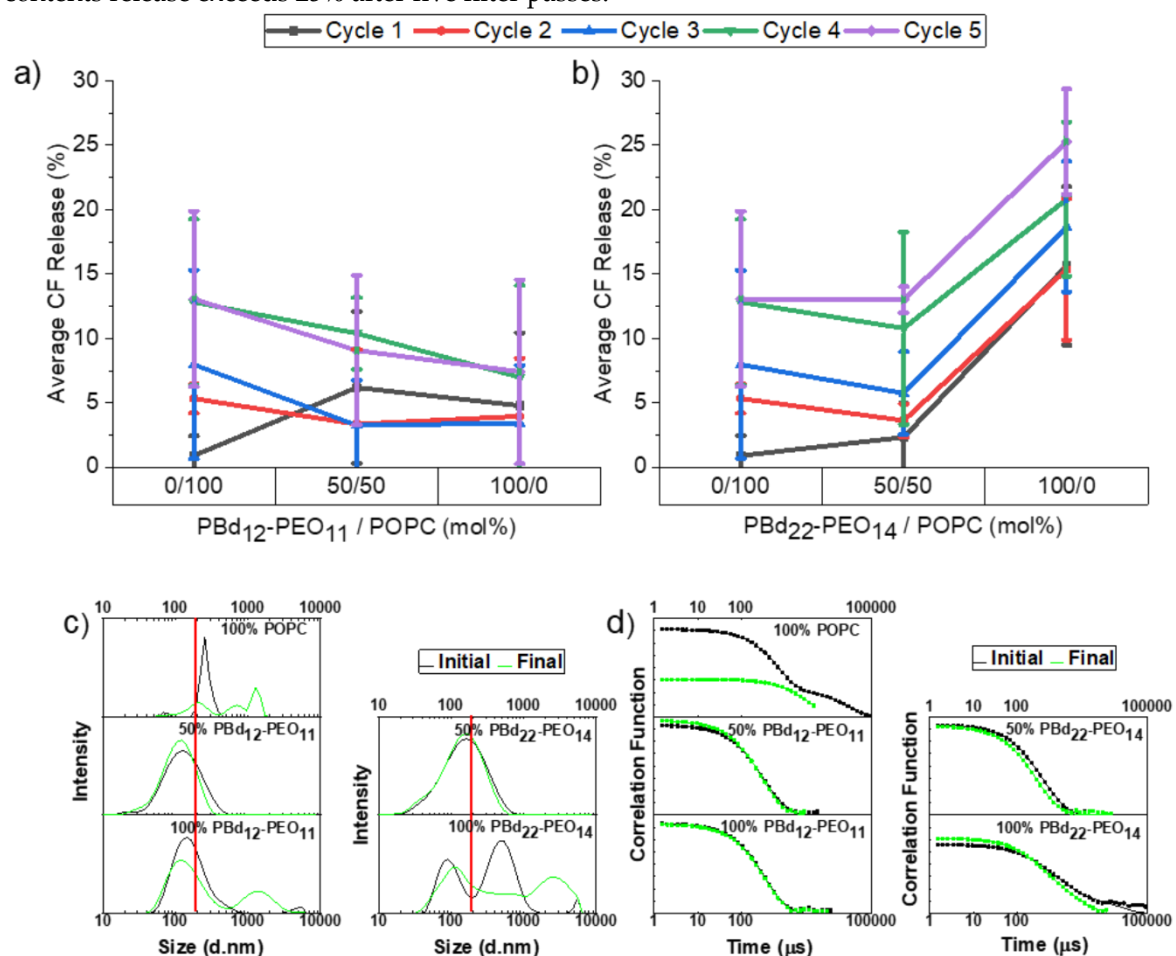


**Figure 3.** Release of encapsulated CF following filtration and size distributions before and after five filtration cycles. CF release % is plotted against membrane composition for hybrid vesicles composed of POPC and (a) PBd<sub>12</sub>-PEO<sub>11</sub>, or (b) PBd<sub>22</sub>-PEO<sub>14</sub>. Data is shown for between one and five filtration cycles through a 0.2  $\mu\text{m}$  pore size filter membrane. Each measurement was performed in triplicate and the errors data points represent mean  $\pm$  s.d. The DLS distributions of hydrodynamic diameters of PBd<sub>12</sub>-PEO<sub>11</sub> or PBd<sub>22</sub>-PEO<sub>14</sub> hybrid vesicles before and after five filtration cycles: (c) CONTIN fit size distributions; (d) the fitted autocorrelation functions. The size distributions shown represent the average distribution from three independent repeats. The line at 0.2  $\mu\text{m}$  denotes the filtration pore size.

Hybrid vesicles (100 nm extrusion pore size) also demonstrate colloidal stability following multiple filtration cycles (Fig. 3c and 3d). Vesicle size distributions obtained by DLS before and after five filtration cycles were comparable for all hybrid vesicle compositions and both polymer sizes. No evidence of break-up or aggregation of vesicles was observed. The red line on these graphs denotes the filter pore size of 200 nm. Vesicles with higher polymer content exhibit a tail in their size distribution which stretch beyond the filtration pore size. While these vesicles can pass the filter without notable changes in the particle size distribution, these also largely correlate with the vesicle compositions that exhibit the highest contents release suggesting that the probability of transient pores forming in the vesicle membrane increases when vesicles are larger than the pore size and must significantly deform during transit of the pore channel. This is particularly notable for the size distribution of 100 mol% PBd<sub>22</sub>-PEO<sub>14</sub> vesicles, where the highest contents release was measured in Fig. 3b.

Given that most of the 100 nm extruded vesicles are smaller than the 200 nm filter size, we presented a more stringent test of hybrid vesicle stability under filtration by using 400 nm extruded vesicles. In this series of experiments we investigated the pure lipid and polymer vesicles as well as the 50 mol% hybrid compositions by both polymer sizes.

Contents release from 400 nm extruded vesicles was significantly greater than previously observed for 100 nm extruded vesicles (Fig. 4). While the shorter PBd<sub>12</sub>-PEO<sub>11</sub> polymer appears to provide a mildly protective effect in hybrid vesicles with a gentle reduction in CF release observed with increasing polymer composition, these differences are not statistically significant (Fig. 4a). The only statistically significant difference in contents release is again observed for pure PBd<sub>22</sub>-PEO<sub>14</sub> polymer vesicles, which show reduced encapsulation stability compared to the POPC liposomes and 50 mol% hybrid vesicles (Fig. 4b). Despite this, overall contents release after five filtration cycles is small, being less than 15% for all compositions except the 100 mol% PBd<sub>22</sub>-PEO<sub>14</sub> vesicles, where contents release exceeds 25% after five filter passes.





**Figure 4. Release of encapsulated CF from 400 nm hybrid vesicles following filtration and size distributions before and after five filtration cycles.** CF release % is plotted against membrane composition for hybrid vesicles composed of POPC and (a) PBd<sub>12</sub>-PEO<sub>11</sub>, or (b) PBd<sub>22</sub>-PEO<sub>14</sub>. Data is shown for between one and five filtration cycles through a 0.2  $\mu\text{m}$  pore size filter membrane. Each measurement was performed in triplicate and the errors data points represent mean  $\pm$  s.d. The DLS distributions of hydrodynamic diameters of PBd<sub>12</sub>-PEO<sub>11</sub> or PBd<sub>22</sub>-PEO<sub>14</sub> hybrid vesicles before and after five filtration cycles: (c) CONTIN fit size distributions; (d) the fitted autocorrelation functions. The size distributions shown represent the average distribution from three independent repeats. The line at 0.2  $\mu\text{m}$  denotes the filtration pore size.

Filtration of PBd<sub>22</sub>-PEO<sub>14</sub> vesicles was more difficult than other vesicle compositions, requiring much higher pressures to be applied to force the vesicle sample past the filter. This indicates that these vesicles are the most rigid due to the high bending stiffness of the thicker polymer membranes. The higher pressures that need to be applied during filtration are therefore the likely cause of the enhanced contents release from these vesicles. On the other hand, the shorter polymer has lower bending resistance allowing these vesicles to more easily pass the filter and may impart some enhanced elasticity to hybrid vesicles, giving a mild protective effect to hybrid vesicles under filtration.

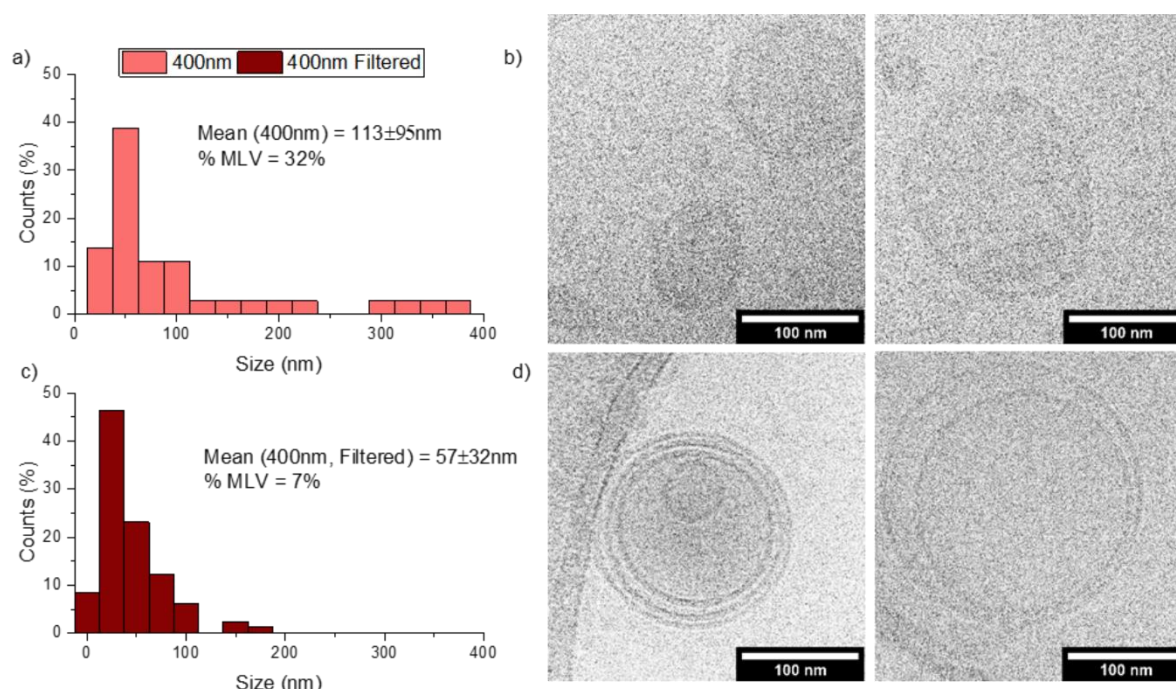
All vesicles were much smaller in size than the 400 nm pore size of the extrusion membrane for vesicle preparation (Fig. 4c and 4d). However a significant proportion of vesicles are larger than the 200 nm filter size, meaning that they would need to significantly deform or break-up to pass the filter. The initial 100% PBd<sub>22</sub>-PEO<sub>14</sub> vesicle size distribution also showed a bimodal distribution with peaks at 108 nm and 519 nm. Following five filter passes, all pure component vesicles, whether lipid or polymer, showed multimodal size distributions with larger structures present in solution that are indicative of aggregation and loss of colloidal stability in these samples.

Interestingly, both 50% hybrid vesicle formulations fared best under filtration with comparable monomodal size distributions before and after filtration. This enhanced colloidal stability might be due to synergistically enhanced properties of the blended lipid-polymer hybrid membranes. However it is also plausible that this is simply due to the smaller initial size distribution of these hybrid vesicles (145 nm for 50/50 mol% POPC/PBd<sub>12</sub>-PEO<sub>11</sub> hybrid vesicles and 182 nm for 50/50 mol% POPC/PBd<sub>22</sub>-PEO<sub>14</sub> hybrid vesicles). We previously observed good colloidal stability for 100 nm extrusion membrane vesicle formulations, therefore this latter explanation seems most likely. This smaller initial size distribution of 50 mol% hybrid vesicles might be due to a preferred curvature of the hybrid vesicle membrane that limits the maximum size of vesicles that form at this composition.

We further investigated the 400 nm 50/50 mol% POPC/ PBd<sub>22</sub>-PEO<sub>14</sub> hybrid vesicles before and after filtration by cryo-electron microscopy (cryo-EM) (Fig. 5). For cryo-EM, an aqueous sample is placed on a carbon-coated copper grid which is plunged in liquid ethane that vitrifies the water into a glass-like state to enable the sample to be seen [43, 44]. Ice thickness can vary depending on the dimensions of the particle but usually range from a few nanometres to a hundred nanometres [44]. The thicker the ice (>100 nm), the worse the resolution [45]. On the other hand, if the ice is too thin then either the sample is pushed towards the edge of the grid holes, or the sample can have a high affinity for the carbon support leaving the grid hole empty of sample and causing particle aggregation [43].

Initial 50 mol% PBd<sub>22</sub>-PEO<sub>14</sub> hybrid vesicles were found to have an average diameter of  $113 \pm 95$  nm and 32% of vesicles were observed to be multilamellar. This compares favourably with the previous DLS analysis where these vesicles have a z-average of 124 nm (PDI 0.279). However following filtration, the cryo-EM analysis gave an average vesicle size of  $57 \pm 32$  nm with 7% of vesicles found to be multilamellar. This differs from our DLS analysis, which showed a post-filtration z-average of 120 nm (PDI 0.269). The reduction in average size observed in cryo-EM can be seen from the histograms to be due to the removal of larger >200 nm vesicles from the post-filtered samples, likely due to vesicle break-up. Vesicle break-up during filtration would also explain the lower proportion of multilamellar vesicles that we observe. While larger vesicles can often be excluded from

the thin ice in the holes of the EM grid, artificially leading to smaller size distributions by cryo-EM compared to DLS, the comparison between the pre- and post- filtered hybrid vesicles by cryo-EM would appear to be significant. The break-up of some larger and multilamellar vesicles during filtration would likely account for the ~15% leakage of vesicle contents observed in Fig. 4.



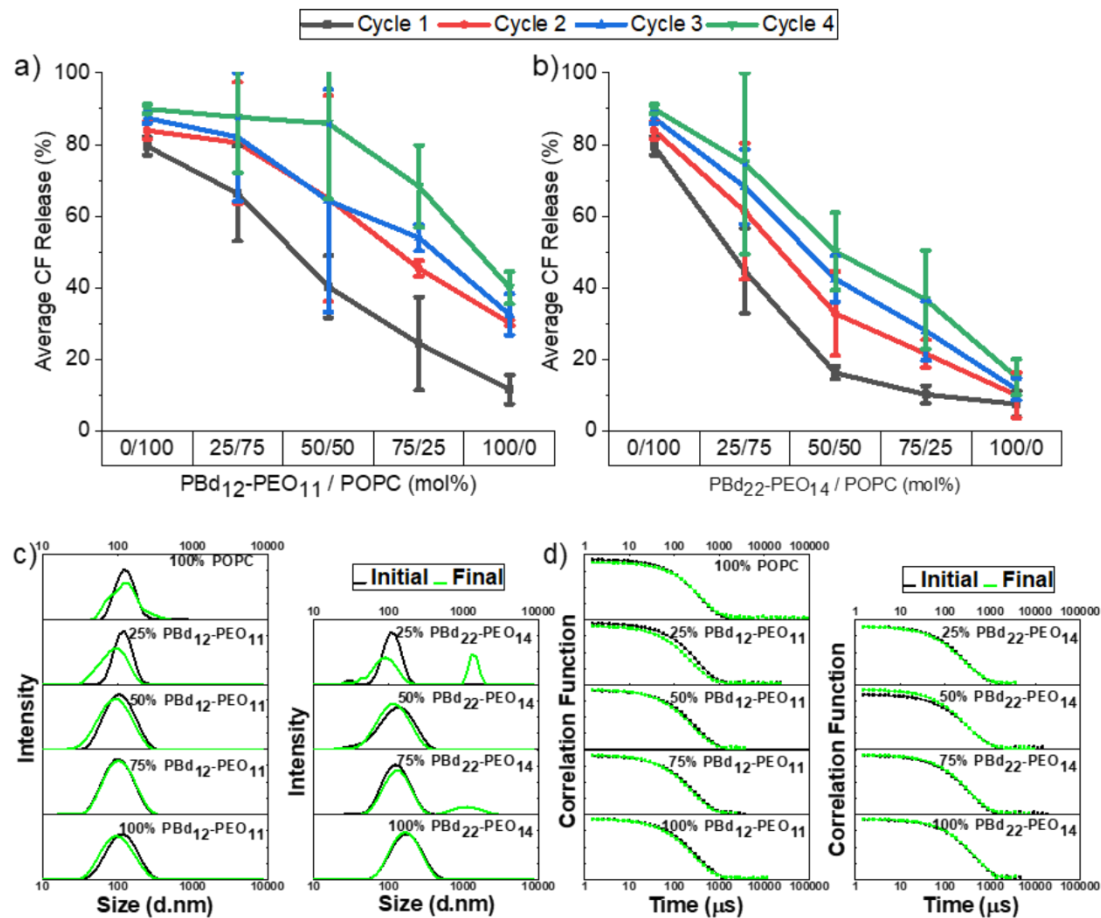
**Figure 5.** Cryo-TEM of 50 mol% PBd<sub>22</sub>-PEO<sub>14</sub> hybrid vesicle (400 nm extrusion membrane) before and after five filtration cycles. (a) Histogram of initial vesicle sizes; (b) representation images of vesicles before filtration; (c) histogram of vesicle sizes after filtration; (d) representation images of vesicles after filtration. Scale bars represent 100 nm.

### 3.3. Freeze-Thaw-Vortex

An alternative preservation process to lyophilisation is to store vesicle sample frozen from the liquid state without sublimation of excess water. Therefore we investigate the stability of vesicles to up to four freeze-thaw-vortex (FTV) cycles. The vortexing step following thawing of frozen samples is included to ensure the vesicles are fully resuspended in the liquid state.

Liposome encapsulation was observed to be highly unstable even after a single FTV cycle (Fig. 6). This is unsurprising as freeze-thaw cycles are frequently used for passive loading of cargo in liposome preparation protocols as this renders the membrane temporarily permeable. Conversely 100% polymer vesicles exhibit much greater encapsulation stability across four FTV cycles with hybrid formulations showing increasing stability with increasing block copolymer composition in the membranes. For all vesicle compositions CF release increased after each FTV cycle.

Vesicles containing the larger PBd<sub>22</sub>-PEO<sub>14</sub> polymer were also observed to have more stable CF encapsulation than those formulated with the PBd<sub>12</sub>-PEO<sub>11</sub> polymer. We interpret this as the thicker membranes formed from the larger block copolymer having greater elasticity, permitting the membrane to stretch without rupture during the volume expansion of freezing. Furthermore the thicker, more elastic membranes of these vesicles enhances protection from damage that might be caused by the local growth of ice crystals in the sample.

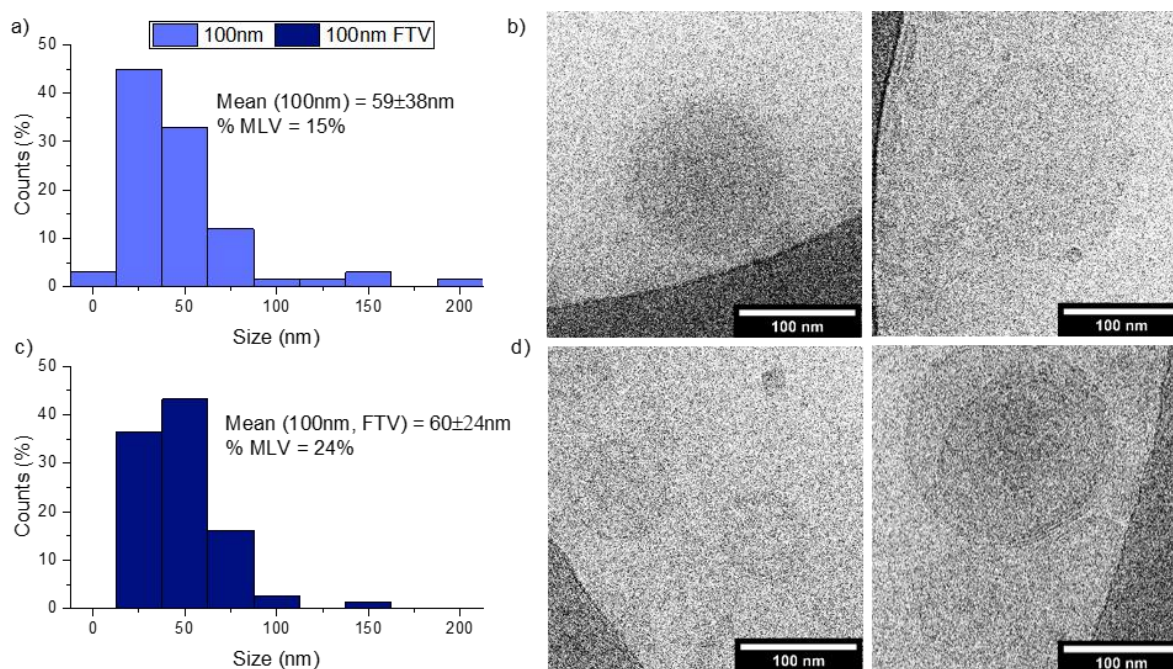


**Figure 6.** Release of encapsulated CF from 100 nm hybrid vesicles following FTV cycles and size distributions before and after four FTV cycles. CF release % is plotted against membrane composition for hybrid vesicles composed of POPC and (a) PBd<sub>12</sub>-PEO<sub>11</sub>, or (b) PBd<sub>22</sub>-PEO<sub>14</sub>. Data is shown for between one and four FTV cycles. Each measurement was performed in triplicate and the errors data points represent mean  $\pm$  s.d. The DLS distributions of hydrodynamic diameters of PBd<sub>12</sub>-PEO<sub>11</sub> or PBd<sub>22</sub>-PEO<sub>14</sub> hybrid vesicles before and after four FTV cycles: (c) CONTIN fit size distributions; (d) the fitted autocorrelation functions. The size distributions shown represent the average distribution from three independent repeats.

FTV cycles had most impact on the colloidal stability of lipid-rich vesicles. We measured the vesicle size distributions by DLS before and after four FTV cycles (Fig. 6c and 6d). While the post-FTV size distributions are mostly monomodal (with the exception of 25 mol% and 75 mol% PBd<sub>22</sub>-PEO<sub>14</sub> hybrid vesicles), the size distributions for 100% POPC and 25 mol% polymer hybrid vesicles significantly broaden following four FTV cycles. In contrast, the size distributions of hybrid vesicles with  $\geq 50$  mol% polymer content are broadly similar before and after the FTV cycles.

We further investigate the effect of freeze-thaw action on the size and morphology of 50 mol% PBd<sub>22</sub>-PEO<sub>14</sub> hybrid vesicles by cryo-EM. Quantitative analysis of the images shown in Fig. 7 错误!未找到引用源。 indicate that the vesicles have a similar size before and after the FTV cycles ( $59 \pm 38$  nm vs.  $60 \pm 24$  nm) and a slightly increase prevalence of multilamellar vesicles following FTV cycles (15% vs. 24%). However the cryo-EM grid preparation appears to favour smaller vesicles being in the grid holes, while the majority of the larger vesicles prefers to sit on the carbon-coated support as there is a large difference in size between the DLS and cryo-EM size distributions. The DLS analysis in Fig. 6c reports z-average sizes of 108 nm (PDI 0.213) and 101 nm (PDI 0.191) before and after four FTV cycles, respectively.





**Figure 7.** Cryo-TEM of 100 nm 50 mol% PBd<sub>22</sub>-PEO<sub>14</sub> hybrid vesicles before and after four FTV cycles. (a) Histogram of initial vesicle sizes; (b) representation images of vesicles before FTV; (c) histogram of vesicle sizes after FTV; (d) representation images of vesicles after FTV. Scale bars represent 100 nm.

#### 4. Discussion

For vesicles composed of the pure lipid or block copolymer components, we find that sterilisation using an autoclave results in loss of colloidal stability and the release of the encapsulated CF. Autoclaving involves exposure to high temperature, which is thought to be detrimental to lipid vesicles by causing aggregation [34, 46]. The aggregation after heat sterilisation has been suggested to lead to instability in lipid vesicles by electrolytes causing dehydration of the hydrophilic moiety [46]. However, in a previous study, it was found that egg or saturated lipid vesicles without encapsulated agents could be sterilised by autoclaving. When calcein or doxorubicin was encapsulated however, the leakage was pronounced [34].

It was expected that the polymeric vesicles would be more resistant to heat exposure as polymer membranes are believed to be more robust than those formed by lipids alone. Polymersomes with a large membrane thickness (PEE<sub>37</sub>-PEO<sub>40</sub> and PBd<sub>46</sub>-PEO<sub>26</sub>) have previously been shown to have both encapsulation and colloidal stability to autoclave conditions, although there is slight shift to a smaller vesicle size distribution [28]. To enhance the stability of the vesicles during heat sterilisation, it has been suggested that sugars or polyols could be used to stabilise the vesicles [46] and the drug could be encapsulated after vesicles have been autoclaved [34].

Lyophilisation also caused complete contents release and loss of colloidal stability in both pure lipid and pure PBd-*b*-PEO polymer vesicles, indicating rupture and aggregation of the vesicles. The initial freezing step could cause damage to vesicles from piercing by the ice crystals that form and expansion of the encapsulated aqueous volume during freezing. However we later show that polymer-rich vesicle compositions in particular are comparatively stable under freeze-thaw action. Therefore damage caused by freezing is not solely responsible for the chronic impact of lyophilisation on these vesicles.

During the second step of lyophilisation, water is removed by sublimation. As water is fundamentally essential to the self-assembly of amphiphiles into vesicle polymorphs and degree of hydration is known to facilitate phase transitions in lyotropic assemblies, it is perhaps not surprising that this dehydration step can cause severe structural instabilities. Here we considered whether the enhanced stability of block copolymers alone might be enough to increase stability to lyophilisation,

however there is no evidence for this under the conditions currently tested. However the damaging effects of lyophilisation have been minimised for liposomes by addition of cryoprotectants to the continuous aqueous phase. Small molecule cryoprotectants such as glycerol or trehalose and other carbohydrates can significantly reduce aggregation, fusion and leakage. Cryoprotectant have been successfully used to enhance the stability of liposomes to lyophilisation and rehydration [39]. However this is notoriously challenging [40] and the potential for synergistic effects from cryoprotectants in the solution phase and block copolymers blended within hybrid vesicle membranes is a worthwhile avenue for future investigation.

While autoclaving and lyophilisation would need further investigation of added molecular protectants in the solvent environment to make them viable for hybrid vesicle processing, filtration and freeze-thaw processes appeared to be more immediately viable for sterilisation and preservation.

Vesicle filtration (200 nm pore size) resulted in relatively low contents release, particularly for vesicles formed by extrusion through a 100 nm membrane. These vesicles also showed good colloidal stability. However this is perhaps relatively unsurprising since the DLS size distribution suggests that only a small proportion of vesicles are larger than the filter pore size, although hydrodynamic sheer stresses passing through a filter pore might cause minimal destabilisation of the membrane and loss of contents.

A more stringent test of vesicle stability under filtration was undertaken with vesicles formed by extrusion through 400 nm membranes. Now, a large proportion of vesicles are larger than the 200 nm filter pore size. More significant contents release is now observed (up to 25%) and there is some loss of colloidal stability due to vesicle break-up and aggregation. Curiously, only 50 mol% PBd-*b*-PEO hybrid vesicles maintained good colloidal stability but this might be explained by the intrinsically smaller size distribution of these hybrid vesicles when initially formed.

When comparing between different vesicle compositions, it is interesting to note that the vesicle compositions with the highest filtration stability are perhaps initially non-intuitive. A reasonable initial hypothesis might be that vesicles with a high proportion of the larger PBd-*b*-PEO block copolymer would be more stable under filtration due to enhanced mechanical robustness from this polymer. However the converse is the case where the worst performing vesicle composition is 100% PBd<sub>22</sub>-PEO<sub>14</sub>. We interpret this to be due to the higher bending rigidity of the thicker membranes of these vesicles that offers higher resistance to deformations required to pass through the filter membrane. This is qualitatively experienced manifest in the higher pressures that are required to force these vesicle samples across the filter membrane. These higher pressures likely have a more severe impact on encapsulation stability. Conversely the smaller PBd<sub>12</sub>-PEO<sub>11</sub> polymer does not have a significant impact on encapsulation stability, likely due to a similarly low bending rigidity to pure liposomes. These hybrid vesicles formed using this smaller polymer may also have enhanced membrane elasticity, imparting improved toughness to these vesicles, but this is not a statistically significant observation, likely due to the inherently low contents release that is already seen for the POPC liposomes.

Polymer-rich vesicles can also withstand several FTV cycles, making this a more viable alternative to lyophilisation for sample preservation. Lipid-rich vesicles have poor encapsulation stability under freeze-thaw action, but high polymer content likely enhances stability due to the increased stretching elasticity and higher lysis strain of polymersome membranes that is critical to their enhanced material toughness and durability. Now membranes-rich in the larger PBd<sub>22</sub>-PEO<sub>14</sub> polymers present the best stability profile across several FTV cycles, having greater capacity to resist damage from solvent expansion stresses during freezing and the growth of ice crystals.

In summary, this initial investigation indicates that filtration and freeze-thaw are the most viable routes to sterilisation and preservation of hybrid vesicles while retaining good encapsulation and colloidal stability of these samples. A complex interplay between the bending rigidity, stretching elasticity and lysis strain of the membrane formulation determines which vesicles are most stable under each of these processes. While functional performance in the desired vesicle application will primarily dictate optimisation of the membrane composition of vesicles, enhancing essential processing stability is a secondary consideration that cannot be completely ignored. While filtration



is sufficient to sterilise small nano-vesicle samples, formulations that use larger vesicle sizes are less stable to this process and further efforts to develop autoclaving as a stable process for hybrid vesicles are worthwhile. Similarly, lyophilised vesicles would be favourable to frozen liquid samples for the preservation of vesicles for storage and transport to reduce economic costs and environmental impact. Therefore further efforts to enhance hybrid vesicle stability to these harsher processes is still of significant interest.

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