

1 Article

2 Optical micro-angiography (OMAG) based range 3 optimization method for liquid flow rate

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14

15 **Abstract:** Optical micro-angiography (OMAG) is a new method of detecting flow rate and widely
16 used for in vivo imaging. Although OMAG can distinguish between flowing and stationary parts,
17 it cannot obtain accurate flow rate information. This study proposed a range formula for OMAG
18 and the ultrahigh-sensitivity OMAG (UHS-OMAG) method to quantify the measurement range of
19 an entire system. The parameters of the angle between beam scanning and flow directions, the
20 angular velocity of the galvanometer, and the offset of incident light were introduced, and a formula
21 for calculating the range was derived. Experiments were conducted to measure fine and ultra-fine
22 flow rates by using OMAG and UHS-OMAG methods. The minimum measured flow rate was
23 approximately 30 $\mu\text{m/s}$, and the maximum measured flow rate was approximately 8 mm/s .
24 Experimental results are in good agreement with the preset results.

25 **Keywords:** OMAG method; flow rate measurement; micro flow rate

26

27 1. Introduction

28 Optical coherence tomography (OCT) is a rapidly emerging optical imaging technology and a
29 non-invasive imaging method [1,2] that is widely used in biology [3], medicine [4–6], and material
30 research [7,8]. Doppler OCT (DOCT) was developed by combining the Doppler principle with OCT.
31 Leigteb et al. implemented the first Fourier-domain OCT flow velocity detection experiment [9].
32 DOCT can determine the position and velocity of moving particles in high scattering media [10–12].
33 It can also be applied to microvascular in vivo imaging in medical diagnostics [13] and flow
34 characteristic measurement in microfluidic monitoring [14], which has a good application prospect.
35 However, DOCT can only measure velocity components parallel to the incident beam [15]. Therefore,
36 the incident beam angle and the flow velocity direction (Doppler angle) must be accurately
37 determined when calculating fluid velocity. However, the Doppler angle is difficult to measure in
38 many practical applications. Consequently, DOCT cannot be used successfully in practical
39 applications, especially those that involve living biological tissues.

40 To overcome these limitations, Wang et al. proposed optical micro-angiography (OMAG)
41 technology in 2007 [16] and made several improvements [17,18]. OMAG is OCT micro-angiography
42 based on complex signals. It utilizes the mathematical properties of Hilbert transform and constructs
43 complex analytical signals using the Hilbert transform of real-interference signals. The structure and
44 flow velocity information of a sample are obtained by Fourier transform. OMAG does not rely on the
45 phase information of OCT, is not sensitive to environmental noise and other factors, and has made

46 great progress in terms of the sensitivity and image quality of flow rate detection [19]. In addition to
47 its capability to achieve micro-structural imaging, OMAG provides volumetric vasculature images of
48 the scanned tissue bed down to the capillary-level imaging resolution [20]. OMAG has a high
49 application value in living microvascular imaging and has been successfully applied in human skin
50 [21], cochlea [22,23], and human retina [24,25]. The ultrahigh-sensitivity OMAG (UHS-OMAG)
51 method [26] was proposed to measure low flow velocities. This method remarkably improves
52 imaging sensitivity.

53 Although changes in sensitivity in actual flow detection can be determined using the OMAG
54 method, the method cannot effectively obtain the exact range of the system. Accurate flow rate
55 information can be obtained when small flow rates, such as capillary flow rates, are detected. This
56 information is limited in practical applications, such as medicine. For example, when measuring
57 capillary information in the human body, the flowing particles in the capillaries can be separated
58 from stationary particles, but the flow velocity information in the blood vessels cannot be accurately
59 determined.

60 In this study, we derived a range calculation formula of OMAG and UHS-OMAG for the first
61 time to quantify the system measurement range. We introduced the angle between beam scanning
62 and flow directions, the angular velocity of the galvanometer, and the offset of incident light and
63 derived a formula for calculating the range. Moreover, the images obtained within the measurement
64 range were analyzed to explore the imaging patterns within this range. Our work provides the
65 following contributions.

66 (1) After obtaining a rough estimate of the flow rate to be measured, the system's parameter
67 values can be set according to the formula so that the measured image is displayed in the best imaging
68 area.

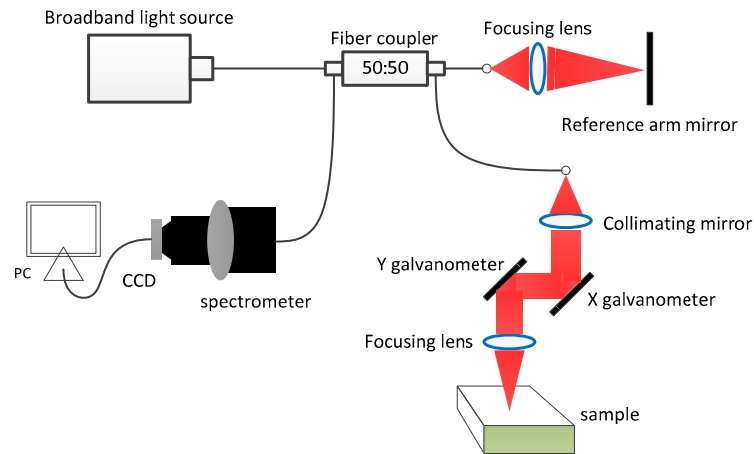
69 (2) When the flow rate to be measured is unknown, the approximate range of unknown flow
70 velocity can be calculated based on the measured image and parameter values of the system.

71 In our experiments, we estimated the flow rate by using our derived range formula, and the
72 experimental results were consistent with the predicted results. We also analyzed the relationship
73 between the intensity value of the obtained experimental result image and flow rate. A linear
74 relationship was established between the intensity value of the image and flow velocity within the
75 range.

76 2. System and theory analysis

77 2.1. System setup

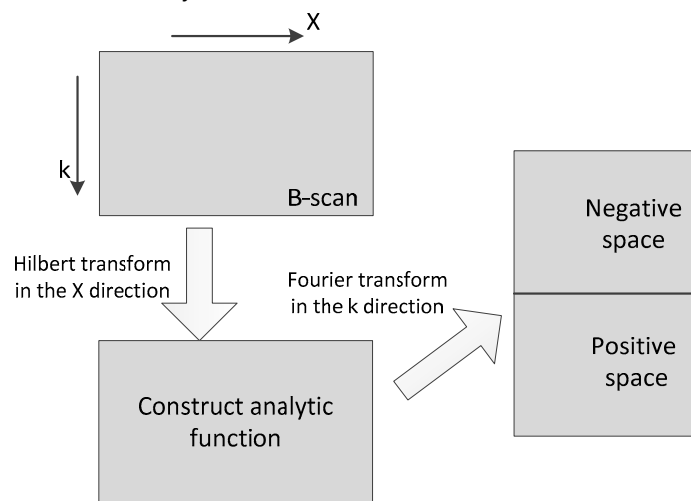
78 The system used in this experiment is shown in Figure 1. The system consists of a
79 superluminescent diode (SLD) as the light source with a center wavelength of 1310 nm and a
80 bandwidth of 75 nm. The theoretical longitudinal resolution determined by the light source is 10 μm .
81 The light from the source is split into two paths through a 50:50 2x2 optocoupler. One light path is
82 directed at a mirror called the reference arm, and the other light path is directed through the sample
83 arm directly toward the sample. The light in the sample arm is coupled into an optical system that
84 includes a collimator, a pair of X- and Y-axis galvanometers, and a 50 mm focal length objective with
85 a theoretical lateral resolution of 17 μm . The beam is reflected from the reference arm, and the sample
86 arm is subsequently coupled into the detection arm and transmitted to a high-speed spectrometer to
87 detect spectral interference signals. SENSORS' GL2048R linear array charge-coupled device (CCD)
88 was the spectrometer used in this study. The number of pixels is 2048, the single pixel size is 10 μm
89 \times 210 μm , and the maximum sampling frequency is up to 147 kHz. The galvanometer imaging speed
90 in our system is 600 mm/s, and the galvanometer reset speed is 3000 mm/s. The sampling frequency
91 of the CCD and the scanning length can be changed in the program to modify the scanning frequency
92 of the B scanning direction and the galvanometer speed of the Y galvanometer.



93
94 **Figure 1.** Schematic of the OMAG system used in this study.

95 *2.2. Theory*

96 The core concept of the OMAG method is to construct a complex analytical signal by using the
97 Hilbert transform of the real-interference signal and obtain the structure and flow rate information
98 of the sample by Fourier transform. Hilbert transform rotates the phase of a signal counterclockwise
99 by 90° . We subsequently constructed an analytical signal whose imaginary part is the Hilbert
100 transform of the real part. Then, we obtained structure and flow rate information in the signal by
101 performing Fourier transform on the obtained analytical signal. Figure 2 shows that Hilbert and
102 Fourier transform need to be performed in X and K directions, respectively, whereas traditional OCT
103 can conduct Fourier transform directly in the K direction.



104
105 **Figure 2.** OMAG flow chart.

106 We can regard the 2D raw data obtained by OCT as a 2D array. The horizontal axis is time t , and
107 the vertical axis is wave number k . We used a function with two variables to represent

$$108 \quad B(k, t) = \cos[2kz_0 + 2\pi(f_c - f_D)t + \phi], \quad (1)$$

109 where z_0 is the initial depth position of the reflective particles at lateral position x and ϕ is a
110 random phase term. f_c is the modulation frequency component, and f_D is the Doppler frequency
111 component. Variables t and k are irrelevant, that is, when t changes, k is constant and vice versa.
112 When the modulation frequency $f_c - f_D$ does not overlap with the signal bandwidth introduced by
113 the random phase term, we can construct the analytic function of t by using the Hilbert transform
114 constructor (1) based on the Bedrosian theorem [27]. In this case, the Hilbert transform of Equation

115 (1) is equal to its orthogonal representation, and $2kz_0$ is currently a constant phase term. If $f_c - f_D >$
 116 0 , then the analytic function of Equation (1) is

$$117 \quad H(k, t) = \cos[2\pi(f_c - f_D)t + 2kz_0 + \phi] + j \sin[2\pi(f_c - f_D)t + 2kz_0 + \phi]. \quad (2)$$

118 If $f_c - f_D < 0$, then the analytic function of Equation (1) is

$$119 \quad H(k, t) = \cos[2\pi(f_c - f_D)t + 2kz_0 + \phi] - j \sin[2\pi(f_c - f_D)t + 2kz_0 + \phi]. \quad (3)$$

120 Mathematically, Equation (3) is a complex conjugate form of Equation (2). We performed Fourier
 121 transform with k as the argument, where t is a constant term. The frequency component z_0 of
 122 Equation (2) is located in the positive space of the entire Fourier domain, and the frequency
 123 component of Equation (3) is located in the negative space of the Fourier domain. This part is the
 124 most critical in the OMAG approach.

125 The derivation shows that a fixed carrier frequency must be introduced to satisfy Hilbert
 126 transform and obtain a quadrature signal. The introduction of carrier frequency aims to add one item
 127 to the phase term of the interference signal, that is, a phase change occurs, and the phase change is
 128 the change in the optical path difference. Thus, the introduction of the fixed carrier frequency
 129 essentially causes the optical path difference to exhibit variety. This objective can be achieved by
 130 using two methods, namely, piezoelectric and offset. In the piezoelectric method, the piezoelectric
 131 ceramic drives the reference arm mirror to move at a uniform speed to introduce a carrier frequency.
 132 The offset method aims to make the collimating light of the sample arm deviate from the rotation
 133 center of the galvanometer to change the optical path and introduce a fixed carrier frequency.

134 The hardware of the piezoelectric OMAG method is different from that of a conventional
 135 frequency-domain OCT device. A piezoceramic needs to be installed on the reference arm mirror to
 136 drive the reference arm mirror to move at a constant speed and thus introduce a fixed frequency shift.
 137 We assumed that the reference mirror moves at a speed of v_{ref} , and the velocity of the moving
 138 particles in the direction of the probe beam is v_s . At this point, we can express the interferogram of
 139 the spectrum as

$$140 \quad B(k, t) = \cos\left\{2k\left[z_0 + (v_{ref} - v_s)t\right] + \phi\right\}. \quad (4)$$

141 Equation (4) shows that when $v_{ref} - v_s > 0$, the region is imaged in the positive space. When
 142 $v_{ref} - v_s < 0$, the region is imaged in the negative space, and moving and static particles are
 143 separated.

144 The offset OMAG method introduces a fixed carrier frequency in such a way that the sample
 145 arm collimates light away from the center of the galvanometer. Compared with the piezoelectric
 146 method, the offset method does not require a single chip microcomputer or a driving circuit, and the
 147 entire system is simpler. Moreover, the piezoelectric method always moves while the reference arm
 148 mirror is moving during the scanning process. Thus, the spectrum of the returning light of the
 149 reference arm is constantly shaking, leading to additional noise in the resulting image. The offset
 150 method can also increase the imaging speed without adding a control module and without affecting
 151 the effect.

152 A schematic of the offset OMAG method is shown in Figure 3. In conventional frequency-
 153 domain OCT, the sample arm's collimated light is usually located at an angle of 45° relative to the
 154 initial galvanometer. We assumed that the optical path difference between the reference and sample
 155 arms is zero. The incident light subsequently moves downward by a distance of δ so that the incident
 156 light deviates from the rotation center of the galvanometer. After the incident light is reflected by
 157 galvanometer M, it is focused by objective lens L onto the focal plane. The focal length of the objective
 158 lens L is f , the distance between the rotation center of the galvanometer and the objective lens is d ,
 159 and the rotation angle of galvanometer M relative to the initial position is α . The change in the optical
 160 path of the galvanometer during lateral scanning can be calculated by ray tracing as follows [28]:

$$161 \quad OPD = \left[d \left(\frac{1}{\cos(2\alpha)} - 1 \right) + \frac{\sin(\alpha)}{\sin(45^\circ - \alpha)} \sqrt{2} \alpha \right]. \quad (5)$$

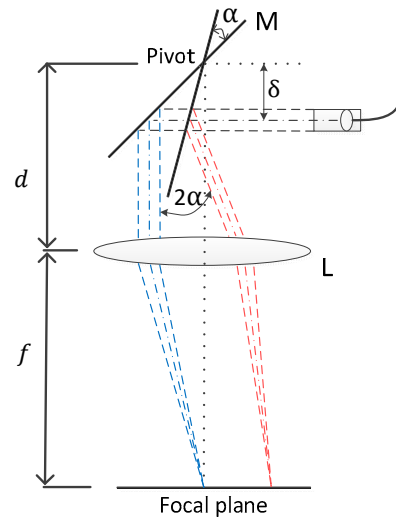


Figure 3. Schematic of the beam offset method at the sample arm.

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164 3. Range derivation

165 Our derivation began with the piezoelectric OMAG method because the minimum
 166 measurement of piezoelectric OMAG is readily available. Then, a range calculation formula of the
 167 offset method was derived according to the relationship between the piezoelectric and offset OMAG
 168 methods. We also derived a range calculation formula of UHS-OMAG.

169 3.1. Derivation process

170 We generally have uneven high-scattering samples when detecting targets. Hence, the random
 171 phase term \emptyset in Equation (1) varies randomly with time $(-\pi, \pi]$. The frequency component of \emptyset
 172 with respect to t is a function of random distribution around zero frequency, and its bandwidth is
 173 BW. The envelope of this spectral distribution depends on the correlation between the interference
 174 signals at different positions of the sample. The bandwidth BW of this envelope is also limited by the
 175 sampling frequency f_s of the system. If BW and f_s are very close, then almost no correlation exists
 176 between the interference signals at different positions of the sample. We introduced modulation
 177 frequency f_c to obtain the analytical signal and subsequently remove its frequency band from the
 178 zero-frequency region until no overlap exists between the frequency band of the parsing signal and
 179 its complex conjugate frequency band. For its Hilbert transform to be strictly equal to its orthogonal
 180 form, the spectrum that corresponds to the phase term that changes over time is shifted to a position
 181 where no overlap with the zero frequency exists. We obtained the applicable conditions of the OMAG
 182 algorithm as follows:

183

$$f_c > \frac{BW}{2}. \quad (6)$$

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BW determines the minimum speed that the system can detect. The smaller BW is, the smaller
 the value of f_c is and the lower the equivalent threshold speed is; hence, a small flow rate can be
 detected. In our derivation, the condition of $BW < 2f_c$ was always met.

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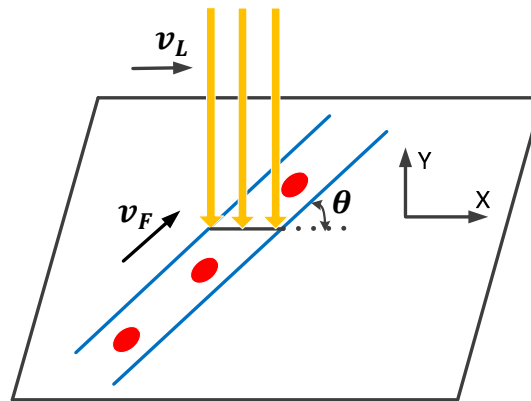
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The optical path difference (OPD) at this time in the piezoelectric OMAG method is the distance
 $v_{ref}t$ of the reference arm motion, the phase change is $2kv_{ref}t$, and the modulation frequency is
 $2k(v_{ref} - v_s)$, that is, the introduced carrier frequency f_c is kv_{ref}/π . Notably, v_{ref} and v_s in
 Equation (4) are vector representations. Relative to the movement of the reference mirror, the
 opposite movement of the particles reduces the difference in optical path length between the sample
 and reference arm and decreases the effective frequency of the modulation. When the value of v_s is
 sufficiently large, the moving particles are projected onto the positive space. In general, when the
 reference arm mirror moves toward the fiber coupler at speed v_{ref} , it is equivalent to the sample arm

195 that moves toward the galvanometer at velocity v_{ref} . At this time, only velocity v_s moves upward,
 196 and the particles of $v_s > v_{ref}$ are imaged on the dynamic plane. The same condition applies when
 197 the reference arm mirror moves in a direction opposite to the fiber coupler. Evidently, the minimum
 198 moving particle that can be measured by the piezoelectric OMAG method is greater than v_{ref} . In
 199 summary, we can obtain the lowest actual speed as follows:

$$200 \quad v_{\min} = \frac{v_{ref}}{\cos \theta}. \quad (7)$$

201 In our work, the angle θ between beam scanning and flow directions was introduced for the
 202 first time to the range calculation of OMAG and UHS-OMAG. Notably, this θ is not the angle between
 203 the incident beam and the direction of flow velocity. Figure 4 shows that v_L is the scanning direction
 204 of the beam, v_F is the moving direction of the particles, and θ is the angle between v_L and v_F .



205
 206 **Figure 4.** Schematic of the angle θ between the scanning direction of the beam and the direction of
 207 flow velocity.

208 In the conventional OMAG method, the phase difference between adjacent A lines in the B-scan
 209 is used to estimate flow velocity. Thus, the velocity during measurement is a component of v_F in X
 210 direction, and the measured velocity is $v_F \cos \theta$. In UHS-OMAG, the A-line density in B-scan is
 211 reduced, the scanning density of B-scan is increased, and the OMAG algorithm is applied to the C-
 212 scan direction. Therefore, the measured speed is v_F . A component of the Y direction, the measured
 213 velocity is $v_F \sin \theta$.

214 In the offset OMAG method, as indicated in Equation (5), α is small when our system collects
 215 data, and the first term in the equation is negligible compared with the second term when making
 216 phase changes. Thus, the phase change of the interference signal can be approximated as

$$217 \quad \varphi = 4k\alpha\delta = 4k\delta\omega t. \quad (8)$$

218 where ω is the angular velocity of the X galvanometer and t is the scan time. Through the phase
 219 change, the change in the OPD of the offset method and the introduced carrier frequency value can
 220 be obtained, as shown in Table 1.

221 **Table 1.** Comparison of piezoelectric and offset methods.

	Piezoelectric method	Offset method
Optical path difference (OPD)	$v_{ref}t$	$2\delta\omega t$
Phase change (φ)	$2kv_{ref}t$	$4k\delta\omega t$
Introducing carrier frequency (f_c)	kv_{ref}/π	$2k\delta\omega/\pi$

222
 223 A comparison of the two methods showed that the minimum speed that can be measured with
 224 the piezoelectric method is the velocity of the reference arm mirror v_{ref} , which can be obtained via
 225 conversion using the offset method as follows:

$$226 \quad v_{\min} = \frac{v_{ref}}{\cos \theta} = \frac{2\delta\omega}{\cos \theta}. \quad (9)$$

227 The maximum detection speed of the system is determined by the sampling frequency.
 228 According to the sampling theorem, the sampling frequency should be greater than twice the highest
 229 frequency component of the signal. Sampling frequency refers to time sampling, which is the
 230 sampling frequency f_{req} of the CCD. In summary, the range of an ordinary OMAG system is

$$231 \quad v_{\max} = f_{req} \frac{\lambda}{4 \cos \theta}. \quad (10)$$

232 3.2. UHS-OMAG range

233 Equation (9) shows that measuring a low flow velocity requires reducing BW and the
 234 galvanometer speed to obtain high sensitivity. However, BW cannot be reduced by reducing the
 235 diameter of the collimated light because the light source of our system is deterministic, and the effect
 236 of this method is limited. Thus, the speed of the galvanometer must be reduced to improve sensitivity.
 237 However, as the galvanometer speed decreases, the overall imaging process time increases
 238 considerably, thereby affecting the final image quality. Moreover, this method cannot achieve a
 239 remarkable increase in sensitivity, so the highly sensitive UHS-OMAG method was proposed. In
 240 contrast to the conventional OMAG method, UHS-OMAG reduces the density of A lines in the B-
 241 scan, increases the scanning density of the B-scan, and applies the ordinary OMAG algorithm to the
 242 C-scan direction. In the actual measurement process, ordinary OMAG only needs to complete a 2D
 243 scan, and the Hilbert transform structure analysis signal is implemented in the B-scan direction. UHS-
 244 OMAG must complete a 3D scan once and take an A line from each B-scan to form a 2D map.
 245 Subsequently, a Hilbert transform structure analysis signal is created for this 2D map. When using
 246 the offset method, the beam at this time needs to deviate from the rotation center of the Y
 247 galvanometer and not that of the X galvanometer.

248 Attention should be paid to the changes in range calculation when using the UHS-OMAG
 249 method. Compared with Equation (9), ω is no longer the angular velocity of the X galvanometer at
 250 this time. Instead, it is the angular velocity ω_Y of the Y galvanometer, δ is the distance δ_Y of
 251 the rotation center of the offset Y galvanometer, and f_{req} in Equation (10) is no longer the sampling
 252 frequency of the CCD but the scanning frequency f_B of B. The influence of angle θ between the beam
 253 scanning and flow velocity directions in the UHS-OMAG method should be given attention. In
 254 summary, the range of the UHS-OMAG method is

$$255 \quad v_{\min} = \frac{2\delta_Y \omega_Y}{\sin \theta}, \quad (11)$$

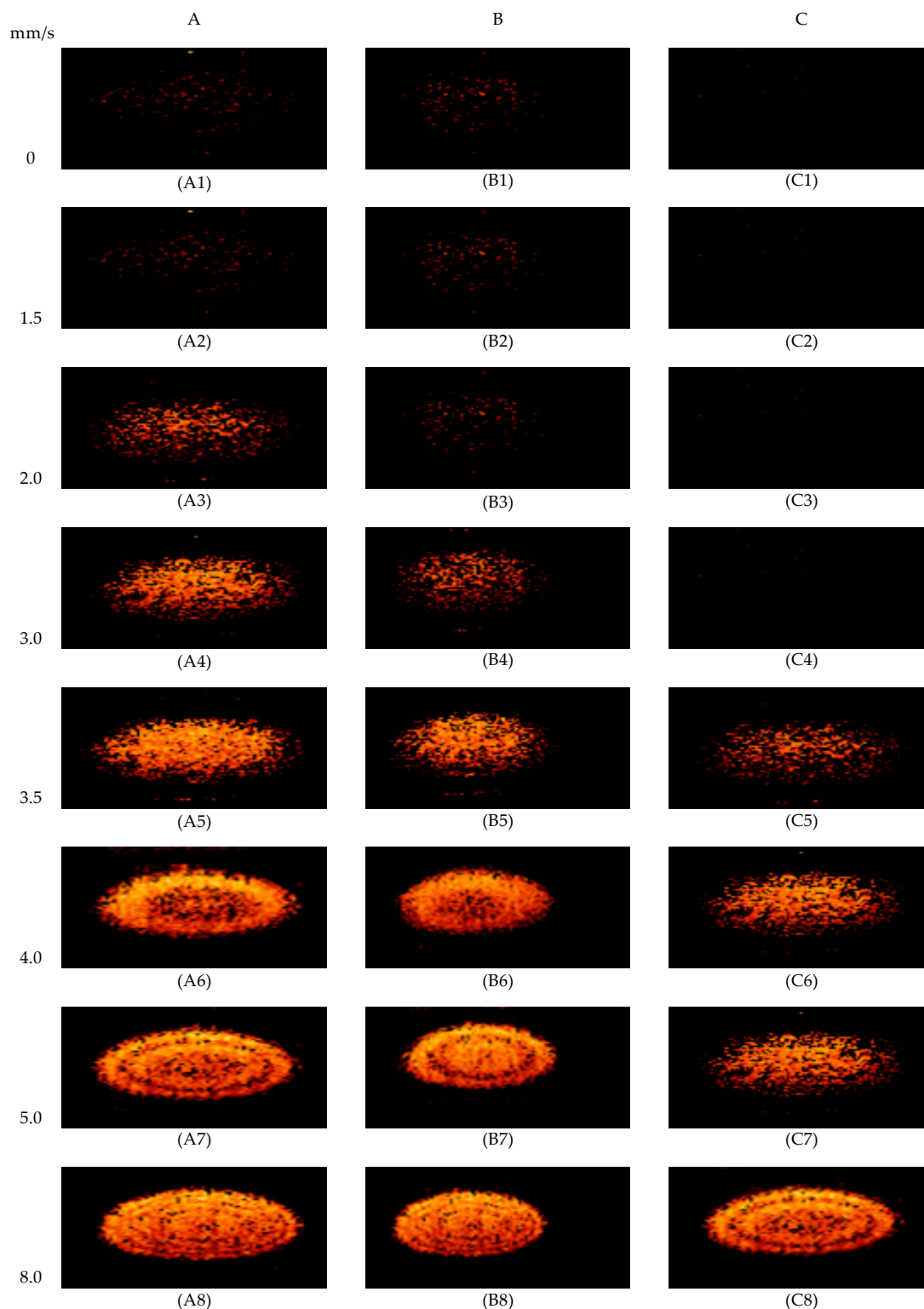
$$256 \quad v_{\max} = f_B \frac{\lambda}{4 \sin \theta}. \quad (12)$$

257 4. Results and discussion

258 We used the offset method in the experiment. A capillary tube with an inner diameter of 0.4 mm
 259 was utilized as a channel, and milk was employed as a test fluid. A constant flow pump was used to
 260 provide a known steady flow rate.

261 From the system in Figure 1, we acquired spectral interference raw data from which the OMAG
 262 signal was calculated. We only needed a B-scan to process in the OMAG algorithm. In the 3D data
 263 block obtained by the acquisition system, we took Hilbert and Fourier transform from the acquired
 264 B-scan to complete the OMAG imaging. We obtained the spectral data matrix row by row to derive
 265 the analysis function using Hilbert transform. Then, we performed Fourier transform on the data
 266 matrix of Hilbert transform column by column. We divided the frequency components into positive
 267 and negative spaces of the Fourier domain. The flow partial region was imaged on a positive plane,
 268 and the stationary partial region was imaged on a negative plane. Positive plane imaging minus
 269 negative plane imaging resulted in an OMAG image.

270 4.1. OMAG range verification



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Figure 5. Experimental results of OMAG. The longitudinal direction is the same group of images at different flow rates, with the flow rate being gradually increased; the lateral direction is the experimental image of different groups at the same flow rate.

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We divided our OMAG experiment into groups A, B, and C. In the group A experiment, our B-scan direction length was set to 3 mm, the CCD sampling frequency f_{req} was 12 KHz, the scanning density was 500 lines/mm, the offset δ was 2.5 mm, and the galvanometer angular velocity was 24 mm/s. In the group B experiment, we did not change the other parameters, we reduced the scanning density to 200 lines/mm, and the galvanometer angular velocity was increased to 60 mm/s. In the group C experiment, the other parameters were unchanged compared with those in group A. The

281 CCD sampling frequency f_{req} was increased to 24 KHz. We compared the variation in the range of
 282 angular velocity of the galvanometer based on the results of groups A and B. By comparing groups
 283 A and C, we determined the range when the CCD sampling frequency changed.

284 According to the parameters of our experimental system, the theoretical ranges of the three sets
 285 of experiments were calculated using Equations (9) and (10), as shown in Table 2.

286 **Table 2.** OMAG experimental parameter settings.

Group	f_{req} (KHz)	Scanning density (lines/mm)	δ (mm)	ω (mm/s)	Range (mm/s)
A	12	500	2.5	24	1.70–3.93
B	12	300	2.5	40	2.83–3.93
C	24	500	2.5	48	3.39–7.86

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 288 The pseudo color image results obtained through our experiments are shown in Figure 5, in
 289 which the leftmost side is the flow rate in mm/s.

290 The experimental results show that several images, such as A1 and A2 in group A; B1, B2, and
 291 B3 in group B; and C1, C2, C3, and C4 in group C, were not removed due to unavoidable slight jitter.
 292 Particles with an effective velocity were not screened out because their velocity was lower than the
 293 measurement range. In such a case, the imaging in each group was the same because the imaging
 294 images of A1 and A2 were the same.

295 As the speed increased, the particles that entered the range of the speed range were screened
 296 out. In the beginning, the velocity of the central portion of the test tube was higher than that of the
 297 wall portion, which conforms to the physical law. As the speed increased, many other particles
 298 entered the speed range, and the particles around the tube wall were also displayed. After the speed
 299 exceeded the range, some of the particles outside of this range were imaged onto the velocity plane,
 300 and some were imaged on the static plane. Phase winding occurred, and a circular pattern was
 301 created. In group A, the imaging at a flow rate of 2 mm/s was A3, at which point moving particles in
 302 the center of the test tube were already observed. As the flow rate and brightness increased, phase
 303 winding began to occur when the image was A6, and the measurable range was exceeded. In group
 304 B, when imaging B4 was just entering the range, imaging B6 was just beyond the range. In group C,
 305 when imaging C5 was just entering the range, imaging C8 was just beyond the range. The
 306 experimental results show that the detectable flow rates of groups A, B, and C were 1.7 to 3.9, 2.8 to
 307 3.9, and 3.4 to 7.9 mm/s, respectively. This result is consistent with the range we calculated using the
 308 formula.

309 4.2. UHS-OMAG range verification

310 The UHS-OMAG experiment was performed differently in comparison with the ordinary
 311 OMAG method. UHS-OMAG requires a C-scan image in a 3D data block. We took all B-scan images,
 312 composed a 3D data block, and took a C-scan image from the block. To complete this process, we
 313 took out the A line of the same position of each B-scan in MATLAB and formed a C-scan image. Then,
 314 we processed the 2D spectrum of the reconstructed C-scan image and performed the same Hilbert
 315 and Fourier transform and subsequent processing as those in ordinary OMAG.

316 We divided our UHS-OMAG experiment into groups D, E, and F. In the group D experiment,
 317 the CCD sampling frequency was 60 kHz, the scanning density was 60 lines/mm, the B scanning
 318 direction length was 1 mm, the C scanning direction scanning density was 600 lines/mm, offset δ_y
 319 was 2.5 mm, and the scanning length was 2 mm.

320 In the group E experiment, we only changed the length of the B-scan direction (set it to 2 mm).
 321 A change in the length of the B-scan direction would change the B-scan frequency and the speed of
 322 the Y galvanometer. In the group F experiment, we continued to increase the length of the B-scan
 323 direction and observed the change in the range.

324 The theoretical ranges for the three sets of experiments were calculated with Equations (11) and
 325 (12). In accordance with our system parameters, we obtained B-scan frequency (f_B) and Y-magnitude
 326 speed (ω_y) (Table 3).

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Table 3. UHS-OMAG experimental parameter settings.

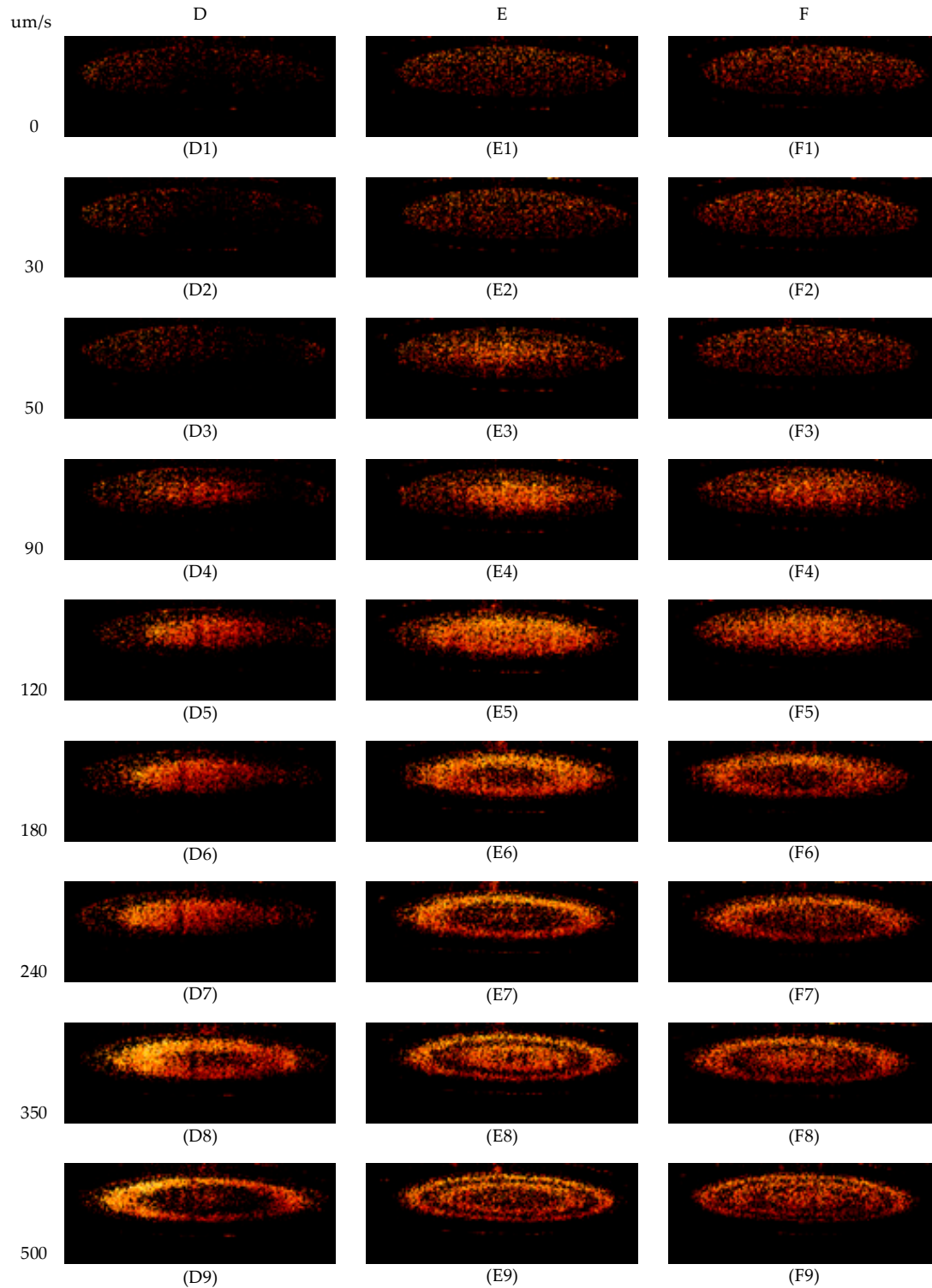
Group	B-scan length(mm)	f_B (Hz)	δ_V (mm)	ω_V (mm/s)	Range ($\mu\text{m/s}$)
D	1	750	2.5	1.250	85–347
E	2	375	2.5	0.625	44–174
F	3	250	2.5	0.417	29–116

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The pseudo color image results obtained through our experiments are shown in Figure 6, in which the leftmost side is the flow rate in $\mu\text{m/s}$.



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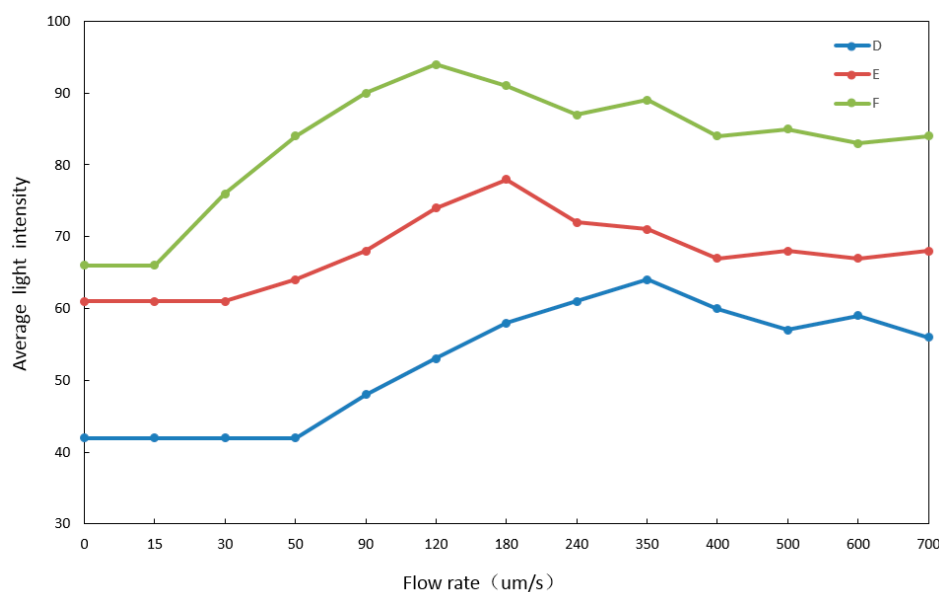
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Figure 6. Experimental results of UHS-OMAG.

333 A comparison of images D1, F1, and E1 with A1, B1, and C1 showed that the mirror image that
 334 was not eliminated was more significant in the same state of 0 flow rate because the UHS-OAG
 335 method acquired more effects due to subtle jitter.

336 The same analysis was applied to group D. When imaging D4 was just entering the range,
 337 imaging D8 began to phase entangle beyond the range. In group E, when imaging E3 was just
 338 entering the range, imaging E6 began to phase entangle beyond the range. In group F, when imaging
 339 F4 was just entering the range, imaging F6 was just beyond the range. Our experimental results
 340 showed the flow rates detected by groups D, E, and F were 90 to 350, 50 to 180, and 30 to 120 $\mu\text{m/s}$,
 341 respectively, which are consistent with the theoretical calculation range values in Table 3.

342 We processed all the collected data by using the UHS-OMAG method. The relationship between
 343 the average light intensity value and the flow rate of the obtained experimental image is shown in
 344 Figure 7.



345

346 **Figure 7.** Relationship between average light intensity values and flow rate in the UHS-OMAG
 347 method.

348 When the flow rate was small, the jitter effect was not eliminated in all three cases; the higher
 349 sensitivity was, the greater the group influence was. In the range, the average light intensity value
 350 gradually increased as the flow rate increased. Beyond the range was exceeded, phase winding began
 351 to occur, and the average light intensity value began to fluctuate. Within the range, the intensity value
 352 of the imaged image was linear to the magnitude of the flow velocity.

353 5. Conclusions

354 We developed a flow rate range calculation formula for the common OMAG method and high-
 355 sensitivity UHS-OMAG method to quantify system sensitivity. We analyzed the piezoelectric OMAG
 356 method and the offset OMAG method. We used the variation in OPD and introduced the angle θ
 357 between beam scanning and flow velocity directions to accurately calculate the range under the
 358 OMAG method. The calculated range can be applied to normal OMAG flow rate detection and in the
 359 more sensitive UHS-OMAG method. We also obtained a linear relationship between the intensity
 360 value of the experimental image obtained under the OMAG method and the flow rate in the range
 361 by analyzing the experimental image. Our work is of considerable value in the practical application
 362 of the OMAG methodology in the future.

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