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Article

Scalable Fabrication of Biomimetic Antibacterial Nanospikes on PMMA Films Using Atmospheric-Pressure Low-Temperature Plasma Treatment

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Abstract

Antibacterial surfaces inspired by biological micro- and nanostructures, such as those found on cicada wings, have attracted interest due to their ability to inhibit bacterial adhesion and damage microbial membranes without relying on chemical agents. However, conventional fabrication techniques like photolithography or nanoimprinting are limited by substrate shape, size, and high operational costs. In this study, we developed a scalable method using atmospheric-pressure lowtemperature plasma (APLTP) to fabricate sharp-edged nanospikes on solvent-cast polymethyl methacrylate (PMMA) films. The nanospikes were formed through plasma-induced modification of pores in the film, followed by annealing to control surface wettability while maintaining structural sharpness. Atomic force microscopy confirmed the formation of micro/nanostructures, and contact angle measurements revealed reversible hydrophilicity. Antibacterial performance was evaluated against Escherichia coli using ISO 22196 standards. While plasma treatment alone reduced bacterial colonies by 30%, the combined plasma and annealing treatment achieved an antibacterial activity value greater than 5, with bacterial counts below the detection limit (<10 CFU). These findings demonstrate that APLTP offers a practical route for large-area fabrication of biomimetic antibacterial coatings on flexible polymer substrates, holding promise for future applications in healthcare, packaging, and public hygiene.

Keywords: scalable antibacterial surface fabrication; atmospheric-pressure low-temperature plasma large-area surface treatment; polymer surface engineering; nanospike-structured surfaces

1. Introduction

Biomimetics, the practice of drawing inspiration from nature, has received increasing attention in recent years, particularly in the development of antibacterial surfaces. Numerous studies have demonstrated that micro- and nanostructured surface topographies inspired by biological organisms can effectively inhibit bacterial adhesion and exert bactericidal effects by physically disrupting bacterial membranes [1–10]. The nanopillar structures found on cicada wings are known to promote a Cassie–Baxter wetting state [11], which reduces bacterial colonization, while their nanoscale protrusions can mechanically rupture bacterial membranes [1,4–6,12–15]. These natural structures exhibit antibacterial activity not only due to their chemical composition but also due to their physical topography [1,3,10,16,17]. Artificial surfaces such as black silicon, fabricated via reactive ion etching, have been shown to replicate similar bactericidal effects [2,18–22]. In particular, nanostructured surfaces that combine superhydrophobicity with mechanical bactericidal activity are of great interest for biomedical applications, where preventing bacterial adhesion and biofilm formation is critical.

Various fabrication techniques have been employed to replicate such natural architectures [23–32], including photolithography [3,33,34], nanoimprinting [35,36], and plasma-based methods [37–39]. Photolithography enables sub-100 nm patterning with high precision [40–45]. However, both techniques impose limitations on substrate size and shape and require dedicated equipment, which restricts their practicality for large-scale or irregularly shaped surfaces. Plasma-based processes [46–50], on the other hand, often require vacuum (low-pressure) environments, adding further complexity and cost. These factors present challenges for implementing such techniques in everyday or industrially scalable settings.

In this study, we focus on atmospheric-pressure low-temperature plasma (APLTP) as a practical and scalable method for fabricating antibacterial microstructures on polymer surfaces. APLTP enables plasma processing under ambient conditions, reduces equipment complexity, and allows for the treatment of large or irregularly shaped substrates [51-55]. Our previous work demonstrated that APLTP treatment of solvent-cast polymethyl methacrylate (PMMA) films can produce hydrophilic surfaces through the formation of micro- and nanostructures originating from pores located on and within the film [51]. We also showed that APLTP treatment applied to the surface of polyethylene (PE) sheets and the inner walls of PE tubes resulted in ultra-hydrophilic surfaces with excellent antifouling performance against oil-based contaminants, resembling the functionality observed in snail shells [53–55]. While such hydrophilic surfaces are effective in fouling prevention, antibacterial applications often demand the coexistence of both sharp-edged nanostructures and water repellency to prevent bacterial adhesion [2,18-22,56]. To address this requirement, we introduce an annealing process following APLTP treatment. By thermally shrinking the surface and closing microscopic pores, we aim to restore hydrophobicity while preserving the bactericidal microstructure. This dual approach seeks to maintain sharp-edged topography and enhance the surface's antibacterial performance through controlled wettability.

2. Materials and Methods

2.1. PMMA Film Preparation

The PMMA (Sigma-Aldrich Corp., LLC, *Mw*=15,000) was dissolved in ethyl lactate (Wako first Grade; Fujifilm Wako Pure Chemical Corp.). Its solution concentration was 30 wt%. The solution was spin-coated onto a glass substrate (1 mm thickness, 76×52 mm², S9111; Matsunami Glass Ind., Ltd.,) using a spin-coater (K-359 S-1; Kyowa Riken Co., Ltd.). The rotation speed of the spin coater was 1800 rpm and the rotation time was 24 s. Pre-baking of the substrate in an oven (CLO-2AH; Koyo Thermo Systems Co., Ltd.) at 100 °C for 60 s. The initial film thickness was measured using a surface profiler (Surfcom 480A; Tokyo Seimitsu Co., Ltd.). The initial PMMA film thickness was about 5 μm.

2.2. Plasma Treatment

PMMA coated substrate was irradiated with atmospheric-pressure low-temperature plasma. Figure 1 portrays the plasma treatment equipment diagram. The He gas (≥99.99%; Takamatsu Teisan Co.) flow rate was fixed at 2.0 slm using a mass flow controllers (SEC-400MK3; STEC Inc.). The O₂ gas (≥99.5%; Iwatani Sangyo Corp.) flow rate was fixed at 60 sccm using another mass flow controller (SEC-E4; HORIBA STEC). The He/O₂ mixture was introduced into an upper electrode. The bottom area of upper electrode is 32 × 52 mm². The upper electrode has a slit. Slit size is 1 × 20 mm. The mixture flows out from the slit. Distance between upper electrode and substrate was 0.7 mm, distance between upper and under electrode was 1.7 mm. RF power supply (RP-200-27M; Pearl Kogyo Co. Ltd.) and auto matching box (ZDK-916S-2 and M-05A2VD-27M; Pearl Kogyo Co. Ltd.) were used to generate an atmospheric pressure low-temperature plasma. The RF power was 120 W. Its frequency was 27.12 MHz. Stage, on which under electrode was put, can be movable by an electrical motor. The plasma irradiation time per irradiation was 5 s. Cooling time after irradiation was 15 s. They were one set; it was repeated several times. The substrate after plasma treatment was put in the oven at 120 °C for 5 days [57,58]. In this study, this heat treatment process will be called annealing.

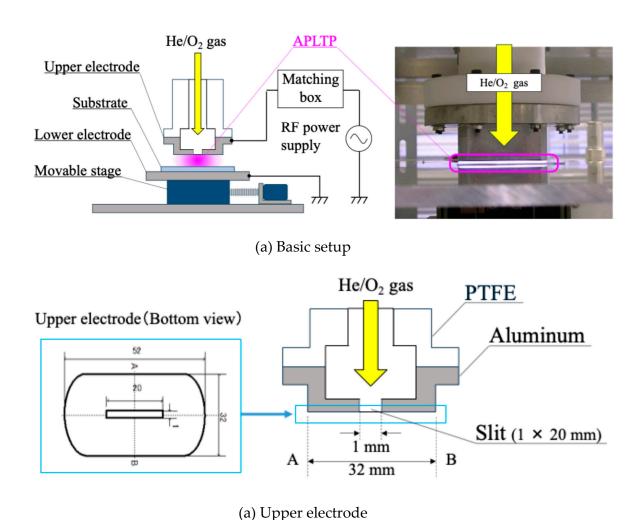


Figure 1. Diagram of APLTP treatment equipment.

2.3. Evaluation of PMMA Film

The relationship between the irradiation cycles of APLTP and the film thickness of PMMA was examined. The plasma resistance of PMMA was evaluated by the etching rate, which was calculated from the decrease in film thickness relative to the irradiation time. The amount of residual solvent in the film was examined using TG-DTA (Rigaku, TG 8121 Thermo plus EVO2), which is thermogravimetry (TG) and differential thermal analysis (DTA). The PMMA film prepared on a glass substrate was scraped off with a scraper. The amount recovered was approximately 5 mg. This was placed in an Al pan and heated from room temperature to 500°C. The heating rate was 20°C/min. Ar gas (≥99.99%; Takamatsu Teisan Co.) was flowed at 150 mL/min. The amount of residual solvent was evaluated from the weight loss at 140-200 °C, which is near the boiling point of ethyl lactate.

The surface profile after irradiation was examined using atomic force microscopy (AFM, Veeco Dimension Icon; Bruker Corp.). The relation of the surface area to the surface roughness to the plasma irradiation condition was evaluated. The evaluation area of AFM was $5 \times 5 \ \mu m^2$ with a resolution of 256×256 points. The surface roughness was analyzed based on AFM results obtained using WSxM [59]. Before the analysis, each AFM image was digitally treated with a parabolic flattening, to suppress three-dimensionality and bow effects.

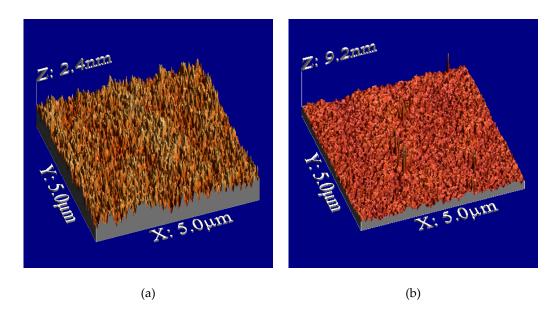
The wettability of the sample surface was evaluated by contact angle (Simage AUTO 100; Excimer Inc.). The water droplet volume was 2 μ L. Pure water (specific resistance value > 18 M Ω ·cm) was used for the droplets. The contact angle was measured 1 s after contact of the droplet on the surface. The contact angle was calculated by the tangent method.

The antibacterial test was performed to verify the potential of atmospheric pressure low-temperature plasma. The antimicrobial performance of the surface was evaluated according to antimicrobial test ISO 22196 using *Escherichia coli* (Escherichia NBRC 3972). Polyethylene sheet was used to reference. Untreated PMMA film was used as a control substrate. Initial number of colonies was 3.7×10^5 CFU. Three PMMA substrates were prepared under each condition for the antimicrobial test. Only one APLTP treatment condition was applied in this experiment. The test was carried out by an external agency. The condition of *E. coli* on the sample surfaces could not be examined because of testing constraints.

3. Results

3.1. Surface Morphology

Figure 2 illustrates the surface morphologies, showing sharp-edged nanospikes on the film surface after plasma treatment. Figure 3 presents the dependence of surface roughness on plasma irradiation cycles for PMMA films. The surface roughness increased up to 10 cycles then after decreasing. Irradiation beyond 10 cycles may lead to the destruction of the microstructures. Annealing after plasma treatment resulted in a decrease in the height of the structures, and the surface roughness reduced to about half of the roughness of plasma-treated surface after irradiation cycles exceeding six. The observed decrease in both the height of the structures and the surface roughness may be attributed to this shrinkage. We will discuss later about thermal shrinking.



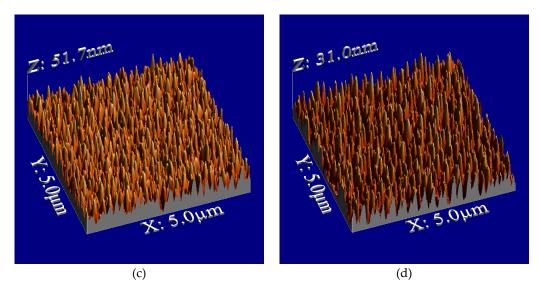


Figure 2. Surface morphologies of PMMA films: (a) Untreated surface, (b) Annealing treatment, (c) Plasma treatment (6 cycles), (d) Plasma (6 cycles) & annealing treatment.

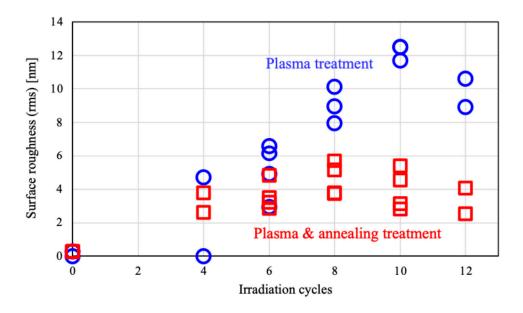


Figure 3. Surface roughness dependence on plasma irradiation times for PMMA films; one is a plasma-treated PMMA film (blue circle), the other is an annealing-treated PMMA film after plasma treatment (red square).

3.2. Wettability

Figure 4 presents photographs of contact angle measurements for PMMA films, while Figure 5 illustrates the dependence of the contact angle on plasma irradiation cycles. The surface treated only with plasma was hydrophilic. This hydrophilicity was almost independent from surface roughness shown in Figure 3. Generally, hydrophilicity induced by microstructures is often explained using the Wenzel model [60]. The increased surface area by the formation of microstructures may be too small to effect wettability. In our previous work, we reported that the formation of microstructures results in *super-nanohydrophilicity*, similar to the surface of a snail's shell [51–55]. In contrast, the wettability of the surface treated with both plasma and annealing recovered to that of the untreated surface. Gotoh et al. have investigated the time course of wettability after plasma treatment and reported that hydrophobicity recovered [61]. One of our ideas is that annealing may promote this recovery. We will also discuss later about wettability with another idea.

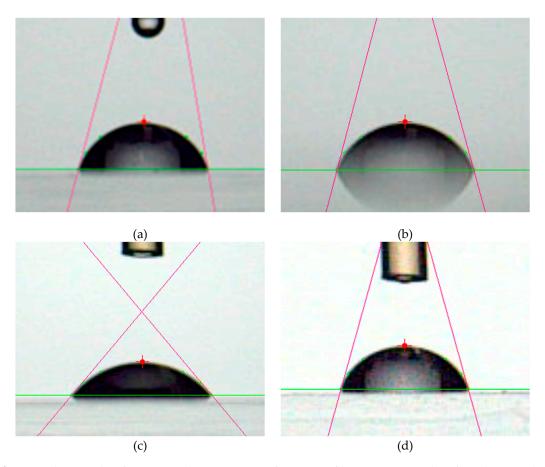


Figure 4. Photographs of contact angle measurement for PMMA films: (a) Untreated surface, (b) Annealing treatment, (c) Plasma treatment (6 cycles), (d) Plasma (6 cycles) & annealing treatment.

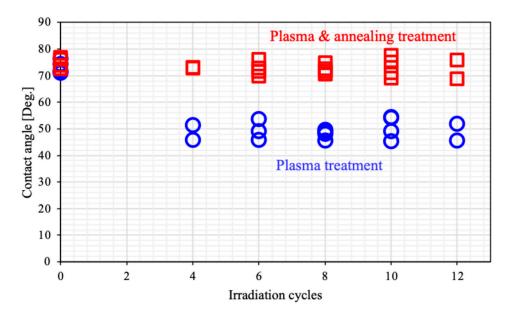


Figure 5. Contact angle dependence on plasma irradiation times for PMMA films; one is a plasma-treated PMMA film (blue circle), the other is an annealing-treated PMMA film after plasma treatment (red square).

3.3. Antibacterial Test

Figure 6 shows the number of colonies on the surface of PMMA films before and after the treatments. The number of colonies on the untreated substrate was comparable to that on the control sheet, polyethylene (PE) sheet. The number of colonies on the substrate subjected to annealing treatment remained similar to that on the untreated one. In contrast, the number of colonies on the plasma-treated substrate was 30% lower than that on the untreated one. However, on these substrates, the number of colonies increased compared to the initial count. In contrast, the surface treated with both plasma and annealing exhibited a colony count at the detection limit (< 10 CFU). This substrate demonstrated high antimicrobial performance. We will discuss later about antimicrobial performance.

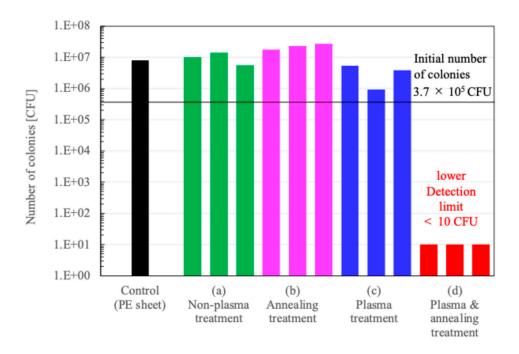


Figure 6. Number of colonies on the surface for PMMA films.

4. Discussion

4.1. Thermal Shrinking

Figure 7 presents the PMMA film thickness on APLTP irradiation cycles for substrates of plasma treatment and plasma & annealing treatment. The initial film thickness is represented by the value at zero irradiation cycles. Prior to annealing, the film thickness ranged from 4.5 to 4.9 μ m, whereas after annealing, it slightly decreased to 4.4 to 4.6 μ m. This reduction in thickness must be attributed to the shrinkage of the PMMA film caused by the heating during the annealing process. No further decrease in film thickness was observed after four or more irradiation cycles, both before and after annealing, suggesting that the surface side of the PMMA film may be more susceptible to shrinkage. The etching rate, about 3.4 μ m/min, was determined for irradiation cycles ranging from 4 to 10, calculated based on the reduction in film thickness relative to the number of irradiation cycles. After 12 irradiation cycles, the observed film thickness deviated from the expected value based on the calculated etching rate. Between 10 and 12 cycles, a decrease in the etching rate was observed, perhaps indicating an increase in the density of the PMMA film at below 2 μ m thickness.

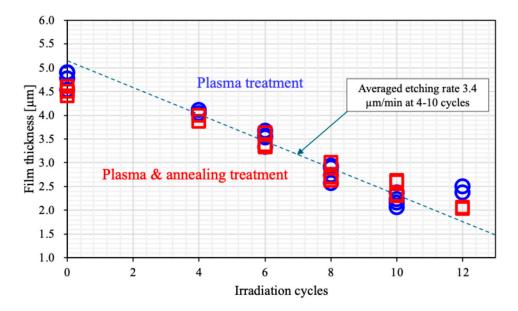


Figure 7. Relationship between the number of irradiation cycle and the film thickness; one is a plasma-treated PMMA film (blue circle), the other is an annealing-treated PMMA film after plasma treatment (red square).

The etching rate remained slow for irradiation cycles between 0 and 4, which may be indicative of substances such as moisture and residue on the surface. Figures 8 and 9 presents the results of thermal analysis (TG-DTA) for raw powder sample of PMMA film and sample recovered from PMMA film. Weight loss was observed starting at approximately 80°C. The DTA results suggested that this weight loss was due to an endothermic reaction. This phenomenon should be consistent across each sample because of the volatilization of adsorbed moisture. The weight loss stabilizes around 140°C, with a total loss of 3%. The weight loss of the film sample was 1% more than that of the powder, suggesting that the film sample had more water adsorption sites. Above 360°C, a sharp weight decrease occurs, which is attributed to the thermal decomposition of PMMA. The temperature at which the weight loss reached -100% was the same for both, 440°C. On the other hand, the weight loss between 260 and 360°C indicates the presence of thermally decomposable substances within the film. DTA shows a large endothermic reaction that partially overlaps with the thermal decomposition of PMMA. Considering that the boiling point of ethyl lactate, the solvent used, is 154°C, the weight decrease observed at that temperatures in the film sample must be ascribed not to solvent remained within the film. This must be made from solvent material during the solvent casting process. It is a kind of solvent residue, and its weight is about 6% of the membrane weight.

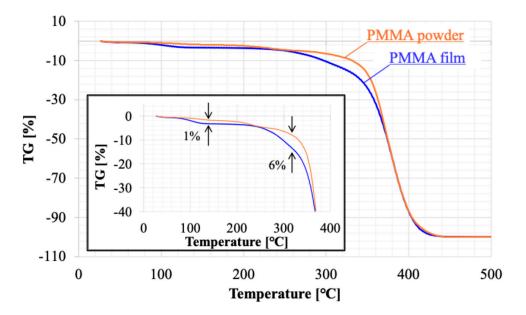


Figure 8. Result of thermogravimetry (TG) analysis; one is a raw powder sample of PMMA film (orange line), the other is a sample recovered from PMMA film (blue line).

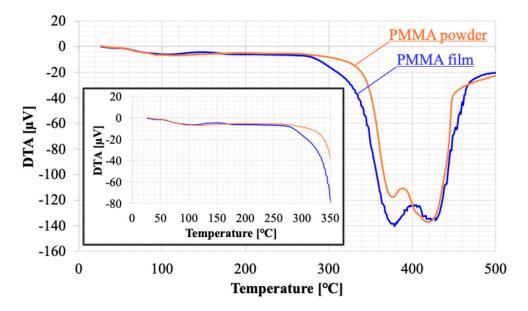


Figure 9. Result of differential thermal analysis (DTA); one is a raw powder sample of PMMA film (orange line), the other is a sample recovered from PMMA film (blue line).

4.2. Wettability

The formation of microstructures using plasma etching should be distinguished from so-called surface roughening. Her et al. reported the formation of microstructures on PMMA surfaces using a focused Ga ion beam [62]. They explain that the formation of microstructures is caused by the penetration of Ga⁺ ions into the bulk of PMMA and these interactions occur not only on the surface but also below the surface. Combining their explanation with our findings [51,52], we explain the relationship between the formation of microstructures and wettability. Micropores, which serve as exits for vaporized solvent molecules, may form both on the surface and inside the PMMA film. Dropped water percolates through the microstructures due to capillary action. The pores then

provide air paths, allowing the water to fill not only the spaces between the spikes but also the internal pores of the film, leading to a decrease in the contact angle. We call this phenomenon as super-nanohydrophilicity [51,53–55]. In contrast, the wettability of the surface treated with both plasma and annealing recovered to that of the untreated surface. This may be attributed to pore blocking, which is likely caused by the annealing treatment, our another idea. The volume of film shrinkage should correspond to the volume of the blocked pores. As shown in Figure 7, the volume shrinkage is about 4%. The decrease in film thickness observed in the untreated PMMA film is likely due to the large number of pores on the surface. The volume shrinkage could be caused by pore blocking. As the film thickness decreases with increased plasma irradiation cycles, no further volume shrinkage was observed, suggesting that the pores are confined to the surface side of the PMMA film [51]. Although water droplets attempt to percolate between the spikes and into the internal pores, the pores are already blocked. Consequently, the trapped air between the water and the spikes prevents further water penetration. This produces the Laplace pressure and is generally seen on hydrophobic surfaces [63]. These experimental facts can support the validity of our explanation.

4.3. Antimicrobial Performance

The bactericidal effects of both natural and synthetic nanopillars have been thoroughly reviewed by Tripathy et al. [9]. However, the complete elucidation of the fundamental mechanisms underlying microbial cell death on such surfaces has not yet been achieved. Several mechanisms have been proposed, but the contributions of factors such as wettability and surface roughness to the bactericidal activity of nanostructured surfaces remain subjects of ongoing debate [64–69]. Our experimental results support the importance of both microstructure and hydrophobicity because *E coli* are gram-negative bacteria that can multiply in water. Under these conditions, it is believed that the surface microstructures contribute to mechanical damage to bacterial cells, resulting in antibacterial activity [5,12]. According to them, droplets are partially supported by surface nanostructures and partially suspended over trapped air pockets beneath the liquid. The presence of these air pockets minimizes the effective contact area between the liquid (e.g., a droplet containing bacteria) and the surface, thereby reducing interfacial adhesion. Both wettability and microstructure may be crucial factors contributing to the observed antimicrobial properties. Starting with this work, hereafter, we would like to investigate the antibacterial performance of the surface produced by APLTP against bacteria other than *E. coli*.

5. Conclusions

In this study, we demonstrated the fabrication of cicada wing-inspired microstructures on polymethyl methacrylate (PMMA) films using atmospheric-pressure low-temperature plasma (APLTP) without relying on conventional lithographic processes. Plasma treatment successfully generated sharp-edged microstructures, while subsequent annealing modified the surface morphology and wettability by inducing densification and pore closure.

The plasma-treated surfaces exhibited increased hydrophilicity due to enhanced surface roughness and capillary-driven infiltration into micropores. After annealing, the wettability reverted to near-initial levels, likely due to pore blocking associated with thermal shrinkage. Antimicrobial evaluation revealed that while plasma treatment alone moderately reduced bacterial adhesion, the combination of plasma treatment and annealing resulted in bacterial colony counts below the detection limit, indicating highly effective antimicrobial performance.

These findings highlight APLTP as a scalable and versatile approach for engineering functional polymer surfaces with antimicrobial properties, bypassing the material and geometric constraints of lithographic methods. This work contributes to the advancement of biomimetic surface engineering and suggests a promising route for the practical development of antimicrobial coatings for large-area polymeric materials. Further research will focus on understanding the underlying bactericidal mechanisms and optimizing process parameters for specific application demands.



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