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# Dental adhesion enhancement on zirconia inspired by mussel's priming strategy using catechol

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**Abstract:** Zirconia has recently become one of the most popular dental materials in prosthodontics being used in crowns, bridges, and to implants. However, weak bonding strength of dental adhesives and resins to zirconia surface has been a grand challenge in dentistry, thus finding a better adhesion to zirconia is urgently required. Marine sessile organisms such as mussels use a unique priming strategy to produce a strong bonding to wet mineral surfaces; one of the distinctive chemical features in the mussel's adhesive primer proteins is high catechol contents among others. In this study, we pursued a bioinspired adhesion strategy, using a synthetic catechol primer applied to dental zirconia surfaces to study the effect of catecholic priming to shear bonding strength. Catechol priming provided a statistically significant enhancement ( $P < 0.05$ ) in shear bonding strength compared to the bonding strength without priming, and relatively stronger bonding than commercially available zirconia priming techniques. This new bioinspired dental priming approach can be an excellent addition to the practitioner's toolkit to improve dental bonding to zirconia.

**Keywords:** Zirconia; primer; priming; bonding; catechol; dental; prosthodontics

## 1. Introduction

Ceramics have been widely used for dental and biomaterials, e.g., for prostheses. Zirconia has recently become one of the most popular ceramic dental and biomaterials with its superior mechanical properties: highly tough and strong, wear resistant, shock resistant, while both chemically and dimensionally stable [1]. Its superior mechanical properties are due to a martensitic type phase transformation that prevents crack propagation [2]. However, owing to its high chemical resistance, traditional dental ceramic bonding techniques (e.g., chemical ceramic etching) are not compatible with zirconia [2]. Traditional mechanical grinding or sand blasting methods on dental ceramics can be an alternative, but it may cause the phase transformation and hydrothermal fatigue degradation [3].

39 Priming (or adhesive priming) is a surface treatment that can promote  
40 adhesion of coatings or adhesives to the substrate of interest. Silane-based primers  
41 (known as silane coupling agents) are commonly used to prime dental surfaces,  
42 including ceramics. Despite many attempts to improve the bonding strength to  
43 zirconia using the silane-based coupling agents, no significant improvement has  
44 been reported yet [3].

45 In the past decades, the National Institute of Dental and Craniofacial Research  
46 (NIDCR) has supported interdisciplinary studies such as marine mussel adhesion  
47 as the oral environment has much in common with the intertidal environment;  
48 both oral and marine adhesions are subjected to opportunistic microbes, cyclic  
49 stress, constant fluid flow with variations in salinity, temperature and pH [4].  
50 Figure 1 shows marine sessile organisms adhere to rocks at the seashore. The  
51 NIDCR's long-term investment to the bioadhesion [4,5] has recently begun to show  
52 potential for practical dental [6] and biomedical [7,8] applications. Several dental  
53 applications of catechol have been reported using catechol-containing polymers  
54 such as tannin as a dental sealant [9] and catecholic methacrylamide for a dental  
55 adhesive [10] via catechol-ferric iron complexation. Despite the inherent aesthetic  
56 limitations of Fe-catechol complexation, (complexes are highly colored and darken  
57 over time) the previous work exposed the potential of catechol chemistry for dental  
58 materials applications. In contrast to these previous approaches which mimic the  
59 mussels use of catecholic complexation and crosslinking chemistry for  
60 enhancement of *cohesive* strength within the byssus, we, in this study instead aimed  
61 to mimic the mussel's means of priming surfaces with catecholic bondings that  
62 increase the *adhesive* strength of mussel plaque to mineral surfaces [11].  
63



64  
65 **Figure 1.** Mussels and other marine sessile organisms such as mussels anchored to mineral surfaces  
66 at seashore in Santa Barbara, California, U. S.

67 One of the useful chemical features of mussel's adhesive mechanism is the use  
68 of catechol- and phospho-rich proteins as surface primers [11-13]. Similarly, in  
69 dentistry phosphorous-based primers such as 10-methacryloyloxydecyl  
70 dihydrogen phosphate (MDP) are commonly used based in part on the strength of  
71 phosphate binding to Calcium ions in hydroxyapatite (the main mineral in human

teeth — higher than 90 wt. % in enamel and 70 wt. % in dentin — and in human bone — up to 70 wt. %). By bridging the surface minerals to a polymerizable methacrylate, MDP helps to achieve bonding performance of methacrylate-based dental resins.

MDP has also been shown to improve adhesion of dental resins to zirconia surface by ionic phosphate-Zr binding [3,14], yet further increases to the strength of such resins bound to zirconia is urgently required and many researchers are looking for alternative chemistry that can fulfill this demand. Very recently, our group has reported adhesion enhancement of dental adhesion to silica, steel and tooth enamel using the catechol-containing primers [6,15]. In contrast to the large body of literature regarding phosphate-primers, and despite over 10,000 peer-reviewed papers published within the past decade on catechol-mediated biological adhesion [11], the use of catechol chemistry for strength enhancement and surface priming in dental settings remains largely unexplored.

In this study, we investigated if one of the most pressing issues in prosthodontics, poor adhesion to zirconia, could be overcome with catecholic bioinspired surface priming. Using a previously reported bifunctional catechol-methacrylate to prime zirconia, we were able to demonstrate significant improvement in the knife shear bonding strength compared to untreated surfaces. Moreover, the bonding performance is superior to commercial dental primers reliant on acidic phosphate and carboxylate functionality. Our results highlight the potential of catechol-mediated surface priming to solve bonding issues with zirconia for dental and biomedical applications. In addition, we were able to correlate bonding performance with surface coverage as measured by SEM and offer an improved synthetic method to access the catechol methacrylate primer in higher purity compared to the previously reported method [6,16,17].

2. Materials and Methods

All chemicals were purchased from Sigma Aldrich. All dental resins and primers were purchased as shown in table 1.

Table 1. Commercial zirconia dental primers.

Primers	Composition <sup>1</sup>	Manufacturer
Zirconia liner (ZL)	4-META	SunMedical Co. Ltd (Japan)
Alloy primer (AP)	10-MDP, VBATDT	Kuraray Dental, Inc. (Japan)
Universal primer (UP)	MAC-10, MTU-6	Tokuyama Dental, Corp. (Japan)

<sup>1</sup> 4-META: 4-methacryloyloxy ethyl trimellitate anhydride; 10-MDP; 10-Methacryloyloxydecyl dihydrogen phosphate, VBATDT: 6-(4-Vinylbenzyl-n-propyl)amino-1,3,5-triazine-2,4-dithiol; MAC-10: 11-Methacryloylundecane-1,1- dicarboxylic acid; MTU-6: 6-methacryloyloxyhexyl-2-thiouracil-5-carboxylate

### 2.1. Synthesis of Catechol Methacrylate Primer

Triethyl silylane (TES)-protected (or silylated) catechol-methacrylate was synthesized from eugenol by the previously reported method [16] and generously provided to us by Osaka Organic Chemical Industry LTD (Japan). By modifying the previously reported conditions for TES-deprotection, the Catecholic Methacrylate could be obtained more economically, with a higher degree of purity according to the following procedure. 411 mg of TES-protected catechol methacrylate (0.855 mmol, 1 equiv.) and 229 mg of benzoic acid (1.88 mmol, 2.2 equiv., 1.1 equiv. per TES group) were dissolved in ca. 3-5 ml of Tetrahydrofuran (THF), (Note: Distilled/anhydrous THF was not used), and stirred at ambient temperature, whereupon a 1 M solution of Tetrabutylammonium fluoride (TBAF) in THF (1.88 ml, 1.88 mmol, 2.2 equiv.) was added dropwise to the stirred mixture. The mixture was stirred at ambient temperature until Thin-layer chromatography (TLC) indicates complete conversion (30-120 min). Once judged complete, the stir bar was removed, and THF was removed by rotary evaporation. The crude residue was then suspended in 150 ml of ether (Et<sub>2</sub>O), and washed twice with DI water, once with brine, dried over sodium sulfate. Once dry, the solution was filtered and evaporated under reduced pressure, whereupon the residue was dissolved in a minimum amount of DCM, loaded on top of a silica column, and purified further by flash chromatography. (Note: Catechols adhere strongly to silica, and are subject to decomposition during chromatography, thus chromatography was performed quickly, and with a minimum amount of silica gel. Oxidative decomposition during chromatography could be mitigated by addition of a small amount (0.1 % v/v) of AcOH to the eluent, although this required prolonged and undesirable amounts of time on high-vacuum to remove traces of acid. The use of silica gel impregnated with ascorbic acid was also found to reduce decomposition) [18]. After eluting sequentially with 0%, 25%, then 60% EtOAc/Hexanes, fractions containing desired material were then pooled in a round bottom flask, and a very small (ca. 0.1-0.4 mg) crystal of BHT as inhibitor was added, then the solution evaporated. A small quantity of DCM was used to transfer the residue to a small, tared vial, and residual volatiles were removed by repeated coevaporation of the residue with pentanes, followed by high vacuum, to afford 147 mg (68% of theoretical) of the title compound as a clear viscous oil. The material was stored in the freezer in glass vials tightly wrapped with parafilm, and protected from light.

The Catechol-Methacrylate primer solution was prepared as follows. First, Methanol was degassed by sparging with Argon for 15-30 minutes. The primer was removed by gently scraping some of the compound with a spatula, into a tared vial, which was then weighed, fitted with a rubber septa, and purged with argon. Sufficient degassed MeOH was then added via syringe to make a 1 mg/ml solution, the septa was then replaced with a screw cap, and the vial was vigorously vortexed for 10-20 minutes until no further primer could be observed adhering to the sides of the vial. Solutions were sealed tightly, protected from light, and stored in the freezer.



2.2. *Zirconia specimen*

A zirconia block for dental crown was cut using a water cooled diamond saw (Buehler Isomet Low Speed saw, model #11-1180, Buehler Ltd., Lake Bluff, IL) with a 0.15 mm thick diamond blade to 2 mm thickness and 5 mm x 5 mm width. All specimens were polished with sandpaper #1200 in order to have the same degree of roughness.

2.3. *Surface treatment*

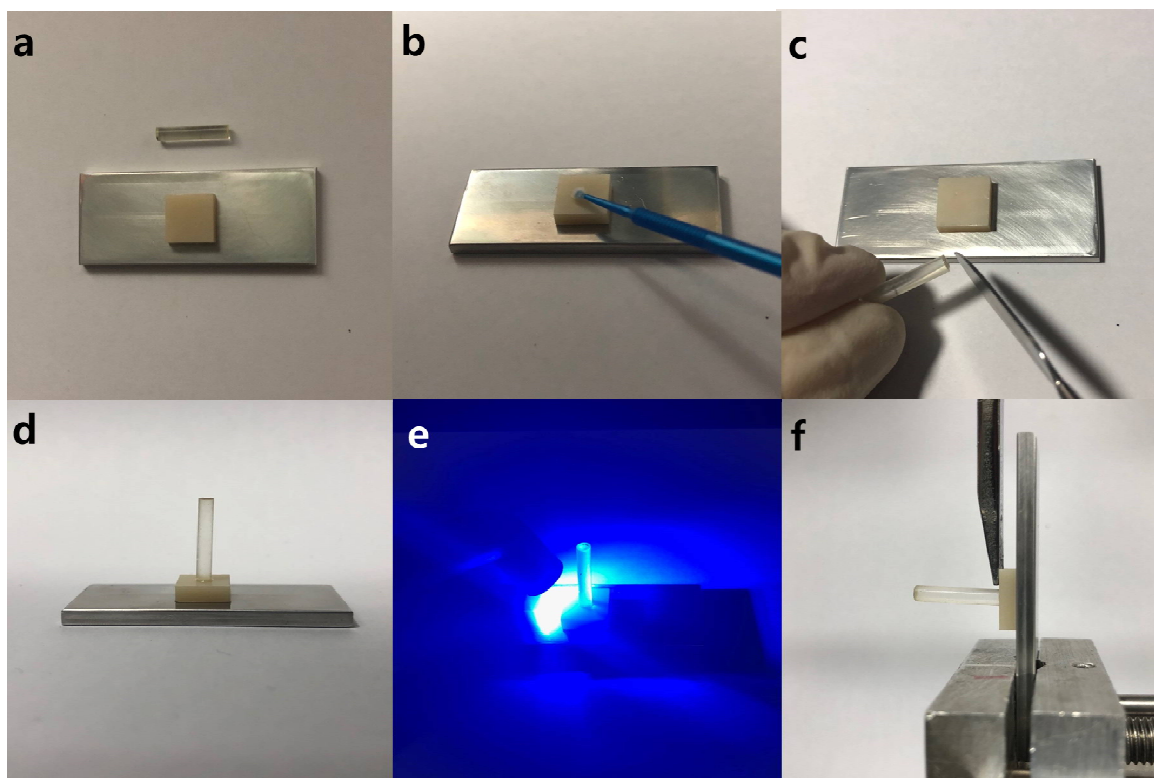
We divided specimens into 5 groups according to the types of used primers. Each group is ZL using Zirconia Liner, AP using Alloy Primer, UP using Universal Primer, CP using fresh Catechol primer (1 mg/mL methanol solution) [15], and Control (non-treated specimen). The primers were applied according to the manufacturer's instructions.

2.4. *Surface morphology*

SEM analysis was conducted for the primed (surface-coated with primers) and the non-primed zirconia surfaces. To prepare the primed samples, the commercial primers were applied on the surfaces as directed in the manuals provided by the manufacturers. Catechol primer solution was applied according to the previous report [15]. The surface images were collected using field emission scanning electron microscope (FESEM, Hitachi S-4700, Hitachi Co., Tokyo, Japan) at two different magnifications (x250, x1000).

2.5. *Knife-edge shear bond strength*

First, a cured dental resin rod 2.5 mm in diameter shown in Figure 2 was prepared using a common dental monomer mixture (49.5 wt.% of Bis-GMA, 49.5 wt. % of TEGDMA, and 1.0 wt. % of DMAEMA and CQ mixture at 1:2 molar ratio). The bottom of the rod was polished and leveled flat with #800 sandpaper. Dental resin cement (Bisco, IL, USA) was then applied onto the bottom surface of the rod (Figure 2 (c)) as to simulate the bottom of the resin. The rod was then placed on the primer-treated zirconia surface at orthogonal to the surface and lightly pushed (Figure 2 (d)). Subsequently, blue light (Demi™ Ultra Dental Curing Lights, Kavo Kerr, CA, USA) was applied all around surface for the complete cure for 20-40 seconds (Figure 2 (e)). All specimens were stored at room temperature for 1 day prior to strength testing. Knife-edge shear bond test was performed at crosshead down speed of 1 mm/min (Figure 2 (f)) by a universal testing machine (UTM 4465, Instron, MA, USA). Each test repeated 10 times (n = 10); average and standard deviation were calculated.

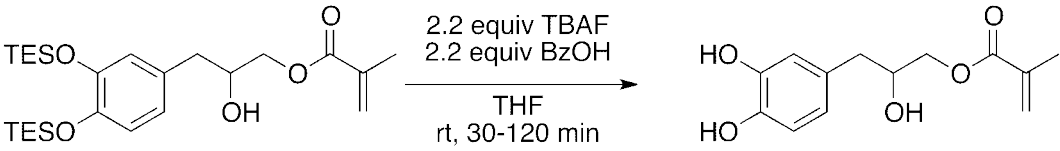


**Figure 2.** Images taken during sample preparation : (a) A zirconia sample adhered to a stainless-steel plate; (b) Apply primer solutions on the zirconia surface; (c) Dental resin cement applied to the bottom of resin rod; (d) The resin rod placed on the surface; (e) Light curing; (f) knife-edge shear bonding test.

### 3. Results and Discussion

#### 3.1. Improved synthesis of Catechol methacrylate primer

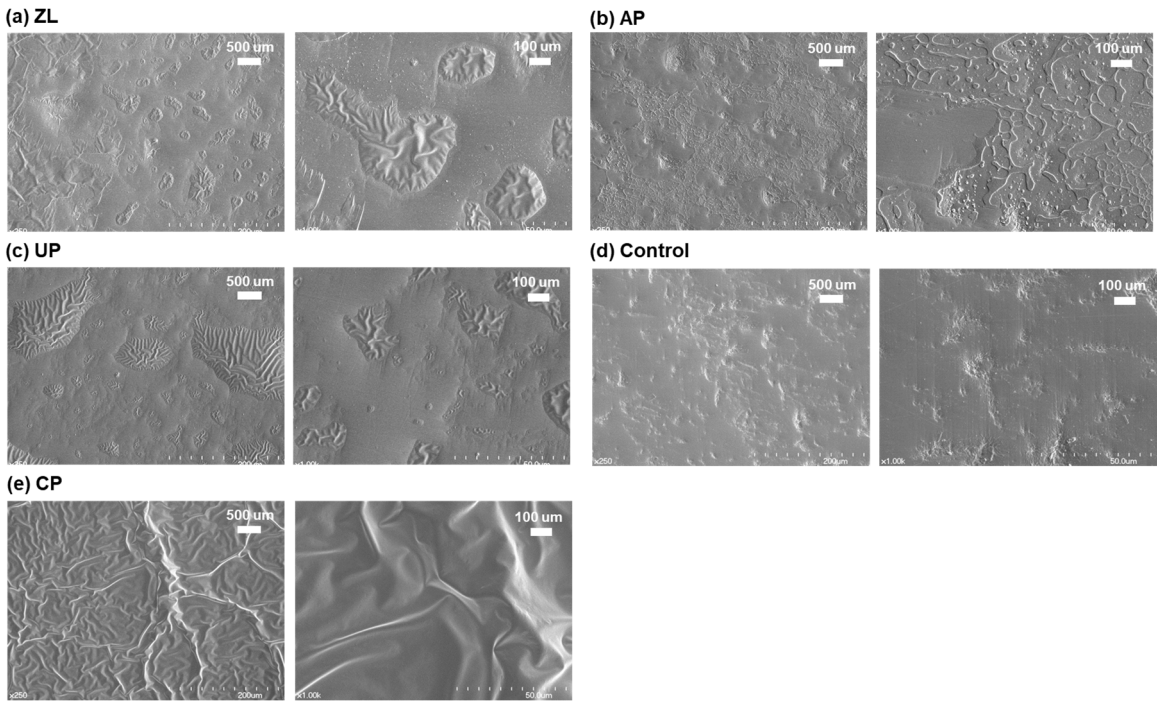
We had some concerns and encountered some difficulties with the previously reported TES-deprotection method [6]. The prior method involved the use of tetrabutylammonium fluoride (TBAF) as limiting reagent, and an excess of the more valuable TES-protected intermediate, the reaction apparently being driven to completion by reaction with adventitious water. Since the prior procedure required that TBAF be used without a buffer, phenolic groups are liable to stay ionized and in the aqueous phase without an acidic workup. Additionally, since the previous conditions are basic due to the use of fluoride anion; catechol moieties are susceptible to autooxidation, resulting in lower yields, yellow sample coloration, and baseline impurities. These basic conditions also apparently are the origin of the observed migration of some of the methacrylates to the internal site visible in the proton NMR. In this study, we have increased the yield, purity, and reproducibility of this silyl-deprotection by buffering the TBAF in the reaction mixture with an equimolar amount of benzoic acid (Scheme 1).



**Scheme 1.** Synthetic scheme of catechol methacrylate from silylated eugenol.

3.2.SEM imaging of primed zirconia surface

Surface morphology of zirconia surfaces with and without primer treatments was studied with a SEM (Figure 3). In the SEM study, CP containing catechol methacrylate shows a complete coverage of zirconia surface, whereas the commercial zirconia primers (ZL, AP and UP) containing phospho- and/or carboxyl- methacrylates show partial coating on zirconia surfaces. We predicted that higher surface coverage would be positively correlated with the adhesive performance of dental resins to zirconia surface, by allowing for a greater number of contacts between zirconia and resin, which was subsequently supported by the results of the shear bonding tests (*vide infra*).

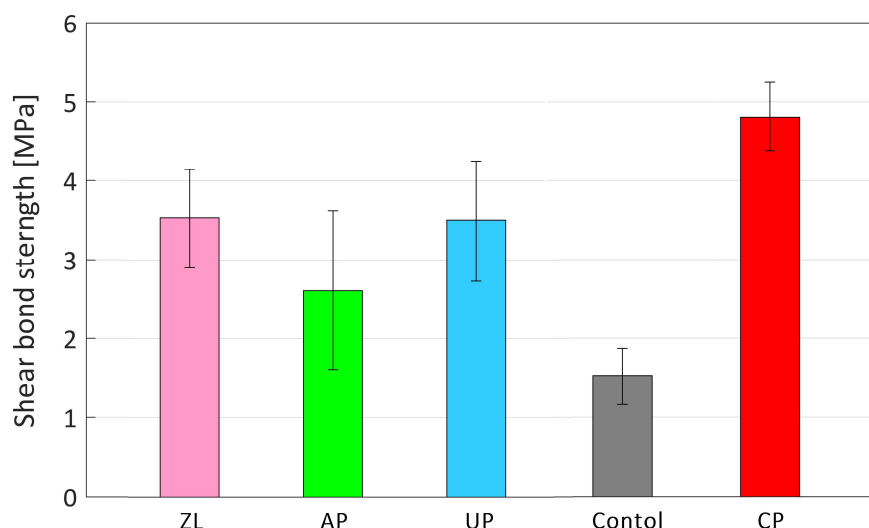


**Figure 3.** SEM images of zirconia surfaces primed with: (a) ZL: Zicornia Liner, (b) AP: Alloy Primer, (3) UP: Universal Primer, (d) Control: No primer, (e) CP: Catechol primer.

3.3. Shear bonding strength of dental adhesives on bioinspired catechol primed zirconica surface

Knife shear bonding test was conducted to measure bonding performance of dental adhesives on zirconia surface. The means, standard deviations of the knife-edge shear bond strengths are shown in Figure 4. With the complete surface coverage of CP on zirconia surface shown in SEM analysis in Figure 3, the shear

bonding of CP ( $4.81 \text{ MPa} \pm 0.43$ ,  $n = 10$ ; the mean of maximum shear strength,  $\pm$  as standard deviation, and the  $n$  is number of experiments) was higher than commercial zirconia primers containing phosphate and carboxylate methacrylates, i.e., ZL ( $3.52 \text{ MPa} \pm 1.01$ ,  $n = 10$ ), AP ( $2.61 \text{ MPa} \pm 0.76$ ,  $n = 10$ ) and UP ( $3.49 \text{ MPa} \pm 1.03$ ,  $n = 10$ ), and three times stronger than the control without any primer ( $1.52 \text{ MPa} \pm 0.35$ ,  $n = 10$ ). The statistical certainty of the comparison ( $p < 0.05$ ) was confirmed by the Student's  $t$ -test.



**Figure 4.** Knife shear bonding strength of ZL, AP, UP, Control (No primer) and CP.

#### 4. Conclusions

In this study, we were able to replicate one of the marine mussel's mechanisms of priming mineral surfaces by using a synthetic small molecule to prime zirconia surfaces. Our strategy of tethering of a polymerizable methacrylate to a catechol moiety was validated by superior bonding performance of our bioinspired primer to zirconia, relative to several popular commercially available formulations. SEM imaging shows that in contrast to those utilizing acidic monomers, the catecholic primer provides a much greater degree of surface coverage, which is correlated with the observed enhancement in dental bonding performance. Considering the catecholic primers' higher strength and ease of application, this priming strategy is well poised for further development in dental applications requiring bonding to zirconia.

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**Conflicts of Interest:** The authors declare no conflict of interest.

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