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Article

Physical Properties and pH Environment of Foam Dressing Containing *Eclipta prostrata* Leaf Extract and Gelatin

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Abstract: *Eclipta prostrata* (*E. prostrata*) has several biological activities, such as antibacterial and anti-inflammatory activities, which improve wound healing. In addition, physical properties and pH environment are also crucial for developing wound dressings containing medicinal plant extracts to create an appropriate environment for wound healing. In this study, we prepared foam dressing containing *E. prostrata* leaf extract and gelatin. Chemical composition was verified using Fourier transform infrared spectroscopy (FTIR), and pore structure was obtained by scanning electron microscopy (SEM). The physical properties, including absorption and dehydration properties, were also evaluated. The chemical properties were measured to determine the pH environment after being submerged with *E. prostrata* dressings. The results revealed that the *E. prostrata* dressings had a pore structure with an appropriate pore size ($313.25 \pm 76.51 \mu\text{m}$ and $383.26 \pm 64.45 \mu\text{m}$ for the *E. prostrata* A and *E. prostrata* B dressings, respectively). The *E. prostrata* B dressings showed a higher percentage of weight increase in the first hour and a faster dehydration rate in the first 4 hours. Furthermore, the *E. prostrata* dressings make a slightly acidic environment (5.28 ± 0.02 and 5.38 ± 0.02 for the *E. prostrata* A and *E. prostrata* B dressings at 48 hours, respectively).

Keywords: *Eclipta prostrata*; gelatin; foam dressing; wound dressing; physical property; absorption; dehydration; pH environment

1. Introduction

Plant-based biomaterials have several benefits over synthetic materials, such as cost-effectiveness, safety for humans, and environmentally friendly [1]. In addition, developing novel wound dressings containing medicinal plant extracts can improve clinical outcomes and plant value [2,3]. In this study, we are interested in *Eclipta prostrata* L. (*E. prostrata* L.) due to their pharmacological properties. *E. prostrata* L., commonly known as False daisy, Ink plant, Bhringraj, Bhumiraj, Aali jhar, or Nash jhar, is a herbaceous plant that belongs to the family Asteraceae [4]. It is a weed that grows in moist places such as rivers, marshes or the edge of rice fields [4,5]. It is found in many parts of the world, including Thailand, China, India, Nepal, and Brazil [4]. It has been long used in several diseases such as coronary heart disease, diabetes, gastrointestinal diseases, respiratory diseases, skin diseases, and wounds [5]. The leaves have various biological activities, including antibacterial, antifungal, and anti-inflammatory activities, which improve wound healing [6–9]. Therefore, wound dressing containing *E. prostrata* L. extract will be used for treating infection and inflammation in wound healing. Kang et al. [10] suggest that *E. prostrata* L. extract is a potential treatment for inflammatory skin conditions such as atopic dermatitis. The *E. prostrata* L. extract improved the allergic inflammation of the skin by restoring the skin barrier dysfunction, decreasing epidermis/dermis thickness, and regulating the immune balance [10]. Raoul et al. evaluated wound healing in rats after applying the ointment containing *E. prostrata* leaf extract [11]. The results showed

that the wounds treated with medicinal ointment completely healed faster than vaseline® and cicatryl® [11]. Babu et al. [12] developed the hydrogel containing *E. prostrata* leaf extract and evaluated its physical properties such as pH, viscosity, and spreadability. However, no studies have developed wound dressing containing *E. prostrata* leaf extract in sheet form or foam dressings. Wound dressing selection is based on the wound's cause, location, healing phase, exudate level, pain, odor, infection, size, and depth [13]. For deep or tunneling wounds, packing wounds with dressing in the form of rope is essential for promoting wound healing from the inside out [14]. On the other hand, superficial or partial-thickness wounds require dressing in the form of a sheet to cover the wound and facilitate wound function [15]. In addition, choosing the physical characteristics of wound dressings according to the exudate level will provide the optimum environment for facilitating wound healing.

Referring to our previous point, the development of foam dressing for wound healing applications should focus on physical properties. According to ideal wound dressing properties, the wound dressings should be able to absorb wound exudate to prevent maceration (softening and breaking down of the surrounding skin because of prolonged exposure to moisture), malodor, local wound infection, and delayed wound healing [15–19]. However, different absorption properties of wound dressings are appropriate for different types of wounds [16,20,21]. For example, a wound dressing with a high absorption capacity should be selected for wounds with a high level of exudate. Additionally, the dehydration rate of wound dressing is also an important property that maintains a moist wound-healing environment [22]. A moist wound environment has several benefits, including increased keratinocyte migration and re-epithelialization, increased collagen synthesis, increased autolytic debridement, reduced pain, and decreased inflammation [23,24].

Moreover, elevated exudate pH correlates with an increased risk of infection and delayed wound healing [25,26]. Therefore, the ideal wound dressing should not provide an alkaline wound environment. Foam dressing's porous structure is also an essential factor in the wound-healing process [27,28]. The wound-healing process is a complex biological process to recover damaged tissues and restore the skin's normal function. The wound-healing process consists of four continuous and overlapping phases, including hemostasis, inflammation, proliferation, and remodeling [29]. The appropriate pore size of the porous structure is essential for the proliferative phase. Natural and synthetic polymers are both used in wound dressings, and each type of polymer can help to produce a porous structure. Natural polymers are commonly chosen for wound dressing development, such as chitosan, cellulose, hyaluronic acid, collagen, alginate, and gelatin [30]. Gelatin could be used to produce porous structures with the freeze-drying technique [31,32]. The porous gelatin materials support cell migration and the development of new tissue [33]. Interestingly, gelatin could also provide biodegradable and biocompatible material [31,34]. Thus, the present study aimed to develop a foam dressing containing *E. prostrata* leaf extract and gelatin, and their physical properties and pH wound environment were subsequently evaluated. The results from this study could deliver the profile of physical characteristics and pseudo-wound environment after being treated with foam dressing containing *E. prostrata* leaf extract and gelatin.

2. Results

2.1. Thickness test

The composition of prepared foam dressings containing *E. prostrata* leaf extract and gelatin is shown in Table 1. The *E. prostrata* A dressing had a lower concentration of *E. prostrata* leaf extract than The *E. prostrata* B dressing. The *E. prostrata* dressings were soft and flexible. The *E. prostrata* A dressing had a thickness of 4.236 ± 0.0519 mm, and the *E. prostrata* B dressing had a thickness of 3.945 ± 0.1403 mm. The *E. prostrata* A dressing was thicker than the *E. prostrata* B dressing.

2.2. Fourier Transform Infrared Spectroscopy (FTIR)

Table 1 shows the FTIR peak values and functional groups of the *E. prostrata* leaf extract and the *E. prostrata* A and B dressings. Figure 1 shows the FTIR spectra of the *E. prostrata* leaf extract. Figure 2 shows the FTIR spectra of the *E. prostrata* A and B dressings. After mixing between gelatin and *E.*

prostrata leaf extract and then lyophilization or freeze drying, Figure 2 showed an increased intensity in the functional groups, including amide I (1646.91 cm^{-1} and 1647.22 cm^{-1} for the *E. prostrata* A and B dressings respectively), and amide II (1553.43 cm^{-1} and 1554.20 cm^{-1} for the *E. prostrata* A and B dressings respectively). The amide I (mainly related to the C=O stretching vibration) and II (mainly related to the N-H bending vibration and the C-N stretching vibration) bands are associated with the presence of gelatin [35,36].

Table 1. FTIR peak values and functional groups of the *E. prostrata* leaf extract and the *E. prostrata* A and B dressings.

Functional groups	Peak values		
	<i>E. prostrata</i> leaf extract	<i>E. prostrata</i> A dressings.	<i>E. prostrata</i> B dressings.
Alkane	1376.65	1378.70	1378.60
	2877.87	2933.99	2933.97
	2931.46	2973.15	2973.45
	2971.77		
Alkene	1654.70	1646.91	1647.22
Halo compound	802.76	837.56	837.51
	837.70		

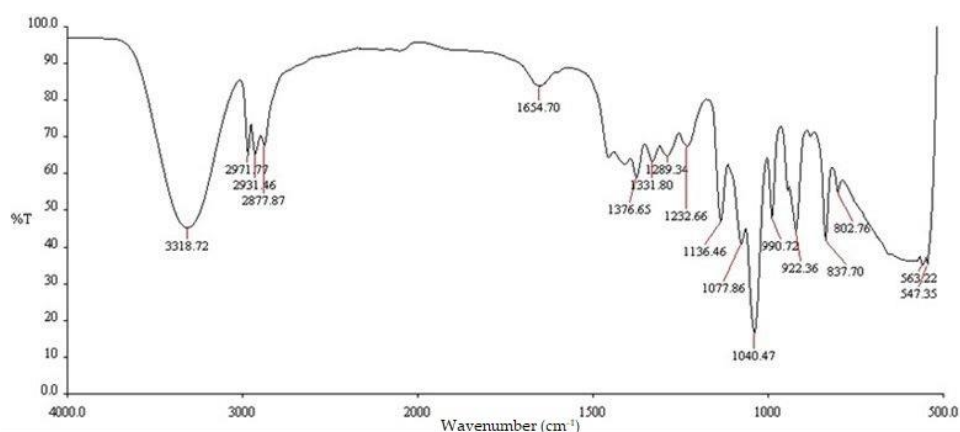


Figure 1. FTIR spectra of the *E. prostrata* leaf extract.

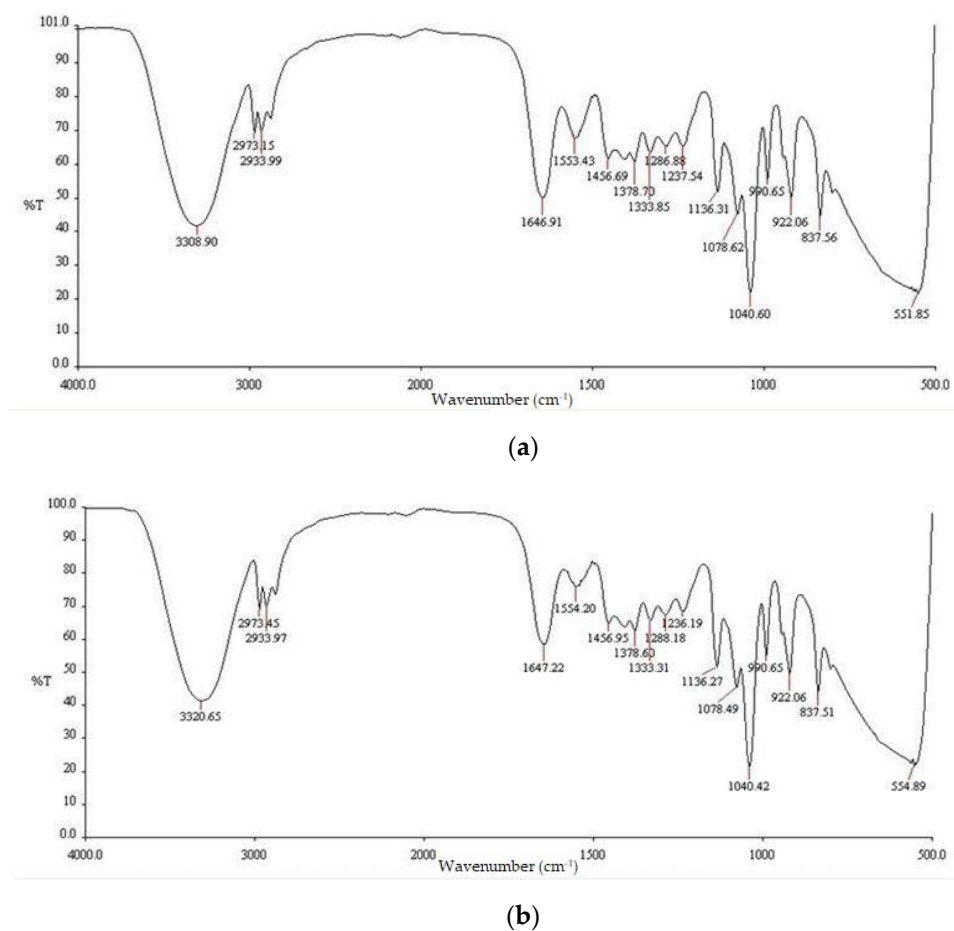


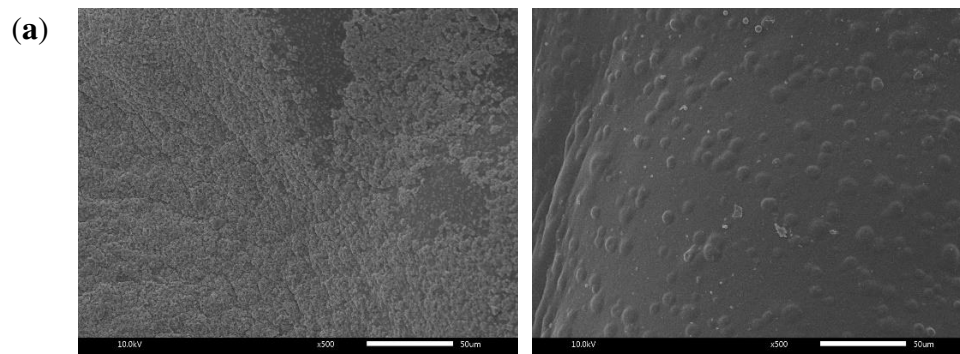
Figure 2. FTIR spectra of the (a) *E. prostrata* A dressing and (b) *E. prostrata* B dressing.

2.3. Morphological Properties

The surface and cross-sectional morphologies of *E. prostrata* dressings were observed using SEM (Figure 3). The size, shape, and distribution of pores are shown in Figure 3b. The average pore sizes were $313.25 \pm 76.51 \mu\text{m}$ and $383.26 \pm 64.45 \mu\text{m}$ for the *E. prostrata* A and B dressings, respectively (Figure 3b). The *E. prostrata* B dressing had more consistent porosity than *E. prostrata* A dressing.

E. prostrata A

E. prostrata B



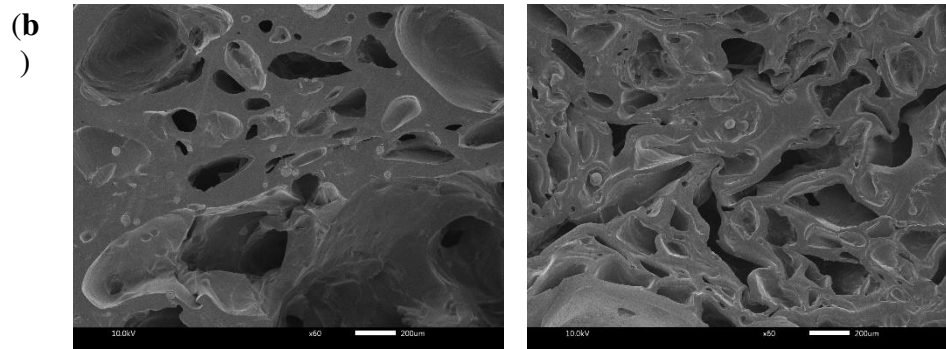


Figure 3. Morphological observation of (a) surface and (b) cross-section of *E. prostrata* dressings by SEM.

2.4. Absorption Properties

The absorption properties determine how well the dressing can manage the wound exudate and promote wound healing. The percentage of weight increase of the *E. prostrata* dressing for different periods is shown in Figure 4. The *E. prostrata* A dressing showed a lower percentage of weight increase than the *E. prostrata* B dressing. The higher *E. prostrata* leaf extract promotes the higher absorption capacity.

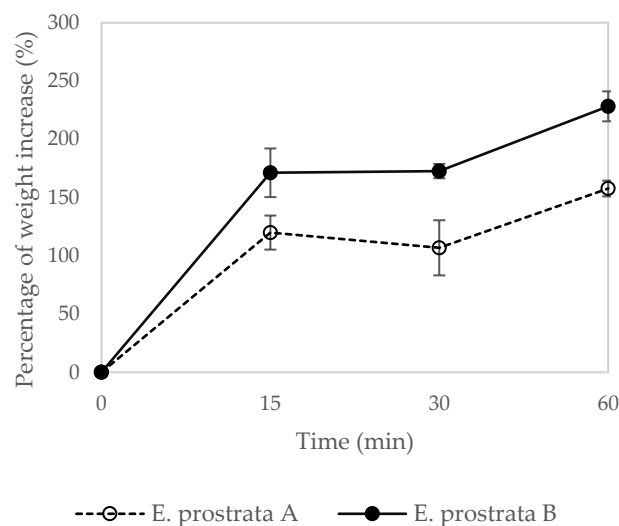


Figure 4. Absorption properties of *E. prostrata* A and B dressings.

2.5. Dehydration Properties

The dehydration rate of the *E. prostrata* dressing for different periods is presented in Figure 5. The *E. prostrata* B dressing showed a higher dehydration rate in the first 4 hours than the *E. prostrata* A dressing. The higher *E. prostrata* leaf extract promotes the higher dehydration rate.

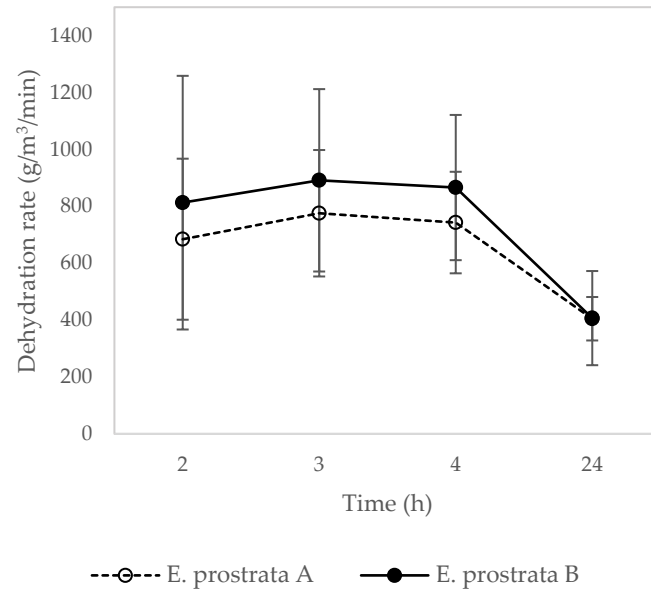


Figure 5. Dehydration properties of E. prostrata A and B dressings.

2.6. pH measurement

Figure 6 demonstrates the pH of deionized water submerged with the E. prostrata dressings. The pH of the deionized water submerged with the E. prostrata A dressing was decreased from 7.55 ± 0.16 to 5.28 ± 0.02 . In the same way, the pH of deionized water submerged with the E. prostrata B dressing was decreased from 7.69 ± 0.24 to 5.38 ± 0.02 .

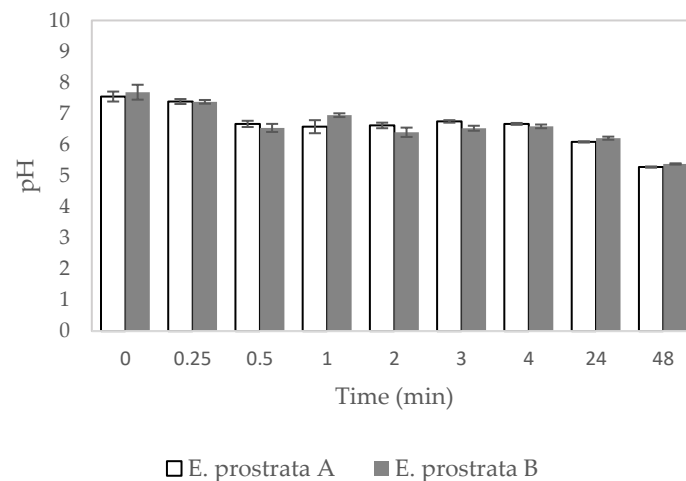


Figure 6. The pH of deionized water submerged with the E. prostrata A and B dressings.

2.7. Dispersion Characteristics

The dispersion characteristics of the E. prostrata dressings are shown in Figures 7 and 8. The E. prostrata A and B dressings did not change much from their original structure after they were immersed in pseudo-wound exudate for 60 seconds at 100 revolutions per minute (Figure 7). However, the spectra of the pseudo-wound exudate after being submerged with the E. prostrata A and B dressings were not similar to those of the pseudo-wound exudate (Figure 8).



Figure 7. Dispersion Characteristics of **(left)** E. prostrata A and **(right)** E. prostrata B dressings.

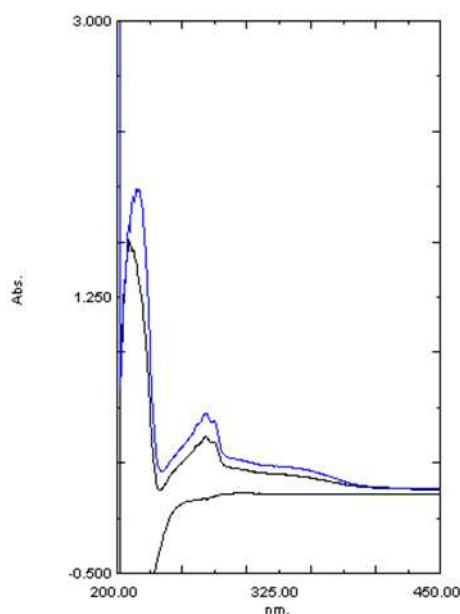


Figure 8. Dispersion Characteristics compared with a pseudo-wound exudate. Spectrum of **(bottom line in black)** NaCl/CaCl₂·H₂O solution, **(blue line)** NaCl/CaCl₂·H₂O solution after submerged with the E. prostrata A dressing, and **(upper line in black)** NaCl/CaCl₂·H₂O solution after submerged with the E. prostrata B dressing.

3. Discussion

E. prostrata leaf extract has been studied for its potential wound-healing benefits, including antimicrobial, and anti-inflammatory properties [6–9]. Prior studies in developing wound healing products containing E. prostrata focus only on ointment and hydrogel formulation [11,12]. Nowadays, no studies have developed wound dressing containing E. prostrata leaf extract in sheet form or foam dressings. Developing wound dressing in sheet form has several advantages, such as preventing trauma, minimizing external contamination, absorbing exudate, and keeping a wound in an optimally moist environment [16].

In this study, the foam dressing containing E. prostrata extract and gelatin was developed to evaluate the physical properties and pH wound environment. Result of the general appearance, the E. prostrata dressings were soft and flexible. These properties help to maintain a moist wound environment, reduce the risk of maceration, and allow use in the movement areas such as the knee or elbow [37]. In addition, the E. prostrata A dressing was thicker than the E. prostrata B dressing. It would be explained by the high protein content in bovine gelatin increased the polymer matrix's solids content. Hence, the increase in gelatin or protein concentration has induced an increase in the

thickness of the foam dressing [38]. However, the thickness was unrelated to the absorption and dehydration properties, as shown in Figures 4 and 5.

The FTIR spectra are used to identify the functional groups present in the *E. prostrata* dressing, as compared to the *E. prostrata* leaf extract. It was found that the FTIR spectra of *E. prostrata* dressing had an increased intensity in the functional groups, including amide I and II (Figure 2). The amide I and II bands in the FTIR spectrum are commonly used to identify the presence of gelatin [35,36]. The amide I band in FTIR spectra is a strong absorption peak corresponding to the stretching vibration of the C=O bond in the peptide backbone [39]. This band of gelatin appears in the region of 1600-1700 cm^{-1} [35]. As shown in Figure 2, the amide I band was around 1646-1648 cm^{-1} , indicating the presence of a predominantly random coil structure [39]. The amide II band in the FTIR spectra also provide information on the vibrational bands of the protein backbone [39]. This band corresponds to the bending vibration of the N-H bond (40–60 % of the potential energy) and the stretching vibration of the C-N bond (18–40 %) in the protein backbone [39]. In the case of gelatin, the amide II band appears in the region of 1565–1520 cm^{-1} [35]. As shown in Figure 2, the amide II band was around 1553-1555 cm^{-1} . The amide II is often used in combination with the amide I band to confirm the presence of gelatin. Therefore, it indicates that our process to develop *E. prostrata* dressing did not affect the structural property of gelatin. Gelatin could provide a porous structure and produce biodegradable and biocompatible material [31,34].

The resulting SEM image provides information about the morphology or porous structure of the *E. prostrata* dressing (Figure 3). The porous structure is crucial in wound healing because it allows cell migration and proliferation [28,40]. When a wound occurs, the first phase of wound healing is hemostasis, with vascular constriction, platelet aggregation, degranulation, and fibrin clot formation [29]. Hemostasis helps to stop bleeding, and inflammatory cells, namely neutrophils, monocytes, macrophages, and lymphocytes, migrate into the wound, which triggers the inflammatory response (also known as the “inflammatory phase”) [29]. The next phase is proliferation, with re-epithelialization, angiogenesis, collagen synthesis, and extracellular matrix (ECM) formation, which generally overlaps with the inflammatory phase [29]. The porous structure supports this phase. Fibroblasts and endothelial cells need to migrate into the wound bed in order to proliferate and form granulation tissue at the site of injury [29]. A porous structure advantage allows for these cells to migrate into the wound bed, promoting efficient wound healing. Following cell proliferation, the final phase is remodeling, with collagen remodeling and vascular maturation, and regression [29]. A previous study by Murphy et al. [41] showed that a mean pore size of 325 μm facilitated the highest cell attachment and proliferation compared with pores in the 85-190 μm . As seen in Figure 3b, our SEM images of the cross-section show the average pore sizes of around 300 μm . This was supposed that the *E. prostrata* A and B dressings had an appropriate pore size for efficient wound healing. Nevertheless, the *E. prostrata* B dressing was more consistent porosity than *E. prostrata* A dressing. The effect of this difference in porosity between the *E. prostrata* A and B dressings could exhibit differences in absorption ability.

We developed the *E. prostrata* dressing that was designed with a porous structure in order to increase the absorption ability. In this study, the absorption ability was obtained by using pseudo-wound exudate. The *E. prostrata* B dressing exhibited a stronger absorption ability than the *E. prostrata* A dressing (Figure 4). The absorption ability of the *E. prostrata* B dressing was derived from a higher-density porous structure (Figure 3b). The ideal wound dressing properties must absorb excess wound exudate and provide a moist environment [18,21,22,42]. Wound exudate or wound drainage is the fluid that discharges from a wound during the healing process [43]. The mechanism of exudate formation is usually due to inflammation or infection [43]. The amount of exudate produced can vary depending on the type and severity of the wound. A moist wound environment is necessary for the wound-healing process to occur effectively. An optimal moisture level enhances cell migration and proliferation, reduces pain and discomfort, and reduces infection rates [22,23]. Macerated peri-wound skin can lead to an increased risk of infection, whereas desiccated peri-wound skin can lead to decreased epithelial migration and cell death [22,44]. Therefore, the selection of absorbent wound dressing depends on the amount of exudate to prevent maceration and desiccation.

Moreover, a moist environment promotes autolysis or breakdown of necrotic tissue, called autolytic debridement [23,45]. In our previous work [20], the commercial hydrocolloid dressing and hydrocolloid with foam layer dressing had the lowest absorption capacity. Therefore it is an appropriate dressing for wounds with a low amount of exudate. In this study, both the *E. prostrata* A and B dressings had absorption characteristics similar to commercial hydrocolloid dressing and hydrocolloid with foam layer dressing [20]. These absorption characteristics meant that both the *E. prostrata* A and B dressings would be chosen for wounds with low exudate.

Apart from absorption properties, the dehydration rate is also essential to control the moisture balance of the wound and enhance wound healing due to water-retaining properties [22,46]. This can be achieved through the use of appropriate wound dressings that are designed to manage moisture levels and prevent dehydration. In addition, the selection of wound dressing also depends on the amount of exudate produced by the wound. The *E. prostrata* B dressing showed a higher dehydration rate than the *E. prostrata* A dressing. It can be explained by the higher-density porous structure of the *E. prostrata* B dressing (Figure 3b). Therefore, the *E. prostrata* B dressing would have the ability to dehydrate exudate to create a moist wound-healing environment rapidly.

Furthermore, the pH wound environment would be an essential factor for wound healing. The pH of healthy human skin is in the range of 5.4-5.9, which is slightly acidic. [47]. *Propionibacterium* is commonly found on human skin. *Propionibacterium* grows well at pH 6.00-6.50 [48]. *Staphylococcus aureus* is a pyogenic bacteria [49]. *S. aureus* prefers a neutral pH environment for optimal growth and survival [50]. Thus, an acidic environment is not favorable for harmful bacterial growth. In addition, the pH environment of chronic wounds exists at a range of 7.15-8.90, which is alkaline and chronic wounds are characterized by excessive protease activity [51-55]. Sim et al. found that faster recovery of wounded tissues was observed in wounds treated by pH 4 buffers compared to pH 6 buffers [25]. A previous study by Leveen et al. showed that a slightly acidic environment significantly inhibits protease activity and may potentially enhance the healing of cutaneous wounds [56]. Previous studies reported fibroblast proliferation and migration behaviors associated with the acidic environment [57,58]. It means rapid wound healing occurs in an acidic environment [25,54]. We found that the *E. prostrata* A and B dressings showed similar pH decreases continuously over the period. Our *E. prostrata* dressings tend to create a slightly acidic environment. Hence, this was supposed that the *E. prostrata* A and B dressings would not interfere wound healing process.

The dispersion of the wound dressing refers to how well the dressing covers the wound surface. In this study, the spectra of the pseudo-wound exudate after being submerged with the *E. prostrata* A and B dressings were not similar to those of the pseudo-wound exudate (Figure 8). In our previous study, commercial alginate dressings also had the spectra of the pseudo-wound exudate after being submerged with the dressings not quite similar to those of the pseudo-wound exudate [20]. Nevertheless, after interacting with the pseudo-wound exudate, the *Eclipta prostrata* A and B dressings did not change much from their original structure (Figure 7). It means that the *E. prostrata* dressing will not be difficult to remove. According to the spectra of the pseudo-wound exudate after being submerged with the dressings, our *E. prostrata* dressings are an immediate-release formulation. The *E. prostrata* dressing should be further modified for controlled release applications by crosslinking techniques with a crosslinker, such as glutaraldehyde [59,60].

4. Materials and Methods

4.1. Materials

Gelatin (from bovine skin, gel strength 225, Type B) was purchased from Sigma-Aldrich, Inc. (St. Louis, MO, USA). *E. prostrata* leaf extract was purchased from SK Herb Co., Ltd. (Samut Sakhon, Thailand). Sodium chloride and calcium chloride dihydrate were purchased from VWR International bvba (Leuven, Belgium).

4.2. Preparation of foam dressing containing *E. prostrata* extract and gelatin

Gelatin solution (10 %w/v) was prepared by dissolving in deionized water at 40 °C and stirring continuously for 1 hour. Then, the *E. prostrata* dressing was prepared by mixing gelatin solution and *E. prostrata* leaf extract, as shown in Table 2. The mixture was stirred for 1 hour to obtain a homogeneous solution. After stirring the solution, it was sonicated to eliminate air bubbles and poured into plastic plates. The plastic plates were transferred into a freezer at -80 °C and frozen for 24 hours. The frozen solution was then lyophilized in a freeze-dryer (SHM 021) for 48 hours to become a sponge. Finally, the sponge or *E. prostrata* dressing was slowly removed from the plastic plate. In order to prevent contamination, the *E. prostrata* dressings were then stored inside an airtight container. The composition with *E. prostrata* leaf extract of more than 40 % could not prepare foam dressing.

Table 2. Composition of prepared foam dressings containing *E. prostrata* extract and gelatin.

<i>E. prostrata</i>	<i>E. prostrata</i> leaf extract : Gelatin (v/v)
A	3:7
B	2:3

4.3. Thickness Test

After lyophilization, the thickness test was performed using the Mitutoyo Dial Thickness Gauge, which provided an accuracy of 0.001 mm. Thickness was measured at five different positions (one in the center and four in the middle of each side).

4.4. Fourier Transform Infrared Spectroscopy (FTIR)

The *E. prostrata* leaf extracts and the *E. prostrata* dressings were recorded on a spectrum 100 FTIR Spectrometer (PerkinElmer Inc.) FTIR spectra were recorded from 500 to 4000 cm^{-1} .

4.5. Morphological Properties

At a voltage of 10 kV, the *E. prostrata* dressings were examined by Scanning Electron Microscope (SEM, JSM-IT300 JEOL). SEM with Energy Dispersive X-ray Spectrometer (EDS) was used to analyze the dressings with the surface (500x) and cross-sectional (60x) images. The *E. prostrata* dressing was first prepared by attaching it to the aluminium stubs and then coating it with gold. This process helps to improve the conductivity of the dressing, allowing for better imaging results. The pore sizes were measured using the Image J® software (National Institutes of Health, Bethesda, MA, USA).

4.6. Absorption Properties

The absorption properties of the *E. prostrata* dressing were examined using BS EN 13726-1: 2002, Part 1: the aspects of absorbency, Section 3.2: free swell absorptive capacities with slight modifications [61]. The *E. prostrata* dressing (2 cm×2 cm) was prepared and weighed. A test solution (8.298 g of NaCl (0.142 mol/L) and 0.367 g of $\text{CaCl}_2 \cdot 2\text{H}_2\text{O}$ (0.0025 mol/L)) was added to one liter of deionized water representing a pseudo-wound exudate. The *E. prostrata* dressing was immersed in the test solution and then incubated at 37 °C. At different periods, the dressing was removed and weighed.

4.7. Dehydration Properties

The *E. prostrata* dressing (2 cm×2 cm) was prepared and weighed. The *E. prostrata* dressing was immersed in the test solution or pseudo-wound exudate for 30 minutes. Afterward, the dressing was removed, weighed, and incubated at 37 °C. At different periods, the dressing was weighed [62]

4.8. pH measurement

The *E. prostrata* dressing (2 cm×2 cm) was suspended in deionized water at a ratio of 1:25 (w/v). At different periods, the deionized water was measured using a pH meter (pH 700) [62].

4.9. Dispersion Characteristics

The dispersion characteristics of the *E. prostrata* dressing were examined using BS EN 137262: 2002, Part 1: the aspects of absorbency, Section 3.6: dispersion characteristics with slight modifications [63]. The *E. prostrata* dressing (2 cm×2 cm) was prepared and immersed in the test solution and shaken for 60 seconds at 100 revolutions per minute. After that, the absorbance of the collected test solution was measured using a UV-spectrophotometer (UV-2501PC) by scanning between a wavelength of 200 and 450 nm.

4.10. Statistical Analysis

The experiments were performed in triplicate and represented in a mean ± standard deviation.

5. Conclusions

This study is the first development of wound dressing sheets containing *E. prostrata* leaf extract and gelatin. Our study investigated the physical properties and pH pseudo-wound environment of the *E. prostrata* dressing. Both the *E. prostrata* A and B dressings had an appropriate pore size ($313.25 \pm 76.51 \mu\text{m}$ and $383.26 \pm 64.45 \mu\text{m}$ respectively) for cell migration and proliferation in the wound healing process. The higher *E. prostrata* leaf extract produces a higher-density porous structure of foam dressing, resulting in a higher absorption capacity and faster dehydration rate. The *E. prostrata* dressings are designed for the low level of exudate due to their absorption capacity. In addition, the *E. prostrata* dressings make the environment slightly acidic. Therefore, this was supposed that our *E. prostrata* dressings would not provide favorable conditions for bacterial growth. Our results provide the wound dressing profiles that are essential for the decision of physicians to select the appropriate wound dressing according to the amount of exudate. Further experimental studies should focus on release patterns, pharmacological properties, such as antibacterial and anti-inflammatory activities, and wound healing assays.

Author Contributions: Conceptualization, S.H.; methodology, S.H.; investigation, J.S., N.S., and O.C.; resources, S.H.; data curation, S.H., J.S., N.S., and O.C.; writing—original draft preparation, S.H.; supervision, S.H.; funding acquisition, S.H. All authors have read and agreed to the published version of the manuscript.

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Data Availability Statement: The data in this study are available on request from the corresponding author.

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Conflicts of Interest: The authors declare no conflict of interest.

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