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## Article

# Evaluation of Selenium Coating on Titanium Miniplates and Screws—An In Vitro Study

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**Abstract:** This in vitro study examined three titanium miniplate systems: Leforte (CMF Leforte system) (Group A), Synthes (DePuy Synthes Co. Zuchwil, Switzerland) (Group B), and Stryker (Stryker Leibinger Inc) (Group C). Each system was divided into control (uncoated) and test (selenium-coated) groups, using 4-hole, 1.5 mm thick plates with 6 mm screws. Surface characteristics and antimicrobial efficacy were assessed through scanning electron microscopy (SEM), energy-dispersive X-ray analysis (EDX), and attenuated total reflectance-Fourier transform infrared spectroscopy (ATR-FTIR), and microbial tests, with statistical analysis via IBM SPSS (version 26). Results showed significant selenium uptake, with uniform uptake in Groups B and C and irregular uptake in Group A. ATR-FTIR indicated chemical changes in the selenium-treated titanium. Group A had the highest scratch resistance (21.156 N) and coating thickness (37.113  $\mu$ m). All selenium-coated groups demonstrated antimicrobial efficacy ( $p < 0.05$  or 0.016). The findings suggest selenium coating on titanium miniplates improves surface characteristics and antimicrobial efficacy, potentially lowering postoperative infection risks.

**Keywords:** Selenium; surface coating; miniplates; postoperative infection; maxillofacial trauma

## 1. Introduction

Cranio-maxillofacial injury [CMF] is any injury to the craniofacial region, that involves hard tissue and/or soft tissue injury and is often associated with high morbidity. Cranio-maxillofacial injuries are prevalent among trauma patients. These injuries may present independently or in conjunction with other injuries, such as spinal, abdominal, upper extremity, and lower extremity injuries [1,2].

Surgical management involves fracture site exposure, reduction, plate fixation, and soft tissue repair. The goal of open reduction and internal fixation (ORIF) is to provide stability for immediate function. In 1973, Michelet ended the search for simple osteosynthesis that would guarantee fracture healing without compression [3] which was modified, and put to practical use by Champy <sup>4</sup>. Miniplates are currently utilized to achieve stability between bony fragments in the maxillofacial region for the fixation of fractures and osteotomies [5].

Initially, stainless steel (SS) material plates and screws were utilised for fracture fixation which had several disadvantages. Thereafter, titanium (Ti) material plates which have better biocompatibility gained popularity and increased acceptance. In vitro simulation studies, animal studies as well as electrochemical studies have shown that both the implant material have the potential to corrode in body fluids [6,7]. Immuno-inflammatory reactions have also been reported following the use of titanium (Ti) and stainless steel (SS) plates and screws in fracture fixation [8,9].

Postoperative infections necessitating the need for removal of miniplate hardware have been reported to range from 10-40% with higher incidence among stainless steel plates and screws [10,11]. Infections often result from bacterial biofilms on the foreign material and adjacent bone, with bacteria such as *Staphylococcus aureus*, *Escherichia coli*, *Streptococcus salivarius*, and *Pseudomonas aeruginosa* being implicated [12]. Titanium and its alloys are favoured for biomedical use due to their mechanical

properties, biocompatibility, and corrosion resistance, leading to a decline in implant-related infections [13]. Nevertheless, additional efforts are still required to further make improvements and provide optimal outcomes.

The use of surface modifications on implant materials has gained attention as a strategy to combat biofilm formation and enhance physical and chemical properties. New antimicrobial agents, free from antibiotics, have been developed and tested [14,15]. Selenium-based compounds, recognized for anticancer activity and low toxicity, have been explored as surface coatings on titanium implants, demonstrating strong antimicrobial effects [16].

However, research on the alterations in the physical and chemical properties of selenium-coated titanium implants, as well as their antimicrobial efficacy, remains limited [17,18,19]. Thus, this study aims to assess the surface properties and antimicrobial efficacy of selenium-coated titanium miniplates and screws.

## 2. Materials And Methods

This invitro study was undertaken after obtaining ethical clearance (CSP/23/FEB/123/139) from the institutional ethics committee, Sri Ramachandra Institute of Higher Education and Research. The study involves three commercially available titanium miniplate systems namely Leforte (CMF Leforte system) (Group A), Synthes (DePuy Synthes Co. Zuchwil, Switzerland) (Group B), and Stryker (Stryker Leibinger Inc) (Group C), for all the experimental procedures. Each system was divided into a control group (uncoated) and test group (coated with selenium). All test samples were treated with commercially available selenous acid (Sigma Aldrich EC 231-974- 7). All reagents used in the procedures were analytical grade. Double distilled (DD) water was utilised for the preparation of solutions.

### 2.1. Preparation Of Selenium Coated Test Samples

Titanium miniplates and screws were polished using 0.3  $\mu\text{m}$  aluminum before being ultrasonically cleaned with double distilled water. The polished titanium surface was first etched with absolute ethanol (99.9%) for 24 hours at 24°C. The titanium samples were then rinsed with double distilled water and dried in a stream of dry air.

The test group samples were treated with a 4 mmol selenous acid solution for 6 hours at 24°C. Visual confirmation of the interaction of selenium with titanium was by the appearance of a bluish hue on the surface on the treated samples (Figure 1).



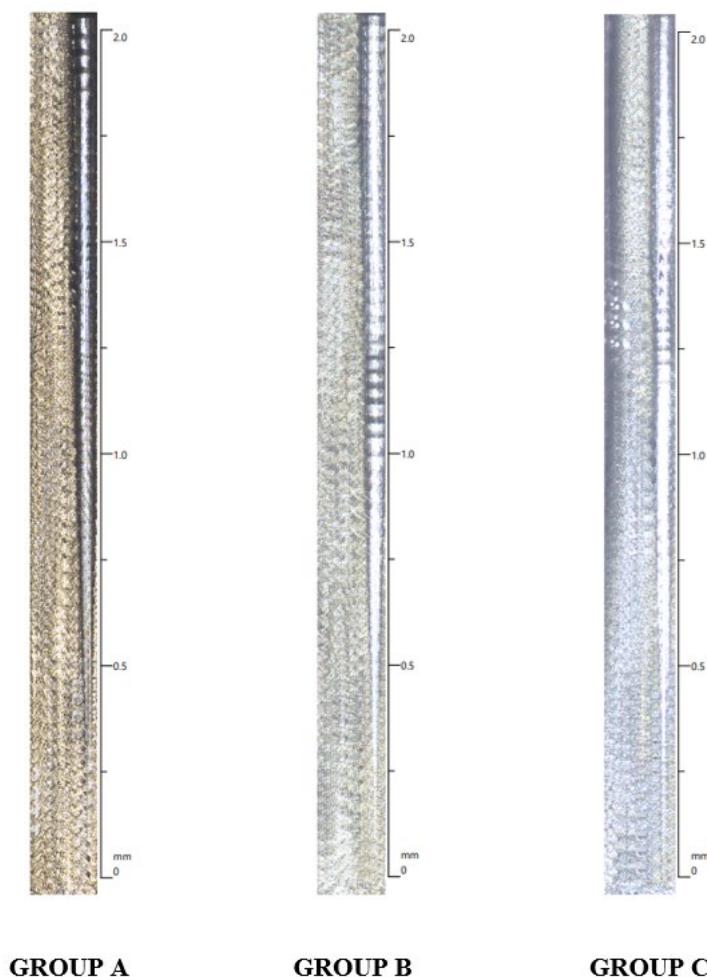
**Figure 1.** - Appearance of bluish hue on titanium sample after selenous acid treatment.

The resultant samples were then rinsed with double distilled water and dried in a stream of dry air.

## 2.2. Characterization of the Samples

Three samples from each group were used for characterization of the selenium on the titanium surface using a Scanning Electron Microscopy (Carl Zeiss Crossbeam 340) under 10, 25 and 50 $\mu$ m magnification. The qualitative analysis of the samples was performed by Fourier Transformer Infra - Red (FTIR) spectroscopy. The FTIR spectra were recorded on spectrometer, using attenuated total reflectance (ATR) mode. Measurements were performed in a spectral range of 400 –4,000 cm<sup>-1</sup> with a resolution of 4 cm<sup>-1</sup>.

Further, scratch tests were conducted using a diamond indenter with a 0.4 mm radius, applying a load that increased from 0.03 to 30 N at a loading rate of 71.3 N per minute. The scratch tracks length was set at a standard of 2mm (Figure 2).

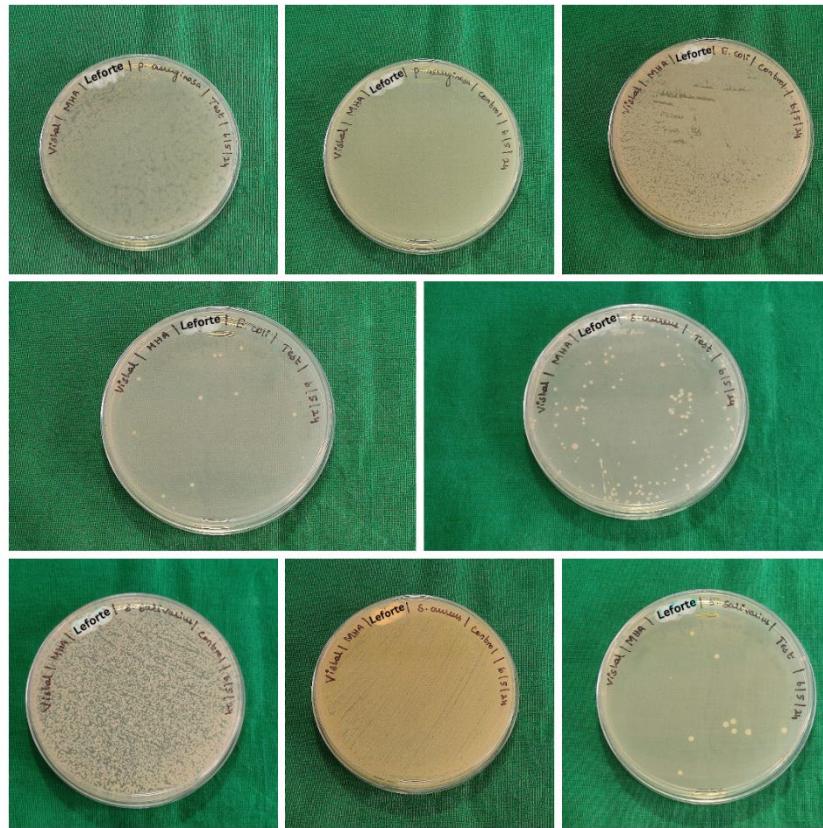


**Figure 2.** - Surface scratch test across all the three selenium coated groups.

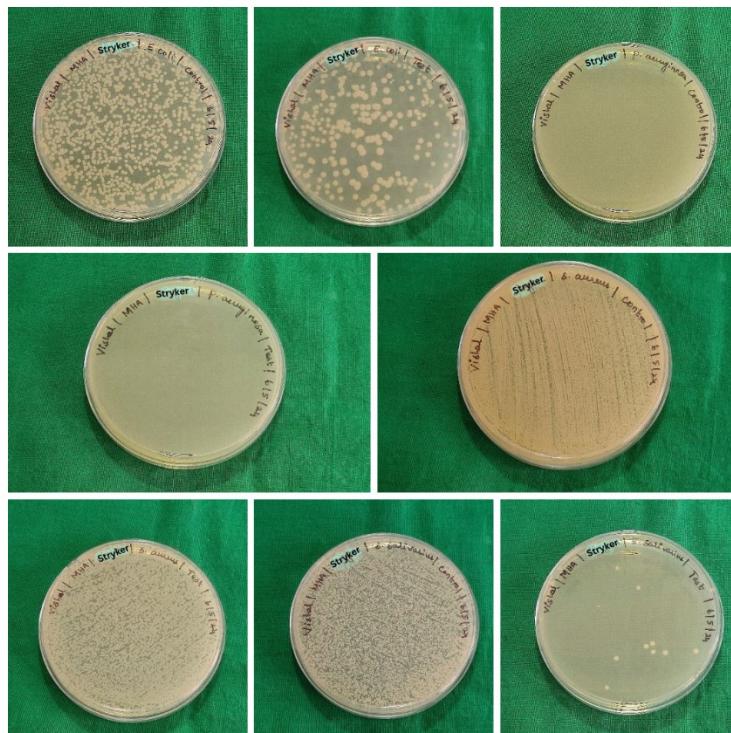
## 2.3. Antimicrobial Efficacy

The antimicrobial activity of the titanium-selenium (Ti-Se) surface was tested against the gram-negative bacteria *Escherichia coli*, gram-positive bacteria *Streptococcus salivarius*, gram negative bacteria *Pseudomonas aeruginosa* and gram-positive *Staphylococcus aureus*. The samples consist of 6 groups (five samples per group) which were immersed in sterile brain heart infusion (BHI) with fresh suspensions of the test organisms. The samples were incubated at 37°C for 5 hours to encourage the growth of biofilms. Following incubation, the samples were gently agitated, swabs were taken and lawn culture was made on the sterile Blood agar (BA) and Mueller Hinton agar (MHA). The culture

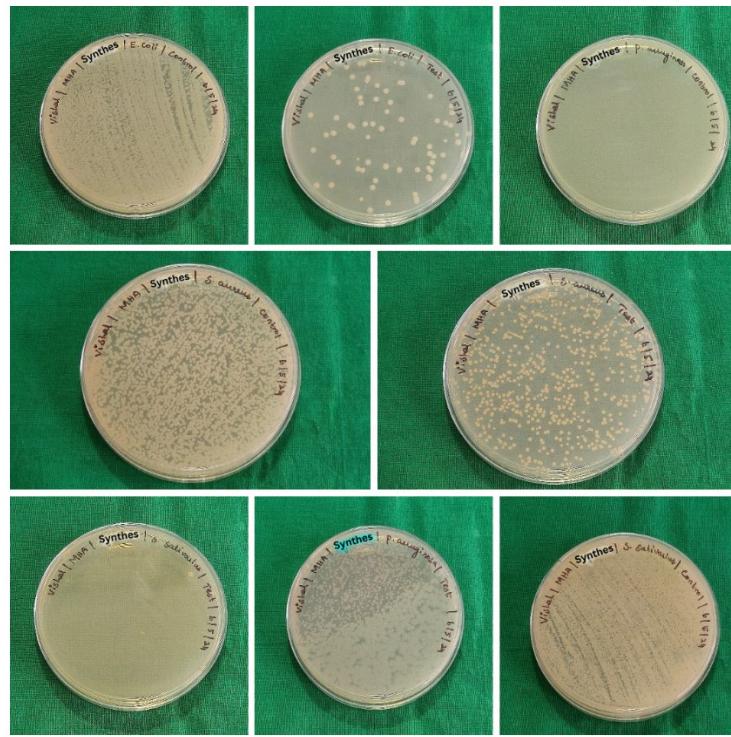
plates were incubated at 37 °C for 48 hours. After incubation, the colonies were counted and recorded as colony forming units (CFU) per ml (Figure 3,4,5).



**Figure 3.** - Culture plates with colony forming units in Group A samples.



**Figure 4.** - Culture plates with colony forming units in Group B samples.



**Figure 5.** - Culture plates with colony forming units in Group C samples.

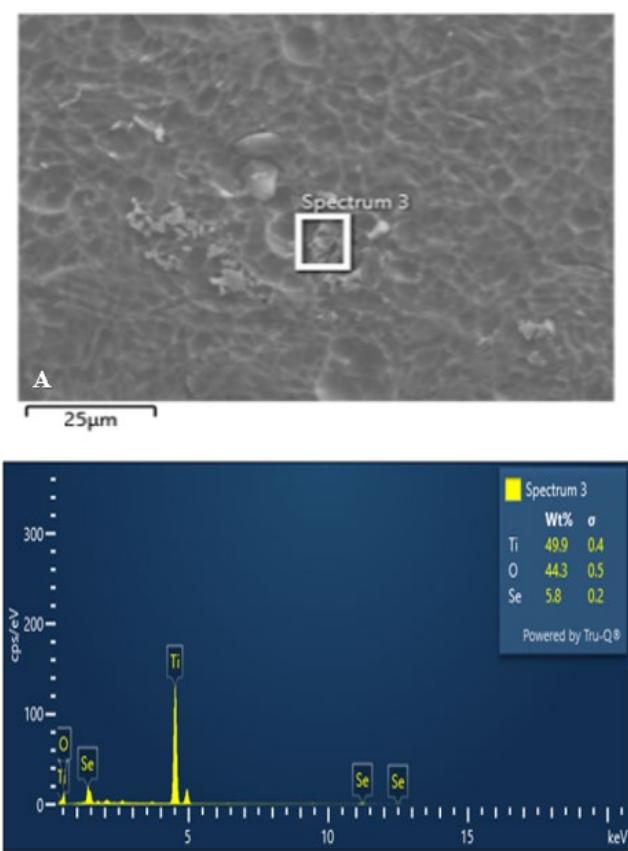
#### 2.4. Statistical Analysis

Statistical analysis was performed using IBM SPSS (version 26). Unpaired t-tests were used to compare contact angles between control and test samples across all three groups. Pairwise comparisons were employed to assess differences in penetration depth. A one-way ANOVA was conducted to analyse the comparisons of colony-forming units (CFU) among all groups.

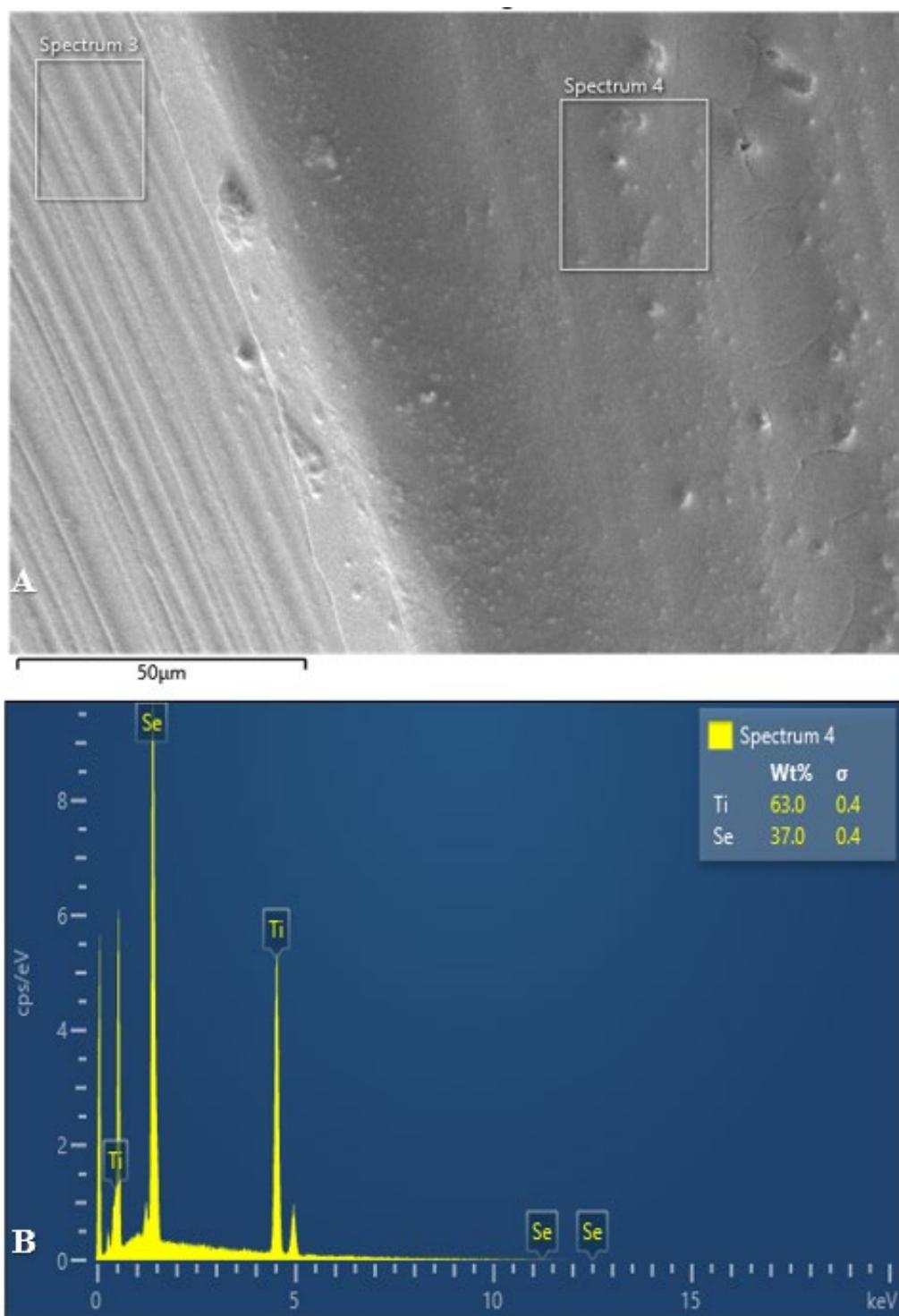
### 3. Results

#### 3.1. Scanning Electron Microscopy and Energy Dispersive X-Ray Analysis

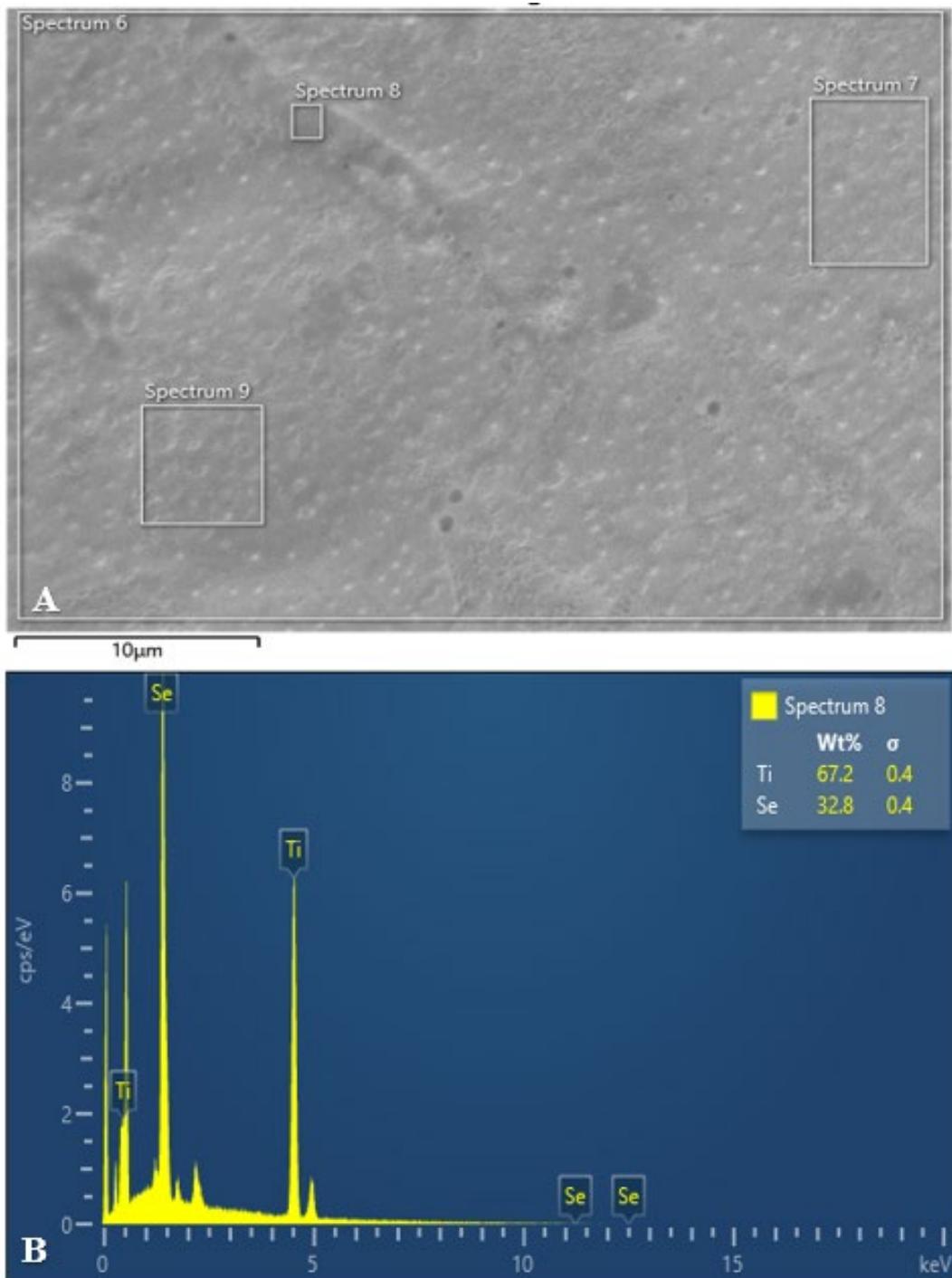
The following figures (Figure 6,7,8) present the SEM and EDX analyses of all test group samples treated with selenous acid.



**Figure 6.** - SEM image and EDX Spectrum of Group A titanium sample after treatment with selenous acid.



**Figure 7.** - SEM image and EDX Spectrum of Group B titanium sample after treatment with selenous acid.

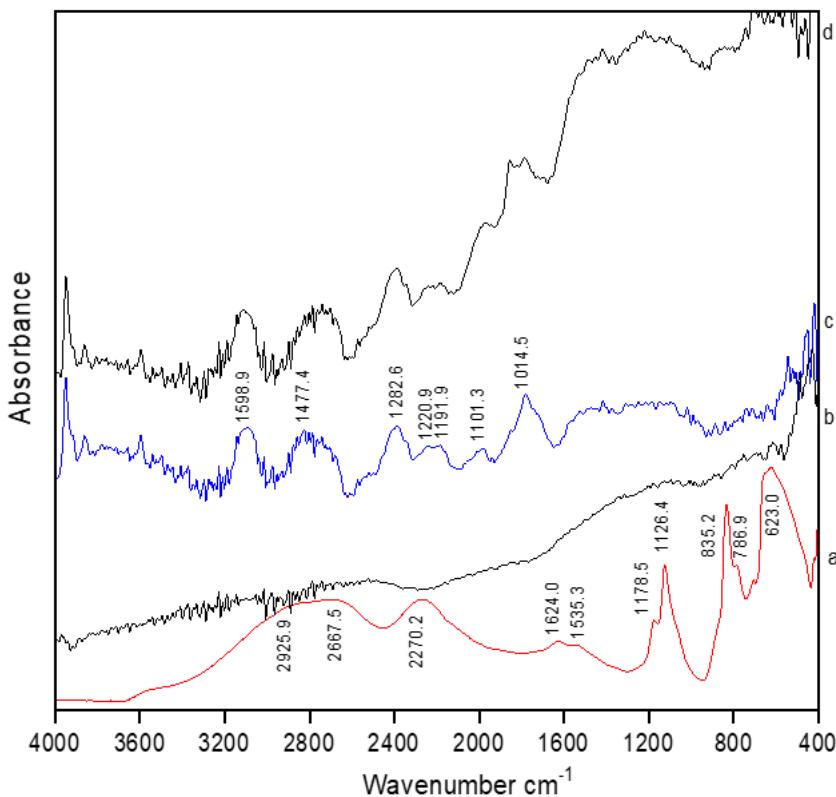


**Figure 8.** - SEM image and EDX Spectrum of Group C titanium sample after treatment with selenous acid.

It was noted that the percentage of selenium adsorption on the surface was uniform in Groups B and C. In contrast, Group A exhibited an irregular and non-uniform uptake, which may be attributed to the surface finish.

### 3.2. Fourier Transform Infrared Spectroscopy (FTIR)

The following graph (Graph 1) represents FTIR analysis of selenous acid for titanium plate & screw. Lines a,c, and d represent selenium coated titanium substrates of group A, B, and C respectively. Line b represents uncoated titanium substrate.



**Graph 1** - FTIR analysis of all three groups of titanium miniplates and screws coated with selenous acid.

The absorption observed at 2925.0 and 2270.0 cm<sup>-1</sup> in line a is due to OH stretching mode of selenous signifying the presence and uptake of selenium in the sample. The significant O-H bending modes observed at 1178.5 and 1126.4 cm<sup>-1</sup> in line c further confirms the activity of selenium.

The selenium oxide (Se-O) stretching mode observed at 835.0 and 623.0 cm<sup>-1</sup> in all three groups further confirms the findings. The observed vibrational frequencies of selenous acid matches with the reported values in literature <sup>20</sup>.

### 3.3. Scratch Test

Table 1 shows the results for scratch force and penetration depth measurements demonstrating significant differences among all the test groups.

**Table 1.** - Differences in penetration depth and scratch forces among all three groups.

PARAMETER	SAMPLES	N	MEAN	STD DEVIATION	P VALUE
LC3 In Newton	GROUP A	3	21.156	1.186	0.000
	GROUP B	3	16.493	0.604	
	GROUP C	3	15.176	0.290	
	TOTAL	9	17.608	2.805	
Penetration depth in microns	GROUP A	3	37.113	0.325	0.000
	GROUP B	3	33.873	0.410	
	GROUP C	3	23.516	1.043	
	TOTAL	9	31.501	6.178	

Significant differences were observed among the groups regarding scratch force, with Group A exhibiting the highest mean scratch force (21.156 N) compared to Groups B and C. Similarly, Group A showed the greatest mean penetration depth (37.113 microns), followed by Groups B and C. These

results indicate distinct performance characteristics among the tested groups for both penetration depth and scratch force.

### 3.4. Antimicrobial Efficacy

The colony forming units (CFU) for test and control samples analysed using unpaired t-tests for each organism across different groups revealed the following: for *Escherichia coli*, no significant difference was found between the control and test samples for group B & group A, indicated by p-values of 0.260 and 0.016, respectively. However, for group C, a significant difference was observed ( $p = 0.047$ ), suggesting a potential impact of the test conditions on *Escherichia coli* CFU counts. For *Streptococcus salivarius*, *Pseudomonas aeruginosa* and *Staphylococcus aureus*, significant differences were observed between control and test samples across all groups, as indicated by p-values less than 0.05 or 0.016 (Table 2,3,4).

**Table 2.** - Statistical analysis of CFU among Group A samples.

GROUP A	CONTROL/TEST	N	MEAN	STD DEVIATION	P VALUE
<i>ESCHERICHIA COLI</i>	CONTROL	3	616.33	54.629	0.260
	TEST	3	177.00	30.265	
<i>STAPHYLOCOCCUS AUREUS</i>	CONTROL	3	1370000	64085900	0.016
	TEST	3	1411.7	1964.71	
<i>PSEUDOMONAS AEURGINOSA</i>	CONTROL	3	4666900	80827400	0.016
	TEST	3	587	531.23159	
<i>STREPTOCOCCUS SALIVARIUS</i>	CONTROL	3	333350	57733500	0.016
	TEST	3	56.333	54.50076	

**Table 3.** Statistical analysis of CFU among Group B samples.

GROUP B	CONTROL/TEST	N	MEAN	STD DEVIATION	P VALUE
<i>ESCHERICHIA COLI</i>	CONTROL	3	616.33	54.629	0.260
	TEST	3	177.00	30.265	
<i>STAPHYLOCOCCUS AUREUS</i>	CONTROL	3	1370000	64085900	0.016
	TEST	3	1411.7	1964.71	
<i>PSEUDOMONAS AEURGINOSA</i>	CONTROL	3	4666900	80827400	0.016
	TEST	3	587	531.23159	
<i>STREPTOCOCCUS SALIVARIUS</i>	CONTROL	3	333350	57733500	0.016
	TEST	3	56.333	54.50076	

**Table 4.** - Statistical analysis of CFU among Group C samples.

GROUP C	CONTROL/TEST	N	MEAN	STD DEVIATION	P VALUE
<i>ESCHERICHIA COLI</i>	CONTROL	3	616.33	54.629	0.260
	TEST	3	177.00	30.265	
<i>STAPHYLOCOCCUS AUREUS</i>	CONTROL	3	1370000	64085900	0.016
	TEST	3	1411.7	1964.71	
<i>PSEUDOMONAS AEURGINOSA</i>	CONTROL	3	4666900	80827400	0.016
	TEST	3	587	531.23159	
<i>STREPTOCOCCUS SALIVARIUS</i>	CONTROL	3	333350	57733500	0.016
	TEST	3	56.333	54.50076	

## 4. Discussion

Initially, miniplates and screws made up of stainless-steel material were commonly used for fracture fixation [21]. While stainless steel materials are cost-effective and exhibit excellent ductility, tensile strength, and compressive strength, they have several limitations in terms of corrosion resistance, biocompatibility, fatigue limit, infection rate, and wear resistance limiting their usage in fracture fixation. However, with the introduction of titanium materials, the field of maxillofacial reconstruction was revolutionized [22]. Compared to stainless steel, titanium alloys exhibit a lower modulus of elasticity, higher strength, excellent biocompatibility, less infection rate, and superior corrosion resistance [23].

These favourable properties have led to their extensive use in clinical applications as bone plate materials [24]. Despite the numerous advantages of titanium plates over stainless steel plates, there remains a significant rate of implant removal performed (10-40%) that requires attention [25,26]. Miniplate removal may be necessitated by various factors, including infection, wound dehiscence, palpability, aesthetic concerns, patient discomfort, and neurosensory disturbances [27,28].

Among these factors, postoperative infection is the most preventable cause. Although titanium materials have shown reduced incidence of postoperative infection compared to stainless materials, the rates are still of significance and concern [29]. Infection of plates and screws may arise as a result of insufficient surgical sterility, inadequate postoperative care, and the implant material's lack of inherent antimicrobial property.

Novel compounds with antimicrobial properties have been tried as coating over the maxillofacial implant substrates [30,31,32]. Recently, selenium, a trace essential metalloid element, has emerged as a promising antimicrobial material. Selenium has garnered significant attention due to its desirable properties, including high absorption, high biological activity, and excellent biocompatibility. The superior antimicrobial capability of selenium may be attributed to cell membrane damage, inhibition of amino acid synthesis, and DNA replication caused by the overproduction of reactive oxygen species [33,34].

Therefore, this *in vitro* study was undertaken to evaluate both the antimicrobial efficacy and the surface changes resulting from selenium coating on titanium miniplates and screws. The presence of selenium over titanium miniplates and screws was confirmed by the appearance of spherical to cuboidal molecules over the surface at 10 $\mu$ m and 25 $\mu$ m magnification in all the three test groups. However, scanning electron microscopy allows for quantitative surface assessment of coated samples. But to effectively assess the chemical functionalisation of selenium and titanium, Fourier Transformer Infra-Red (FTIR) spectroscopy and Energy dispersive X-ray spectroscopy (EDX) were used in this study.

In the current study, the surface functionalisation of selenium with titanium was proved with Fourier Transformer Infra-Red (FTIR) spectroscopy and Energy dispersive X-ray spectroscopy (EDX) analysis. The coated miniplates and screws from all the three groups showed varying amounts of selenium present with Group C showing maximum uptake (Figure). Furthermore, coated screws showed more selenium absorption when compared to coated plates in all the three groups which may be attributed to the difference in surface area.

In general, according to literature, postoperative infection is the most common indication for plate removal. Ironically, it is also the most preventable. Some authors advocate the routine removal of miniplates and screws to avoid this potential undesirable complication [35,36]. A variety of microorganisms have been associated with infection of miniplates in the maxillofacial region [37]. The challenge lies in the ability to distinguish and cultivate these locally clustered bacteria because they are frequently metabolically inactive.

Thus, an implant material that has antibacterial characteristics while still preserving acceptable mechanical qualities and biocompatibility is desirable. The results of this study show that selenium as a surface coating can significantly reduce the bacterial colony count of *Staphylococcus aureus*, *E. coli*, *Streptococcus salivarius*, and *Pseudomonas aeruginosa* on titanium miniplates and screws.

The concentration of selenium used in this study at which significant bacterial load reduction occurred is relatively less compared to the value reported by Wang and Webster et al and Tran PA et al [38,39].

One of the most important characteristics of surface coating is its close adherence to the underlying material. Thus, to evaluate surface adherence as well as the strength of selenium coating, scratch tests were performed. In the current study, surface changes indicating removal of selenium coating was observed in the range of 10-20 newton with Group A showing highest resistance. Forces in the range of 100-200 newton are observed to torque screws and plates in desired position [40]. This in comparison with forces at which selenium coating shows surface changes is significantly less. This may signify the suitability of selenium coated plates and screws for self-drilling systems may be of limited use.

On assessing the depth of penetration, the surface coating was observed to be of mean thickness of 30 microns with Group A demonstrating the maximum thickness (37.113 microns). Thus, we demonstrated that selenium coatings exhibit excellent adhesion to the underlying titanium substrate; however, their capacity to withstand substantial forces may be questionable.

Furthermore, clinical trials are necessary to ascertain the definitive antimicrobial effects of these selenium-coated plates and screws to support their broader application. Further research into optimizing the surface coating protocol could enhance efficacy while minimizing surface alterations of these plates and screws. Moreover, investigating the incorporation of selenium into the titanium substrates, rather than merely surface coating, could offer a more comprehensive understanding of the material's effectiveness.

## 5. Conclusions

This study establishes a proof of concept that selenium coating on titanium miniplates and screws may offer significant advantages. Although the selenium coatings demonstrated good adherence, they may not withstand substantial forces, indicating potential limitations for self-drilling applications. Importantly, selenium coated titanium plates and screws showed a significant reduction in bacterial colony counts of common pathogens, including *Streptococcus salivarius*, *Pseudomonas aeruginosa*, *Staphylococcus aureus*, and *Escherichia coli*. Overall, selenium appears to be a promising antimicrobial coating for titanium implants, with the potential to reduce infection rates and subsequently lower the incidence of miniplate removal.

**Conflicts of Interest:** The authors declare no conflicts of interest.

**Author Contributions:** Conceptualization, Vishal Ramachandran, Deepak Chandrasekaran, Ravindran Chinnasamy and Naveen Kumar Jayakumar; Data curation, Vishal Ramachandran; Formal analysis, Vishal Ramachandran, Ravindran Chinnasamy and Naveen Kumar Jayakumar; Investigation, Deepak Chandrasekaran, Ravindran Chinnasamy and Naveen Kumar Jayakumar; Methodology, Vishal Ramachandran, Deepak Chandrasekaran, Ravindran Chinnasamy and Naveen Kumar Jayakumar; Resources, Naveen Kumar Jayakumar; Supervision, Deepak Chandrasekaran, Ravindran Chinnasamy and Naveen Kumar Jayakumar; Visualization, Deepak Chandrasekaran; Writing – original draft, Vishal Ramachandran, Deepak Chandrasekaran, Ravindran Chinnasamy and Naveen Kumar Jayakumar; Writing -review & editing, Vishal Ramachandran, Deepak Chandrasekaran, and Ravindran Chinnasamy.

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