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Article

# Microwave Humidity Sensor for Early Detection of Sweat and Urine Leakage

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**Abstract:** A planar microwave sensor devoted to the detection of humidity in underwear and clothes in general is proposed. The ultimate goal of the sensor is to detect the presence of liquids in fabrics, of interest to aid patients that suffer from certain pathologies, such as hyperhidrosis and enuresis. The main target in the design of the sensor, considering the envisaged application, is simplicity. Thus, the sensor operates at a single frequency, and the working principle is the variation in the magnitude of the transmission coefficient of a matched line loaded with an open-ended quarter-wavelength sensing stub resonator. The stub, which must be in contact with the so-called fabric under test (FUT), generates a notch in the transmission coefficient with a resonance frequency that depends on the humidity level of the fabric. By designing the stub with a moderately high quality factor, the variation in the resonance frequency causes a significant change in the magnitude level at the operating frequency, the resonance frequency when the sensing stub is loaded with the dry fabric, and the presence of liquid can be detected by means of an amplitude detector. A prototype device is proposed and experimentally validated.

**Keywords:** planar microwave sensor; humidity sensor; microstrip technology; detection of sweat; detection of urine leakage; enuresis; hyperhidrosis

## 1. Introduction

Planar microwave technology is of the highest interest for the implementation of a wide variety of sensors [1,2]. Among their advantages, planar microwave sensors exhibit low cost and profile, and they can be implemented in many different types of substrates, including rigid substrates (such as low-cost FR4, or low-loss microwave substrates), or flexible substrates (including polymeric substrates, organic substrates, e.g., paper, or fabric, among others). Planar microwave sensors can be fabricated by means of either subtractive (e.g., photoetching or milling) or additive (e.g., inkjet-printing, screen-printing, or 3D-printing) processes. Moreover, planar microwave sensors are compatible with many other technologies such as microfluidics, micromachining, textiles, etc., and can be equipped with functional films, that make these sensors of interest in applications as diverse as liquid sensing [3–7], bio-sensing [8,9], gas sensing [10–16], wearables [17,22], measurement of physical variables (such as temperature or ambient humidity [23–25]), etc. Nevertheless, the most canonical application of planar microwave sensors is the dielectric characterization of materials (permittivity measurements [7,26–28]). Microwave sensors are sensitive to the dielectric properties of the material surrounding the sensitive element (typically, a transmission line section or a planar resonator). Thus, the permittivity of such material, or any other variable related to it, can be retrieved. The sensor to be developed in this paper is based on the change in the permittivity of fabric (the fabric under test –FUT) caused by liquid absorption (sweat or urine in real environment). Such change will modify the electrical characteristics of the sensitive element (capacitance, characteristic impedance, electrical length, etc.), which in turn will generate a variation in the output variable of the sensor (resonance frequency, quality factor, group delay, phase and/or magnitude of the reflection or transmission coefficient, etc.).

Planar microwave sensors can be categorized according to the output variable as frequency-variation sensors [7–9,26–35], frequency-splitting sensors [4,22,36–39], magnitude variation sensors (or coupling modulation sensors [40–51]), and phase-variation sensors [52–69]. Nevertheless, in some cases, two combined output variables are used. For example, for the determination of the complex permittivity of materials, resonant sensors that exploit the resonance frequency variation (mainly correlated with the dielectric constant of the material under test) and the magnitude of the notch or peak in the frequency response (mainly correlated with the loss tangent), have been used [7,26–28]. Frequency-variation and frequency-splitting sensors are robust against electromagnetic interference (EMI) and noise (as corresponds to frequency measurements), but such sensors need wideband sweeping interrogation signals for sensing, covering the output dynamic range (an aspect that complicates the implementation of the associated electronics in real environment). The solution to this issue is given by the so-called single-frequency sensors, fed by a harmonic (single-tone) interrogation signal. Coupling-modulation and phase-variation sensors belong to this class of sensors. Phase-variation sensors, additionally, are robust against EMI and noise (similar to frequency-variation sensors) and result very attractive for sensing. Nevertheless, retrieving the phase of either the reflection or the transmission coefficient in operational environment (i.e., without the use of a vector network analyzer), in general, is not as simple as inferring the magnitude [70]. Magnitude measurements are more prone to the effects of EMI and noise, but the simplicity of the associated electronics is important in certain applications, in particular, the intended application in this work (the detection of liquid absorption in fabric). Note that a simple amplitude detector suffices to convert the magnitude of the transmission coefficient in a voltage variable (an easy measurable magnitude) [49–51]. Thus, in the present paper, we exploit the magnitude of the transmission coefficient at a single frequency for sensing, with an eye towards sensor simplicity.

The proposed sensing device is a resonant sensor, where the sensitive element is an open-ended quarter-wavelength stub resonator that must be in contact with the FUT. Such element is the load of a matched transmission line, and the output variable is the magnitude of the transmission coefficient at the operational frequency, the resonance frequency of the open-ended stub (given by the notch in the transmission coefficient) when it is loaded with the dry FUT. When the FUT absorbs liquid (urine or sweat in a real scenario), the frequency response shifts downwards (because the effective dielectric constant “seen” by the stub increases), and the magnitude of the transmission coefficient at the operational frequency varies. Thus, liquid absorption by the fabric can be detected with this method.

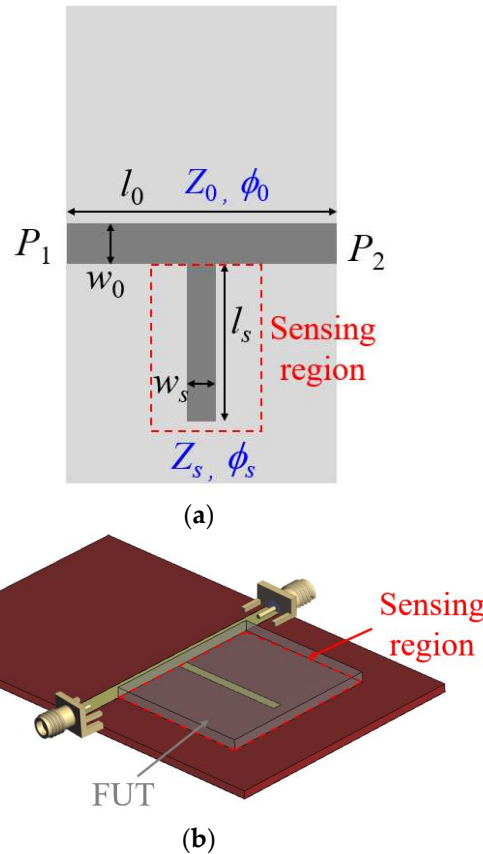
The work is organized as follows. Section 2 presents the proposed humidity sensor and the working principle in detail. The specific sensor design is the subject of Section 3, where validation at simulation level is included. Experimental validation is carried out in Section 4, by considering fabric, and different levels of water absorption. Finally, the main conclusions of the work are highlighted in Section 5.

## 2. The Proposed Sensor and Working Principle

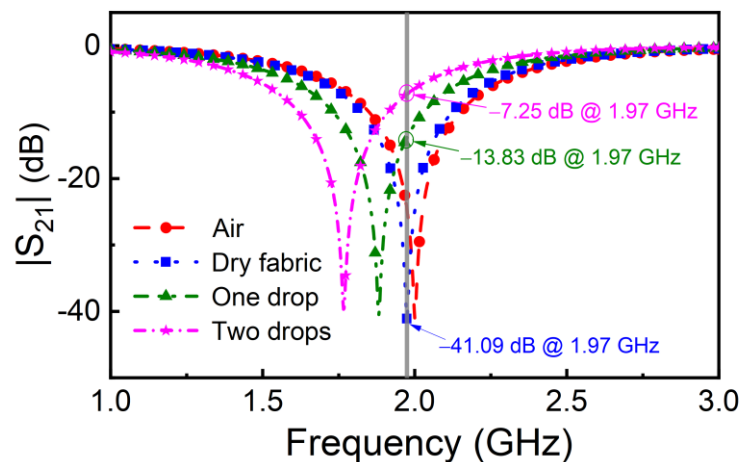
The topology and perspective view of the proposed sensor is depicted in Figure 1. It consists of a transmission line loaded with an open-ended quarter-wavelength stub resonator, the sensitive element. The transmission line is matched to the reference impedance of the ports ( $Z_0 = 50 \Omega$ ), namely, its characteristic impedance is  $Z_c = Z_0$ . The design variables are the length and width of the sensitive stub. The length determines the resonance frequency (notch frequency) of the sensor, whereas the width is related to the characteristic impedance of the stub,  $Z_s$ . In turn,  $Z_s$  is the key parameter that determines the quality factor of the stub resonator. An extreme (i.e., very high or very low) quality factor, should be avoided. The reason is that if the quality factor is very small, a soft variation in the magnitude of the transmission coefficient at the resonance of the stub loaded with the dry FUT (the reference FUT) is expected. By contrast, if the quality factor is very high, tuning to the resonance frequency of the stub when it is loaded with the dry FUT is not absent of certain difficulty. Thus, a tradeoff is necessary.

The working principle of the sensor is the shift in the frequency response (magnitude of the transmission coefficient) when the FUT absorbs a certain liquid. This modifies the dielectric constant

of the FUT, and the resonance frequency of the stub shifts down (Figure 2). As consequence, the magnitude of the transmission coefficient at  $f_0$  (the resonance frequency of the sub loaded with the reference –dry– FUT), varies (increases), and liquid absorption is thereby detected. The output variable in the proposed sensor is thus the magnitude of the transmission coefficient at  $f_0$ , whereas the input variable is the dielectric constant of the FUT, intimately related to the level of liquid absorption by the FUT.



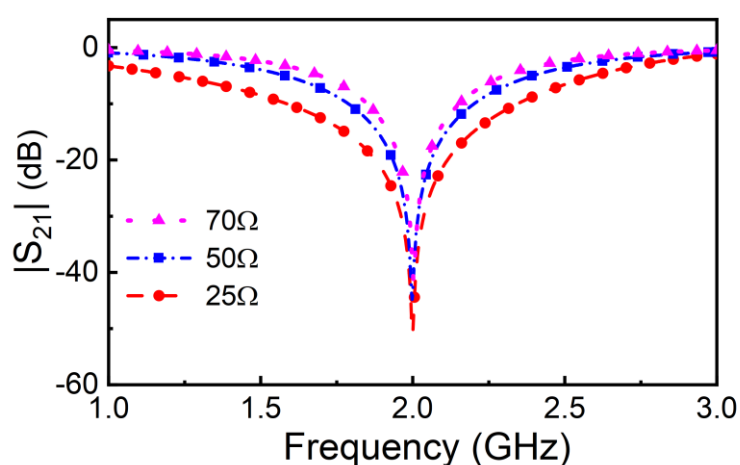
**Figure 1.** Topology (a) and perspective view (b) of the proposed sensor. The sensing region is indicated by the dashed rectangle. The ground plane in (a) is depicted in soft grey color.



**Figure 2.** Simulated results from ANSYS HFSS simulator showing the working principle of the humidity sensor. Note that the dry fabric is set with thickness 0.3 mm and dielectric constant 1.5; and the one drop and two drops of liquid in the fabric are emulated by changing the dielectric constant to 4 and 9, respectively, just for inductive purpose. The open-ended stub has characteristic impedance of  $70 \Omega$  when it is empty (surrounded by air), and it resonates at 2 GHz.

### 3. Sensor Design

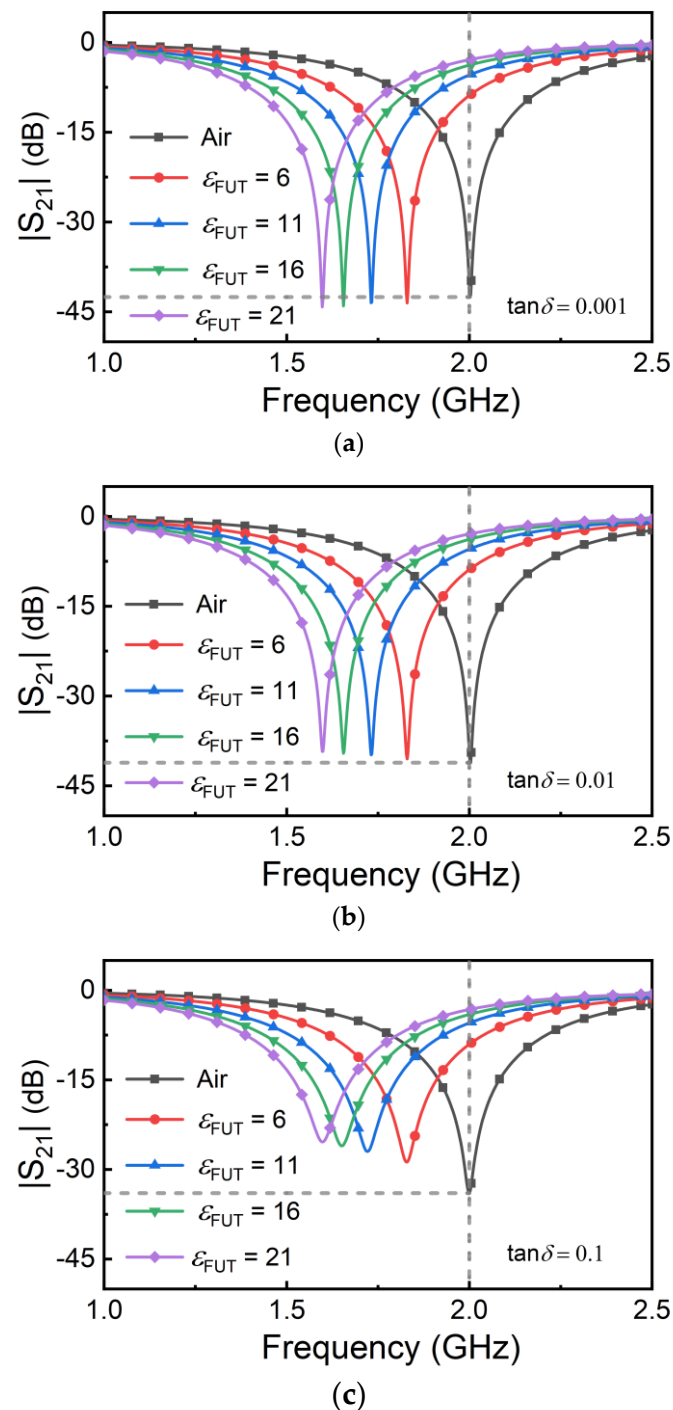
The proposed sensor is designed to exhibit a resonance frequency of 2GHz when the stub is in contact with air (bare sensor). The frequency of operation,  $f_0$ , is expected to be slightly smaller since it should be tuned to the resonance frequency of the stub coated with the reference (dry) FUT. Nevertheless, the dielectric constant of fabric is expected to be very close to that of air, and hence  $f_0$  should not vary excessively from the resonance frequency of the bare sensor (2 GHz). The considered substrate for sensor implementation is the *Rogers 4003C* substrate with dielectric constant  $\epsilon_r = 3.55$ , thickness  $h = 1.524$  mm and loss factor  $\tan\delta = 0.0022$ . With the considered substrate, the width of the 50- $\Omega$  host line is  $W = 3.36$  mm. For the stub, let us consider three different values of the characteristic impedance,  $Z_{s,1} = 25 \Omega$ ,  $Z_{s,2} = 50 \Omega$ , and  $Z_{s,3} = 70 \Omega$ . The corresponding widths, with the considered substrate, are  $W_{s,1} = 9.04$  mm,  $W_{s,2} = 3.36$  mm, and  $W_{s,3} = 1.85$  mm. We have adjusted the length of the open stub in all three cases, in order to generate a notch (bare sensor) at 2 GHz, as indicated. The lengths are not identical, since the effective dielectric constant of the stub depends on its width, but the values are very similar ( $l_{s,1} = 21.03$  mm,  $l_{s,2} = 22.15$  mm, and  $l_{s,3} = 22.45$  mm). The responses of the bare sensors (magnitude of the reflection and transmission coefficient) for all three cases, inferred from full wave electromagnetic simulation using the *ANSYS HFSS* commercial software, are depicted in Figure 3. The length of the host line has been set to 50 mm in all cases, but this length does not affect the magnitude of the reflection and transmission coefficient, since the impedance of that line coincides with the reference impedance of the ports. The stop band bandwidth, or quality factor of the stub, varies with its characteristic impedance. According to the previously mentioned tradeoff, we consider that the stub with impedance  $Z_{s,3} = 70 \Omega$  (and width  $W_{s,3} = 1.85$  mm) is appropriate for our purposes since it exhibits a moderate quality factor. Therefore, the sensor will be implemented by considering such stub impedance and width.



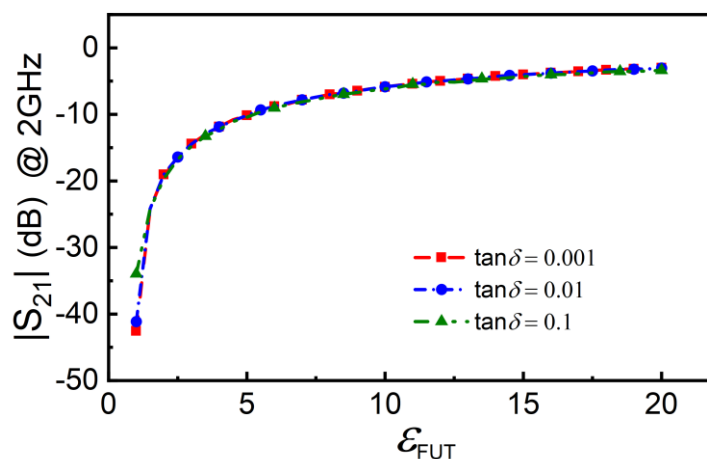
**Figure 3.** Simulated frequency response of the bare sensor for different stub impedances (and widths).

Before experimental validation (left for the next section), let us anticipate the behavior of the sensor by electromagnetic simulation. For that purpose, let us consider that the sensing region is coated with a hypothetical material, with varying dielectric constant, that emulates the FUT with different levels of liquid absorption. The considered thickness of that material is 0.3 mm since this thickness can be comparable to the one of fabric, such as underwear or clothes made of cotton. We have varied the dielectric constant of the FUT between  $\epsilon_{FUT} = 1$  (the value of air and expected to be very close to the dielectric constant of dry fabric) and  $\epsilon_{FUT} = 21$  (a relatively high value, as expected in situations where significant liquid absorption by the fabric occurs). Note that this maximum value of  $\epsilon_{FUT}$  is somehow arbitrary, since the actual value (in a real environment) is expected to depend on the specific liquid (sweat, urine, etc.). Nevertheless, it is a representative value providing a reasonable input dynamic range, useful to qualitatively predict the behavior of the sensor. We have carried out the simulations parametrized by the loss tangent of the FUT (by considering values of 0.001, 0.01 and

0.1). The simulated frequency responses are depicted in Figure 4, whereas Figure 5 depicts the dependence of the magnitude of the transmission coefficient at  $f_0$  (2GHz) with the dielectric constant of the FUT, for the different considered values of the loss tangent. According to Figure 5, the transmission coefficient at  $f_0$  varies significantly with  $\epsilon_{FUT}$  for the three considered values of the loss tangent of the FUT. Nevertheless, the variation (and hence the sensitivity) is more pronounced for small values of the loss tangent. Note also that the sensitivity for small values of  $\epsilon_{FUT}$  degrades as the loss tangent of the FUT increases. However, for moderate and high values of  $\epsilon_{FUT}$ , the sensitivity does not depend on the loss tangent of the FUT. These simulation results reveal that the intended sensor can work to detect the presence of liquid absorption in fabric, an aspect to be discussed in the next section, where the sensor is experimentally validated.



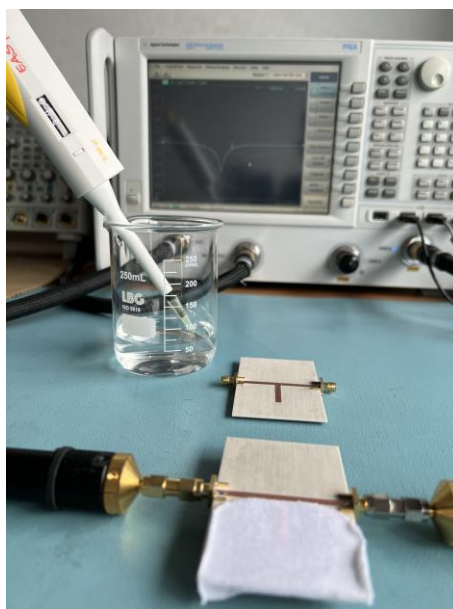
**Figure 4.** Simulated frequency responses of the sensor for different values of the dielectric constant of the FUT, and loss tangent of the FUT set to 0.001 (a), 0.01 (b) and 0.1 (c).



**Figure 5.** Dependence of the magnitude of the transmission coefficient at  $f_0 = 2$  GHz with the dielectric constant of the FUT for different values of the loss tangent of the LUT.

#### 4. Experimental Validation

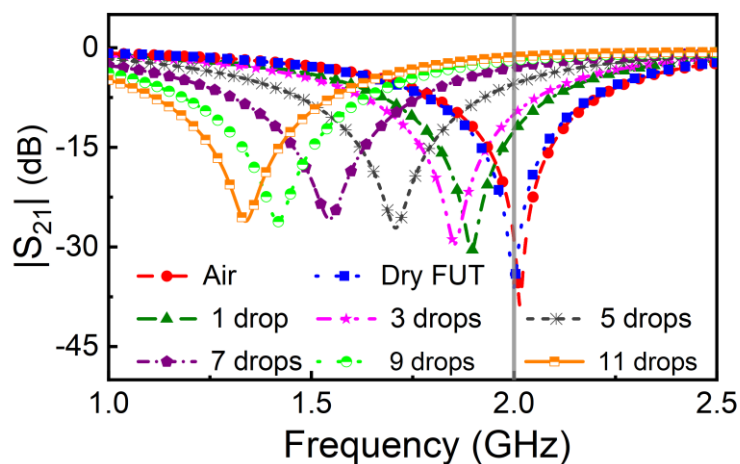
For experimental validation, we have fabricated the sensor with dimensions and substrate corresponding to the simulations of Figs. 4 and 5. The sensor was fabricated by means of the *LPKF H100* drilling machine, available in our laboratory (the photograph is depicted in Figure 6). The measured frequency response of the bare sensor and the one of the sensor loaded with the reference (dry) FUT, depicted in Figure 7, and inferred by means of the *Keysight N5221A* vector network analyzer, reveal that the dielectric constant of the dry FUT is very similar to the one of air, as anticipated (note that the responses are very similar). Indeed, the notch frequency of the sensor loaded with the dry FUT is slightly inferior to the one of the bare sensor, and it is the considered operating frequency of the sensor,  $f_0 = 2$  GHz. The FUT is a piece of cotton underwear, which has been cut in a rectangular shape to accommodate it to the dimensions of the sensing region.



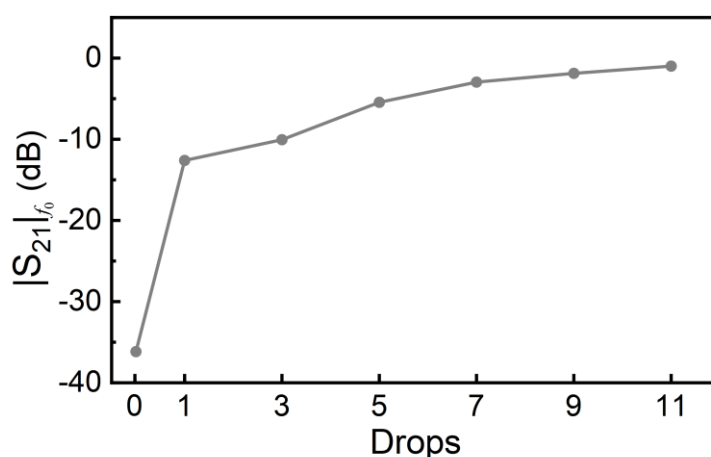
**Figure 6.** Measurement setup of the fabricated sensor.

Next, we have emulated sweat or urine absorption by the fabric by dropping DI water with a pipette on top of it. Specifically, we have sequentially added a water drop on top of the fabric and made the measurement of the frequency response after each drip. The results, also included in Figure 7, reveal that, as the number of accumulated drops in the fabric increase, the frequency response

progressively shifts down. The result is an increase of the magnitude of the transmission frequency at  $f_0$ ,  $|S_{21}|_{f_0}$ . The variation of  $|S_{21}|_{f_0}$  with the accumulated number of drops is depicted in Figure 8. (It follows a similar trend to that of Figure 5). According to the results of Figure 8, the presence of water in the fabric can be detected, and therefore the sensor is experimentally validated.



**Figure 7.** Frequency responses of the bare sensor, sensor loaded with the reference (dry) FUT, and sensor loaded with the FUT with water absorbed (indicated with the number of drops). Note that the volume of water of one drop from the pipette is 50  $\mu\text{L}$ .



**Figure 8.** Dependence of the magnitude of the transmission coefficient at  $f_0$  with the number of cumulative water drops deposited on the FUT.

## 5. Conclusions

In conclusion, it has been experimentally demonstrated that humidity in fabric (particularly, cotton of underwear clothes) can be detected by means of a simple planar microwave sensor consisting in a microstrip line loaded with an open-ended quarter-wavelength resonant stub, the sensitive element. For simplicity, it has been considered that the output variable is the magnitude of the transmission coefficient measured at a specific frequency, i.e., the resonance frequency of the stub when it is coated with the dry fabric. Thus, the sensor works at a single frequency, an important aspect for operation in real environment, where vector network analyzers used at laboratory level should be replaced with signal generators and detectors (in the considered structure, a narrow band voltage-controlled oscillator and an amplitude detector would suffice). According to the obtained experimental results, a single drop (with estimated volume of 50  $\mu\text{L}$ ) generates a magnitude variation in the transmission coefficient of the sensor at the operating frequency of roughly 25 dB, more than enough to detect the presence of small amounts of water in fabric. Thus, with these results, it can be

envisaged that the reported sensor can be applied to the detection of sweet in fabric or urine leakage in underwear. In next future, the focus will be the direct implementation of the sensor in a fabric substrate, more compatible with the intended application.

**Author Contributions:** Conceptualization, Ferran Martín; Funding acquisition, Ferran Martín; Methodology, Lijuan Su and Paris Vélez; Project administration, Ferran Martín; Software, Lijuan Su and Paris Vélez; Supervision, Ferran Martín; Validation, Lijuan Su, Paris Vélez, Pau Casacuberta and Jonathan Muñoz-Enano; Writing – original draft, Lijuan Su and Ferran Martín; Writing – review & editing, Lijuan Su, Paris Vélez, Pau Casacuberta, Jonathan Muñoz-Enano and Ferran Martín.

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**Data Availability Statement:** The article contains the necessary data to verify the results (circuit dimensions and substrate used, as well as setup conditions). Text-based files containing the S-parameter data obtained in simulations and measurement can be requested to the corresponding author.

**Conflicts of Interest:** The authors declare no conflict of interest. The funders had no role in the design of the study; in the collection, analyses, or interpretation of data; in the writing of the manuscript; or in the decision to publish the results.

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