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## 2 **Investigation of ISFETs' polyurethane matrix** 3 **membrane to suppress drift in saliva**

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15 **Abstract:** We have studied on the stress measurement by making use of salivary nitrate, which can  
16 be a candidate of stress markers, with ion-selective field-effect transistors (ISFETs). ISFETs are  
17 suitable for on-site single-drop analysis of salivary nitrate within 10 seconds. However, when  
18 ISFETs are used for salivary nitrate, ISFETs have a problem which is called the initial drift. The  
19 initial drift makes it difficult for determination of an accurate nitrate monitoring. Thus, the purpose  
20 of this study is to suppress an initial drift and to search for new easy polymer to possess more  
21 performance of sensor responses than conventional matrix membrane such as PVC. In this  
22 research, we investigated ISFETs using specific matrix membrane for example, KP-13, Pellethane®  
23 and P7281-PU. The initial drift was evaluated from the fluctuation of the response values generated  
24 by ISFETs which are immersed in saliva or aqueous solution. As a result, P7281-PU showed its  
25 suppression effect for the initial drift in the whole saliva and various solutions. Furthermore, the  
26 cause of drift may be H<sup>+</sup> diffusion, and drift suppression effect of P7281-PU may be affected by  
27 urethane bond capturing H<sup>+</sup> in ion-selective membrane. This result suggests a continuous nitrate  
28 monitoring and development of wearable sensors.

29 **Keywords:** ISFETs; ISE; polyurethane; salivary nitrate; stress; drift; ion-selective membrane

### 30 **1. Introduction**

31 The cause of depression is stress and genetic vulnerability [1-3]. In addition, there are various  
32 diseases and physical disorders associated with stress. Therefore, stress measurement is an  
33 important issue and it contributes to the prevention of diseases such as depression. In this study,  
34 we are focusing on the biochemical method to evaluate stress from the stress-marker in body fluid.  
35 One of the body fluids, blood which contains typical stress-markers (adrenaline and noradrenaline  
36 [4,5]) is collected invasively accompanied by stress. In contrast, saliva which is derived from blood  
37 is collected non-invasively. Hence saliva is suitable for stress-measurement. Salivary nitrate is  
38 secreted by blood nitrate which is a NO metabolite through salivary gland [6]. NO is an  
39 endothelium-derived relaxing factor (EDRF) [7] which is produced in response to vascular tone  
40 associated with the effect of the autonomic nervous system. Therefore, salivary nitrate is expected  
41 to be used as a stress-marker of the autonomic nervous system. The candidates of salivary  
42 stress-marker are cortisol, chromogranin A [8],  $\alpha$ -amylase [9]. However these candidates are not  
43 suitable for the on-site stress measurement, because they are determined with ELISA, it takes time  
44 to measure stress hormone. As a measurement device, Ion-Selective Field Effect Transistors  
45 (ISFETs) are the most suitable for on-site single-drop analysis of salivary nitrate within 10 seconds.  
46 Hence, the ISFETs are adapted as the stress measurement making use of saliva. On the other hand,

47 current salivary NO<sub>3</sub>-ISFETs have the problem that drift occurs during measurement. Drift is the  
48 phenomenon in which the response value of the sensor changes gradually, making difficult to  
49 determinate salivary nitrate accurately. The ISFETs' gate part consists of H<sup>+</sup> sensitive metal oxide,  
50 for example, SiO<sub>2</sub>, S<sub>3</sub>N<sub>4</sub> and Ta<sub>2</sub>O<sub>5</sub>. Fogt, et al. considered that the cause of drift is the pH change at  
51 the ISM/Gate interface's aqueous layer. It's concerned with CO<sub>2</sub>-gas diffusion which approaches the  
52 ISM/Gate interface's aqueous layer through the ion-selective membrane [10]. The gate part which  
53 we use in this paper is Ta<sub>2</sub>O<sub>5</sub>, hereinafter pH sensitive ISFETs called pH-ISFETs. Other previous  
54 researches attempted to insert the inner layer in the ISM/Gate interface. For example, pHEMA-gel  
55 saturated buffer [11], Ag/AgCl [12] and H<sup>+</sup> selective membrane [13]. On the other hand, Abramova,  
56 et al. considered that the cause of drift is protein adsorption to the ISM surface. Photocurable  
57 polyurethane as a matrix membrane is effective in the measurement of blood plasma [14]. However,  
58 there is no report that aims to suppress drift in saliva. Therefore, we report that polyurethane is  
59 used as the matrix membrane to suppress drift for salivary nitrate. The actual used polyurethanes  
60 are Pellethane<sup>®</sup>, KP-13, and P7281-PU. Pellethane<sup>®</sup> is widely used in the medical field such as a  
61 catheter. Hence, Pellethane<sup>®</sup> is expected to suppress the adsorption of glycoproteins in saliva.  
62 Espadastorre and Meyerhoff reported Pellethane<sup>®</sup> based ISM showed somewhat less platelet  
63 adhesion [15]. KP-13 is the polyurethane urea containing 13 wt% of dimethylsiloxane. Wakida  
64 reported KP-13 is the effective matrix membrane to measure blood electrolyte [16] and salivary  
65 nitrate [17]. Although P7281-PU has not been used as a matrix membrane, P7281-PU used ISM has  
66 adhesiveness and can be closely adhered to the gate to restrict appearance of the water layer.

## 67 2. Materials and Methods

### 68 2.1. Materials

69 Original ISFETs for pH measurement (pH-ISFETs) were purchased from ISFETCOM (Saitama,  
70 Japan). The pH-ISFETs are integrated a reference electrode. As a nitrate ionophore,  
71 Bis(dimethyl-phenanthroline) Copper(I) nitrate ([Cu(bcp)<sub>2</sub>]NO<sub>3</sub>) was synthesized with reference  
72 [18]. As a plasticizer, 2-Nitrophenyl dodecyl ether (NPDDE) was purchased from Wako Pure  
73 Chemical Industries (Osaka Japan). NPDDE was used for stable ISFET to improve the adhesion to  
74 gate material of ISFETs [19]. Polyvinyl chloride (PVC, n=1000) used as a matrix membrane was  
75 purchased from Kishida Chemical (Osaka, Japan). KP-13 was received from Kaneka Chemistry  
76 (Osaka, Japan). Pellethane<sup>®</sup> was received from Lubrizol (Ohio, USA). P7281-PU was purchased from  
77 Polymer source (Dorval, Quebec, Canada).

78 NaCl, KCl, KH<sub>2</sub>PO<sub>4</sub>, Urea, Na<sub>2</sub>SO<sub>4</sub>, NH<sub>4</sub>Cl, CaCl<sub>2</sub> · 2H<sub>2</sub>O, NaHCO<sub>3</sub>, KNO<sub>3</sub> were used reagent  
79 grade as much as possible. Tetrahydrofuran (THF) which was purchased from Wako. THF was used  
80 as a volatile solvent to dissolve the nitrate ionophore, plasticizer, and polymer. Mucin from bovine  
81 submaxillary glands was purchased from MP Biomedicals, LLC (California, USA). Real saliva was  
82 collected by *salivette* purchased from Sarstedt (North Rhine-Westphalia, Nümbrecht, Germany) and  
83 a metal spoon.

84 All chemicals were used without purification. All standard solutions and artificial saliva were  
85 prepared with Milli-Q water (18.2MΩ cm).

### 86 2.2. Preparation of NO<sub>3</sub>-ISFETs

87 Nitrate selective ISFETs (NO<sub>3</sub>-ISFETs) used to evaluate the sensor response and initial drift  
88 were prepared by the following procedure. After forming a THF solution of the nitrate selective  
89 membrane containing 5 wt% of nitrate ionophore ([Cu(bcp)<sub>2</sub>]NO<sub>3</sub>), 65 wt % of a plasticizer (NPDDE)  
90 and 30 wt% of the matrix membrane polymer, which was completely dissolved in the solution at  
91 room temperature. NO<sub>3</sub>-ISFETs were prepared by casting THF solution onto the gate part in the  
92 pH-ISFETs. After the casting, THF solution onto the gate was completely evaporated in a clean space  
93 (Pure Space 01; AS ONE, Osaka, Japan) and the same manner repeated several times. The resulting  
94 sensing membrane was allowed to dry overnight. The thickness of the nitrate selective membrane  
95 was ca. 0.2 mm.

### 96 2.3. Determination of calibration curves and selectivity coefficients in NO<sub>3</sub>-ISFETs

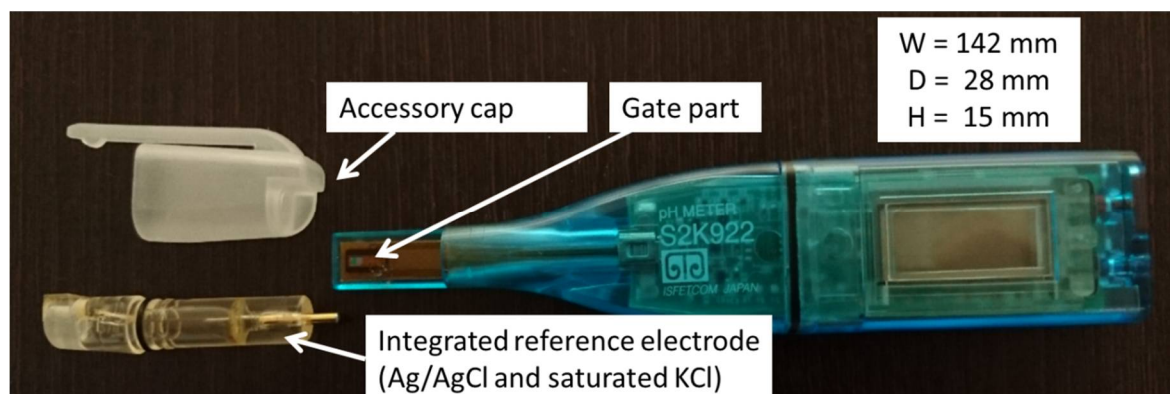
97 After the prepared ISFETs were conditioned in 1 mM (mol/L) KNO<sub>3</sub> solution (standard  
98 solution) for 3 hours. Its calibration curves and selectivity coefficients were determined using the  
99 Nicolsky-Eisenman's equation (1) as follows where E is the potential of the NO<sub>3</sub>-ISFETs, E<sub>0</sub> is the  
100 standard potential of NO<sub>3</sub>-ISFETs, Z<sub>i</sub> and Z<sub>j</sub> are the charges of the primary ion i (NO<sub>3</sub>) and  
101 interfering ions j, and a<sub>i</sub> and a<sub>j</sub> are the activities of ions i and j, respectively. R, T, and F have the  
102 usual meanings.

$$E = E_0 + 2.303 \cdot RT / (Z_i F) \cdot \ln ( a_i + K_{ij}^{pot} a_j^{z_i/z_j} ) \quad (1)$$

103 According to the theoretical response at 25 Celsius, the slope sensitivity of the NO<sub>3</sub>-ISFETs is  
104 -59.16 mV per decade change of the activity a<sub>i</sub>. a<sub>i</sub> was calculated from the Debye-Huckel's equation  
105 based on the simple ionic-strength theory.  $K_{ij}^{pot}$  is the selectivity coefficient of the NO<sub>3</sub>-ISFETs in  
106 the presence of interfering ion, j.  $K_{ij}^{pot}$  was evaluated by the mixed-solution method, and can be  
107 considered to be a reliable selectivity parameter. The potential responses were measured in the NO<sub>3</sub>  
108 standard solutions in the presence of each interfering ion using 5.0 × 10<sup>-1</sup> M NaCl, 5.0 × 10<sup>-1</sup> M  
109 Na<sub>2</sub>SO<sub>4</sub>, 5.0 × 10<sup>-2</sup> M NaNO<sub>2</sub>, 5.0 × 10<sup>-5</sup> M KI and 5.0 × 10<sup>-5</sup> M KSCN. Furthermore the calibration curve in  
110 artificial saliva is also determined. Artificial saliva is an aqueous solution reproducing human's  
111 salivary electrolytes. Reagents used for artificial saliva and their concentrations are as follows: 2.15  
112 mM NaCl, 12.9 mM KCl, 4.81 mM KH<sub>2</sub>PO<sub>4</sub>, 0.33 mM Urea, 2.37 mM Na<sub>2</sub>SO<sub>4</sub>, 3.33 mM NH<sub>4</sub>Cl, 1.55  
113 mM CaCl<sub>2</sub> · 2H<sub>2</sub>O, 7.51 mM NaHCO<sub>3</sub>.

### 114 2.4. Evaluation of initial drift in NO<sub>3</sub>-ISFETs

115 Evaluation of initial drift is performed by looking at the output value of ISFETs immersed in  
116 solution about 8 hours. Main measurement target is human saliva. Two types of human saliva are  
117 prepared according to the sampling method. The one is obtained from the saliva collection kit:  
118 salivette and another one is obtained from a metal spoon. Four kinds of solutions 10<sup>-3</sup> M potassium  
119 nitrate (standard solution), artificial saliva, the standard solution with 0.5 wt% Mucin (mucin  
120 solution), and standard solution with CO<sub>2</sub> bubbling (CO<sub>2</sub> solution), are used for comparison. Artificial  
121 saliva used for this section is added 1 mM KNO<sub>3</sub>. In experiments, evaluation of initial drift was  
122 conducted in a closed system using a cap attached to the ISFETs in order to prevent volatilization of  
123 the aqueous solution and contact with air (shown in Fig.1). All subjects gave their informed consent  
124 for inclusion before they participated in the study. The study was conducted in accordance with the  
125 Declaration of Helsinki, and the saliva sample experiments were approved by the Ethics Committee  
126 of National Institute of Advanced Industrial Science and Technology (AIST) (Project identification  
127 code is human 2015-195) in January 29th 2016.  
128



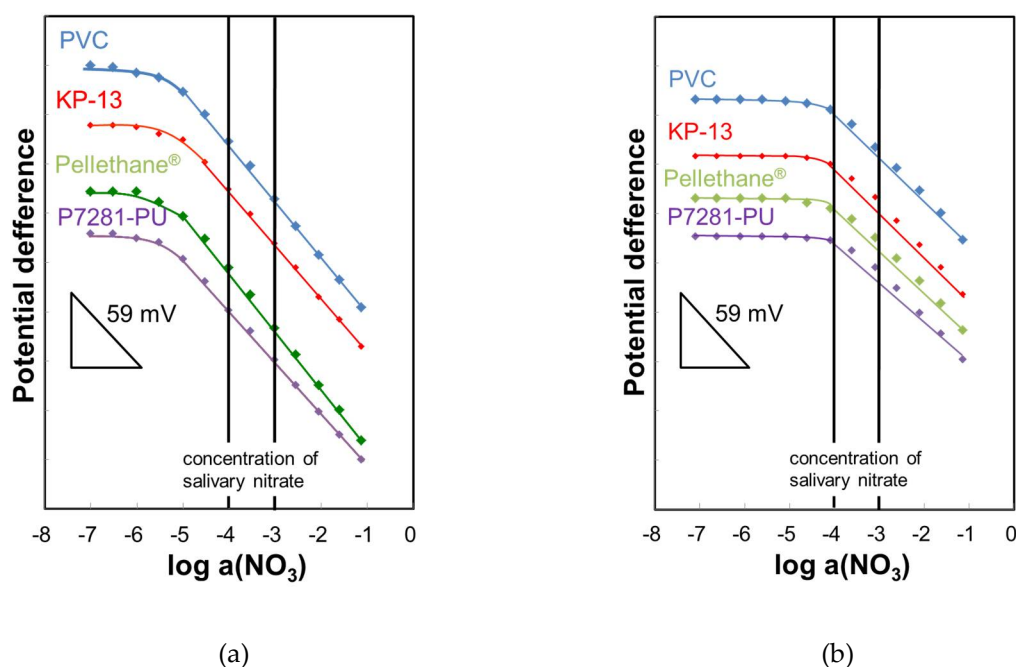
129 **Figure 1.** pH-ISFETs and accessory cap

130

### 131 3. Results and Discussion

#### 132 3.1. Calibration curves and Selectivity coefficients

133 The calibration curves of NO<sub>3</sub>-ISFETs are showed in Figure 2(a). The vertical line shows the  
 134 potential difference and the horizontal one shows logarithm of nitrate activity. All NO<sub>3</sub>-ISFETs  
 135 show a linear response to nitrate activity in the range 10<sup>-5</sup> M to 10<sup>-1</sup> M. The selectivity of ISFETs is  
 136 represented by the selectivity coefficients  $K_{NO_3}^{pot}$  defined with Nicolsky-Eisenman's equation.  
 137 Selectivity coefficients for typical anions were measured by the mixed solution method and are  
 138 summarized in Table 1. The linear response range and the selectivity coefficients of the  
 139 polyurethane-based ISFETs are coincident those of the PVC based ISFETs. Therefore potential  
 140 determinants are ionophore and plasticizer but matrix membrane. The calibration curves in  
 141 artificial saliva are showed in Figure 2(b). All ISFETs show a linear response to nitrate activity in the  
 142 range of 10<sup>-4</sup> M to 10<sup>-1</sup> M. Concentration of nitrate in saliva is approximately 10<sup>-4</sup> M to 10<sup>-3</sup> M [19].  
 143 Therefore, NO<sub>3</sub>-ISFETs are adapted to nitrate measurement in saliva.  
 144



145 **Figure 2.** Calibration curves of NO<sub>3</sub>-ISFETs. (a) only KNO<sub>3</sub> solution. (b) in artificial saliva

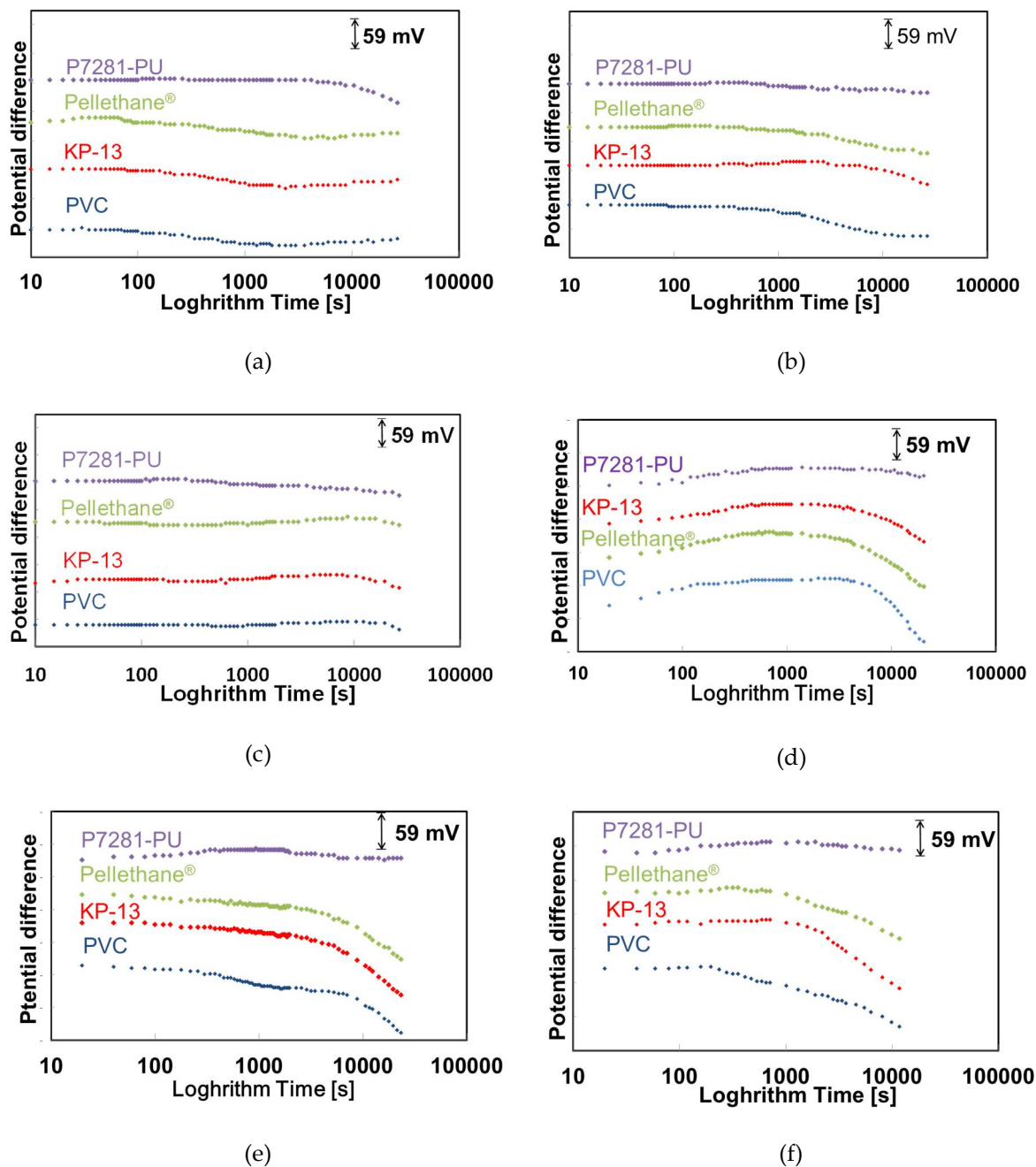
146 **Table 1.** Selectivity coefficients

Polymer matrix	Selectivity coefficients, $K_{NO_3,j}^{pot}$				
	I	SCN	NO <sub>2</sub>	Cl	SO <sub>4</sub>
PVC	0.82	0.95	-1.53	-2.55	-4.10
KP-13	0.56	0.95	-1.53	-2.59	-4.03
Pellethane®	0.78	1.09	-1.50	-2.71	-4.11
P7281-PU	0.69	1.07	-1.40	-2.30	-4.13

#### 147 3.2. Evaluation of initial drift in saliva and various solutions

148 The drift characteristics in saliva and various solutions are showed in Figure 3. The vertical  
 149 line shows the potential difference and the horizontal one shows logarithm of time. In standard  
 150 solution and CO<sub>2</sub> solution, all NO<sub>3</sub>-ISFETs show a comparatively stable response. In mucin solution,

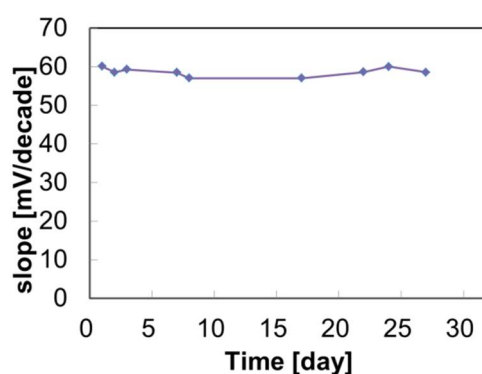
151 PVC based ISFETs show a slightly drift but in other polyurethane-based ISFETs show a stable  
 152 response. It is suggested that CO<sub>2</sub> is not the cause of drift. Furthermore, mucin is the cause of drift  
 153 for PVC based ISFETs not in other polyurethane-based ISFETs. PVC, KP-13, and Pellethane® based  
 154 ISFETs show drift in salivary samples (Fig. 3(d), (e) and (f)). However, P7281-PU based ISFETs  
 155 show a comparatively stable response in salivary samples. Figure 4 shows long-term stability of  
 156 P7281-PU based ISFETs. The vertical line shows the slope sensitivity and the horizontal one shows  
 157 the time. P7281-PU based ISFETs maintain the same slope sensitivity for within 27days. It is  
 158 considered that the stable response of the P7281-PU based ISFETs is due to the strong adhesion of  
 159 the ion-selective membrane to the Ta<sub>2</sub>O<sub>5</sub> gate and the formation of water layer at the gate/ISM  
 160 interface is suppressed.  
 161



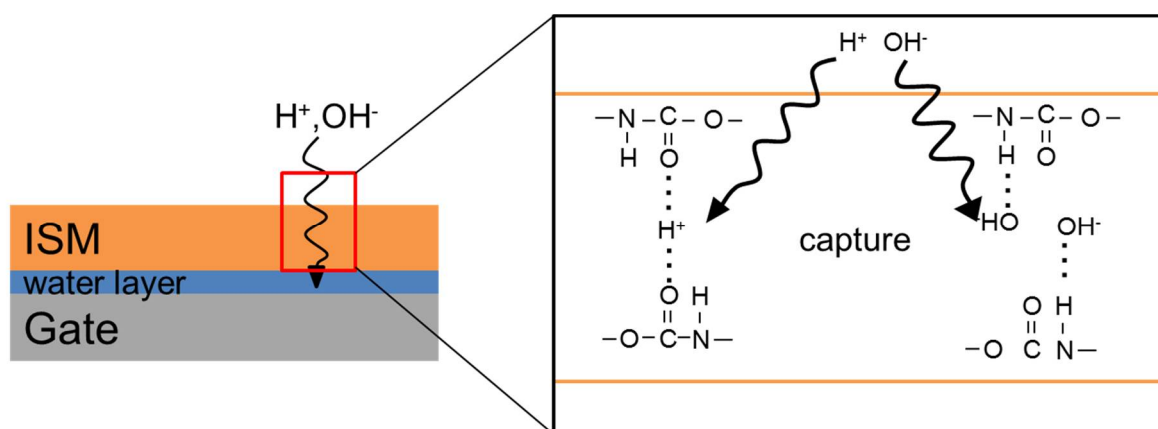
162 **Figure 3.** Initial drift of NO<sub>3</sub>-ISFETs (a) in standard solution; (b); in standard solution with 0.5  
 163 wt% mucin; (c) in standard solution with CO<sub>2</sub> bubbling;(d) in artificial saliva; (e) in saliva via  
 164 *salivette*; (f) in whole saliva (non-pretreatment)

165 Note that the drift characteristic of P7281-PU based ISFETs is superior stable in whole saliva. It  
 166 is considered that urethane bond in P7281-PU capture  $H^+$ ,  $OH^-$  in the aqueous layer. This hypothesis  
 167 suggests in Figure 5.

168 However the cause of drift is not clear, it is currently being investigated using matrix  
 169 membranes that have the same molecular structure as P7281-PU but only differ in molecular weight.  
 170 Anyway, P7281-PU is effective matrix membrane for  $NO_3^-$ -ISFETs for measurement of saliva. In the  
 171 future, it can be expected to achieve continuous nitrate monitoring and deployment to wearable  
 172 sensors.  
 173



174 **Figure 4.** Long-term stability of P7281-PU based ISFETs



175 **Figure 5.** The hypothesis of urethane bond capture  $H^+$  and  $OH^-$  by hydrogen bond

176 **Author Contributions:** conceptualization, S.W.; methodology, S.O. and S.W.; validation, T.K. and K.K.; formal  
 177 analysis, S.O. and T.K.; investigation, S.O.; resources, S.O. and S.W.; data curation, S.O., T.K. and S.W.;  
 178 writing—original draft preparation, S.O.; writing—review and editing, K.K. and S.W.; visualization, S.O.;  
 179 supervision, T.M. and S.W.; project administration, S.W.; funding acquisition, S.W.

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