

Complete removal of arbitrarily strong and arbitrarily located auto correlation artifacts in spectral domain optical coherence tomography: Demonstration of an efficient and cost effective technique

Hari Nandakumar, Satya Prasanna Mallick and Shailesh Srivastava

Department of Physics, Sri Sathya Sai Institute of Higher Learning, Prasanthi Nilayam, AP, 515134 India

Abstract

The proof-of-principle demonstration of a simple, yet effective method of autocorrelation artifact removal for optical coherence tomography (OCT) is presented using a custom-designed parallel spectral-domain OCT (SD-OCT) instrument. Our real-time method is based on time-averaged sampling of a sinusoidal phase modulation in the reference arm. Unlike other existing methods, our technique can completely eliminate arbitrarily located, arbitrarily strong autocorrelation artifacts.

Keywords: Optical coherence tomography, Imaging systems, Tomographic imaging

1. Introduction

Optical Coherence Tomography (OCT) is a non-destructive tomographic imaging modality using non-ionizing photons. OCT can be regarded as an op-

Email address: hari@radiosai.org (Hari Nandakumar, Satya Prasanna Mallick and Shailesh Srivastava)

4 tical analog to Ultrasound scanning commonly used in medicine, but delivers
5 micron-level depth resolution compared to centimeter-scale resolutions with
6 Ultrasound [1]. OCT first became popular in ophthalmology in the 1990s [2, 3]
7 and subsequently became an established eye care tool [4]. Advances in OCT
8 technology have seen several generations of products with improved resolu-
9 tions and shorter acquisition times. Initial time-domain systems (TD-OCT)
10 were followed by Fourier-domain systems (FD-OCT) which could be imple-
11 mented without a moving reference arm. FD-OCT devices can be further
12 of two types, spectral-domain systems (SD-OCT) or swept-source devices
13 (SS-OCT). OCT now sees applications in cardiology, dentistry, pathology
14 and dermatology in addition to non-destructive materials testing, historical
15 artifact analysis and many other fields [5].

16 Recently, our group demonstrated a fresh approach to background sub-
17 traction in TD-OCT, which we termed the J_0 null technique [6], briefly men-
18 tioning that the technique should also work for autocorrelation removal in
19 FD-OCT. In this paper, we apply that technique to SD-OCT and convinc-
20 ingly demonstrate its utility in the removal of arbitrarily strong autocorre-
21 lation artifacts. Autocorrelation artifact removal is particularly important
22 for OCT studies on samples which have multiple layers with strong reflec-
23 tivities. The traditional method of ignoring autocorrelation by increasing
24 the reference arm reflectivity [7] would not suffice in such cases. A variety
25 of autocorrelation removal techniques have been suggested over the years,
26 like averaging spectra over multiple points [8], using resonant acquisition
27 [9], using an off-axis reference beam [10], dispersion encoding [11], various
28 phase shifting methods [12, 13, 14] and various balanced detection methods

[15, 16]. Additionally, several computational autocorrelation removal techniques [17, 18, 19] have also been proposed. Comparing these with our J_0 null method, we find that the most important advantages of our method are: its application to removal of arbitrarily strong and arbitrarily placed autocorrelation artifacts, ease of implementation, and suitability for use with low-cost parallel OCT devices.

2. Theoretical background

OCT theory tells us that in the frequency domain, the intensity at a particular point on the image plane is represented by the spectral interferogram [20]

$$\begin{aligned}
 I(x, y, k) = & S(k) \cdot r_R^2 \\
 & + 2S(k)r_R \int_{-\infty}^{\infty} r'_s(x, y, l_s) \cos(2k(n_s l_s - l_R)) dl_s \\
 & + S(k) \left| \int_{-\infty}^{\infty} r'_s(x, y, l_s) \exp[i2k(n_s l_s)] dl_s \right|^2
 \end{aligned} \tag{1}$$

where $S(k)$ is the source power spectral density, r_R is the reference arm amplitude reflectivity, $r'_s(x, y, l_s)$ is the sample arm amplitude reflectivity density located at a path length l_s inside the sample and n_s is the refractive index of the sample. The first term in the right-hand side of equation (1) is the DC or reference intensity term. The second term in equation (1) is the desirable one in FD-OCT, and is used to extract $r'_s(x, y, l_s)$ using the inverse Fourier transform. The third term is the self-interference or autocorrelation term, which is undesirable and causes artifacts in OCT reconstruction. As mentioned above, various methods have been used to minimize artifacts from

the autocorrelation term. We find that the J_0 null technique presents a simple and robust way of eliminating this term when phase noise due to vibration or sample motion causes difficulties in implementing phase shifting methods.

If the reference arm undergoes a sinusoidal phase modulation, the spectral interferogram in equation (1) becomes

$$I_{J_0}(x, y, k) = S(k) \cdot r_R^2 + 2S(k)r_R \int_{-\infty}^{\infty} r'_s(x, y, l_s) \cos[2k(n_s l_s - l_R) - M \sin(\omega t + \theta)] dl_s + S(k) \left| \int_{-\infty}^{\infty} r'_s(x, y, l_s) \exp[i2k(n_s l_s)] dl_s \right|^2 \quad (2)$$

Here, the Bessel function of the first kind J_0 makes its appearance by the use of the series

$$\cos[x \sin(\theta)] = J_0(x) + 2 \sum_{n=1}^{\infty} J_{2n}(x) \cos(2n\theta) \quad (3)$$

and

$$\sin[x \sin(\theta)] = 2 \sum_{n=1}^{\infty} J_{2n-1}(x) \sin[(2n-1)\theta] \quad (4)$$

The second term of equation (2) completely vanishes when the amplitude M equals the J_0 null amplitude, provided the acquisition time of the spectral interferogram is an integral multiple of the modulation time-period [21] or is long enough to average over several cycles of the phase modulation of the reference arm. Subtracting the spectral interferogram obtained with the J_0 null from the interferogram in Eq. 1, we obtain a spectral interferogram free

62 from autocorrelation artifacts. This forms the basis for our autocorrelation
 63 artifact removal scheme, which we refer to as the J_0 null technique.

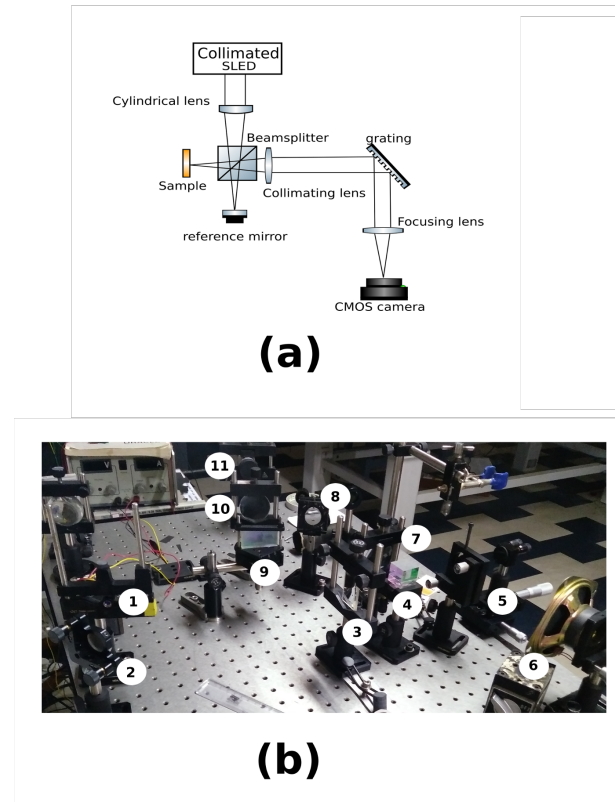


Figure 1: (a) Schematic and (b) photograph of the parallel FD-OCT instrument used in our study. Labelled components: 1, SLED source; 2, steering mirror; 3, cylindrical lens; 4, cube beamsplitter; 5, sample; 6, reference mirror; 7, collimating lens; 8, steering mirror; 9, grating; 10, imaging lens; 11, camera.

64 3. Experimental results and conclusions

65 Experimental validation of our technique was done using a lab-made par-
 66 allel SD-OCT [22] instrument, also known as line-field OCT [23, 24] as shown

in figure 1. A cylindrical lens with $f = 15\text{cm}$ focused the collimated beam from an SLED source (Exalos EXS210022-03) onto a $50\ \mu\text{m}$ vertical line on the sample. A reflection grating with 1200 lines/mm (Newport 33067FL01-360R) and a CMOS camera (QHY5L-II M) made up the spectrometer of our SD-OCT. Light from each point on the illuminated vertical line on the sample was dispersed horizontally into a spectrum, thus filling the 2D camera surface. Since the camera acquires the spectra of all the points on the illuminated vertical line on the sample in a single exposure, this parallel SD-OCT setup delivers single-shot B-scans. At low resolutions, 320x240 frame rate captures resulted in 240x80 B-scans at 148 frames per second (fps) with our system, which is 35,520 A-scans per second. At full 1280x960 resolution, 2x2 binning and FFT resampling to 2096 points resulted in 10 fps 480x320 B-scans, ie. 4,800 A-scans per second, limited by our real-time computational speed. Lateral resolution was limited by our optics, and was experimentally found to be $40\ \mu\text{m}$ by clearly resolving Group 3 Element 5 of a USAF target, using a translation stage for repeated B-scans across its surface. Axial

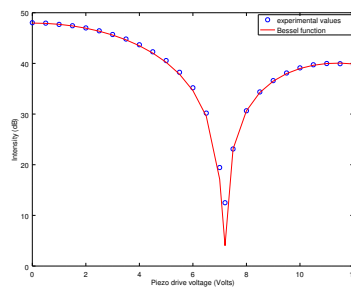


Figure 2: Calibration curve, showing intensity of OCT reflectance at a point as a function of piezo drive voltage. The J_0 function is traced out, with a null at 7.20 V for vibration at 2.5 kHz.

83 resolution was limited by our choice of spectrometer bandwidth. We chose
 84 to be able to image a larger depth, 6.4mm , at the cost of $20\mu\text{m}$ per pixel
 85 axial resolution. Data acquisition and real-time signal processing was done
 86 on a desktop computer (Intel i5, 8 GB RAM) running our open source soft-
 87 ware [25] which uses OpenCV[26]. The reference arm mirror modulation was
 88 done by a piezo actuator (Steminc SMPAK155510D10) driven by a function
 89 generator (Scientific SM5070). Representative calibration data relating the
 90 reference arm vibration and piezo drive voltage is presented figure 2, wherein
 91 the null of the J_0 curve is clearly defined.

92 Our OCT system had a sub-50 dB dynamic range due to the $23ke^-$ equiv-
 93 alent full-well-capacity of our camera [27]. The ease in which the J_0 null
 94 subtraction can be implemented helps us to use it for repeated subtraction,
 95 which yields higher Signal to Noise Ratio (SNR) than a single subtraction,
 96 due to the effect of averaging. Figure 3 shows a stack of glass cover-slips
 97 imaged with our OCT instrument. Since the cover-slips have reflectivities
 98 similar to our reference arm, strong autocorrelation artifacts are seen in fig-
 99 ure 3 (a). Figure 3 (b) shows autocorrelation removal by a single J_0 null
 100 subtraction. Figure 3 (c) and (d) show around 40 dB of autocorrelation re-
 101 moval by repeated J_0 null subtraction. The process we followed for repeated
 102 null subtraction is explained below.

103 In order to bring out signal buried in our noisy acquired data, we re-
 104 peated adding B-scans and subtracting J_0 null frames 10 times for 10 av-
 105 eraged frames. This is similar to the standard lock-in detection techniques
 106 commonly used with optical choppers, wherein the signal gets sequentially
 107 added while the noise gets cancelled due to being alternately added (+1)

108 and subtracted (-1) on account of the square wave reference. For enhanced
 109 autocorrelation removal efficiency, since the autocorrelation signal may be
 110 riding on top of noise and hence may be higher in some B-scan frames than

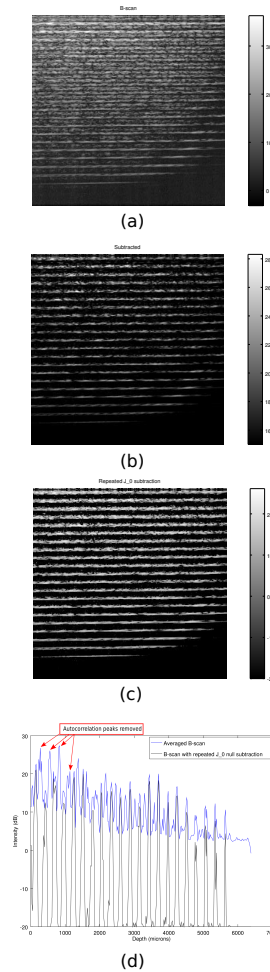


Figure 3: (a) 10x10 averaged B-scan of a stack of coverslips with strong autocorrelation artifacts. Lateral extent (x axis) is 6.29 mm and axial extent (y axis) is 6.6 mm. (b) Autocorrelation artifacts removed by single J_0 null subtraction. (c) Autocorrelation artifacts removed more efficiently and dynamic range improved by repeated J_0 null subtraction. (d) A representative A-scan, with some autocorrelation artifacts labelled by arrows.

111 in the J_0 null frames, we multiplied the B-scan frames by a fudge-factor of 0.8
112 before the subtraction. After each subtraction, any negative numbers were
113 thresholded to zero before repeating the process for the next set of frames.
114 This thresholding process allows even weak signals which are just able to
115 raise above the noise floor in any one signal frame to be added to the final
116 averaged result. The fudge factor is finally divided out.

117 We note that the J_0 null technique is insensitive to phase noise due to
118 vibration, due to the fact that no particular phase relationship needs to be
119 maintained between the two spectral interferogram acquisitions. This is the
120 advantage of our technique over multi-shot phase shifting [13] techniques.
121 Single-shot phase shifting techniques [14] would also have vibration insen-
122 sitive behaviour similar to our technique, but when used with 2-D sensors,
123 single-shot phase shifting is generally cumbersome, either having to use mul-
124 tiple cameras [28] or results in lowering of available pixels in the sensor [29].
125 Our technique results in a subtraction similar to using an optical switch in
126 the reference arm [30], but with the advantage of low-cost implementation for
127 single-shot B-scan imaging. Other advantages of our J_0 null technique over
128 the use of an optical switch are, enhanced DC removal along with subtraction
129 of reference mirror blemishes. Computational autocorrelation removal comes
130 with caveats on the location and strength of the autocorrelation artifact,
131 while the J_0 null technique has no such limitations. Dispersion encoding and
132 subsequent reconstruction of a full-range signal is an attractive technique,
133 but requires more than double the computational effort [11] needed in our
134 method. The efficiency of autocorrelation removal with the J_0 null technique
135 does depend on the accuracy with which the null point was determined by

the initial calibration, but is thereafter only limited by the SNR of the measurements. In conclusion, we have demonstrated a new technique for removal of autocorrelation which can work with arbitrarily strong and arbitrarily located autocorrelation artifacts. Our technique is specially suited for parallel or line-field FD-OCT devices [22, 6, 23, 24] using spectrometers with 2-D sensors (cameras) which result in single-shot B-scans.

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References

- [1] C. A. Puliafito, J. S. Schuman, M. R. Hee, J. G. Fujimoto, Optical coherence tomography of ocular diseases, SLACK Inc., 1996.
- [2] A. F. Fercher, K. Mengedocht, W. Werner, Eye-length measurement by interferometry with partially coherent light, Optics Letters 13 (1988) 186–188.

- 158 [3] C. K. Hitzenberger, W. Drexler, A. F. Fercher, Measurement of corneal
159 thickness by laser Doppler interferometry, *Investigative ophthalmology*
160 & visual science 33 (1992) 98–103.
- 161 [4] J. Fujimoto, E. Swanson, The development, commercialization, and
162 impact of optical coherence tomography, *Investigative ophthalmology*
163 & visual science 57 (2016) OCT1–OCT13.
- 164 [5] W. Drexler, J. G. Fujimoto, *Optical Coherence Tomography: Technol-*
165 *ogy and Applications*, Second Edition, Springer International Publishing
166 Switzerland, 2015.
- 167 [6] H. Nandakumar, S. Parameshwaran, R. Gamini, S. Srivastava, Artifact-
168 free robust single-shot background subtraction for optical coherence to-
169 mography, *OSA Continuum* 2 (2019) 1556–1564.
- 170 [7] A. F. Fercher, C. K. Hitzenberger, G. Kamp, S. Y. El-Zaiat, Measure-
171 ment of intraocular distances by backscattering spectral interferometry,
172 *Optics communications* 117 (1995) 43–48.
- 173 [8] R. K. Wang, Z. Ma, A practical approach to eliminate autocorrelation
174 artefacts for volume-rate spectral domain optical coherence tomography,
175 *Physics in Medicine & Biology* 51 (2006) 3231.
- 176 [9] M. Shalaby, S. S. Al-Sowayan, Autocorrelation noise free optical coher-
177 ence tomography using the novel concept of resonant oct (roct), *Journal*
178 *of the European Optical Society-Rapid Publications* 12 (2016) 10.
- 179 [10] D. Hillmann, H. Spahr, H. Sudkamp, C. Hain, L. Hinkel, G. Franke,

- 180 G. Hüttmann, Off-axis reference beam for full-field swept-source oct
181 and holoscopy, *Optics Express* 25 (2017) 27770–27784.
- 182 [11] F. Köttig, P. Cimalla, M. Gärtner, E. Koch, An advanced algorithm
183 for dispersion encoded full range frequency domain optical coherence
184 tomography, *Opt. Express* 20 (2012) 24925–24948.
- 185 [12] M. V. Sarunic, M. A. Choma, C. Yang, J. A. Izatt, Instantaneous
186 complex conjugate resolved spectral domain and swept-source oct using
187 3x3 fiber couplers, *Opt. Express* 13 (2005) 957–967.
- 188 [13] M. Wojtkowski, A. Kowalczyk, R. Leitgeb, A. F. Fercher, Full range
189 complex spectral optical coherence tomography technique in eye imag-
190 ing, *Opt. Lett.* 27 (2002) 1415–1417.
- 191 [14] E. Bo, S. Chen, D. Cui, S. Chen, X. Yu, Y. Luo, L. Liu, Single-camera
192 full-range high-resolution spectral domain optical coherence tomogra-
193 phy, *Appl. Opt.* 56 (2017) 470–475.
- 194 [15] W.-C. Kuo, C.-M. Lai, Y.-S. Huang, C.-Y. Chang, Y.-M. Kuo, Balanced
195 detection for spectral domain optical coherence tomography, *Optics*
196 *Express* 21 (2013) 19280–19291.
- 197 [16] E. Bo, X. Liu, S. Chen, X. Yu, X. Wang, L. Liu, Spectral-domain optical
198 coherence tomography with dual-balanced detection for auto-correlation
199 artifacts reduction, *Optics Express* 23 (2015) 28050–28058.
- 200 [17] A. Ozcan, M. J. F. Digonnet, G. S. Kino, Minimum-phase-function-
201 based processing in frequency-domain optical coherence tomography sys-
202 tems, *J. Opt. Soc. Am. A* 23 (2006) 1669–1677.

- [18] B. J. Davis, T. S. Ralston, D. L. Marks, S. A. Boppart, P. S. Carney, Autocorrelation artifacts in optical coherence tomography and interferometric synthetic aperture microscopy, *Opt. Lett.* 32 (2007) 1441–1443.
- [19] Y. C. S. Hon Luen Seck, Ying Zhang, Autocorrelation noise removal for optical coherence tomography by sparse filter design, *Journal of Biomedical Optics* 17 (2012) 1 – 7 – 7.
- [20] L. V. Wang, H.-i. Wu, *Biomedical optics: principles and imaging*, John Wiley & Sons, 2012.
- [21] V. Sudarshanam, K. Srinivasan, Universal dynamic phase-calibration technique for fiber-optic interferometric sensors and phase modulators, *Optics Letters* 14 (1989) 1287–1289.
- [22] B. Grajciar, M. Pircher, A. F. Fercher, R. A. Leitgeb, Parallel fourier domain optical coherence tomography for in vivo measurement of the human eye, *Optics Express* 13 (2005) 1131–1137.
- [23] S. Lawman, Y. Dong, B. M. Williams, V. Romano, S. Kaye, S. P. Harding, C. Willoughby, Y.-C. Shen, Y. Zheng, High resolution corneal and single pulse imaging with line field spectral domain optical coherence tomography, *Opt. Express* 24 (2016) 12395–12405.
- [24] A. Kazaili, S. Lawman, B. Geraghty, A. Eliasy, Y. Zheng, Y. Shen, R. Akhtar, Line-field optical coherence tomography as a tool for in vitro characterization of corneal biomechanics under physiological pressures, *Scientific reports* 9 (2019) 6321.

- 225 [25] H. Nandakumar, FDOCT, <https://github.com/hn-88/FDOCT>, 2019.
- 226 [26] G. Bradski, A. Kaehler, Opencv, Dr. Dobbs journal of software tools
227 (2000).
- 228 [27] H. Nandakumar, S. Srivastava, Data and code for analyzing performance
229 of qhy cmos cameras, Preprints 2018 (2018) 2018100179.
- 230 [28] Y. Zhu, W. Gao, Single-shot wavelength-independent phase-shifting
231 method for full-field optical coherence tomography, Appl. Opt. 58 (2019)
232 806–813.
- 233 [29] H. M. Subhash, Full-field and single-shot full-field optical coherence
234 tomography: A novel technique for biomedical imaging applications,
235 Advances in Optical Technologies vol. 2012 (2012) Article ID 435408.
- 236 [30] J. Ai, L. V. Wang, Spectral-domain optical coherence tomography:
237 Removal of autocorrelation using an optical switch, Applied Physics
238 Letters 88 (2006) 111115.