

1 Article

2 PEDOT:PSS-based temperature-detection thread for 3 wearable devices

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13 **Abstract:** In this research, we developed a wearable temperature-sensing element by dip dyeing
14 threads in poly (3, 4-ethylenedioxythiophene) polystyrene sulfonate (PEDOT:PSS) (p-type
15 conducting polymer) solution. The PEDOT:PSS was used to dye the textile and it exhibited
16 negative temperature coefficient characteristics in which the resistance decreases as the
17 temperature increases. The fabricated temperature-detection thread achieved a sensitivity of 167.1
18 $\Omega/^\circ\text{C}$ with 99.8% linearity in the temperature range of -50 to 80 $^\circ\text{C}$. We anticipate that temperature
19 sensors that apply our technology will be made as stitch- or textile-type for wearable devices, and
20 they will be widely adopted for different applications such as in fitness, leisure, healthcare, medical
21 treatment, infotainment, industry, and military applications, among others.

22 **Keywords:** temperature-detection; thread; PEDOT:PSS; wearable devices

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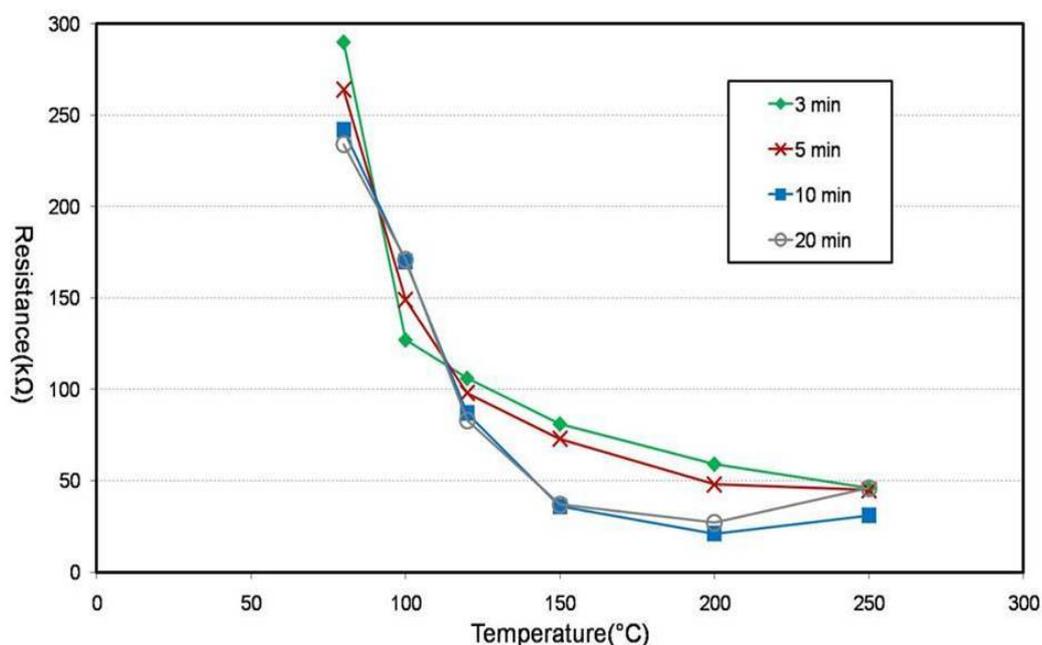
24 1. Introduction

25 Wearable technology — a promising technology that will offer us lighter, more flexible and
26 more mobile electronic devices — has recently gained increasing attention [1]. The category of
27 wearable technology goes beyond that of conventional portable electronics carried by hand, such as
28 smart phones and laptops, so now it includes electronic devices that can be worn close to the body
29 [2, 3]. With technological advancement, the boundaries of electronics have been stretched from what
30 we can carry to what we can wear [4]. Because of their ability to continuously communicate near
31 human body; wearable devices can collect real-time information of the body and in the environment
32 [5, 6]. However, the current status of wearable technology still remains at a research level where
33 computing devices are simply miniaturized and attached to apparel to monitor vital signals, e.g.
34 smart watches and smart shirts [7]. A more meaningful deployment of the technology will be
35 achieved once the technology matures to a point where we can form electronic circuits in textile
36 threads [8]. As the interdisciplinary research between thread manufacturing and IT has recently
37 accelerated, various cases of smart textile that incorporate display elements have been reported, and
38 smart textile technology is evolving to integrate information-processing and data-transmission
39 elements into textiles [9]. Smart textiles that incorporate sensors can be utilized in various
40 applications such as in military [10], medical [11-16], fashion, and sport [17] applications. Because of
41 their flexibility and stretchability, textiles can be easily applied to large surface areas, and
42 approximately 70% of the surfaces that people touch every day (e.g., clothes, beds, wall materials,
43 interior decorations, and floor materials) use textiles. We believe that textile-based materials and
44 structures integrated with active electronic elements/ systems will enable emergence of more
45 efficient and sustainable electronic textiles and bring about a groundbreaking technological turning
46 point in improving mechanical properties during bending, one of the biggest issues in the field of

47 modern flexible electronics/displays [18, 19]. Electronic textiles — threads dyed with conductive inks
48 — can be prepared by the following methods: dip dyeing, roller printing, screen printing, inkjet
49 printing, spray printing, and transfer printing (which includes spin coating). In the current research,
50 we prepared temperature sensors for wearable devices by dip dyeing threads in poly (3,
51 4-ethylenedioxythiophene) polystyrene sulfonate (PEDOT:PSS) (conductive polymer) solution and
52 evaluated their characteristics.

53 2. Design and Fabrication

54 Textile temperature-sensor samples were prepared by dip dyeing 3-cm cotton threads with a
55 diameter of 0.25 mm (cross-sectional area: 0.049 mm²) in PEDOT:PSS (Heraeus, CLEVIOS™ PH1000).
56 In cotton threads, the sericin layer swells when it comes in contact with water; thus, cotton threads
57 have the best swelling capacity compared with other threads. They also possess excellent thermal
58 conductivity; thus, they were chosen as dip dyeing material [20]. Fig. 1 shows the changes in the
59 resistance of the PEDOT:PSS ink dip-dyed textile temperature sensors according to the variations in
60 the annealing temperature and time.

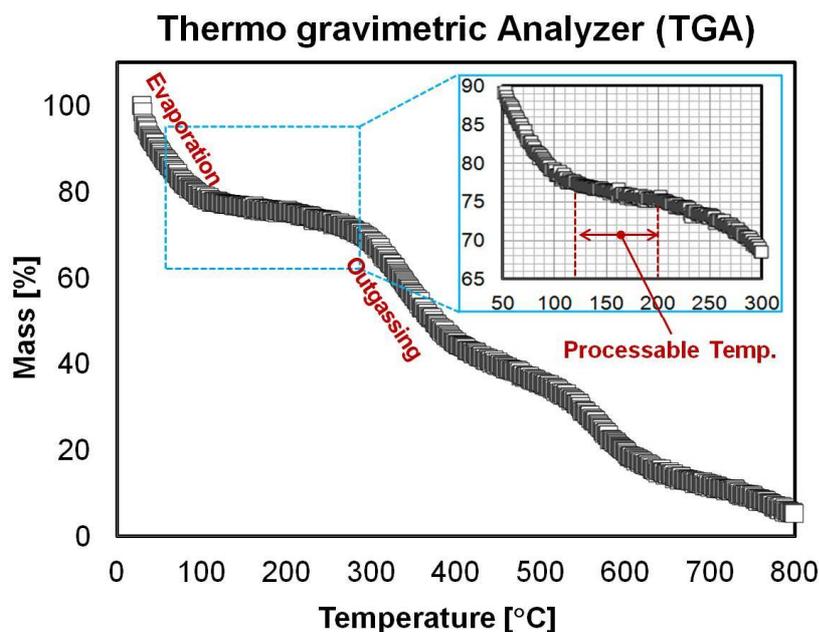


61
62 **Figure 1.** Influence of annealed time and temperature on the resistance of a thread-type sensor. The
63 resistance of PEDOT:PSS changes depending on the annealing temperature and time.

64 The resistance of the PEDOT:PSS (a mixture of PEDOT, a conductive polymer, and PSS, a
65 water-soluble polymer electrolyte) changes depending on the annealing temperature. As the
66 annealing temperature increases, the PSS that surrounds the PEDOT disassociates, decreasing the
67 resistance [21-24].

68 A thermogravimetric analyzer (TGA) was used to monitor the changes in the weight of the
69 PEDOT:PSS due to the chemical and physical changes according to temperature. Fig.2 shows two
70 regions where decrease in the PEDOT:PSS is apparent.

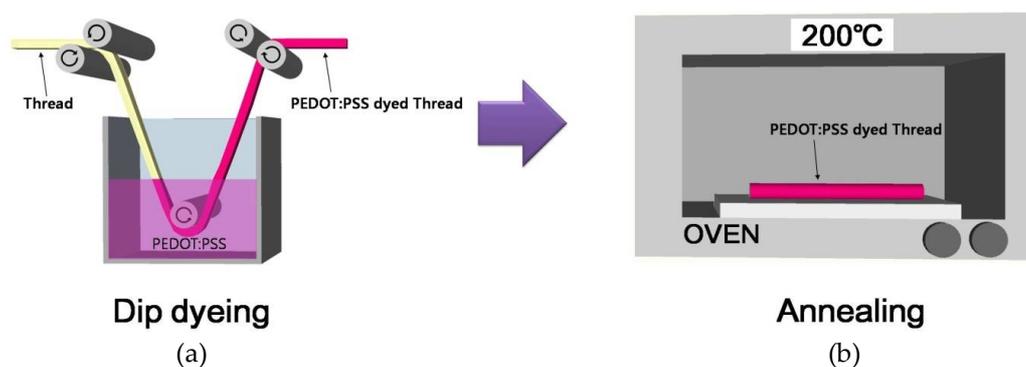
71 The first decrease (up to 150 °C) was due to water evaporation; the second decrease (220-320 °C)
72 observed at the PSS dissociation phase was due to SO₂/SO₃ outgassing around 250 °C [21, 25].
73 Therefore, we chose 200 °C as the annealing temperature to obtain maximum conductivity without
74 exceeding 250 °C. At 200 °C, different annealing times (10 and 20 min) yielded similar low resistance
75 values; therefore, we chose 10 min as the annealing time for higher efficiency with respect to the
76 processing time and energy consumption.



77

78 **Figure 2.** Thermogravimetric analyzer (TGA) curve of PEDOT:PSS. It shows two regions where
 79 decreases in the PEDOT:PSS are apparent. The first decrease (up to 150 °C) was due to water
 80 evaporation. The second decrease (220-320 °C) observed at the PSS dissociation phase was due to
 81 SO₂/SO₃ outgassing around 250 °C.

82 The optimal recipe we used to prepare the sensors was to first dip dye the thread samples for 10
 83 min then perform annealing at 200 °C for 10 min (Fig. 3). The procedure was repeated twice to
 84 increase the density of the PEDOT:PSS absorbed in the threads [20]. Electrical pads were formed at
 85 the two ends of the PEDOT:PSS-dyed threads by applying a silver paste. To protect the sensors from
 86 moisture and dust, an encapsulation layer was formed by dip dyeing the threads in polystyrene
 87 [(C₈H₈)_n] solution [(C₈H₈)_n:toluene = 1:10] and air drying them at room temperature.



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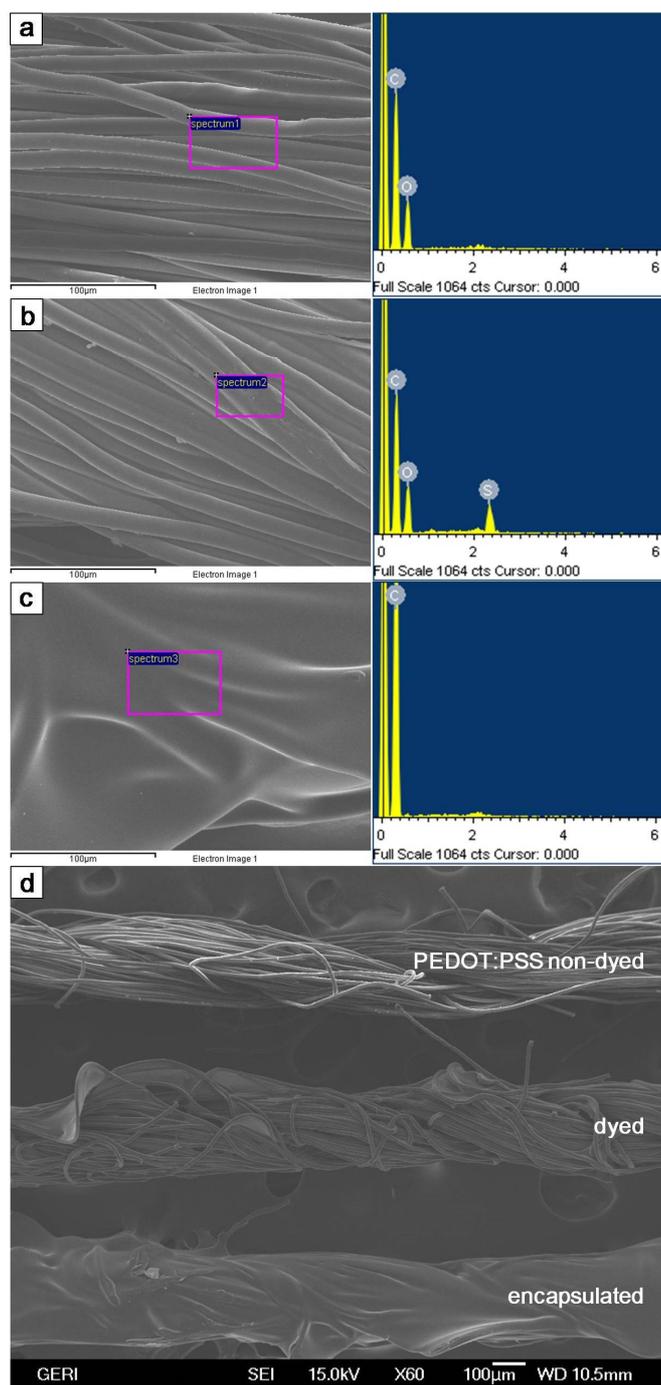
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Figure 3. Schematic of the process of the thread dyeing. (a) Dip dyeing and (b) annealing.

91 3. Result and Discussion

92 Scanning electron microscope (SEM) and energy dispersive X-ray spectroscopy (EDX) images
 93 (Fig.4 left and right, respectively) show the micromorphology and components of the fabricated
 94 textile sensors. The non-dyed cotton threads (Fig. 4(a)) were composed of cellulose polymer
 95 ((C₆H₁₀O₅)_n·H₂O), apparent in the EDX results, confirming the presence of C and O [26]. The
 96 PEDOT:PSS-dyed cotton thread (Fig. 4(b)) showed EDX peaks in the locations of C, O, and S,
 97 confirming the presence of PEDOT:PSS [27]. The PEDOT:PSS-dyed cotton threads encapsulated
 98 with (C₈H₈)_n (Fig. 4(c)) showed the most prominent EDX peaks in the location of C [28,29]. Fig. 4(d)
 99 shows the SEM image of all three thread types: non-dyed (original cotton thread) (upper),
 100 PEDOT:PSS-dyed (middle), and PEDOT:PSS-dyed and encapsulated (lower). The SEM image of the

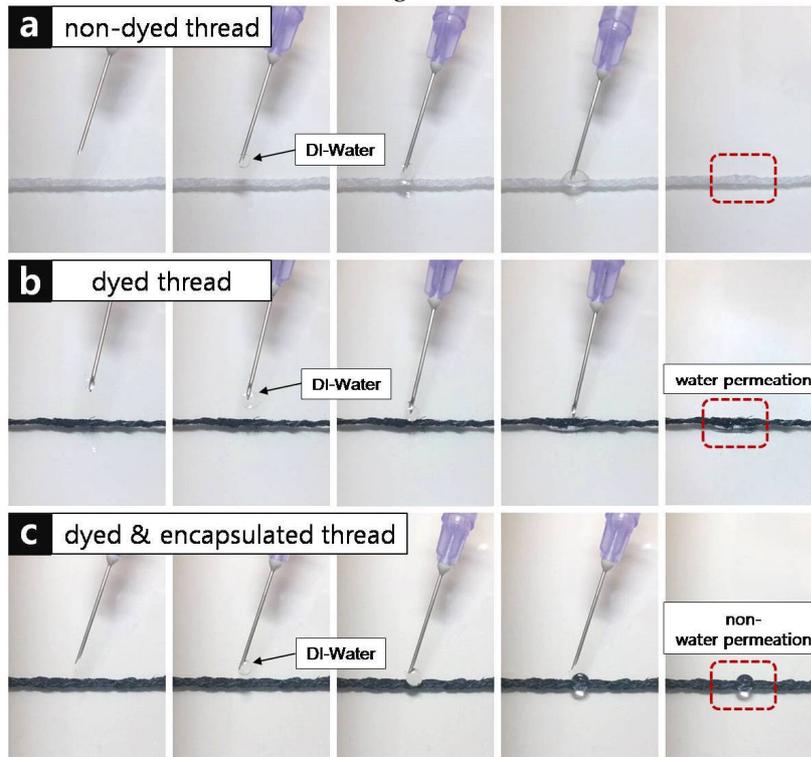
101 PEDOT:PSS-dyed threads shows that the spaces between threads are filled with PEDOT:PSS (clearly
 102 different from the non-dyed threads). The SEM image of the encapsulated threads failed to show the
 103 threads because the $(C_8H_8)_n$ solution has completely covered them.



104
 105 **Figure 4.** EDX analysis of the PEDOT:PSS non-dyed, dyed, and encapsulated threads. Surface
 106 morphological and componential analysis of (a) the PEDOT:PSS non-dyed thread, (b) dyed thread,
 107 and (c) dyed and encapsulated thread. (d) SEM micrograph of the PEDOT:PSS non-dyed,
 108 PEDOT:PSS dyed, and PEDOT:PSS dyed and encapsulated threads.

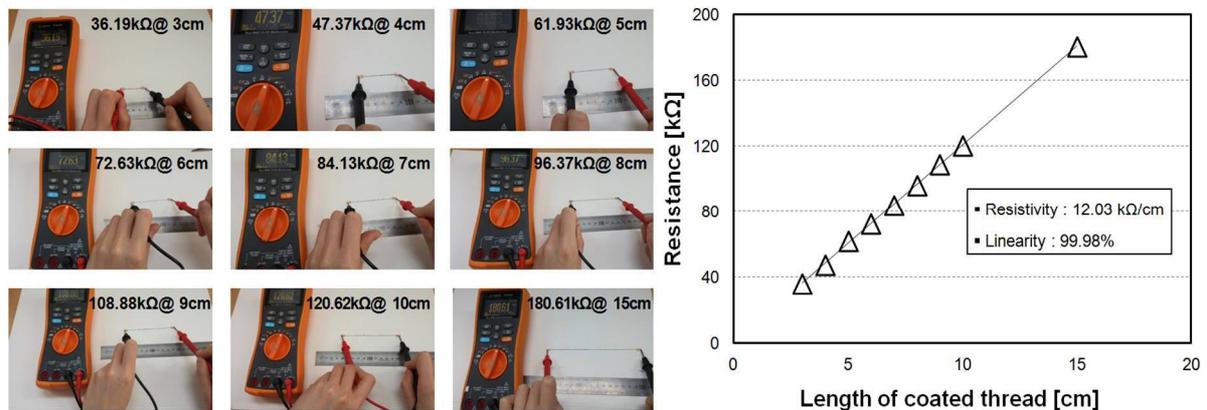
109 The non-dyed, PEDOT:PSS-dyed, and PEDOT:PSS-dyed and encapsulated threads were tested
 110 under water to test the encapsulation effect, i.e., the hydrophobic properties of $(C_8H_8)_n$ [30]. The
 111 non-dyed threads showed hydrophilic behavior (Fig. 5(a)) as deionized (DI)-water droplets applied
 112 to the non-dyed threads were absorbed. The PEDOT:PSS-dyed threads showed similar hydrophilic
 113 behavior as that of the non-dyed threads (Fig. 5(b)). In contrast to the non-dyed and

114 PEDOT:PSS-dyed threads, the PEDOT:PSS-dyed and encapsulated threads showed hydrophobic
 115 behavior (Fig. 5(c)) as the DI-water droplets applied to the PEDOT:PSS-dyed and encapsulated
 116 threads remained on the threads without being absorbed.



117
 118 **Figure 5.** Hydrophilic test by dropping water on each thread sample. (a) PEDOT:PSS non-dyed
 119 thread, (b) PEDOT:PSS dyed thread, and (c) PEDOT:PSS dyed and encapsulated thread.

120 The resistance of the textile temperature sensors under different textile lengths was measured at
 121 25 °C. By dip dyeing at a uniform amount of time, the amount of absorbed PEDOT:PSS was the
 122 same, which yielded a uniform thread thickness. To verify this result, the resistance of the textile
 123 sensors under different textile lengths was measured as shown in Fig. 6. As the textile length
 124 increased, the resistance of the textile sensors proportionally increased with a slope of 12.03 kΩ/cm
 125 and linearity of 99.98%.



126
 127 **Figure 6.** Resistance of a length of the PEDOT:PSS dyed thread.

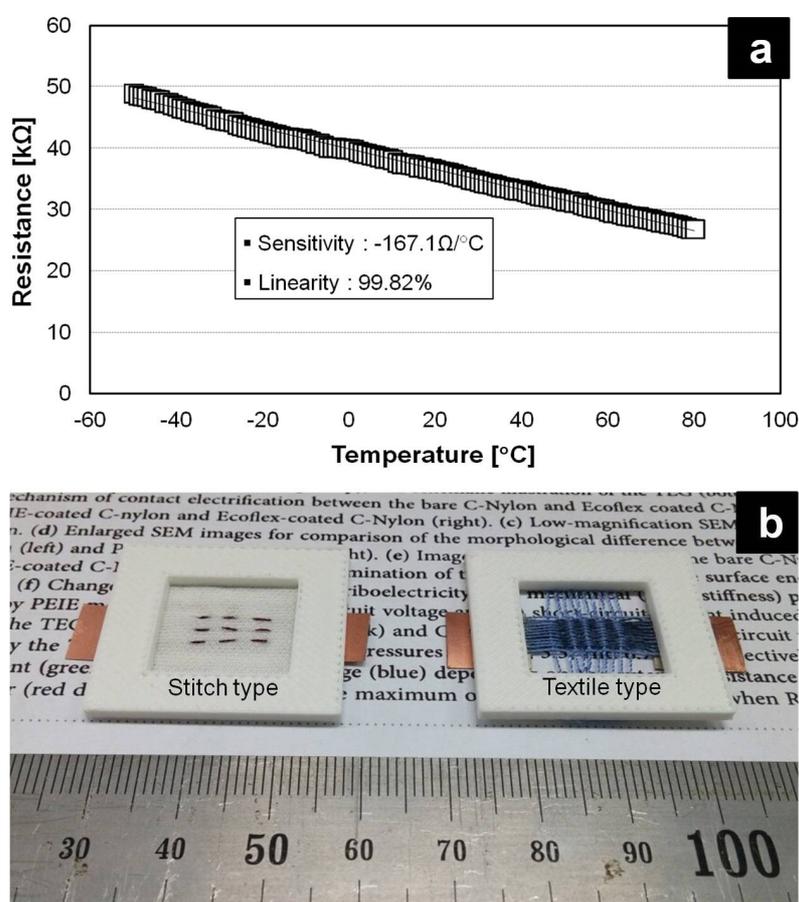
128 PEDOT:PSS exhibits p-type semiconductor properties and forms an impurity state (acceptor
 129 level) near the valance band with a Fermi energy level that can be calculated as follows:

$$E_f = E_{fi} - kT \ln(P_o/N_i), \quad (1)$$

130 Where E_f is the Fermi level of the extrinsic semiconductor, E_{fi} is the Fermi level of the intrinsic
 131 semiconductor, k is the Boltzmann constant, T is the temperature in Kelvin, N_i is the carrier
 132 concentration of the intrinsic semiconductor, and P_o is the hole concentration of the p-type extrinsic
 133 semiconductor.

134 Electrical conductivity increases as the temperature increases because electrons are excited in
 135 the valence band due to thermal energy, which creates holes in the valence band [31, 32]. In other
 136 words, the resistance decreases as the temperature increases, which is a negative temperature
 137 coefficient (NTC) of the resistance characteristic.

138 The fabricated textile temperature sensors possess an NTC characteristic, and their thermal
 139 responsivity was obtained by measuring the sensor resistance (using a fixed textile length of 3 cm) as
 140 the temperature was increased at an increment of 1 °C from -50 to 80 °C. The sensors exhibited a
 141 sensitivity of 167 $\Omega/^\circ\text{C}$ with 99.8 % linearity as shown in Fig. 7. The prepared textile temperature
 142 sensors were used for a normal fabric stitch application and a textile-type application in which a
 143 PEDOT:PSS-coated fabric for temperature sensors was woven using normal threads as shown in
 144 Fig.7(b).



145
 146 **Figure 7.** Resistance-temperature characteristics of a temperature-detection thread. (a) The
 147 temperature detection thread exhibited a sensitivity of 167 $\Omega/^\circ\text{C}$ with 99.8% linearity. (b) The
 148 fabricated thread is possible to utilize as stitch and textile type wearable temperature sensor.

149 5. Conclusions

150 In this research, we have developed wearable textile temperature sensors by dip dyeing cotton
 151 threads in p-type conductive polymer (PEDOT:PSS) solution. The fabricated sensors achieved a
 152 sensitivity of 167.1 $\Omega/^\circ\text{C}$ with 99.8% linearity in the temperature range of -50–80 °C. The applicability
 153 of the developed textile sensors was demonstrated by sewing or weaving them into an actual cloth
 154 to form two different types of sensors: stitch and textile types.

155 Our developed sensors have an advantage in terms of flexibility, low cost, simple and fast
156 fabrication processes, and applicability to light and small devices. We anticipate that they will be
157 useful in various applications such as in fitness, well-being, leisure, healthcare, medical,
158 infotainment, industry, and military applications.

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161 **Conflicts of Interest:** The authors declare no conflict of interest

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