

Review

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Review

Pharmacoscintigraphy: Advancing Nanotheranostic Development through Radionuclide Imaging

María Jimena Salgueiro^{1,2,*}, Marcela Moretton^{2,3,4}, Vanina Medina^{3,5}, Diego Chiappetta^{2,3,4} and Marcela Zubillaga^{1,2,3}

¹ Universidad de Buenos Aires, Facultad de Farmacia y Bioquímica, Cátedra de Física, Buenos Aires, Argentina.

² Universidad de Buenos Aires, Instituto de Tecnología Farmacéutica y Biofarmacia (InTecFyB), Buenos Aires, Argentina

³ Consejo Nacional de Investigaciones Científicas y Técnicas (CONICET), Buenos Aires, Argentina

⁴ Universidad de Buenos Aires, Facultad de Farmacia y Bioquímica, Cátedra de Tecnología Farmacéutica I, Buenos Aires, Argentina

⁵ Laboratory of Tumor Biology and Inflammation, Biomedical Research Institute (BIOMED), Faculty of Medical Sciences, Pontifical Catholic University of Argentina (UCA-CONICET), Buenos Aires, Argentina

* Correspondence: jsalgueiro@ffyb.uba.ar

Abstract: Pharmascintigraphy has emerged as an essential tool in the research and development of nanomedicines, particularly in the field of nanotheranostics. By enabling real-time, non-invasive tracking of their biodistribution, pharmacokinetics, and therapeutic efficacy, these imaging techniques provide invaluable insights that drive the optimization of nanomedicine formulations. The integration of gamma scintigraphy, SPECT, and PET imaging has significantly enhanced our understanding of nanocarrier behavior, supporting their clinical translation by ensuring precise targeting, minimizing off-target effects, and improving therapeutic outcomes. Future advancements in hybrid imaging modalities, novel radionuclide tracers, and personalized imaging-guided therapies will further expand the impact of pharmacoscintigraphy in nanomedicine. Additionally, the increasing recognition of imaging-based validation in regulatory approval processes underscores the growing importance of these techniques in drug development. As nanotheranostics continue to evolve, radionuclide imaging will remain a pivotal component in their preclinical and clinical evaluation, facilitating safer and more effective precision medicine approaches.

Keywords: pharmacoscintigraphy; radionuclide imaging; nanotheranostics; gamma scintigraphy; SPECT imaging; PET imaging; radiolabeled nanomedicine; drug delivery systems; molecular imaging; nanomedicine

1. Introduction

The evolution of nanomedicine from its inception to its application in diagnostics and therapy can be summarized in several key stages [1–35]. Foundation and Theoretical Concepts of nanotechnology were first introduced by physicist Richard Feynman in 1959. His ideas laid the groundwork for manipulating matter at the atomic level. In the early 1980s, Nadrian Seeman pioneered the field of DNA nanotechnology, proposing the use of nucleic acids to construct complex nanostructures. Technological Advancements during the 1990s in materials science and biotechnology facilitated the development of nanomaterials. Researchers began exploring the unique properties of nanoparticles, such as increased surface area and reactivity, which could be harnessed for medical applications including targeted drug delivery and their ability to improve the solubility and bioavailability of drugs. The early 2000s marked a period of significant investment and interest in nanomedicine. The U.S. government prioritized nanotechnology through initiatives like the

National Nanotechnology Initiative, funded by the 21st Century Nanotechnology Research and Development Act. Researchers developed innovative nanocarriers designed to deliver therapeutic agents more effectively to target sites, such as tumors, while minimizing systemic toxicity; this was achieved by engineering nanoparticles with specific ligands or antibodies that could bind to tumor-specific receptors. This represented a critical advancement in improving the efficacy of traditional chemotherapy and radiotherapy. Concurrently, nanotechnology enabled the creation of highly sensitive diagnostic tools, including nanobiosensors and nanodevices. These tools significantly improved disease detection, monitoring, and biomarker identification, allowing for earlier and more accurate diagnosis. Nanoparticles were used as contrast agents in imaging modalities like MRI and CT scans, enhancing the sensitivity and resolution of tumor detection. For instance, dendrimers and gold nanoparticles were explored for their imaging capabilities, showing compatibility with biological systems. The term "nanotheranostics" emerged in the early 2000s as a combination of "nano," referring to nanoscale materials, and "theranostics," which is a portmanteau of "therapy" and "diagnostics." The concept signifies the integration of therapeutic and diagnostic functions into a single system, utilizing nanoparticles and nanomaterials. It represents an innovative approach that utilizes nanotechnology to simultaneously diagnose and treat diseases, particularly in the field of cancer. This dual capability of simultaneous diagnosis and therapy not only enhances the precision of medical interventions but also offers improved personalization of treatment strategies, making nanotheranostics a promising area of research and application in modern medicine. As nanomedicine technologies matured, a variety of nanopharmaceuticals and diagnostic products entered clinical trials. Some of these products have obtained regulatory approvals and are now commercially available, demonstrating real-world applications in medical settings. Through these stages, nanomedicine has transitioned from theoretical concepts and laboratory research to practical applications in diagnostics and therapy, showcasing its potential to revolutionize healthcare. Overall, the journey from early research to the current applications of nanomedicine in cancer diagnosis and therapy demonstrates a continuous evolution from non-targeting to targeting, from simple materials to mixed systems, and from single to combined technologies driven by interdisciplinary collaboration and technological advancements, with a focus on improving patient outcomes and precision medicine.

2. Contribution of Radioisotopic Imaging Techniques to Nanomedicine

Imaging techniques, particularly radioisotopic methods, play a crucial role in the development of nanomedicine and nanotheranostics and their contributions are multifaceted since they are instrumental during preclinical and clinical trials to evaluate the safety and efficacy of new nanomedicine therapies. They help in determining optimal dosages, understanding pharmacokinetics, and monitoring tumor responses [36–39].

By tagging nanoparticles with radioisotopes, researchers can track their distribution and localization *in vivo*. Radioisotopic imaging techniques, such as Positron Emission Tomography (PET) and Single Photon Emission Computed Tomography (SPECT), allow for non-invasive real-time monitoring of agents within the body which is essential for assessing the efficacy of nanotherapeutics in targeting specific tissues or tumors thus enabling adjustments in therapy based on the observed effectiveness [40–42]. This capability is crucial for personalized medicine, where treatment protocols can be dynamically adapted to individual patient responses. Understanding the biodistribution, metabolism and excretion of nanomedicines helps optimize their design and functionality, ensuring that the agents are delivered precisely where needed, thereby minimizing systemic side effects. In the context of nanotheranostics, radioisotopic imaging allows for the evaluation of how effectively nanoparticles target tumor sites. By tracking the accumulation of radiolabeled nanoparticles in tumors, clinicians can assess treatment responses and adjust therapeutic strategies accordingly. On the other hand, certain nanotheranostic platforms utilize radioisotopes not only for imaging but also for therapeutic purposes. This approach involves delivering radiation directly to tumor cells while monitoring the treatment's impact through imaging techniques, combining therapy and diagnostics

effectively [43–49]. The application of radioisotopic imaging in nanomedicine is prominent in oncology, where it aids in the diagnosis and treatment of various cancers. Furthermore, these imaging techniques are also being explored in other fields, such as cardiovascular disease, neurology, and infection management [50]. They facilitate understanding disease mechanisms and evaluating new treatment approaches. In summary, radioisotopic imaging techniques significantly contribute to the advancement of nanomedicine and nanotheranostics by enhancing diagnostic precision, enabling real-time therapeutic monitoring, optimizing targeted drug delivery, and facilitating innovative treatment strategies across multiple medical disciplines.

Pharmacoscintigraphy (Figure 1) is a term that encompasses radioisotopic imaging techniques, including planar gamma imaging, SPECT, and PET, to denote their specific role and application in pharmacological research. In this article, we will use this term to broadly refer to this specialized field, highlighting its role in the investigation and development of nanotheranostics [51–53].

Pharmacoscintigraphy in the pipeline of nanotheranostics research



Figure 1. The diagram outlines key stages of pharmacoscintigraphy in the research pipeline of nanotheranostics.

As personalized medicine gains prominence, pharmacoscintigraphy contributes to the development of tailored therapies by elucidating individual patient responses to different formulations. The integration of radionuclide tagging into pharmacoscintigraphy thus boosts nanotheranostics research by ensuring efficacy, safety, and compliance with regulatory standards, ultimately leading to improved therapeutic outcomes.

3. Pharmacoscintigraphy in the Development of Nanotheranostics

The principles of scintigraphy involve the use of radioactive materials to visualize biological processes in vivo (Figure 2). These substances are administered to a subject and then localize in specific tissues based on their chemical properties and physiological interactions. When the radioactive isotope decays, it emits radiation. These gamma rays are what scintigraphy detects. Scintigraphy involves specialized detection systems which are designed to capture the emitted radiation from the radioactive material within a living body. The light produced by the interaction of radiation with the scintillation crystals is then converted into electrical signals, which are processed to create an image. These images reflect the distribution and concentration of the radioactive material, indicating how organs function rather than merely their anatomical structure. Unlike conventional imaging techniques that primarily focus on anatomical details (such as X-rays or MRI), scintigraphy provides functional imaging. It allows researchers and clinicians to assess physiological functions such as blood flow, metabolic activity, and organ perfusion. Scintigraphy can produce both two-dimensional and three-dimensional images. This multidimensional capability allows for more

detailed analysis of organ function and pathology. Advanced data processing techniques allow quantitative analysis of the images, enabling researchers and clinicians to measure various parameters related to drug biodistribution and PK, such as uptake rate and elimination half-life providing significant insights into physiological processes [54].

What is pharmacoscintigraphy?

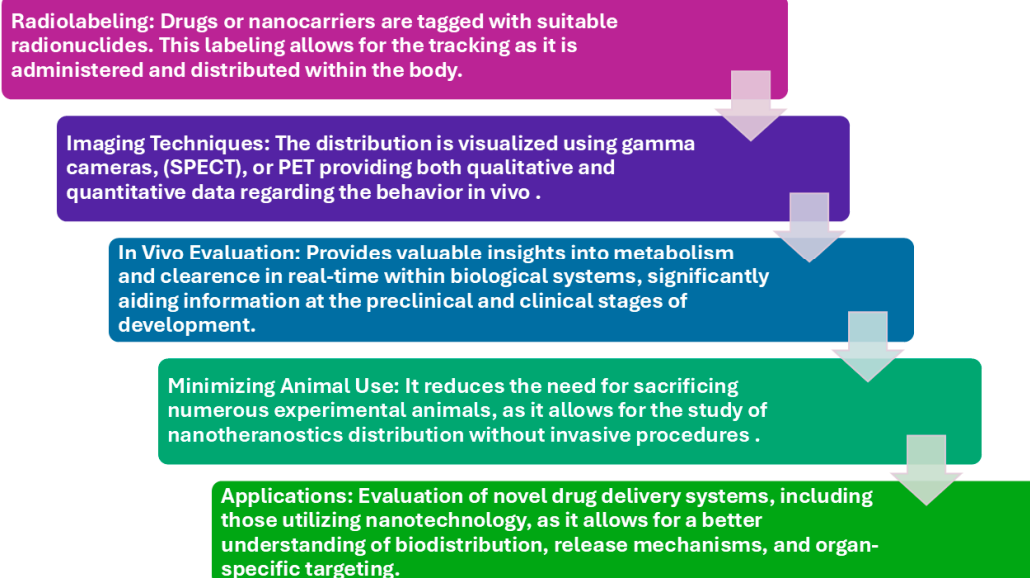


Figure 2. Conceptual overview of pharmacoscintigraphy, a nuclear imaging technique used to study the biodistribution and pharmacokinetics of radiolabeled drugs and nanomedicines. The schematic highlights the fundamental principles of this technique, emphasizing its role in preclinical and clinical research for optimizing nanotheranostic platforms.

3.1. Imaging Modalities

Table 1 shows the comparative analysis of imaging techniques summarizing different features of each modality [54–58].

Table 1. Comparative Analysis of Imaging Techniques.

Feature	Gamma Scintigraphy	SPECT	PET
Spatial Resolution	Low	Moderate	High
Sensitivity	Moderate	High	Very High
Quantification	Limited	Semi-quantitative	Fully Quantitative
Cost	Low	Moderate	High
Applications	• Gastrointestinal transit and retention studies	• Imaging organ-specific drug accumulation and clearance	• Studying tumor targeting efficiency of nanomedicines

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- | | | |
|--|--|--|
| • Pulmonary drug deposition evaluation | • Evaluating nanoparticle targeting to tumors and inflammation sites | • Quantifying receptor-mediated nanoparticle uptake |
| • Nanoparticle biodistribution assessments | • Monitoring therapeutic responses in nanotheranostics | • Investigating drug metabolism and clearance pathways |
-

3.1.1. Gamma Scintigraphy

This is a fundamental technique in nuclear medicine that relies on gamma-emitting radionuclides to provide real-time imaging of pharmaceutical formulations. The principle of gamma scintigraphy is based on the emission of gamma photons from radiotracers, typically labeled with Technetium-99m (^{99m}Tc), Iodine-123 (^{123}I), or Indium-111 (^{111}In). These emissions are captured to construct two-dimensional images of drug distribution, allowing for precise tracking of drug transit and retention in different organs. This technique has been widely used for assessing gastrointestinal transit, pulmonary drug deposition, and nanoparticle biodistribution [54,56].

3.1.2. Single-Photon Emission Computed Tomography (SPECT)

SPECT imaging extends gamma scintigraphy by enabling three-dimensional visualization of radiotracer distribution. This is achieved by acquiring multiple planar images from different angles, which are then reconstructed into a volumetric dataset. The ability of SPECT to provide high-resolution spatial localization makes it a valuable tool in nanomedicines research. One of the primary applications of SPECT is imaging organ-specific drug accumulation and clearance. This is particularly useful in evaluating the targeting efficiency of nanoparticles designed for tumor therapy or inflammation sites. Additionally, SPECT has been employed to monitor therapeutic responses in nanotheranostics, providing critical data for optimizing drug formulations [54–56,59].

3.1.3. Positron Emission Tomography (PET)

PET is a highly sensitive imaging modality that provides quantitative molecular insights into nanomedicines interactions. Unlike SPECT, which detects single-photon emissions, PET relies on positron-emitting radiotracers such as Fluorine-18 (^{18}F), Zirconium-89 (^{89}Zr), and Copper-64 (^{64}Cu). The annihilation of emitted positrons with electrons results in the production of gamma photons, which are detected to generate high-resolution images. The application of PET in nanomedicine has been particularly promising in studying tumor targeting efficiency. The technique allows for real-time assessment of receptor-mediated nanoparticle uptake and quantification of drug metabolism and clearance pathways. Furthermore, PET's high sensitivity enables the detection of low concentrations of radiolabeled nanomedicines, making it an invaluable tool in early-phase drug development [54–59].

3.2. Radiolabeling Techniques

Radiolabeling methods for nanoparticles have been extensively reported and reviewed by numerous authors in recent years. These studies have contributed to the development of various strategies for incorporating radionuclides into nanoplatforms, ensuring their stability, biocompatibility, and applicability for both diagnostic and therapeutic purposes. Given the breadth of research in this field, the present section provides a concise summary of the most relevant and widely employed radiolabeling techniques. Readers seeking a more comprehensive understanding

of these methodologies, including detailed protocols for reproducibility in their own investigations, are encouraged to refer to the cited references in this section [60–69].

There are several methods available for radiolabeling nanotheranostics as well as many dosage forms, primarily used in gamma scintigraphy. Table 2 summarizes the radioisotopes most commonly used for radiolabeling and their physical properties.

Table 2. Common Radionuclides Used in PET and SPECT Imaging.

Radionuclide	Imaging Modality	Half-Life	Energy (keV)	Primary Applications
Fluorine-18 (18F)	PET	109.8 min	511	Oncology, neurology, cardiology
Carbon-11 (11C)	PET	20.4 min	511	Neurology, oncology, molecular imaging
Zirconium-89 (89Zr)	PET	78.4 h	511	Immuno-PET, antibody labeling
Copper-64 (64Cu)	PET	12.7 h	511	Radiotherapy, imaging of hypoxia
Gallium-68 (68Ga)	PET	68 min	511	Peptide receptor imaging, neuroendocrine tumors
Technetium-99m (99mTc)	SPECT	6.0 h	140	General nuclear medicine imaging
Indium-111 (111In)	SPECT	2.8 d	171, 245	Infection imaging, leukocyte labeling
Iodine-123 (123I)	SPECT	13.2 h	159	Thyroid imaging, neuroimaging
Lutetium-177 (177Lu)*	SPECT-therapy	6.7 d	113, 208	Oncology

*177Lu also emits β^- particles with median energies of 47.6, 111.7 and 149.3 keV which are intended for therapy purposes.

Each method has its advantages and limitations, with the choice depending on several factors, including the type of nanocarrier, the physicochemical properties of the radionuclide, and the intended clinical application. The selected method should not compromise the performance of the dosage form while ensuring that the radioactive labeling is effective for imaging purposes. These methods include direct radiolabeling, chelator-based labeling, covalent binding, encapsulation, and neutron activation, each offering distinct advantages and limitations.

3.2.1 Direct radiolabeling involves incorporating the radionuclide directly into the nanocarrier without requiring external chelators or complexation agents. This process can occur through chemisorption, isotopic exchange, or surface interaction, depending on the material composition. For instance, metallic nanoparticles, such as gold or iron oxide can adsorb 99mTc due to their high affinity for metal ions [70,71]. Additionally, sulfhydryl-containing nanoparticles can bind reduced 99mTc to form stable complexes [72–75]. However, while direct radiolabeling is simple and fast, it may suffer from lower labeling efficiency and in vivo instability, which could lead to radionuclide dissociation.

3.2.2 **Chelator-based radiolabeling** remains one of the most widely used strategies due to its high stability and versatility [76–80]. In this approach, a bifunctional chelator (Table 3) is conjugated to the nanocarrier, forming a stable complex with radiometals such as gallium-68 (^{68}Ga), copper-64 (^{64}Cu), or lutetium-177 (^{177}Lu). Chelators like DTPA (Diethylenetriaminepentaacetic acid) and DOTA (1,4,7,10-Tetraazacyclododecane-1,4,7,10-tetraacetic acid) provide strong coordination with radiometals, preventing their premature release. This method is particularly useful for polymeric micelles and liposomal formulations, where DOTA-functionalized systems allow stable binding of therapeutic radionuclides such as ^{177}Lu , supporting their dual role in imaging and therapy.

Table 3. Common Chelators and Applications:

Chelator	Commonly Used Radionuclides	Application
DTPA (Diethylenetriaminepentaacetic acid)	$^{99\text{m}}\text{Tc}$, ^{111}In	SPECT imaging
DOTA (1,4,7,10-Tetraazacyclododecane-1,4,7,10-tetraacetic acid)	^{177}Lu , ^{68}Ga , ^{64}Cu	PET imaging & radiotherapy
NOTA (1,4,7-Triazacyclononane-1,4,7-triacetic acid)	^{68}Ga , ^{64}Cu	PET imaging
DFO (Deferoxamine)	^{89}Zr	Immuno-PET imaging

3.2.3 **Covalent radiolabeling** is another approach that provides strong radionuclide attachment through chemical reactions, improving in vivo stability. Iodination methods, such as electrophilic substitution, are commonly employed for labeling proteins, peptides, and polymeric nanocarriers with iodine-125 (^{125}I) or iodine-131 (^{131}I). Additionally, click chemistry-based strategies, such as copper-catalyzed azide-alkyne cycloaddition (CuAAC), facilitate the radiolabeling of nanoparticles with isotopes like ^{64}Cu or ^{18}F , ensuring site-specific conjugation without altering the physicochemical properties of the nanoparticles.

3.2.4 **Encapsulation** or incorporation of radionuclides within the nanoparticle matrix represents another effective labeling technique, particularly for systems with a high capacity for drug loading. Liposomes, micelles, and mesoporous silica nanoparticles can incorporate hydrophilic radionuclides, such as ^{111}In or $^{99\text{m}}\text{Tc}$ -pertechnetate, into their aqueous core. Similarly, some inorganic nanocarriers, including cerium oxide-based systems, allow the incorporation of radiometals like ^{68}Ga or ^{177}Lu into their structure. The primary challenge of encapsulation-based radiolabeling is the potential leakage of the radionuclide, requiring additional stabilization strategies to prevent premature release.

3.2.5 **Neutron activation** is an alternative radiolabeling technique that involves irradiating preformed nanoparticles with thermal neutrons, converting a stable isotope within the nanostructure into a radioactive one. This method is particularly useful for nanocarriers containing elements such as holmium-165 (^{165}Ho), which, upon neutron activation, transforms into the beta-emitting holmium-166 (^{166}Ho) [81]. The advantage of neutron activation is that it does not require chemical modification or surface functionalization, preserving the integrity of the nanosystem. However, this technique requires access to nuclear reactors, limiting its widespread applicability in routine radiolabeling procedures.

Advances in radiochemistry and nanotechnology continue to refine these methods, offering new opportunities for developing multimodal imaging probes and radiotherapeutics. Table 4 summarizes the key characteristics of different radiolabeling methods.

Table 4. Characteristics of radiolabeling methods.

Radiolabeling Method	Nanocarrier Examples	Radionuclides Used	Advantages	Limitations
Direct Radiolabeling	Gold, Iron Oxide NPs	^{99m} Tc, ¹⁸⁸ Re	Simple and fast	Lower in vivo stability
Chelator-Based	Liposomes, Micelles	⁶⁸ Ga, ¹⁷⁷ Lu, ⁶⁴ Cu	High stability	Requires chemical modification
Covalent Binding	Proteins, Peptides	¹²⁵ I, ¹³¹ I, ⁶⁴ Cu	Strong attachment	May alter nanocarrier properties
Encapsulation	Liposomes, Silica NPs	¹¹¹ In, ^{99m} Tc	Maintains nanoparticle integrity	Risk of leakage
Neutron Activation	Holmium Oxide NPs	¹⁶⁶ Ho, ⁸⁹ Zr	Nochemical modification required	Limited availability

The choice of radioisotopes significantly affects the study outcomes in radiolabeled absorption, distribution, metabolism, and excretion (ADME) studies due to several factors [82–98]. The specific radioisotope selected can influence the stability and behavior of the radiolabeled compound because of radiolytic processes or interfering with how the compound interacts within biological systems by an active site specially if the radioactive element is not typically present in the drug molecules or the nanocarrier. The location of the radiolabel within the molecule may influence the drug's metabolism and distribution patterns. Labeling at a position that is prone to metabolic degradation can lead to challenges in interpreting distribution data. The purity of the radiolabeled compound and its specific activity (radioactivity per unit of mass) are critical parameters. High specific activity is preferred as it allows for better detection and quantification without significantly altering the PK of the drug. The half-life of the radioisotope affects the duration of the study and the type of analysis that can be performed. For instance, isotopes with shorter half-lives may require rapid in vivo studies, complicating the design. Overall, the careful selection of radioisotopes is essential to obtain reliable and interpretable results from ADME studies, facilitating accurate assessments of a drug's behavior in vivo. Examples of applications of radiolabeling strategies are summarized in Table 5.

Table 5. Example Applications:.

Nanotheranostic System	Radionuclide	Labeling Strategy	Application
Polymeric micelles	^{99m} Tc	Direct adsorption	Tumor imaging
Liposomes	¹¹¹ In	Encapsulation	Drug delivery tracking
Iron oxide nanoparticles	⁸⁹ Zr	Chelation (DFO)	Long-term biodistribution studies

Mesoporous silica	¹⁷⁷ Lu	Lattice incorporation	Radionuclide therapy
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3.3. Choosing An Imaging Modality

The choice of imaging modality for pharmacoscintigraphy is influenced by several factors [99–105], including the type of study, radionuclide characteristics, specificity needs, availability of equipment and expertise, ethical considerations, and regulatory compliance. The specific goals of the investigation, such as biodistribution, PK, or pharmacodynamics of drug formulation, dictate the imaging modality. For example, SPECT is often chosen for three-dimensional imaging of internal structures, while planar gamma cameras may be sufficient for simpler studies. The choice of radionuclide, such as gamma-emitting isotopes like ^{99m}Tc or ¹¹¹In, plays a crucial role, as different radionuclides have distinct energy levels and half-lives. Positron emitters like Carbon-11 or Fluorine-18 require specialized equipment like PET scanners due to their higher photon energies and shorter half-lives. The level of anatomical detail required for the study also influences modality selection. While SPECT provides higher spatial resolution and can generate cross-sectional images, planar imaging may not deliver the necessary detail for certain applications, especially when complex structures are involved. The availability of equipment and expertise is another determining factor, as some techniques, like PET, are more expensive and require specialized training. Ethical considerations regarding radiation exposure levels and safety limits, as recommended by nuclear regulatory authorities on radiological protection, are of utmost importance when dealing with human subjects. The chosen modality should balance the need for quality imaging with participant safety. Regulatory compliance, including adherence to Good Manufacturing Practices, also impacts the choice of imaging modality and the overall study design. By considering these factors, researchers can select the most appropriate imaging modality for their specific needs in imaging scintigraphy [105].

3.4. Limitations of Imaging Techniques

These techniques do not provide detailed anatomical insights, making it challenging to visualize the exact location of the radiolabeled agent unless it outlines clearly identifiable organs. Hybrid imaging techniques overcome this limitation. Not all drugs or compounds or nanosystems can be effectively labeled with radioisotopes, which limits the applicability of the technique. The equipment is often expensive, especially if hybrid modalities are used, and its operation requires skilled personnel, which can be a barrier to widespread use. While the radiation doses used are low and generally considered safe, the need to handle radioactive materials still requires adherence to strict safety protocols. These limitations indicate that while radioisotopic imaging techniques are a valuable tool in drug evaluation, there are specific challenges that researchers must navigate to effectively utilize this technique [101–105].

4. Applications in Nanomedicines Research

4.1. Objectives

The main objectives of conducting pharmacoscintigraphic ADME studies are as follows [106]:

- **Determine Mass Balance:** To compare the amount of administered radioactivity to the amount recovered in excreta.
- **Routes of Elimination:** To identify routes of elimination and evaluate the extent of absorption.
- **Metabolite Identification:** To identify circulatory and excretory metabolites.
- **Clearance Mechanisms:** To determine the mechanisms of clearance (renal, biliary, metabolic).
- **Distribution Characterization:** To characterize the distribution of the compound within tissues and organs.

- Exposure Determination: To ascertain the exposure levels of the parent compound and its metabolites.
- Validation of Animal Models: To help validate the animal species used for toxicological testing.
- Pharmacological/Toxicological Contribution: To explore whether metabolites contribute to the pharmacological or toxicological effects of the drug.

4.2. Why Pharmacoscintigraphic ADME Studies Are Recommended

Nanomedicines and drug delivery systems often exhibit unique PK profiles compared to conventional drugs due to their small size, surface properties, and ability to interact with biological barriers. Radiolabeled studies allow researchers to characterize the ADME properties of these nanomaterials accurately. Understanding how nanomedicines distribute in the body is critical, especially because they may accumulate in specific tissues (e.g., tumors) due to the enhanced permeability and retention (EPR) effect. Radiolabeled compounds can be tracked non-invasively to delineate their distribution across different organs and tissues over time. The metabolism of nanomedicines may differ significantly from that of traditional drugs. Investigating how a nanocarrier is metabolized or cleared can inform the design of drug delivery systems and help predict potential toxicological concerns. Regulatory authorities may require comprehensive ADME data for the registration of nanomedicines. Radiolabeled studies provide essential data needed to demonstrate safety and efficacy through systematic evaluation of how these formulations behave in biological systems [102,103,106–108].

4.3. How Pharmacoscintigraphic ADME Studies Are Conducted for Nanomedicines

The first step is the selection of radiolabels. Assess the appropriate radiolabel based on the chemical structure and application. The chosen label should not interfere with the nanomaterial's properties or function. Then, preparation of radiolabeled nanoparticles by synthesizing the nanomedicine with the appropriate radiolabeling strategy may involve encapsulating the radioisotope within the nanoparticle or attaching it to the surface. It is crucial to maintain the stability and integrity of the formulation during this process and quality control are part of the evaluation before using it in the imaging studies. Once the nanosystem is ready, it is administered to suitable animal model and in vivo studies are conducted by acquiring functional images and may be also collecting biological samples (e.g., blood, urine, feces, organs) over time to complement or validate the PK and biodistribution results. Quantitative analysis of images (and samples) to assess the extent of radioactivity associated with the administered nanosystem is crucial for determining mass balance, routes of elimination, and clearance mechanisms. Additionally, metabolite identification, is possible, helps understanding the biotransformation pathways to establish the safety profile of the nanomedicine [102,103,106–108]. In summary, radiolabeled ADME studies are invaluable for the development and regulatory evaluation of nanomedicines and drug delivery systems, as well as of nanotheranostics, assisting in the understanding of their unique PK profiles and safety assessments (Figure 3).

How Pharmacoscintigraphic ADME Studies are Conducted for Nano-drugs

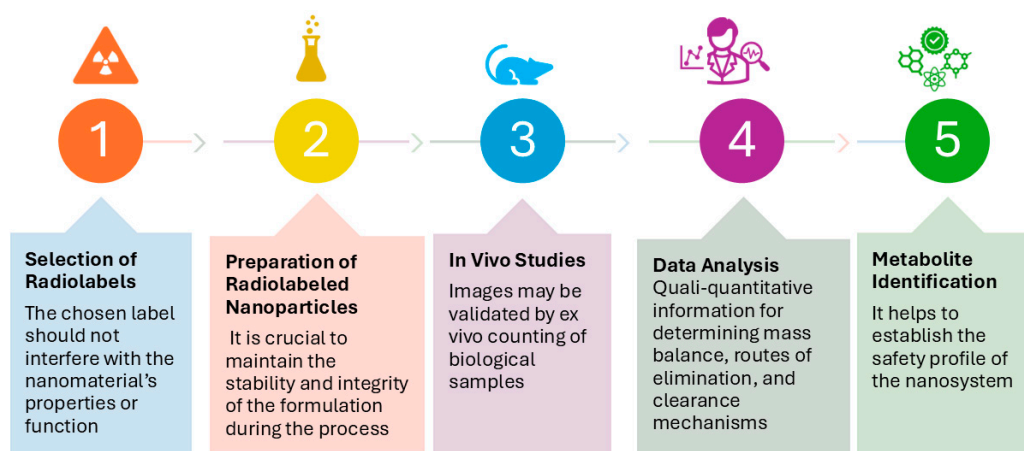


Figure 3. Overview of pharmacoscintigraphic Absorption, Distribution, Metabolism, and Excretion (ADME) studies for nanomedicines. It details the methodologies employed for radiolabeling nanocarriers, imaging techniques for tracking biodistribution, and strategies for analyzing excretion pathways. These studies are crucial for ensuring the safety and efficacy of nanomedicines before clinical translation.

5. In-House Experience: Nanotheranostics in Cancer

The advancement of nanotheranostics has needed the development of sophisticated imaging techniques to evaluate their biodistribution, PK, and therapeutic efficacy. Among these, radionuclide imaging has played a pivotal role, providing non-invasive, real-time insights into the behavior of nanosystems in vivo. The research conducted in our institution has significantly contributed to this field by employing ^{99m}Tc radiolabeling to study various polymeric nanomicelles (Figure 4). The investigations have provided crucial data on micelle performance, functionalization strategies, and the potential for targeted imaging and therapy in oncology [109–114].

The work has primarily focused on TPGS-based nanomicelles, Soluplus® micelles, and hybrid micelles composed of TPGS and Soluplus®, all of which exhibit excellent solubilizing properties and biocompatibility. The use of ^{99m}Tc radiolabeling enabled precise tracking of these nanosystems, allowing us to evaluate their stability, tumor uptake, and clearance rates. Beyond their imaging potential, these nanomicelles have been investigated as theranostic platforms as well, capable of serving as both drug delivery vehicles and imaging agents.

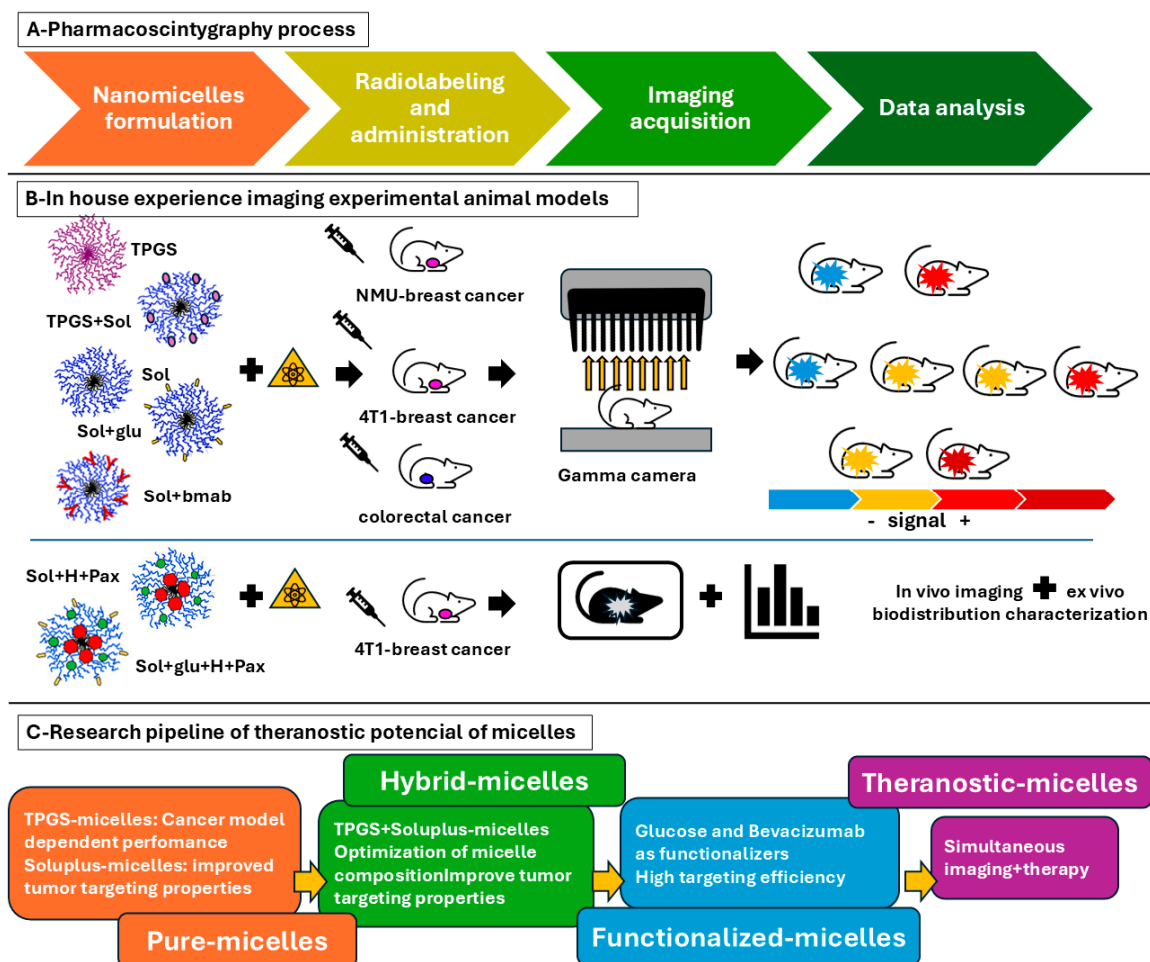


Figure 4. Comprehensive overview of preclinical imaging studies conducted to evaluate the theranostic potential of nanomicelles in different cancer models (4T1 breast cancer, NMU-induced breast cancer, and colorectal cancer). The schematic categorizes micelles into pure, hybrid, and functionalized formulations, highlighting their targeting efficiency and therapeutic capabilities. Key functionalization strategies, such as glucose and bevacizumab conjugation, are also illustrated to demonstrate their impact on tumor targeting and therapeutic outcomes. A-Schematic representation of the experimental workflow for radiolabeling, in vivo administration, and imaging of nanotheranostic formulations. The process begins with the synthesis and radiolabeling of micelles, followed by intravenous administration in tumor-bearing animal models. Serial imaging acquisitions are performed at different time points to track biodistribution, tumor accumulation, and excretion pathways; B-Representative imaging results from three different tumor models: 4T1 breast cancer, NMU-induced breast cancer, and colorectal cancer. The images illustrate the dynamic distribution of radiolabeled micelles within the body, highlighting differences in tumor uptake and clearance patterns among the different formulations; C-Comparative analysis of micelle formulations, categorized into pure micelles, hybrid micelles, and functionalized micelles. Functionalization strategies, such as glucose and bevacizumab conjugation, are shown to increase tumor targeting efficiency. Graphical representations of quantitative imaging data are included to demonstrate variations in tumor-to-background ratios and excretion kinetics across different formulations. Abbreviations: TPGS: D- α -tocopheryl polyethylene glycol succinate, Sol: Soluplus®, NMU: N-nitroso-N-methylurea, TPGS+sol: hybrid micelle with Soluplus®+TPGS, Sol+glu: Soluplus® micelle functionalized with glucose, Sol+bmab: Soluplus® micelle functionalized with bevacizumab, Sol+H+Pax: Soluplus® micelle loaded with histamine and paclitaxel, Sol+glu+H+Pax: Soluplus® micelle functionalized with glucose loaded with histamine and paclitaxel.

TPGS (D- α -tocopheryl polyethylene glycol succinate) is a nonionic surfactant with self-assembling properties that form stable nanomicelles. The foundational studies focused on the

radiolabeling efficiency, stability, and PK of ^{99m}Tc -TPGS micelles in healthy Wistar rats. Planar gamma imaging was performed at multiple time points to evaluate micelle stability in blood circulation, accumulation in organs of clearance (liver, kidneys, and intestines) and excretion pathways (renal and hepatobiliary clearance). The results demonstrated that ^{99m}Tc -TPGS micelles could be successfully radiolabeled with ^{99m}Tc , retaining their physicochemical properties, remained stable in circulation, exhibited controlled hepatic and renal clearance, and maintained a favorable PK profile, supporting their potential for in vivo imaging applications [110]. TPGS micelles were later tested in a chemically induced breast cancer model using N-nitroso-N-methylurea (NMU) in Sprague-Dawley rats and compared against ^{99m}Tc -sestamibi. Imaging analysis revealed that ^{99m}Tc -TPGS micelles achieved higher tumor uptake and contrast than ^{99m}Tc -sestamibi, exhibiting superior imaging performance because of their higher tumor-to-background ratios demonstrating their potential as a more efficient diagnostic agent [111,112]. However, in the 4T1 murine breast cancer model, the same formulation exhibited low tumor accumulation, suggesting that passive targeting via the EPR effect was insufficient. To overcome this limitation, hybrid micelles composed of TPGS and Soluplus® were tested, demonstrating improved tumor uptake and superior imaging contrast, likely due to optimized micelle stability and biodistribution. Then, Soluplus® micelles and hybrid Soluplus® + TPGS micelles were further evaluated for tumor accumulation and imaging efficiency. These formulations demonstrated superior imaging performance in the 4T1 breast cancer model, achieving higher tumor-to-background ratios compared to TPGS micelles alone. Planar gamma imaging was used to monitor biodistribution and retention over time, confirming that these formulations offered better tumor retention. To improve active targeting, Soluplus® micelles were functionalized with glucose, aiming to exploit the overexpression of glucose transporters (GLUT1) in breast cancer cells. Imaging studies showed that glucose-functionalized micelles exhibited significantly increased tumor uptake, confirming that GLUT1-mediated targeting enhanced retention and imaging contrast. Beyond their imaging applications, polymeric micelles have demonstrated the potential for drug delivery, making them ideal candidates for theranostic applications [113]. One particularly study investigated the co-loading of histamine and paclitaxel in nanomicelles, demonstrating the capacity of these systems to improve chemotherapy while being tracked via radionuclide imaging. The theranostic potential of polymeric micelles was further demonstrated, when Soluplus® micelles alone and functionalized with glucose were co-loaded with paclitaxel and histamine aimed to improve therapeutic outcomes through different mechanisms. These micelles demonstrated significantly greater antitumor efficacy compared to the other formulations as this experimental group showed a more pronounced reduction in triple negative breast cancer cell viability and increased apoptosis compared to micelles containing paclitaxel alone or histamine alone. The formulations exhibited differing effects on neovascularization, with histamine-loaded micelles (both with and without paclitaxel) significantly reducing new blood vessel formation, which is crucial for tumor growth, while the empty micelles did not show this effect. The ability of these micelles to carry therapeutic payloads while being imaged in vivo suggests their future role as integrated diagnostic and therapeutic platforms [114].

In a separate study focused on colorectal cancer, Soluplus® micelles were functionalized with bevacizumab, a monoclonal antibody targeting vascular endothelial growth factor (VEGF), to enhance active targeting in a colorectal cancer xenograft model [109]. Planar gamma imaging was used to track the biodistribution of radiolabeled micelles in tumor-bearing mice, demonstrating that bevacizumab-functionalized micelles showed higher tumor accumulation and prolonged retention compared to non-functionalized micelles demonstrating a synergistic effect between passive EPR and active targeting mechanisms. These findings support the role of VEGF-targeting micelles in improving nanoparticle-mediated tumor imaging and therapy guidance [109].

Table 6 summarizes the performance of the different radiolabeled nanomicelles in the studies carried out in house.

Table 6. Comparative Analysis of Nanomicelle Performance.

Nanomicelle Type	Functionalization	Tumor Uptake	Imaging Performance	Theranostic Potential
TPGS-Based Micelles	None	Low (4T1 model) High (NMU model)	Poor imaging contrast Superior to 99mTc-sestamibi	Limited as standalone therapy Potential imaging agent
Soluplus® Micelles	None	Moderate (EPR effect)	Good imaging contrast	Potential for passive drug release
Soluplus® + TPGS Micelles	None	High (4T1 model)	Improved tumor localization	Synergistic tumor targeting
Soluplus® Micelles	Glucose Bevacizumab	High (GLUT1-mediated) Very High (VEGF-targeting)	Improved imaging contrast retention Strong imaging contrast retention	Greater tumor targeting capability Optimal for guided drug delivery

6. Discussion and Future Perspectives

The integration of pharmacoscintigraphy into nanomedicine research has significantly improved our ability to assess nanotheranostics behavior *in vivo*, providing critical data on biodistribution, pharmacokinetics, and therapeutic efficacy. Pharmacoscintigraphy, encompassing gamma scintigraphy, SPECT, and PET, has demonstrated its value in evaluating nanotheranostics, enabling the precise tracking of radiolabeled nanocarriers in both preclinical and clinical studies. This capability has facilitated the optimization of nanoformulations, ensuring their stability, targeted delivery, and therapeutic potential. One of the major advantages of radionuclide imaging is its ability to provide real-time, non-invasive monitoring of drug-loaded nanocarriers. This feature is particularly relevant in oncology, where nanotheranostic formulations must efficiently reach and accumulate in tumor tissues while minimizing systemic toxicity. By allowing dynamic visualization of drug distribution, these imaging techniques contribute to the rational design of nanomedicines, refining their pharmacological profiles and improving therapeutic outcomes. Future advancements in imaging technology both in the preclinical and clinical settings hold promise for further enhancing the precision of nanotheranostics tracking. Multimodal approaches that integrate the high sensitivity of PET with the superior anatomical resolution of MRI or CT, provide a more comprehensive understanding of nanotheranostics behavior at both molecular and structural levels. Additionally, the emergence of longer-lived positron-emitting radionuclides, such as Zirconium-89 (⁸⁹Zr), offers extended imaging windows, which are particularly beneficial for evaluating slow-releasing nanotheranostic platforms. Beyond their application in biodistribution studies, pharmacoscintigraphy is proving instrumental in assessing the therapeutic efficacy of nanotheranostics. Imaging studies allow for the quantification of tumor response following treatment, revealing changes in tumor volume, perfusion, and metabolic activity. This capability is

critical in evaluating whether nanotheranostics achieve sufficient therapeutic concentration at the target site. Moreover, imaging-based tracking of biomarkers of disease progression, such as hypoxia levels or angiogenesis, can provide deeper mechanistic insights into nanotheranostics action, guiding further refinements in formulation design. Another crucial contribution of pharmacoscintigraphy to nanomedicine research is its role in regulatory approval processes. Regulatory agencies, increasingly require in vivo imaging data to support the approval of nanomedicines, particularly those involving novel drug delivery systems. Imaging-derived pharmacokinetic and biodistribution data provide essential safety and efficacy assessments, expediting the transition of nanotheranostics from preclinical studies to human trials. Furthermore, pharmacoscintigraphy allows for the early identification of off-target effects, helping to refine dosing regimens and reduce potential adverse reactions before first-in-human administration. The impact of pharmacoscintigraphy is not limited to preclinical and regulatory applications; it also plays a crucial role in the development of personalized medicine strategies. By tailoring therapies based on patient-specific imaging data, clinicians can optimize treatment regimens, adjusting dosing and formulation strategies to maximize efficacy while minimizing toxicity. The ability to track individual patient responses in real time could lead to a more adaptive, precision-based approach to nanotheranostic applications, particularly in oncology and other complex disease settings. Lastly, pharmacoscintigraphy provides valuable information on the long-term stability and integrity of nanocarriers. Given that many nanoformulations rely on the controlled release of therapeutic agents, imaging studies can reveal how these formulations behave under physiological conditions over extended periods. This aspect is particularly relevant for theranostic applications, where both diagnostic imaging and therapeutic delivery must be tightly coordinated to achieve optimal patient outcomes.

7. Conclusions

In conclusion, imaging techniques play a vital role in the research and development of nanotheranostics providing real-time, non-invasive insights into their biodistribution and pharmacokinetics, therapeutic efficacy, formulation stability, and mechanisms of action, while also facilitating the transition to clinical applications. As technological advancements continue to refine imaging modalities and regulatory frameworks increasingly recognize their value, pharmacoscintigraphy will remain an indispensable tool for the successful translation of nanomedicines from preclinical research to clinical applications, contributing to more effective and personalized treatment strategies.

Conflicts of Interest: The authors declare no conflicts of interest.

Abbreviations

The following abbreviations are used in this manuscript:

ADME Absorption, Distribution, Metabolism, Excretion

CT Computed Tomography

DNA Desoxyribonucleic-acid

EPR Enhanced Permeability and Retention

GLUT-1 Glucose Transporter 1

GMP Good Manufacturing Practices

MRI Magnetic Resonance Imaging

NMU: N-nitroso-N-methylurea

PET Positron Emission Tomography

PK Pharmacokinetic

Sol: Soluplus®

Sol+glu: Soluplus® micelle functionalized with glucose

Sol+bmab: Soluplus® micelle functionalized with bevacizumab

Sol+H+Pax: Soluplus® micelle loaded with histamine and paclitaxel

Sol+glu+H+Pax: Soluplus® micelle functionalized with glucose loaded with histamine and paclitaxel
SPECT Single Photon Emission Computed Tomography
TPGS: D- α -tocopheryl polyethylene glycol succinate
TPGS+sol: hybrid micelle with Soluplus®+TPGS
US United States
VEGF Vascular Endothelial Growth Factor

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