

1 *Review*2 **Targeting Early Dementia: Using Lipid Cubic-**
3 **Phase Nanocarriers to Cross the Blood-Brain Barrier**4 **Joseph S. D'Arrigo[†]**

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12 **ABSTRACT:** Over past decades, a frequent co-morbidity of cerebrovascular pathology
13 and Alzheimer's disease pathology has been observed. Numerous published studies
14 indicate that preservation of healthy cerebrovascular endothelium can be an important
15 therapeutic target. By incorporating appropriate drug(s) into biomimetic (lipid cubic-
16 phase) nanocarriers, one obtains a multitasking combination therapeutic which targets
17 certain cell-surface scavenger receptors, mainly class B type 1 (i.e., SR-BI), and crosses
18 the blood-brain barrier. This targeting allows for various Alzheimer's-related cell types to
19 be simultaneously searched out for localized drug treatment in vivo.

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23 **Keywords:** Alzheimer's disease; biomimetic nanocarriers; blood-brain barrier; dementia;
24 drug targeting; lipid cubic phases; nanoemulsion; SR-BI; scavenger receptors

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27 **Abbreviations:**

28

29 AcLDL acetylated LDL
30 ApoA-I apolipoprotein A-I
31 BBB blood-brain barrier
32 BCEC brain capillary endothelial cell(s)

33

34 CLA-1 (human ortholog of SR-BI)
35 DHA docosahexaenoic acid
36 *Fd3m* (micellar or discontinuous cubic-phase lipid structure)
37 GLUT glucose transporter protein

38

39 HDL high-density lipoprotein(s)
40 LCM lipid-coated microbubble(s)
41 LCM/ND lipid-coated microbubble/nanoparticle-derived
42 LDL low-density lipoprotein(s)

43

44 OxLDL oxidized LDL

45 RMT receptor-mediated transcytosis
46 SR-BI scavenger receptor(s), class B type I
47 VCID vascular cognitive impairment and dementia
48

49 **1. Introduction**

50 The fundamental involvement of the cerebrovasculature in the pathogenesis of common
51 dementias, widely reported in the biomedical literature, has recently been reviewed (e.g.
52 [1,2]). Small-vessel disease is commonly found in patients who have other brain
53 pathologies, such as the plaques and tangles associated with neurodegenerative disease;
54 small-vessel disease also increases the risk of Alzheimer's disease. Accordingly, vascular
55 cognitive impairment and dementia (VCID) is the second leading cause of dementia
56 behind Alzheimer's disease, and is a frequent co-morbidity in the Alzheimer's patient [3-
57 9]. On a worldwide basis, 47 million people had dementia in 2016; of these dementia
58 patients, 60%–80% have Alzheimer's disease [4,10,11].
59

60 **2. Central Role of Endothelial Dysfunction**

61 It has been reported repeatedly that *endothelial* modulation and repair is feasible by
62 pharmacological targeting [1,12-26] via SR-BI receptors (cf. [25]). As the detailed review
63 by Mahringer et al. [27] points out, the blood-brain barrier (BBB) is equipped with
64 several endocytic receptors at the luminal surface (i.e., the capillary endothelial
65 membrane), including the type BI scavenger receptor (SR-BI). Furthermore, very
66 recently published experimental work has demonstrated in detail [28] that high-density
67 lipoproteins (HDL), acting via scavenger receptors (class B type I, i.e., SR-BI), blocks β -
68 amyloid uptake into endothelial cells – in experimental monolayers as well as, the authors
69 argue, in the human cerebrovascular endothelium (cf. [29-31]).
70

71 Almer et al. [14] explain in their recent review that the integration of lipoprotein-related
72 or apolipoprotein-targeted nanoparticles, as drug carriers, is an expanding concept in
73 nanomedicine to exploit the intrinsic characteristics of lipoprotein particles as being the
74 natural transporter of lipophilic compounds in human circulation. Discrete lipoprotein
75 assemblies and lipoprotein-based biomimetics offer a versatile nanoparticle platform for
76 constructing drug loaded, reconstituted or artificial lipoprotein particles for specific

77 medical applications. As naturally occurring nanoassemblies, lipoprotein particles are not
78 readily (nor rapidly) cleared by the mononuclear phagocyte system (of the liver and
79 spleen) and remain in circulation for a longer period of time [14]. More recently,
80 Srimanee et al. [12] further explain that receptor-mediated transcytosis (RMT) at the
81 BBB occurs in three steps: 1) receptor-mediated endocytosis at luminal (capillary
82 endothelial lining/blood) side via the ligands (i.e., lipoprotein-related, apolipoprotein-
83 targeted nanoparticles) binding to specific membrane receptors (e.g., SR-BI); 2) transfer
84 of endocytic vesicles through the cytoplasm; 3) and exocytosis of the carried (small-
85 molecule or biomolecular) drug at the abluminal (brain/endothelial) side. Currently,
86 several receptors are known to be expressed on the luminal surface of the BBB, which
87 include scavenger receptors (such as SR-BI) [12]. Particularly, SR-BI was found in
88 bovine and porcine brain capillary endothelial cells (BCEC), and also expressed in
89 murine brain. The rodent SR-BI was studied and showed the same structure/(behavior) as
90 human SR-BI [12,13]. With regard to their own experimental work, Srimanee et al. report
91 that SR-BI are also involved (among several receptor types studied by their group) in the
92 uptake of nanocomplexes into brain endothelial cells, and also mediate the transport of
93 nanocomplexes across their BBB model [12]. Moreover, other published studies [13]
94 have shown that lipophilic compounds bound to HDL (and probably to “HDL-like”
95 nanoparticles as well) have the possibility to be internalized by a “piggy-back”-like
96 mechanism. It was shown that uptake of HDL-associated α -tocopherol by porcine BCEC
97 via SR-BI exceeded the uptake of HDL particles up to 13-fold, suggesting a selective
98 uptake of this compound without the concomitant internalization of the lipoprotein
99 (HDL) particle [13]. In addition, other work has demonstrated apolipoprotein (apo) A-I
100 expression in porcine brain capillaries. Further research indicated that apoA-I, the major
101 protein component of HDL, was effluxed by porcine BCEC (whereas aortic endothelium
102 did not efflux any detectable amount of apoA-I). ApoA-I-inducing compounds, such as
103 cholesterol, could upregulate apoA-I in BCEC. It was concluded these data together
104 indicate that at porcine BCEC, apoA-I is effluxed apparently by the SR-BI receptor [13].
105
106 Also, in 2017, Fung et al. [32] separately report that SR-BI mediates the uptake and
107 transcytosis of HDL across brain microvascular endothelial cells (i.e., across the blood-

108 brain barrier). The authors assert that elucidating the mechanisms of HDL transcytosis
109 across the BBB, in particular, may be significant pathologically as its constituent
110 apolipoprotein A-I has been demonstrated to confer a protective effect against
111 Alzheimer's disease. Using a combination of spinning-disc confocal and total-internal-
112 reflection fluorescence microscopy, these authors examined the internalization and
113 transcytosis of fluorescently labeled HDL by human primary brain microvascular
114 endothelial-cell monolayers. Using these approaches, these investigators reported that
115 HDL internalization requires dynamin, but not clathrin heavy chain, and that its
116 internalization and transcytosis are saturable. The authors conclude that these (and other
117 reported) findings indicate that HDL transcytosis across the blood-brain barrier involves
118 a signaling pathway downstream of SR-BI. These investigators further argue that
119 manipulation of HDL transcytosis across the BBB to increase delivery of plasma apoA-I
120 may, in turn, facilitate increasing the transport of “*HDL-like synthetic particles*”
121 containing therapeutic drug across the BBB to treat neurodegenerative disorders such as
122 Alzheimer's disease [32] (cf. [28,33-42]).

123

124 **3. Targeted Drug Treatment for Early Dementia**

125 This targeted-drug-delivery approach, using an apoA-I-based (SR-BI mediated)
126 therapeutic agent for treating the more common (late-onset) dementias, receives added
127 impetus from continual findings of cerebrovascular pathology [1,43–53] and an apparent
128 *endothelium*-dysfunction [2,33–41,49,54–60] in both Alzheimer's disease and its major
129 risk factors [1,2,53–72]. By incorporating drug candidates (such as Edaravone, DHA, or
130 antibody therapeutics) into the “lipid-coated microbubble/nanoparticle-derived”
131 (LCM/ND) lipid nanoemulsion type (yielding particle sizes mostly < 0.1 μm in diameter),
132 known to be a successful drug carrier [73,74], one is likely to obtain a multitasking
133 combination therapeutic capable of targeting cell-surface SR-BI. This combination
134 therapeutic would make it possible for various cell types, all potentially implicated in
135 Alzheimer's disease (cf. [71,72]), to be simultaneously sought out and better reached for
136 localized drug treatment of brain tissue *in vivo*.

137

138 With regard to receptor-mediated membrane transport across the BBB, brain
139 microvascular endothelial cells are believed to control iron uptake and efflux, under the
140 direct guidance of neighboring astrocytes [75,76]. Detailed evidence has been reported
141 recently [75] showing that human brain microvascular endothelial cells, which constitute
142 most of the blood-brain barrier, receive brain-iron status information via paracrine signals
143 from ensheathing astrocytes. Lastly, aging, obesity, and smoking are significant
144 determinants of brain iron accumulation in human subjects [77] and all have been long-
145 associated with Alzheimer's disease incidence [25,50-52,54,55,65,78-80].

146

147 Note that the above-mentioned (cf. preceding paragraph) long association of specifically
148 both obesity and diabetes with Alzheimer's disease incidence has also renewed attention
149 to the brain's main facilitative glucose transporter protein, GLUT-1, involvement in and
150 probable contribution to neurodegenerative diseases [81-83]. More than two decades ago
151 it was already recognized that normal human-brain capillary endothelium has a high
152 density of GLUT-1, whereas the cerebral microvessels in subjects with Alzheimer's
153 disease showed a markedly decreased GLUT-1 density when compared with age-matched
154 controls [84,85]. More recently, Winkler et al. [86] demonstrated that GLUT-1 deficiency
155 in cerebral endothelium (but not in astrocytes), in a mouse model of Alzheimer's disease,
156 initiates blood-brain barrier breakdown. These authors observed from their detailed
157 experiments that reduced GLUT-1 expression (at the BBB) worsens Alzheimer's disease
158 cerebrovascular degeneration, neuropathology, and cognitive function – suggesting that
159 (cerebral endothelial) GLUT-1 may represent a therapeutic target for Alzheimer's disease
160 vasculo-neuronal dysfunction and degeneration [86]. Further, other investigators [87] (cf.
161 [88]) have recently provided evidence for brain glucose dysregulation as a critical event
162 in Alzheimer's disease pathogenesis that closely reflects both the severity of Alzheimer's
163 disease pathology and the expression of symptoms. Moreover, abnormalities in brain
164 glucose homeostasis may begin several years before the onset of clinical symptoms [87].

165

166 In summary, endothelial cells are the main component of the BBB, which is seriously
167 disrupted in various neurological pathologies – including many neurodegenerative
168 disorders [89-91]. An early BBB breakdown and/or dysfunction has been documented

169 [92] in Alzheimer's disease before dementia, neurodegeneration, and/or brain atrophy
170 occur, and investigators have reported that targeting the BBB can influence the course of
171 neurological disorder [92]. Hence, vascular-targeted therapies become plausible for the
172 prevention and treatment of common dementias [4,36,89,93-95]. In respect to vascular
173 tone, vasodilators (nitric oxide, acetylcholine) are repressed while vasoconstrictor
174 (endothelin-1) is enhanced, thus contributing to endothelial dysfunction in Alzheimer's
175 disease [90,96]. Also, β -amyloid can induce apoptosis and/or necrosis of brain
176 endothelial cells. Presence of β -amyloid, as well as tau protein oligomers, leads to
177 accumulation of inflammatory molecules in microvessels – which further fosters
178 endothelial dysfunction [90,97-99]. Other component cell types of the neurovascular unit
179 are affected as well in Alzheimer's disease [90]. For example, deposition and aggregation
180 of β -amyloid within vascular smooth muscle cells leads to inflammation, oxidative stress,
181 impaired vasorelaxation, and disruption of BBB integrity. At the same time, midlife
182 vascular-risk factors such as hypertension, cardiovascular disease, diabetes, dyslipidemia,
183 and obesity all increase the relative risk for Alzheimer's disease [89,100-103]. These co-
184 morbidities are all characterized by low and/or dysfunctional HDL, which itself is an
185 Alzheimer's risk factor. Namely, (in addition to long-published lipid transport,) HDL
186 regulates vascular health via modulating vasorelaxation, inflammation, and oxidative
187 stress as well as promoting endothelial cell survival and integrity [36,102,104]. Since SR-
188 BI has already been identified as a major receptor for HDL (with their major
189 apolipoprotein (apo)A-I) as well as for the earlier-described LCM/ND nanoemulsion
190 [1,2], this multitasking lipid nanoemulsion can arguably serve as a targeted, apoA-I-
191 based, (SR-BI mediated) therapeutic agent for common (late-onset) dementias (cf.
192 [28,33,35,37-42]). In this particular targeted-delivery approach, the self-assembled HDL-
193 related “lipid nanoemulsion particle” structure itself (after i.v. injection) likely binds to
194 apoA-I in the blood plasma; subsequently, such apo A-I-targeted LCM/ND nanoemulsion
195 particles are recognized by SR-BI receptors on various Alzheimer's-related cell types
196 [73].

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199

200 **4. LCM/ND Nanoemulsion Type contains Lipid Cubic-Phase Nanocarriers**

201 The self-assembling LCM/ND lipid nanoemulsion class comprises nonionic lipids
202 exclusively (cf. [105,106]) throughout its coated microbubble's and/or related
203 nanoparticle's (i.e., related lipid polymorphs') supramolecular structures(s). This biobased
204 lipid composition of LCM/ND nanoemulsions (i.e., glycerides and cholesterol
205 compounds) is similar to lipids contained in several types of plasma lipoproteins;
206 accordingly, when these LCM/ND nanoemulsion particles are injected into the
207 bloodstream, they likely acquire (i.e., bind) plasma apolipoprotein(s) – including notably
208 apoA-I [73]. Hence, the molecular composition of the LCM/ND nanoemulsion particles
209 resulted in both microbubble/nanoparticle stability and marked targeting toward tumors
210 and certain hyperproliferative-disease lesions/sites; this very rapid targeting has been
211 demonstrated to occur by an “active uptake” process, i.e., “endocytosis” – which likely
212 involves certain “lipoprotein receptor”-mediated endocytic pathways [2].

213

214 The collection of powdered solid lipid surfactants used to produce the LCM/ND lipid
215 nanoemulsions, which is described with all structural details of the molecular components
216 in the published patents covering this technology [105,106], can be outlined as
217 comprising the following:

- 218 **a.** “a member selected from the group consisting of glycerol monoesters of saturated
219 carboxylic acids containing from about 10 to about 18 carbon atoms ... ;
- 220 **b.** a sterol aromatic ester;
- 221 **c.** a member selected from the group consisting of sterols ... ;
- 222 **d.** a member selected from the group consisting of sterol esters of aliphatic acids
223 containing from one to about 18 carbon atoms; ... and
- 224 **e.** a member selected from the group consisting of glycerol, glycerol di-, or triesters
225 of aliphatic acids containing from about 10 to about 18 carbon atoms ...”.

226 “The surfactant mixture of the present invention can be readily prepared by admixing
227 components a through e in a weight ratio a:b:c:d:e of 2-4:0.5-1.5:0.5-1.5:0-1.5:0-1.5,
228 respectively. Preferably, ... the components of the surfactant mixture of the present
229 invention are combined in a weight ratio a:b:c:d:e of 2-4:1:1:1:1. Since each of the
230 components of the surfactant mixture of the present invention is a dry powder, the

231 resultant admixture is conveniently obtained in a dry powdered form.” In a particularly
232 preferred form (i.e., “Example 1”) of the invention, the “surfactant mixture” was prepared
233 in accordance with the present invention by admixing glycerol monolaurate, cholesterol
234 benzoate, cholesterol, cholesterol acetate, and glycerol tripalmitate in a weight ratio of
235 3:1:1:1:1, respectively, to obtain a dry powdery surfactant mixture” [105,106].

236

237 Importantly, monoglyceride is the largest single-lipid fraction (by wt. %) of the powdered
238 solid lipid surfactants used to produce the (Filmix®) LCM/ND nanoemulsions [73]. As a
239 group, monoglycerides exhibit different phase behaviors when they are exposed to water
240 [107] (cf. [108,109]). The ability to exist in several different phases is an important
241 property of pure lipids and lipid mixtures; it depends upon temperature, hydration, and
242 lipid class [107]. Although monoglycerides typically have poor water solubility, they
243 have free hydroxyl groups which can hydrogen bond with water, surfactants, cosolvents,
244 etc. As polar lipids, monoglycerides typically: (1) are better solvents for drugs; (2) act as
245 “cosurfactants” which promote mutual solubility between excipients (i.e., inactive
246 ingredients); (3) enhance water uptake; and (4) promote self-dispersibility of lipid
247 formulations [110]. The above properties of monoglycerides place them in a lipid class
248 known as “insoluble swelling amphiphiles”. These lipid molecules form stable
249 monolayers (at the air/water interface), but also swell in water to form liquid-crystalline
250 phases [111]. In their detailed review, Kaasgaard and Drummond [112] explain that these
251 lyotropic (i.e., solvent induced) liquid-crystalline phases of monoglycerides include the
252 one-dimensional lamellar phase, which has been widely studied and employed as a model
253 system for biomembranes and drug-delivery applications. More recently studied are the
254 structurally more complex two- and three-dimensional ordered (lyotropic) liquid-
255 crystalline phases, of which inverse hexagonal and cubic phases are two prominent
256 examples. In agreement with numerous other investigators, Kaasgaard and Drummond
257 also state that all these types of liquid-crystalline phases are frequently stable in excess
258 water, which facilitates the preparation of nanoparticle dispersions and makes them
259 suitable candidates for the encapsulation and controlled release of drugs ([112]; cf. [113-
260 119]).

261

262 In the “preferred form” of the LCM/ND nanoemulsion formulations (cf. [105,106]), the
263 monoglyceride content employed consists entirely of the saturated variety. Using only
264 saturated monoglyceride in such nanoemulsion formulations carries an additional benefit.
265 Namely, saturated fatty chains (i.e., saturated acyl groups) are advantageous because they
266 are incapable of undergoing peroxidation reactions, which would lessen the acceptable
267 storage life (cf. [120]) of these (“oil-in-water”) nanoemulsions.

268

269 The self-assembly of varied and useful *dispersed cubic* phases (among other liquid-
270 crystalline phases) depends heavily on the acyl chain length of the glycerides (primarily
271 monoglycerides) placed in contact with water [73]. As Yaghmur et al. [119] point out, the
272 significant interest in the formulation and the characterization of these complex and
273 varied, self-assembled, liquid-crystalline *cubic* phases is driven by both fundamental and
274 practical considerations: They offer many advantages compared to conventional
275 dispersed systems (such as simple emulsions or double emulsions) because of their
276 confined equilibrium nanostructures with high interfacial area, their low viscosity, and
277 their capabilities to solubilize a wide variety of active molecules. Therefore, there is great
278 interest to utilize these *dispersed cubic* phases for the administration of drugs, or for the
279 formulation of new delivery systems [119].

280

281 The (lyotropic) *cubic* liquid-crystalline phases may be classified into two distinct classes:
282 *bicontinuous cubic phases and micellar or discontinuous* (e.g., type *Fd3m*) cubic phases.
283 [Representative illustrations (under copyright), including suitable micrographs, of these
284 dispersed cubic phases can be found in [107, 112, 114, 121-124].]As Abraham et al.
285 [125] explain, two alternate structural representations have been utilized to describe the
286 bicontinuous cubic phases, one in terms of rodlike elements and the other in terms of
287 folded surfaces, that is, infinite periodic minimal surfaces (IPMS). (Alternatively, the
288 representations in terms of nodal surfaces have been used to describe the dynamic
289 structure of cubic phases.) Three different “inverse bicontinuous” cubic lipid phases have
290 been observed experimentally, having the symmetry *Pn3m*, *Ia3d*, and *Im3m* –
291 corresponding to the following IPMS: the diamond type (D-surface), the gyroid type (G-
292 type), and the primitive type (P-surface), respectively [125]. As reviewed by Garg et al.

293 [107], monoglycerides spontaneously form bicontinuous cubic phases upon the addition
294 of water, are relatively insoluble (allowing the formation of colloidal dispersions of cubic
295 phases, and are resistant to changes in temperature. Accordingly, lipid nanoparticles
296 comprising interior liquid-crystalline structures of curved lipid membranes (i.e., dispersed
297 cubic phases) have been used to solubilize, encapsulate, and deliver medications to
298 disease areas within the body [107].

299

300 Besides certain glyceride-based liquid-crystalline systems displaying colloidal stability in
301 excess water, the same important attribute has been documented for cholesterol and
302 cholesterol esters – all of which are present in LCM/ND nanoemulsion formulations [73].
303 For example, cholesterol and its esters change the packing structure of lipids, and in high
304 concentrations they are known to induce the formation of a liquid-crystal phase [120]. In
305 addition, Kuntsche et al. [126,127] have prepared lipid nanoparticles in the (mesomorphic
306 or) liquid-crystalline phase from cholesterol esters with saturated acyl chains. These
307 investigators were motivated by the knowledge that many cholesterol esters are
308 physiologic lipid compounds which can form liquid-crystalline phases (thermotropic
309 mesophases) and, hence, they were interested in their potential for the development of
310 liquid-crystalline nanoparticles as a carrier system for lipophilic drugs [127]. In accord
311 with the above observations and considerations, the substantial concentrations of
312 cholesterol esters and cholesterol in the LCM/ND nanoemulsion formulation likely
313 further contribute to the known long-term stability of this nanoemulsion's (liquid-
314 crystalline) lipid nanoparticles in excess water, thereby providing a persistent carrier
315 matrix upon exposure to liquids such as blood plasma [73].

316

317 **5. Promising Developments regarding Supplementary Neurotherapy using Targeted** 318 **Sonoporation**

319 A completely separate advantage of such LCM/ND (drug-delivery) nanoemulsion(s)
320 stems from the characteristic lipid-coated microbubble (LCM) subpopulation existing in
321 this nanoemulsion type [1,2,73]. Over the past decade, neuroscientists have been
322 exploring the use of ultrasound in combination with preformed (intravenous)
323 microbubbles to temporarily open the BBB (cf. [128-149]), allowing drugs or the

324 immune system to target brain tumors or Alzheimer's brain plaque in vivo effectively,
325 repeatedly, and safely [150-156] in animals up to primates [150,157] and even in humans
326 [157]. It is worth noting that this proposed mechanism of plaque-burden reduction, by
327 sonoporation (i.e., "loosening the tight junctions of the cells forming the BBB" via
328 ultrasound irradiation [158,159]), might carry an additional effect. (Microbubble-
329 assisted) sonoporation not only facilitates localized delivery of drugs and/or "activated"
330 immune cells to target Alzheimer's brain plaque in vivo [158], but *also facilitates*
331 *(passive-transport?) reduction* of β -amyloid plaque burden from brain tissue in a mouse
332 model of Alzheimer's disease [160]. Specifically, this same mechanism might also
333 function to *counteract* characteristic *decreased "brain clearance"* of neurotoxic β -
334 amyloid "monomer" [160]– which has been described as a central event in the
335 pathogenesis of Alzheimer's disease (cf. [1,2,161]).

336

337 The actual cellular and biophysical mechanisms of the reversible BBB "opening" process
338 by sonoporation, when employing focused *transcranial* ultrasound coupled with injected
339 preformed microbubbles, have been described further in other published studies over the
340 last several years [1,162-168]. [Also, representative illustrations (under copyright)
341 picturing such opening of the BBB, by postulated loosening of tight junctions (and other
342 mechanisms), can be found in [141,164].] In the foreseeable future, taking full advantage
343 of this ongoing, noninvasive, and targeted use of preformed (such as LCM/ND
344 nanoemulsion-based) microbubbles to transiently and reversibly increase BBB
345 permeability via sonoporation, while optimizing drug-delivery efficiency (through
346 judicious choice of acoustic parameters [152,156]) and minimizing side effects, may
347 assist in advancing transcranial sonoporation to the clinic (cf. [1,167-182]).

348

349 **6. LCM/ND Nanoemulsion Particles function as Biomimetic Cubic-Phase**

350 **Nanotransporters**

351 As alluded to in Sect. 4 (cf. its first paragraph), the previously documented similarities in
352 lipid composition among HDL (as well as native LDL and modified LDL) and LCM/ND
353 nanoemulsion particles can partially simulate or mimic the known heterogeneity (i.e.,
354 subpopulations or subspecies) of HDL particles (see [73] for a review). Moreover, the

355 above-described type BI scavenger receptor (i.e., either SR-BI (rodent) and/or CLA-1
356 (human) orthologs [29]) has been shown to be a multifunctional receptor able to bind a
357 broad variety of ligands, including HDL, LDL, OxLDL, AcLDL, VLDL, and
358 chylomicron remnants [183-185]. The presence of amphipathic helices is a common
359 feature of “exchangeable apolipoproteins”, which are known to be the primary ligands
360 (including notably apoA-I) for SR-BI [183].

361

362 One example of a *reconstituted (biomimetic) lipoprotein* complex utilizing the SR-BI
363 cell-surface receptor, in the research literature, concerns manufactured (lipid) emulsions
364 which were designed to mimic chylomicrons in vivo, and therefore were expected to
365 acquire apolipoproteins upon incubation with serum [186]. The experimental data
366 obtained led investigators to conclude that SR-BI is clearly involved in facilitating
367 chylomicron (remnant) metabolism, and might function as an initial recognition site for
368 chylomicron remnants [185]. Note that in this example, the “reconstituted lipoprotein
369 vehicle” was at first constructed solely of lipids, that is, apolipoprotein(s) (needed for
370 targeting) were acquired only after incubation with serum. This concept of a pure-lipid
371 nanocarrier, which can successfully acquire apolipoprotein(s) upon contact with blood
372 plasma, is similarly described elsewhere in the literature. For example, Williams and
373 Scanu report that phosphoglyceride liposomes, injected intravenously, pick up
374 endogenous apoA-I; in vitro, phosphoglyceride liposomes incubated with plasma acquire
375 apoA-I at the expense of HDL [73,187] (cf. [188]). [Explanatory illustrations (under
376 copyright) picturing the apoA-I chemical structure, the apoA-I conformation on discoidal
377 and spherical HDL particles, and their relative sizes can be found in [189].]

378

379 To conclude, self-assembled (colloidal mesophase) lipid nanoemulsions (e.g., [190-195]),
380 particularly those predominantly containing dispersed cubic-phase lipid nanoparticles
381 (e.g., [196-200]), continue to receive growing attention in pharmaceutical and/or
382 biological fields. The main reason behind much of this attention is the fact that
383 nonlamellar lipid nanostructures, such as cubic liquid-crystalline phases, have wide
384 potential as delivery systems for numerous drugs, cosmetics, and food applications (e.g.,
385 [201-203]). Namely, using various lipids and their mixtures to form self-assembled non-

386 lamellar nanostructures, it has continually been reported possible to successfully obtain
387 stable colloidal dispersions of (liquid-crystalline) lipid cubic phases with well-defined
388 particle size and morphology (e.g., [202,203]). In particular, within the range of self-
389 assembled phases in model surfactant-like lipid systems, Yaghmur et al. [204] further
390 emphasized that the monoglyceride-based lyotropic liquid-crystalline phases are
391 relatively unique owing to their rich polymorphism in water and potential application as
392 drug nanocarriers (cf. [205] and Sect. 4 above). A recurring example of a largely
393 monoglyceride-based drug-delivery agent category (cf. Sections 4-6) is the multitasking
394 LCM/ND nanoemulsion formulation. In this particular targeted-delivery approach, the
395 self-assembled “lipid particle” structure itself (upon intravenous injection of the
396 LCM/ND nanoemulsion) is apparently successfully utilized as the “active” targeting
397 ligand – which is directed via (adsorption of) plasma lipoproteins toward the appropriate
398 receptors on the target-cell surface. These dispersed liquid-crystalline lipid particles, of
399 the LCM/ND nanoemulsion formulation, are colloiddally stable nanocarriers which very
400 likely represent liquid-crystalline inverse-topology nanotransporters (nanocarriers), i.e.,
401 dispersed lipid cubic phases (cf. [73]).

402

403 **7. Conclusion**The proposed multitasking combination therapeutic appears likely to
404 display greater efficacy at different stages of Alzheimer's disease (cf. [72]). Furthermore,
405 the effects on various cell types targeted may be additive, multiplicative, or otherwise
406 synergistic [26]. As a result, this multitasking (drug-delivery) therapeutic could represent
407 a promising way to treat, delay, or even prevent the disease in the future [1,2]. In
408 particular, the LCM/ND (lipid) nanoemulsion particles have a composition (consisting of
409 various glycerides, cholesterol, and cholesterol esters) similar to lipids contained in
410 several plasma lipoproteins (i.e., resembles the lipid content of a “generic” lipoprotein
411 [184,190]). Accordingly, when this specific nanoemulsion type is injected intravenously,
412 its colloiddally-stable lipid particles apparently acquire apolipoprotein A-I from the plasma
413 and, subsequently, can be recognized by and bind to certain lipoprotein receptors
414 (predominantly SR-BI) on various Alzheimer's-related cell types.

415

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421

422

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